



Circular exponential amplification of photoinduced electron transfer using hairpin probes, G-quadruplex DNAzyme and silver nanocluster-labeled DNA for ultrasensitive fluorometric determination of pathogenic bacteria

Xueqi Leng¹ · Yu Wang² · Rongguo Li³ · Su Liu¹ · Jianzhuang Yao² · Qianqian Pei⁴ · Xuejun Cui⁴ · Yuqin Tu¹ · Dan Tang² · Jiadong Huang^{2,4}

Received: 31 October 2017 / Accepted: 20 January 2018
© Springer-Verlag GmbH Austria, part of Springer Nature 2018

Abstract

The authors describe a fluorometric strategy for the detection of pathogenic bacteria with ultrasensitivity and high specificity. This strategy relies on the combination of target-modulated photoinduced electron transfer (PET) between G-quadruplex DNAzyme and DNA (labeled with silver nanoclusters) along with hairpin probe-based circular exponential amplification. The reaction system involves three hairpin probes (H1, H2 and H3). Probe H1 contains an aptamer against *S. Typhimurium* and the recognition sequence for nicking endonuclease. It is used to recognize *S. Typhimurium* and participates in polymerase-catalyzed target recycle amplification and secondary-target recycle amplification. Probe H2 contains an aptamer against hemin and is used to form the G-quadruplex DNAzyme in the presence of hemin and potassium ion. It acts as the electron acceptor and quenches the fluorescence of the labeled DNA. Fluorescence is best measured at excitation/emission wavelengths of 567/650 nm. Probe H3 contains the template sequence for the synthesis of AgNCs and the H2-annealing sequence. Both H2 and H3 are utilized to perform a strand displacement reaction and to achieve PET between G-quadruplex DNAzyme and DNA/AgNCs. To the best of our knowledge, this is the first example of a PET between G-quadruplex DNAzyme and DNA/AgNCs coupled with circular exponential amplification. The assay has an ultra-low detection limit 8 cfu·mL⁻¹ of *S. Typhimurium*. The assay is rapid, accurate, inexpensive and simple. Hence, the strategy may represent a useful platform for ultrasensitive and highly specific detection of pathogenic bacteria as encountered in food analysis and clinical diagnosis.

Keywords Biosensor · Polymerase · Nicking endonuclease · Signal amplification · Strand displacement amplification · Hairpin · Gel electrophoresis · *S. Typhimurium* · Bioanalysis

Electronic supplementary material The online version of this article (<https://doi.org/10.1007/s00604-018-2698-5>) contains supplementary material, which is available to authorized users.

✉ Su Liu
stu_lius@ujn.edu.cn

¹ College of Resources and Environment, University of Jinan, Jinan 250022, People's Republic of China

² College of Biological Sciences and Technology, University of Jinan, Jinan 250022, People's Republic of China

³ Jinan Maternity and Child Care Hospital, Jinan 250022, People's Republic of China

⁴ Key Laboratory of Chemical Sensing & Analysis in Universities of Shandong, College of Chemistry and Chemical Engineering, University of Jinan, Jinan 250022, People's Republic of China

Introduction

Pathogenic bacteria, a major public health concern worldwide, can cause many problems such as water pollution, hospital-acquired infections and food poisoning [1–3]. Besides pesticides, pharmaceuticals, and toxins, pathogenic bacteria are the most prominent contaminants in drinking water. It can trigger an outbreak of water-borne diseases [4]. The United States Centers for Disease Control has reported that pathogenic bacteria caused 48 million people to fall sick, 128,000 to be hospitalized, and 3000 to die each year in the United States [5]. Therefore, it is of great importance to monitor pathogenic bacteria in drinking water and the environment samples. The common method for pathogenic bacteria identification is culture and colony counting methods. Although the sensitivity of this method has been made

great progress, it takes both time and effort for routine analysis [6]. Nowadays, enzyme-linked immunosorbent assay (ELISA) [7] and polymerase chain reaction (PCR)-based assay [8] have been developed as the effective techniques. However, these techniques suffers from the need of professional technical personal and tedious operation [9, 10]. Thereby, it's still a challenge to develop simple, rapid, inexpensive and high sensitive methods for the detection of pathogenic bacteria.

DNA-based fluorescence quantitative analysis has been recognized as an very useful technique due to their simplicity, rapidness, high sensitivity, and little proclivity to sample damage. It has been widely applied for the detection of various analytes [11–13]. One of the most used fluorescent probes is molecular beacon (MB), a hairpin-shaped nucleic acid probe labeling with a fluorescent dye and a quencher, in which the change of fluorescent signal can be modulated by the hybridization of MBs with the specific nucleic acid probes [14]. However, these fluorescent sensing strategies suffer from complicated synthesis procedure and high analysis cost. Some fluorescent metal nanoparticles, such as DNA-templated silver nanoclusters (DNA/AgNCs), have attracted considerable interest of the researchers [15–18], which possess unique photophysical properties reflected by facile synthesis, good biocompatibility, high quantum yields, tunable fluorescence colors, and excellent photostability [19]. They have been explored for effective fluorescent nanoprobe in a wide range of new application. For instance, Willner and co-workers developed a multiplexed analysis of genes using DNA/AgNCs quantum dots [20]. Dong reported a detection platform based on the assembly of grapheme oxide and DNA/AgNCs and Ye developed a label-free silver nanoclusters-assisted fluorescent sensing for sequence-specific DNA [21, 22]. Among these approaches, the fluorescence signal output is mainly dependent on fluorescence resonance energy transfer (FRET) [23, 24], and surface plasmon enhanced energy transfer (SPEET)-based photophysical mechanisms [22]. Although its widespread availability, the shortcoming of lacking of enough accuracy and efficiency for modulating the fluorescence of DNA/AgNCs needs to be further overcame. Alternatively, G-quadruplex DNAzyme can act as the electron acceptor to efficiently quench the fluorescence of certain fluorophores. It is attributed to the electron accepting ability of Fe(III)/Fe(II)-protoporphyrin IX center in the complexes. Such G-quadruplex/hemin-based electron transfer (ET) phenomenon has been developed as a novel photophysical mechanism for signal transform in the fluorescent assay strategies. For example, Wang and co-workers reported a versatile fluorescent biosensor based on photoinduced electron transfer (PET) between G-quadruplex/hemin complexes and DNA/AgNCs [25]. Yang developed a distance-dependent PET-based fluorescence light-up biosensing strategies for the detection of miRNA [26]. By the utilization of the PET mechanism, the signal switch of “OFF-ON” or “ON-OFF” can be

effectively modulated by the separation or close between G-quadruplex DNAzyme and DNA/AgNCs.

The authors describe a rapid, simple and inexpensive fluorescent biosensing platform for detecting pathogenic bacteria. This assay is based on the combination of target-modulated PET between G-quadruplex DNAzyme and DNA (labeled with silver nanoclusters) along with hairpin probe-based circular exponential amplification. Considering the requirement of trace detection of pathogenic bacteria in drinking water and the environment samples, pathogenic bacteria isothermal nucleic acid amplification strategies involving of polymerase-assisted signal amplification and strand displacement amplification are integrated with target-activated PET. The reaction system includes three different hairpin probes (HAPs), polymerase, and nicking endonuclease. One of HAPs is designed to contain anti-target aptamer and the recognition sequence for nicking endonuclease. It is used for specific recognition of target and participation in polymerase-catalyzed target recycle amplification and secondary-target recycle amplification. The two other HAPs is designed to contain anti-hemin aptamer and the template sequence for AgNCs synthesis, respectively. They are utilized to execute strand displacement reaction and achieve PET between G-quadruplex DNAzyme and DNA/AgNCs. On the basis of the HAPs-based circular exponential amplification strategy, the ultrasensitivity of the method for pathogenic bacteria quantification can be achieved. Moreover, this method has the advantages of rapidness, low cost, simple operation with only one-step operation. As far as we known, this is the first report that PET between G-quadruplex DNAzyme and DNA/AgNCs coupled with HAP-based circular exponential amplification for detecting analytes. Therefore, this strategy might create an useful biosensing platform for detecting pathogenic bacteria and related food safety analysis and environmental samples inspect.

Materials and methods

Materials and reagents

All oligonucleotides were HPLC-Purified and synthesized by Sangon Biotechnology Co. Ltd. (Shanghai, China). The sequences of oligonucleotides are listed in Table S1. *Phi29* DNA polymerase (*Phi 29*) and nicking endonuclease *Nt.AlwI* (*Nt.AlwI*) were purchased from New England Biolabs (Ipswich, MA, USA). deoxyribonucleoside triphosphates (dNTPs) were purchased from Takara Biotechnology Co., Ltd. (Dalian, China). *Salmonella Typhimurium* (KCTC 1925), *E. coli* (KCTC 2571), *Bacillus subtilis* (KCTC 1028) and *Listeria* (KCTC 3569) were obtained from Institute of Microbiology Chinese Academy (Beijing, China). Peptone, beef extract powder, bacto-tryptone and bacto-yeast extract were obtained from Qingdao Biological Technology Co.

Ltd. (Qingdao, China). Agarose G-10, 10-bp DNA ladder marker and 10 × TAE buffer were from Sangon Biotech Co., Ltd. (Shanghai, China). Silver nitrate (AgNO₃), sodium borohydride (NaBH₄) and hemin were obtained from Sigma-Aldrich (St. Louis, MO). Other chemicals were of analytical grade and were used without further purification. All solutions were prepared using ultrapure water with an electric resistance >18.25 MΩ·cm, which was obtained through a Millipore Milli-Q water purification system (Billerica, MA, USA).

Apparatus

Gel electrophoresis was conducted using a DY CZ-24DN electrophoresis cell (LIUYI, Beijing, China; <http://www.zg17w.cn/brand/beijngliuyi.html>) and a Bio-Rad Gel imaging system (Bio-Rad, USA; <http://www.bio-rad.com/>). Transmission electron microscopy (TEM) measurements were made on a JEM-3010 transmission electron microscope (<http://www.jeol.co.jp/>). The samples for TEM characterization were prepared by adding a drop of sample solution on a carbon-coated copper grid and drying at room temperature. Fluorescence spectra were recorded using a Agilent Cary Eclipse spectrofluorometer (Agilent, USA; www.agilent.com) with excitation at 567 nm. The slit was set to be 5 nm for both the excitation and the emission.

Gel electrophoresis

The gel electrophoresis was performed at 145 V for 35 min using prepared samples (5 µL per well) on a 4% (w/w) agarose containing 1% (w/w) ethidium bromide in 50 mM Tris-borate running buffer (pH 7.9) containing 2 mM EDTA. The Cyber Gold was used as an oligonucleotide dye and mixed with samples. After electrophoresis, the gel was visualized using a Bio-Rad Gel imaging system.

Transmission electron microscopy (TEM)

The samples for TEM characterization were prepared by pipetting 5 µL of the solution of samples onto a carbon-coated copper grid. After the evaporation of solvent, the grid was dried overnight. All of the images were bright-field images.

S. Typhimurium detection procedures

All samples were prepared in 6 µL Tris-HCl reaction buffer (50 mM, pH 7.4 containing 100 mM NaCl, 10 mM MgCl₂) for the detection of *S. Typhimurium*. The detailed procedure was as follows: H1 (3 µL, 10 µM), P (3 µL, 100 µM), 10 U phi 29, 10 U *Nt.AlwI*, 10 mM dNTPs, equal volumes (3 µL) of different concentrations of *S. Typhimurium* (or other foodborne diseases), H2 (3 µL, 100 µM), 1 µM hemin

and H3 with DNA/AgNCs (20 µL, 15 µM) were mixed at 37 °C for 2 h. At last, the above mixed solution (60 µL) was mixed with 90 µL of ultrapure water and scanned using Agilent Cary Eclipse spectrofluorometer. Unless noted otherwise, all experiments for *S. Typhimurium* measurements were repeated three times.

The bacterial culture and the preparation of DNA/AgNCs are given in the Electronic Supporting Material.

Results and discussion

Principle of this biosensor for pathogenic bacteria detection

Scheme 1 illustrates the working principle of the biosensing strategy for ultrasensitive detection of pathogenic bacteria using HAP-based circular exponential amplification of PET. The HAP-based circular exponential amplification reaction includes *Nt.AlwI*-aided polymerization reaction activated by the specific binding of target and aptamer, and the strand displacement reaction designed to further amplification and signal transduction. The operate in series is at a constant temperature. To demonstrate the principle design of the strategy, *S. Typhimurium* is selected as a model analyte. The reaction system involves of three ingeniously HAP (denoted as H1, H2, and H3, respectively), one primer probe (P, denoted in blue), phi 29 polymerase, and nicking endonuclease *Nt.AlwI*. H1 is designed to contain anti-*S. Typhimurium* aptamer (denoted in red), a specific recognition sequence of *Nt.AlwI* (denoted in yellow), and a nucleic acid segment complementary to P (denoted in blue). H2 is specifically designed to contain a overhang nucleic acid segment that is anti-hemin aptamer at 3' terminus (denoted in black), and H3 includes a overhang nucleic acid segment that is the synthesis template of DNA/AgNCs at 5' terminus (denoted in hot pink). In our assay, DNA/AgNCs is prepared according to the previous reported methods. When target *S. Typhimurium* is introduced into the system, the specific binding of *S. Typhimurium* and aptamer induces the unfolding of H1, resulting in the hybridization of P with 3' terminal of H1. Then P functions as a primer to initiate an extension reaction and replicates H1 with the aid of phi 29 polymerase and dNTPs, thus the specific recognition site for *Nt.AlwI* is generated in the DNA duplex. Immediately, *Nt.AlwI* cleaves one strand of DNA, generating a new replication site for phi 29 and releasing a single stranded-DNA (S, denoted in red). Its acts as both a secondary-target and triggers the strand displacement reaction. At the same time, the dissociated

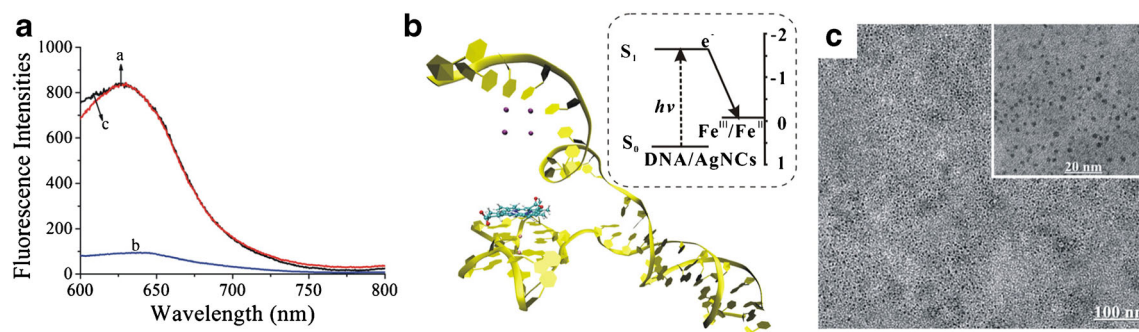


Fig. 1 **a** Fluorescence spectra responses to validate the PET mechanism. **b** The model of the PET mechanism between the DNA/AgNCs and G-quadruplex DNAzyme (inset: the energy levels of DNA/AgNCs and the

redox state of G-quadruplex DNAzyme in the PET process). **c** TEM image of the prepared DNA/AgNCs

in the previous work. In addition, the prepared DNA/AgNCs is uniformly with a narrow size distribution, which is suitable for bio-analysis.

Feasibility study

To verify the feasibility of this strategy, different fluorescence response obtained upon quantifying *S. Typhimurium* in a series of control experiments were studied, and the results are depicted in Fig. 2. As shown in Fig. 2, there was a significantly strong fluorescence response for blank sample (red curve). In contrast, a negligible fluorescent signal at around 650 nm was obtained in the presence of *S. Typhimurium*, indicating the fluorescence of the vast majority of DNA/AgNCs was effectively quenched by G-quadruplex DNAzyme (magenta curve). This suggests the specific binding of target and aptamer activated HAP-based circular exponential amplification reaction, resulting in the PET between

DNA/AgNCs and G-quadruplex DNAzyme due to the close proximity of both. In addition, when *Phi 29* (blue curve) or *Nt.AlwI* (green curve) was absent in the system, dramatically strong fluorescent responses similar to that of the blank sample were observed, signifying the HAP-based circular exponential amplification was initiated by *Nt.AlwI*-assisted polymerization reaction. Furthermore, when non-target *E.coli* was in place of *S. Typhimurium*, a strong fluorescence was obtained, demonstrating the PET between DNA/AgNCs and G-quadruplex DNAzyme was triggered by specific binding of target and aptamer (yellow curve). On the basis of these results, it is reasonably concluded that this strategy held potential for quantitative assay of *S. Typhimurium* with high specificity.

Gel electrophoresis characterization of the HAP-based circular exponential amplification

Additional evidence of the amplification strategy can be acquired through gel electrophoresis analysis. The results and related description are in Fig. S2. These results verify HAP-based circular exponential amplification is triggered by the specific binding of target and aptamer.

Optimization of experimental conditions

The following parameters were optimized: (a) concentration of hemin; (b) time of amplification reaction. Respective data and Fig. S3 are given in the Electronic Supporting Material. The following experimental conditions were found to give best results: (a) optimum concentration of hemin: 1 μM ; (b) Optimal time of amplification reaction: 2 h.

Selectivity of the biosensor

To evaluate the selectivity of the biosensor for *S. Typhimurium* assay, we challenged the system with

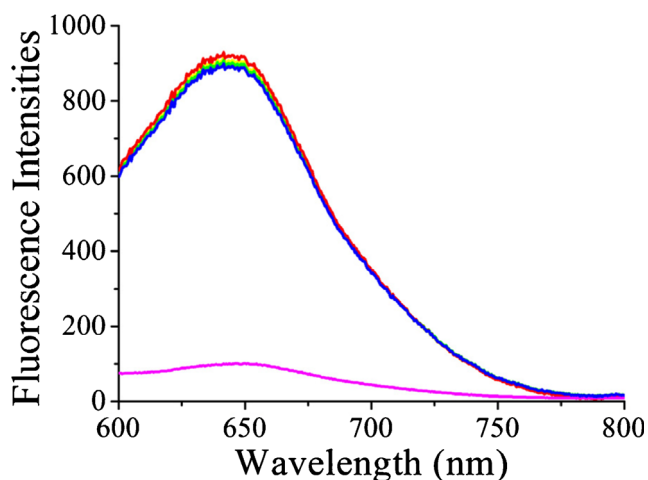


Fig. 2 Fluorescence emission spectra responses of the biosensor in the absence of *S. Typhimurium* (red curve); in the presence of 5.0×10^5 cfu·mL⁻¹ *S. Typhimurium* (magenta curve); without *Phi29* DNA polymerase (blue curve); without *Nt.AlwI* (green curve); *E.coli* in place of *S. Typhimurium* (red curve). The excitation/emission wavelengths are 567 nm/650 nm

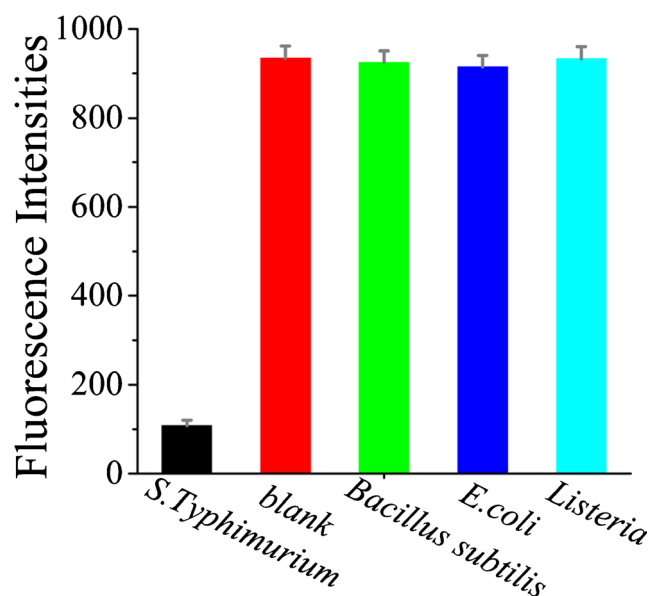


Fig. 3 Specificity evaluation of this isothermal Fluorescence assay for *S. Typhimurium* detection at excitation/emission wavelengths of 567 nm/650 nm. The concentration of *S. Typhimurium* is 5.0×10^5 cfu·mL⁻¹. The concentration of non-target bacteria is 5.0×10^7 cfu·mL⁻¹. Error bars are standard deviations across three repetitive experiments

target and several non-target pathogenic bacteria including *E. coli*, *Listeria*, and *Bacillus subtilis*. The results are shown in Fig. 3. The fluorescence intensity variation in the presence of even 100-fold excess of the non-target bacteria was all less than 4.8% compared to that of the blank sample, conforming the high specificity of the biosensor towards *S. Typhimurium* assay.

Analytical performance of the biosensor for *S. Typhimurium* detection

Under the optimal experimental conditions, the analytical performance of the biosensor were investigated towards *S. Typhimurium* at various concentrations. As seen from Fig. 4a, the fluorescence peak intensity decreased with

increasing *S. Typhimurium* concentration from 0 to 5.0×10^5 cfu·mL⁻¹. A linear dependence between the peak intensity and the logarithm of *S. Typhimurium* concentration was obtained in the range from 10 cfu·mL⁻¹ to 5.0×10^5 cfu·mL⁻¹, which was over 4 orders of magnitude (Fig. 4b). The linear regression equation was $F = 971.29 - 159.87 \times \log(C_{S. Typhimurium} / \text{cfu} \cdot \text{mL}^{-1})$ with a correlation coefficient of -0.995 . The limit of detection (LOD) was calculated to be 8 cfu·mL⁻¹ in terms of the rule of 3 times standard deviation over the blank response. Besides, the analytical performance of our biosensor for quantitative assay of *S. Typhimurium* was compared with that of some earlier reported methods. The results are shown in Table 1. It is found that the sensitivity of our biosensor improved at least by 2 orders of magnitude as compared to the existing methods for pathogenic bacteria assay. Moreover, this homogeneous fluorescent sensing system is implemented by only one-step operation, which offers the advantages of simplicity, rapidness, and excellent resistance to possible contaminants. As a result, our biosensor might satisfy the requirements for the profiling low abundance of *S. Typhimurium* in food and environmental samples.

Real sample analysis

To challenge the potential application of this biosensor for *S. Typhimurium* detection, we applied our fluorescent sensing in complex environment. We used this method to detect *S. Typhimurium* in milk samples. The milk from supermarket is absence of *S. Typhimurium*, so we used the quantitative assay of spiked milk samples. Different concentrations of *S. Typhimurium* (1×10^1 , 1×10^2 , 1×10^3 , 1×10^4 , 1×10^5 cfu·mL⁻¹) were respectively spiked into the milk samples (the dilution ratio between milk and buffer is 1:10) and the milk sample were detected by a classic plate count method and compared with the results obtained by our assay. As shown in Tab. S2., the results obtained by our method are slightly difference compared with those obtained by the plate count

Fig. 4 **a** Fluorescence spectra responses to different concentrations of *S. Typhimurium*. **b** The calibration curve of the fluorescence intensity at excitation/emission wavelengths of 567 nm/650 nm for different *S. Typhimurium* concentrations. The error bars are standard deviations across three repetitive experiments

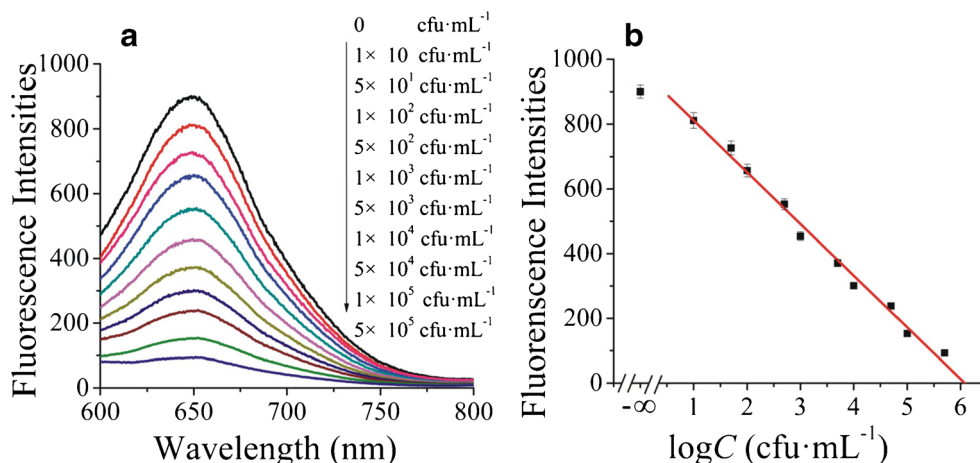


Table 1 Comparison of different assay methods for pathogenic bacteria determination

Detection methods	Detection range (cfu·mL ⁻¹)	Detection limit (cfu·mL ⁻¹)	The whole time of detection	Reference
Fluorescent nanospheres	1×10^5 – 1×10^7	1×10	5.5 h	[9]
pELISA	8×10 – 8×10^8	8×10^1	4.5 h	[28]
SPR	2×10^{-1} – 10^2	2×10	10 h	[29]
Sandwich Fluorescence	1×10^3 – 1×10^9	2.9×10^2	3 h	[30]
Electrochemical	6×10^2 – 6×10^6	6×10^2	~4.5 h	[31]
Chemiluminescence	5.0×10^2 – 5.0×10^5	1.2×10^2	3 h	[32]
Graphene oxide-based fluorescence	1×10^3 – 1×10^8	1×10^2	2.75 h	[12]
Colorimetric immunoassay	8.4×10^3 – 8.4×10^7	1.7×10^3	1.5 h	[33]
Fluorescent aptasensor	1×10^2 – 1×10^5	3×10^2	~3 h	[34]
This work	10 – 5.0×10^5	8	~2 h	–

method, the discrepancies between the two methods were all smaller than 9%. The results reveal that the presence of *S. Typhimurium* in milk can be accurately detected by our fluorescent sensing, indicating it with the great applicability for real sample.

Conclusion

In summary, we have developed a simple, rapid, inexpensive fluorescence sensing strategy for pathogenic bacteria determination with ultrasensitivity and high specificity using HAP-based circular exponential amplification of PET between G-quadruplex DNAzyme and DNA/AgNCs. On the basis of the HAP-based circular exponential amplification strategy, the fluorescence sensing system can detect *S. Typhimurium* with widened detection range from $10 \text{ cfu} \cdot \text{mL}^{-1}$ to $5.0 \times 10^5 \text{ cfu} \cdot \text{mL}^{-1}$ and a limit of detection of $8 \text{ cfu} \cdot \text{mL}^{-1}$. This biosensor also exhibits very high selectivity toward *S. Typhimurium* against other interfering pathogenic bacteria. Moreover, the sensing system can be implemented with only one-step homogeneous reaction. And it is simple, rapid, accurate and inexpensive. Additionally, this sensing strategy holds the potential of being extended for the detection of various aptamer binding molecules by the specific design of the probe H1. Besides, this biosensor can be used for the determination of *S. Typhimurium* in complex samples with high specificity and sensitivity. In principle, the proposed HAP-based circular exponential amplification of PET strategy belongs to “signal-off” fluorescent assays. Such “signal-off” sensing strategies suffer from limited signal capacity, in which only a maximum of 100% signal suppression can be attained under any experimental conditions. To further enhance the functionality of the sensor, “signal-on” fluorescent assay can be achieved by using

DNA/AgNCs-based molecular beacon. Actually, this biosensor might create a useful and versatile platform for ultrasensitive detection of pathogenic bacteria and related food safety analysis and environmental samples inspect.

Acknowledgements This work was supported by the National Natural Science Foundation of China (31471644, 21405060), Primary Research & Development Plan of Shandong Province (2017GSF220009, 2016GSF120006) and Shandong Province Natural Science Foundation of China (ZR2016BL27).

Compliance with ethical standards The author(s) declare that they have no competing interests.

References

1. Duan N, Wu S, Dai S, Miao T, Chen J, Wang Z (2015) Simultaneous detection of pathogenic bacteria using an aptamer based biosensor and dual fluorescence resonance energy transfer from quantum dots to carbon nanoparticles. *Microchim Acta* 182: 917–923
2. Tokonami S, Nakadoi Y, Takahashi M, Ikemizu M, Kadoma T, Saimatsu K, Dung L, Shiigi H, Nagaoka T (2013) Label-free and selective bacteria detection using a film with transferred bacterial configuration. *Anal Chem* 85:4925–4929
3. Leng XQ, Wang Y, Liu S, Pei QQ, Cui XJ, Tu YQ, Liu XJ, Huang JD (2017) Enzymatic repairing amplification-based versatile signal-on fluorescence sensing platform for detecting pathogenic bacteria. *Sens Actuators B: Chem* 252:689–696
4. Donhauser SC, Niessner R, Seidel M (2011) Sensitive quantification of *Escherichia Coli* O157: H7, *salmonella enterica*, and *campylobacter jejuni* by combining stopped polymerase chain reaction with chemiluminescence flow-through DNA microarray analysis. *Anal Chem* 83:3153–3160
5. Scallan E, Griffin PM, Angulo FJ, Tauxe RV, Hoekstra RM (2011) Foodborne illness acquired in the United States—unspecified agents. *Emerging Infect Dis* 17:16–22
6. Brooks BW, Devenish J, Lutze-Wallace CL, Milnes D, Robertson RH, Berlie S (2004) Evaluation of a monoclonal antibody-based enzyme-linked immunosorbent assay for detection of

- campylobacter fetus in bovine preputial washing and vaginal mucus samples. *G Vet Microbiol* 103:77–84
7. Pappert G, Rieger M, Niessner R, Seidel M (2010) Immunomagnetic nanoparticle-based sandwich chemiluminescence-ELISA for the enrichment and quantification of *E. coli*. *Microchim Acta* 168:1–8
 8. Roda A, Mirasoli M, Roda B, Bonvicini F, Colliva C (2012) Recent developments in rapid multiplexed bioanalytical methods for foodborne pathogenic bacteria detection. *Microchim Acta* 178:7–28
 9. Wen CY, Hu J, Zhang ZL, Tian ZQ, Ou GP, Liao YL, Li Y, Xie M, Sun ZY, Pang DW (2013) One-step sensitive detection of salmonella typhimurium by coupling magnetic capture and fluorescence identification with functional nanospheres. *Anal Chem* 85:1223–1230
 10. Roda A, Mirasoli M, Roda B, Bonvicini F, Colliva C, Reschiglian P (2012) Recent developments in rapid multiplexed bioanalytical methods for foodborne pathogenic bacteria detection. *Microchim Acta* 178:7–28
 11. Nakano S, Fukuda M, Tamura T, Sakaguchi R, Nakata E, Morii T (2013) Simultaneous detection of ATP and GTP by covalently linked fluorescent ribonucleopeptide sensors. *J Am Chem Soc* 135:3465–3473
 12. Duan YF, Ning Y, Song Y, Deng L (2014) Fluorescent aptasensor for the determination of salmonella typhimurium based on a graphene oxide platform. *Microchim Acta* 181:647–653
 13. Zhang Y, Tang L, Yang F, Sun Z, Zhang GJ (2015) Highly sensitive DNA-based fluorometric mercury(II) bioassay based on graphene oxide and exonuclease III-assisted signal amplification. *Microchim Acta* 182:1535–1541
 14. Tyagi S, Kramer F (1996) Molecular beacons: probes that fluoresce upon hybridization. *Nat Biotechnol* 14:303–308
 15. Katz E, Willner I (2004) Integrated nanoparticle–biomolecule hybrid systems: synthesis, properties, and applications. *Angew Chem Int Ed* 43:6042–6108
 16. Feng C, Tu J, Liang C, Yang B, Chen C, Chen X (2016) Fluorescent drug screening based on aggregation of DNA-templated silver nanoclusters, and its application to iridium (III) derived anticancer drugs. *Microchim Acta* 183:1571–1577
 17. Bruchez M, Moronne M, Gin P, Weiss S, Alivisatos AP (1998) Semiconductor nanocrystals as fluorescent biological labels. *Science* 281:2013–2016
 18. Medintz IL, Uyeda HT, Goldman ER, Mattoussi H (2005) Quantum dot bioconjugates for imaging, labelling and sensing. *Nat Mater* 4:435
 19. Petty JT, Story SP, Juarez S, Votto SS, Herbst AG, Degtyareva NN, Sengupta B (2011) Optical sensing by transforming chromophoric silver clusters in DNA nanoreactors. *Anal Chem* 84:356–364
 20. Enkin N, Sharon E, Golub E, Willner I (2014) Ag nanocluster/DNA hybrids: functional modules for the detection of nitroaromatic and RDX explosives. *Nano Lett* 14:4918–4922
 21. Fan D, Zhu J, Liu Y, Wang E, Dong S (2016) Label-free and enzyme-free platform for the construction of advanced DNA logic devices based on the assembly of graphene oxide and DNA-templated AgNCs. *Nano* 8:3834–3840
 22. Ma JL, Yin BC, Le HN, Ye BC (2015) Label-free detection of sequence-specific DNA based on fluorescent silver nanoclusters-assisted surface plasmon-enhanced energy transfer. *ACS Appl Mater Interfaces* 7:12856–12863
 23. Enkin N, Wang F, Sharon E, Albada HB, Willner I (2014) Multiplexed analysis of genes using nucleic acid-stabilized silver-nanocluster quantum dots. *ACS Nano* 8:11666–11673
 24. Wu M, Xu X, Wang J, Li L (2015) Fluorescence resonance energy transfer in a binary organic nanoparticle system and its application. *ACS Appl Mater Interfaces* 7:8243–8250
 25. Zhang L, Zhu J, Guo S, Li T, Li J, Wang E (2013) Photoinduced electron transfer of DNA/ag nanoclusters modulated by G-quadruplex/hemin complex for the construction of versatile biosensors. *J Am Chem Soc* 135:2403–2406
 26. Lu S, Wang S, Zhao J, Sun J, Yang X (2017) Fluorescence light-up biosensor for MicroRNA based on the distance-dependent Photoinduced electron transfer. *Anal Chem* 89:8429–8436
 27. *Molecular Operating Environment (MOE)*, 2013.08; Chemical Computing Group ULC, 1010 Sherbooke St. West, Suite #910, Montreal, QC, Canada, H3A 2R7, 2017
 28. Chen R, Huang X, Xu H, Xiong Y, Li Y (2015) Plasmonic enzyme-linked immunosorbent assay using nanospherical brushes as a catalase container for colorimetric detection of ultralow concentrations of listeria monocytogenes. *ACS Appl Mater Interfaces* 7:28632–28639
 29. Bulard E, Bouchet-Spinelli A, Chaud P, Roget A, Calemczuk R, Fort S, Livache T (2015) Carbohydrates as new probes for the identification of closely related *Escherichia coli* strains using surface plasmon resonance imaging. *Anal Chem* 87:1804–1811
 30. Kong W, Xiong J, Yue H, Fu Z (2015) Sandwich fluorimetric method for specific detection of *Staphylococcus Aureus* based on antibiotic-affinity strategy. *Anal Chem* 87:9864–9868
 31. Wang X, Zhu P, Pi F, Jiang H, Shao J, Zhang Y, Sun X (2016) A sensitive and simple macrophage-based electrochemical biosensor for evaluating lipopolysaccharide cytotoxicity of pathogenic bacteria. *Biosens Bioelectron* 81:349–357
 32. Li Z, Yang H, Sun L, Qi H, Gao Q, Zhang C (2015) Electrogenated chemiluminescence biosensors for the detection of pathogenic bacteria using antimicrobial peptides as capture/signal probes. *Sens. Actuators B: Chem.* 210:468–474
 33. Zhu H, Zhao G, Wang SQ, Dou W (2017) Photometric sandwich immunoassay for salmonella pullorum and *Salmonella Gallinarum* using horseradish peroxidase and magnetic silica nanoparticles. *Microchim Acta* 184:1873–1880
 34. Liu K, Yan X, Mao B, Wang S, Deng L (2016) Aptamer-based detection of *Salmonella enteritidis* using double signal amplification by Klenow fragment and dual fluorescence. *Microchim Acta* 183:643–649