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# Development of a new electrochemical DNA biosensor based on $\text{Eu}^{3+}$ -doped NiO for determination of amsacrine as an anti-cancer drug: Electrochemical, spectroscopic and docking studies

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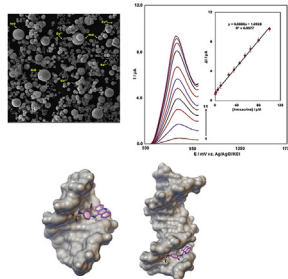
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## HIGHLIGHTS

- $\text{Eu}^{3+}$ -doped NiO as a novel nanocomposite was synthesized.
- An electrochemical biosensor was fabricated with new nanocomposite.
- The interaction between ds-DNA and amsacrine was studied.
- Determination of amsacrine were done by DNA biosensor in urine and serum samples.

## GRAPHICAL ABSTRACT



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## ABSTRACT

The present research reported a new electrochemical biosensor based on ds-DNA/ $\text{Eu}^{3+}$ -doped NiO/CPE to detect amsacrine. Therefore, UV–Vis spectrophotometry, docking, and differential pulse voltammetry (DPV) have been used to study the interactions between amsacrine and dsDNA. Then, experimental parameters affected DNA immobilization and interactions between amsacrine and ds-DNA have been optimized. Afterwards, guanine oxidation peak current of ds-DNA has been chosen as a signal to analyze amsacrine in a concentration ranging between 0.1 and 100.0  $\mu\text{M}$  and finally, limit of detection (LOD) of 0.05  $\mu\text{M}$  has been calculated at optimal condition. Ultimately, it was found that the suggested biosensor is able to determine amsacrine in human serum and urine samples successfully.

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## 1. Introduction

Conducting studies on interaction of some molecules with DNA has become important for obtaining a perception of their action mode at molecular level, the origins of numerous diseases and drugs repositioning in the role of anti-cancer agents [1,2].

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The interaction of drug with DNA was characterized utilizing the different methods such as circular dichroism [3], fluorescence spectroscopy [4], UV–Vis spectrophotometry [5], electrophoresis [6], Fourier Transform Infrared spectroscopy (FT-IR) [7], molecular modeling techniques [8] and Resonance Raman spectroscopy [9]. Although these techniques are expensive, time-consuming and several of them indicate low sensitivity.

In the past few years, electrochemical approaches were given priority in comparison to other techniques, as a result of their highly selective, sensitive, cost-efficient, prompt and simple nature [35,36][10–13].

Amsacrine as the first medicine performing as topoisomerase II poison is a well-known anti-cancer agent entailing favorable activity towards refractory acute leukemias along with Hodgkin and non-Hodgkin lymphomas [15]. In order to assess adverse effects, toxicity, therapeutic efficiency, interactions and monitoring the concentration of amsacrine in urine and serum of patients is important. In past researches, limited methods such as HPLC and GC were documented in determining amsacrine [16,17].

The investigations on DNA biosensors attracted a huge deal of interests in recent years because of exceptional characteristics, namely selectivity, sensitivity, cost-efficient, expeditious and simplicity [37]. Nanomaterials such as graphene, graphene oxide, carbon nanotubes, silver, gold, metal oxide and quantum dots provide well-organized and stable platforms for immobilization of DNA onto the surface of sensor [19][20,21].

Recently, NiO NPs have been considered as one of the good immobilizing matrices for biosensors. These are magnetic and have a high ratio of surface area-volume. One of the other reasons for current attention to the NiO NPs would be that they have one of the highest isoelectric points of popular metal oxide nano-materials, which would make them with constant surface charge features in a wide range of environmental pHs. Additionally, NiO NPs possess reasonable electro-catalytic activities, more capability of the electron transfer that present them as perfect substances to modify biosensors [22,23].

It is notable that rare earth elements exhibited specific features like reliable optical activities and acceptable catalytic functions; therefore, they could be used in the electric, optical, catalytic, and magnetic fields. Due to the unique properties of 4f–5d electron orbitals of the rare earth elements, researchers have been started to developing the novel nanocomposite by doping rare earth elements with metal oxides and have used them as the electrode modifiers [25]. Therefore, europium as a rare earth element with 4f orbitals could generate a coupling between the s and d states of the host substances like NiO to improve the performance of electrode to detect the analyte [26].

Therefore, in this study we constructed  $\text{Eu}^{3+}$  doped NiO as a novel nanocomposite and used it for modification of carbon paste electrode.

Moreover, we used a carbon paste electrode modified with  $\text{Eu}^{3+}$  doped NiO nanocomposite and ds-DNA as a highly sensitive DNA label-free biosensor for the determination of amsacrine in biological samples. For this purpose, the effects of dsDNA immobilization time, dsDNA concentration, interaction time and amsacrine concentrations on the electrochemical response of guanine were investigated. After the successful interaction of the amsacrine with the dsDNA, a decrease in guanine oxidation signals were used as an analytical tool for determination of amsacrine. The results showed interaction of ds-DNA and amsacrine leads to more preconcentration of amsacrine in ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE and improve the detection limit of proposed method. Moreover, the interaction between the ds-DNA and amsacrine were evaluated by other techniques such as spectrophotometry method and docking tool

which confirmed the effective interaction between amsacrine and ds-DNA.

## 2. Experimental

### 2.1. Material and methods

It is notable that Metrohm with 797 VA Computrace 1.3.1 software has been used to perform the electrochemical investigation. Each measurement has been done at room temperatures. Consequently, a UV-1800 spectrophotometer (Shimadzu: Japan) has been utilized to obtain the UV–vis absorption spectra.

Sigma-Aldrich has been chosen to purchase the double-stranded fish sperm DNA (dsDNA), amsacrine hydrochloride and europium (III) chloride hexahydrate. In addition, Merck has been selected to receive  $\text{NiCl}_2 \cdot 6\text{H}_2\text{O}$  and graphite powder. All of the materials were of analytical grade with high purity. The molecular docking procedure, UV–Vis spectroscopic and preparation of real samples have been described in supplementary information data part.

### 2.2. Synthesis of $\text{Eu}^{3+}$ doped NiO nano composite

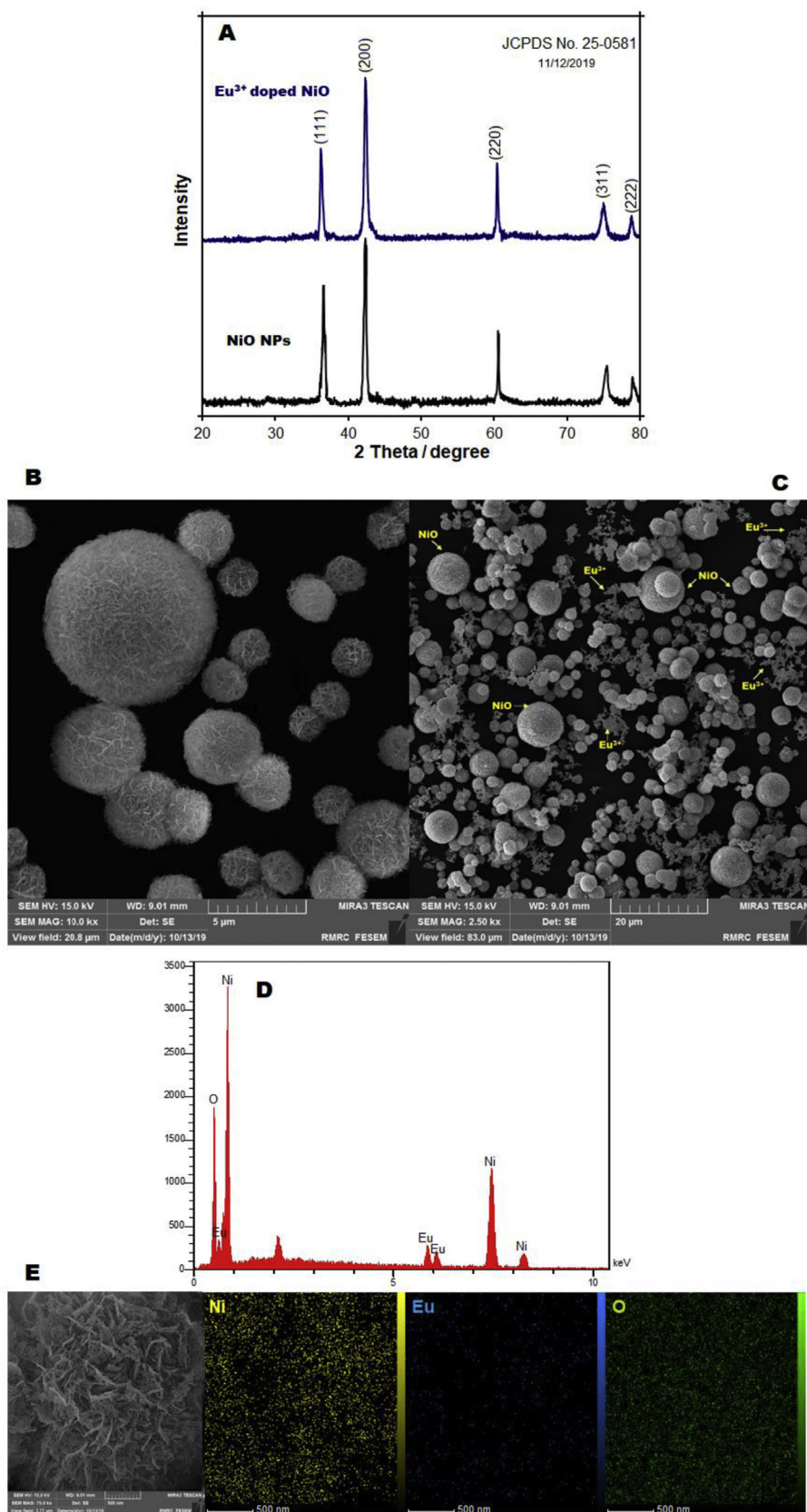
In this stage, 0.546 g cetyl trimethylammonium bromide (CTAB) has been dissolved in 40 mL distilled water shaking for 10 min. After that, 0.01 g europium (III) chloride hexahydrate, 0.300 g urea, and 0.475 g  $\text{NiCl}_2 \cdot 6\text{H}_2\text{O}$  have been dissolved in the obtained mixed solution at moderate agitating for 30 min. Then, the solution has been transported to a 50 mL Teflon-lined steel autoclave and stored at 160 °C for 8 h. Upon the natural cooling, centrifuging has been done to collect the blue precipitate and distilled water and absolute ethanol have been used to wash it 3 times. Afterwards, it dried at 60 °C for 12 h. Ultimately,  $\text{Eu}^{3+}$  doped NiO nanocomposite have been gained via sintering the precipitate at 500 °C for 2 h under air atmosphere. The NiO NPs were prepared using mentioned method without the addition of europium (III) chloride hexahydrate [27].

### 2.3. Electrode preparation

For preparing carbon paste electrodes (CPEs), 0.5 g of the paste has been procured using a mix of 0.45 graphite powder and paraffin oil (0.8 ml). In the next stage, paste has been firmly pressed into a 3-mm (i.d) glassy tube and the copper wire has been placed in it from the opposite end of the tube for acting as a conductor. Moreover, CPEs surfaces have been smoothed by rubbing their external surfaces on a piece of paper prior to utilization. Then, the modified CPEs such as NiO NPs/CPE and  $\text{Eu}^{3+}$  doped NiO/CPE have been procured with a similar procedure and addition of 0.05 gr of NiO NPs and 0.05 gr of  $\text{Eu}^{3+}$  doped NiO for two electrodes respectively.

### 2.4. Immobilization of ds-DNA on the modified CPE surface

Notably, for immobilization of ds-DNA at the surface of  $\text{Eu}^{3+}$  doped NiO/CPE, the modified CPE has been immersed in the stirred 15.0 mg/L ds-DNA, and potential equal to +0.50 V has been applied for 250 s. Afterwards, acetate buffer solution (pH 4.8) has been utilized to wash the dsDNA-modified CPE (ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE) for removing unbonded ds-DNA. Next, ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE has been immersed in 0.5 M acetate buffer solution (pH = 4.8) and potential has been scanned between +600 and +1000 mV for recording the oxidation currents of the guanine.



**Fig. 1.** A) XRDs of NiO NPs and  $\text{Eu}^{3+}$ -doped NiO, B) SEM images of NiO NPs and C)  $\text{Eu}^{3+}$ -doped NiO, D) EDS spectrum and (E) EDS mapping for  $\text{Eu}^{3+}$ -doped NiO nanocomposite.

### 3. Results and discussion

#### 3.1. Nanocomposite characterization

It is notable that powder XRD has been used to examine the detailed crystal structure data of the synthesized nanocomposite. According to the XRD pattern in Fig. 1A, five major peaks of the  $\text{Eu}^{3+}$ -doped NiO at  $2\theta$  values of  $37.3^\circ$ ,  $43.2^\circ$ ,  $62.4^\circ$ ,  $75.4^\circ$ , and  $79.1^\circ$  that respectively has been corresponded to the crystallographic planes of (111), (200), (220), (311), and (222) and could be completely indexed to NiO standard spectrum (JCPDS, No. 04-0835). Additionally, typical peaks of impurities could not be distinguished that has been clearly confirmed crystalline NiOs have been substantially synthesized through the facile hydrothermal procedure. The two procured  $\text{Eu}^{3+}$ -doped NiO and NiO nanocrystals (Fig. 1A) exhibited a similar phase matched completely with NiO standard spectrum, representing ineffectiveness of the  $\text{Eu}^{3+}$  substitution in the crystalline structure of the NiO NPs; therefore,  $\text{Eu}^{3+}$  ions have been substantially and smoothly doped into NiO NPs host lattice.

Furthermore, crystallite size of NiO nanocrystals have been approximated from greater intense peak of the XRD pattern (200) with Debye Scherer's equation (1);

$$D = 0.9\lambda/\beta \cos \theta \quad (1)$$

where  $D$  stands for average crystal size,  $\lambda$  refers to the X-ray radiation wave-length and  $\beta$  represents the complete width at half maximum (FWHM). Finally, the computed crystallite size from the intense plane of (200) was 12.7 nm.

In addition, scanning electron microscopy (SEM) shows

morphologies of the NiO NPs in Fig. 1B which have spherical structure and the nano-sphere shell has been made of multiple porous plates. Moreover, the SEM image of  $\text{Eu}^{3+}$ -doped NiO in Fig. 1C displays, all NiO NPs have retained their spherical shape, and europium has been uniformly dispersed between these nano-spheres.

It should be noted that energy dispersive spectroscopy (EDS) has been utilized to perform the element analysis of the  $\text{Eu}^{3+}$ -doped NiO and detect the element distribution in the selected micro areas. Through the EDS spectrum, presence of  $\text{Eu}^{3+}$ , Ni, and oxygen could be observed without impurity (Fig. 1D). According to the  $\text{Eu}^{3+}$ -doped NiO EDS mapping images (Fig. 1E),  $\text{Eu}^{3+}$ , Ni, as well as oxygen have been the composites of the synthesized product.

#### 3.2. Electrochemical characterization of the $\text{Eu}^{3+}$ doped NiO/CPE

In this stage, the cyclic voltammograms of  $\text{Fe}[\text{CN}]_6^{3-/4-}$  redox couple as one of the indicators for immobilizing DNA have been recorded at the surface of the bare CPE, NiO NPs/CPE,  $\text{Eu}^{3+}$ -doped NiO/CPE and ds-DNA/ $\text{Eu}^{3+}$ -doped NiO/CPE. Based on the outputs presented in Fig. 2, redox peaks current and reversibility at NiO NPs/CPE (curve b) enhanced as compared with the unmodified electrode (curve a). Such a condition might be due to the accelerated transfer of electron and larger surface areas of the NiO/CPE, resulting in the greater current responses. At the  $\text{Eu}^{3+}$ -doped NiO/CPE (curve c),  $\Delta E_p$  declined and the peak current increased significantly on comparison with CPE and NiO/CPE. The results may be ascribed to synergic effect of Eu and NiO which is caused the increasing of modified electrode performance such as fast electron transfer rate, good antifouling property and high conductivity.

Following the DNA immobilization at  $\text{Eu}^{3+}$ -doped NiO/CPE

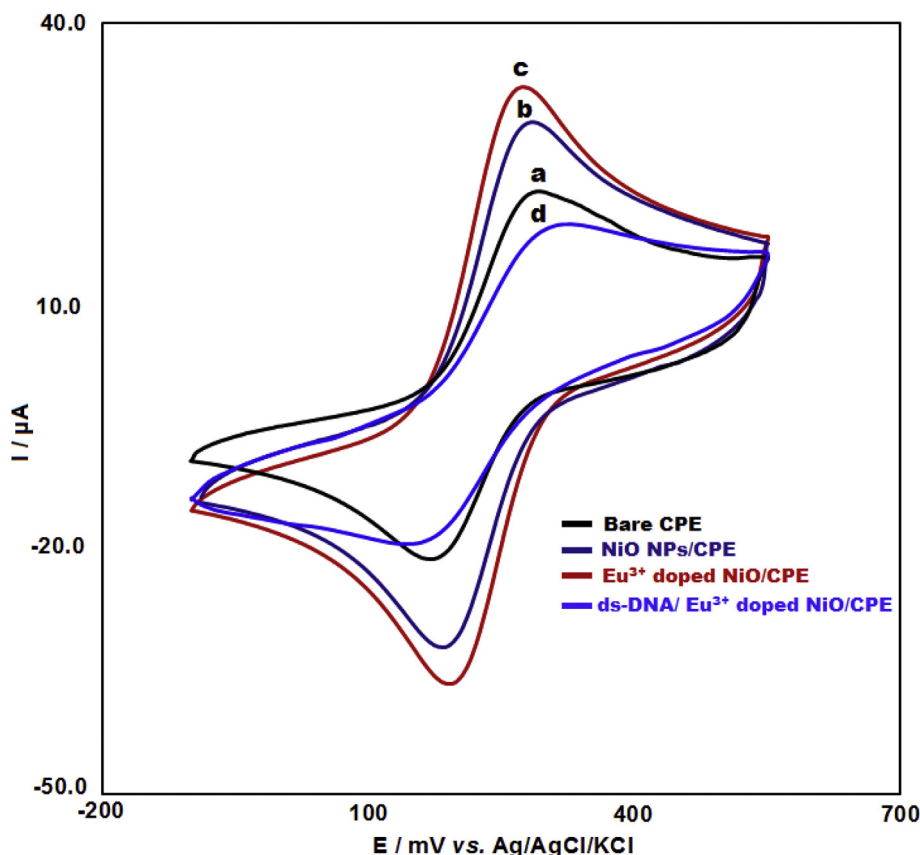


Fig. 2. (A) Cyclic voltammograms of 5 mM  $[\text{Fe}(\text{CN})_6]^{3-/4-}$  in 0.1 M KCl: (a) CPE, (b) NiO/CPE (c)  $\text{Eu}^{3+}$ -doped NiO/CPE, (d) ds-DNA/ $\text{Eu}^{3+}$ -doped NiO/CPE. Scan rate: 50 mV/s.

surface, the two cathodic and anodic peak currents notably declined as the peak-to-peak potential separation enhanced (curve d). Results showed the resistance of the phosphate groups with negative charge of the immobilized DNA to the access of redox couple to the electrode and besides this electrostatic repulsion, the immobilized ds-DNA can also act as a physical blocker for electron transfer; therefore, the current would be declined [37]. The above findings demonstrated DNA immobilization at the  $\text{Eu}^{3+}$ -doped NiO/CPE surface.

### 3.3. Optimization of DNA immobilization

For preparing DNA biosensor, variables such as accumulation time and ds-DNA concentration on accumulation of ds-DNA at the  $\text{Eu}^{3+}$ -doped NiO/CPE surface have been examined with regard to guanine oxidation peak as an index. Therefore, for achieving the most acceptable concentration of ds-DNA, multiple concentrations of DNA in a range between 2.0 and 30.0 mg/L have been selected and outputs confirmed the greatest guanine current of 15.0 mg/L of DNA in comparison to other concentrations (Fig. S1A). Hence, this concentration has been chosen to construct ds-DNA  $\text{Eu}^{3+}$ -doped NiO/CPE. In addition, effects of the deposition time has been examined in ranges between 50 and 350 s. Results indicated increase of the oxidation peak current of guanine with the deposition time of 250 s and levelling by additional enhancement of the deposition time, which represented a saturated adsorption of ds-DNA (Fig. 1B). With regard to analysis efficiency and sensitivity, optimum deposition time of 250 s would be utilized for additional experimentations.

### 3.4. Study of interaction of guanine and amsacrine at the surface of the sensor

The effect of amsacrine-guanine interaction have been electrochemically investigated in comparison to the alterations in the guanine oxidation peak in the absence and presence of amsacrine. So, we registered DPV signal by means of the ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE in the absence (curve a) and the presence of 5.0, 30.0 and 50.0  $\mu\text{M}$  amsacrine (curve b, c and d respectively) (Fig. 3). According to the curve a, ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE generated the oxidation current signal of 10.0  $\mu\text{A}$  relative to guanine oxidation in ds-DNA. It should be noted that in the presence of 5.0, 30.0 and 50.0  $\mu\text{M}$  amsacrine, we observed that the oxidation current has been reduced to 8.7, 6.5 and 4.0  $\mu\text{A}$ , respectively, supporting interaction between amsacrine and guanine base in the ds-DNA structure. Generally, negative shifts found in the peak potential have been corresponding to the electrostatic binding, whereas the positive shifts found in the peak potential have been corresponding to the intercalation [28]. According to Fig. 3, DPVs of the ds-DNA-amsacrine complex displayed a partial positive shift in the guanine peak potential with the enhancement of amsacrine concentration. Therefore, this behavior could be attributable to intercalations of amsacrine with ds-DNA.

### 3.5. Effect of incubation time of amsacrine on the guanine signals

Determining the influences of the interaction time of amsacrine and ds-DNA on the guanine oxidation signal demonstrated that as the accumulation time enhanced by 350 s, the guanine peak

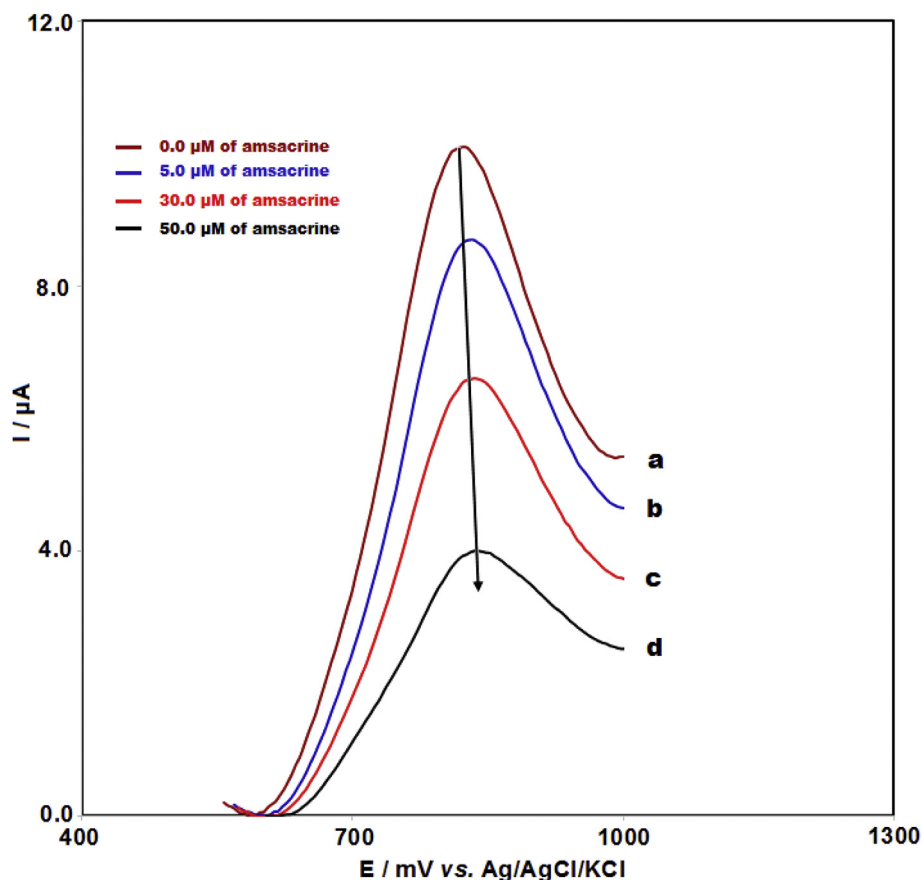
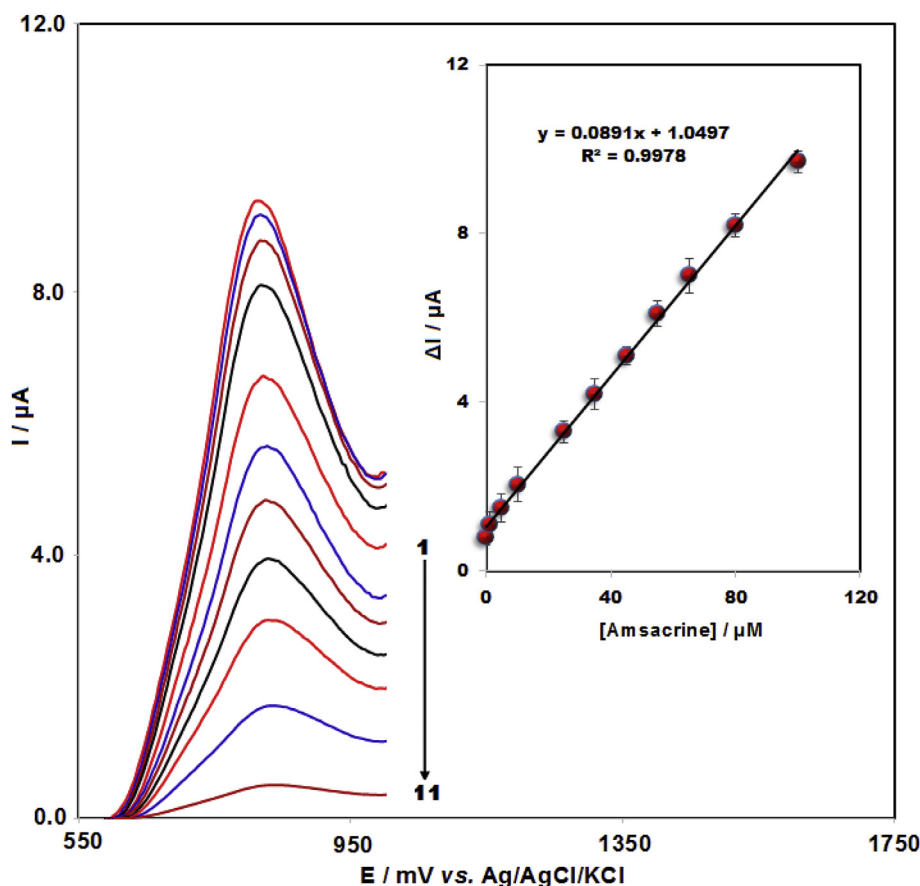


Fig. 3. Differential pulse voltammograms of guanine after the interaction between 0.0, 5.0, 30.0 and 50.0  $\mu\text{M}$  amsacrine (curves a-d, respectively) and ds DNA at ds-DNA/ $\text{Eu}^{3+}$  doped NiO/CPE.



**Fig. 4.** Voltammograms of ds-DNA/Eu<sup>3+</sup> doped NiO/CPE for different concentrations of amsacrine in phosphate buffer (0.1 M, pH 7.0). From top to bottom (1–11), 0.1, 1.0, 5.0, 10.0, 25.0, 35.0, 45.0, 55.0, 65.0, 80.0 and 100.0 μM. Inset: Dependence of the net oxidation guanine current (different between guanine current in the absence and presence of amsacrine) vs. concentration of amsacrine.

notably declined to 300 s and then it has been nearly leveled off (Fig. S2). Hence, 300 s has been confirmed as an optimum interaction time.

### 3.6. Linear range and LOD

DPV has been utilized to detect amsacrine concentration (Fig. 4). As seen,  $\Delta I$  plot (difference between the guanine current in the absence and presence of amsacrine) versus the amsacrine concentration have been linear in ranges between 0.1 and 100.0 μM (Fig. 4- inset). In addition, LOD was calculated 0.05 μM. Table 1 compared functions of the designed biosensor and performance of the formerly published methods, confirming the wider linear range and lower LOD of the introduced procedure in comparison to some techniques. Therefore, ds-DNA/Eu<sup>3+</sup>-doped NiO/CPE has been considered to be one of the effective sensing platforms.

### 3.7. Examination of selectivity

In the presence of 10.0 μM amsacrine, impacts of the foreign species on the guanine signals, as listed in Table S1, have been examined by DPV to assess the sensor selectivity. Moreover, the highest interfering material concentration leading to an error under  $\pm 5\%$  for guanine detection has been defined as the tolerance limit. Outputs approved that up to a 550-fold excess of uric acid, citrate, sucrose, epinephrine, ascorbic acid, folic acid, dopamine, and L-tyrosine and 400-fold excess of K<sup>+</sup>, Cl<sup>−</sup> and Ca<sup>2+</sup> did not affect guanine oxidation current (Fig. S3). Hence, ds-DNA/Eu<sup>3+</sup>-

doped NiO/CPE biosensor has reasonable selectivity to detect amsacrine.

### 3.8. Stability, reproducibility, and repeatability

The developed sensor could be employed to detect 50 μM amsacrine for ten times in one day with reasonable RSD value equal to 2.23% that confirmed repeatability of the sensor. In addition, the biosensor reproducibility has been addressed. Therefore, 5 DNA biosensors have been procured for detection of the 50.0 μM amsacrine. It has been found that RSD of the measurements for 5 electrodes has been 3.1%, showing the satisfactory of electrode reproducibility. Moreover, the biosensor stability has been separately examined during four weeks by means of one biosensor. It is notable that the attained values did not show any distinctive alterations (RSD 3.8%). Therefore, such an acceptable stability could be ascribed to the firm attachment of DNA sequences over the surface of Eu<sup>3+</sup>-doped NiO/CPE.

**Table 1**  
Performance comparison of different methods for determination of amsacrine.

| Method           | LOD        | Linear range      | Ref.      |
|------------------|------------|-------------------|-----------|
| GC               | 50.0 ng/ml | —                 | [17]      |
| HPLC             | —          | 20.0–2000.0 ng/ml | [16]      |
| HPLC             | 50.0 μM    | 0.1–10.0 μM       | [33]      |
| Electrochemistry | 0.3 μM     | 0.7–100.0 μM      | [34]      |
| Electrochemistry | 0.05 μM    | 0.1–100.0 μM      | This work |

**Table 2**  
Analytical results of spiked amsacrine in human serum and urine (n = 5).

| Sample | Added (μM) | Found (μM) | Recovery (%) | RSD (%) |
|--------|------------|------------|--------------|---------|
| Serum  | -          | N.D        | —            | —       |
|        | 3.0        | 3.1        | 103.3        | 3.0     |
|        | 9.0        | 9.2        | 102.2        | 1.7     |
|        | 12.0       | 11.7       | 97.5         | 2.6     |
| Urine  | -          | N.D        | —            | —       |
|        | 5.0        | 5.2        | 104.0        | 1.9     |
|        | 10.0       | 9.8        | 98.0         | 2.2     |
|        | 15.0       | 14.8       | 98.6         | 3.3     |

### 3.9. Analyzing the real samples

In this stage, human serum and urine samples with the use of ds-DNA/Eu<sup>3+</sup>-doped NiO/CPE on the basis of a standard addition procedure have been investigated to test functional utility of the introduced technique. Certain content of amsacrine has been used to spike the serum and urine samples and DPV has been performed to determine its content. Table 2 reports the outputs. As seen, recovery values ranged between 98.0% and 104.0% that were satisfactory, representing a potent utilization of the designed biosensor for detecting amsacrine in the real samples.

### 3.10. UV–Vis spectrophotometry

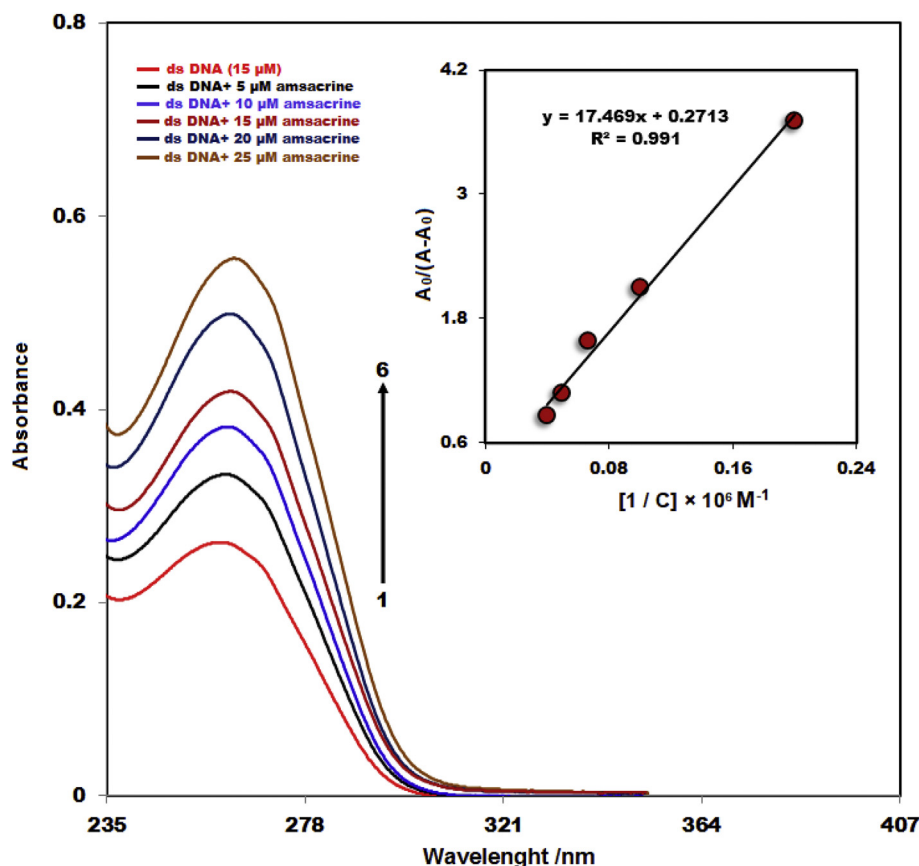
The amsacrine absorption peak appeared at about 265 nm, which was close to the absorption peak of dsDNA at 260 nm. Fig. 5 is a UV–Vis absorption spectra recorded for a constant concentration

of dsDNA (15 μM) in the presence and absence of diverse concentrations of amsacrine (5–25 μM). As seen, a peak at 260 nm has been found in the absorption spectrum of free dsDNA, which has been the result of absorption of pyrimidine and purine in DNA. By increasing amsacrine concentration added to the constant concentration of dsDNA, due to exposing pyrimidine and purine bases of DNA, absorbance intensity of the dsDNA peak enhanced. In fact, alterations in the absorption spectrum for dsDNA could be ascribed to forming amsacrine-dsDNA complex and this form of interaction leads to slight changes in DNA conformation.

The binding constant of DNA with drug can be determined by applying the Benesi-Hildebrand equation (2) [29]:

$$\frac{A_0}{A - A_0} = \frac{\varepsilon_G}{\varepsilon_{H-G} - \varepsilon_G} + \frac{\varepsilon_G}{\varepsilon_{H-G} - \varepsilon_G} \times \frac{1}{K [Drug]}$$

where  $A_0$  and  $A$  are the corresponding absorbance of ds-DNA in the absence and presence of amsacrine, respectively.  $\varepsilon_G$  and  $\varepsilon_{H-G}$  are their respective molar absorbance coefficients. Fig. 5-inset showed a good linear dependence of  $A_0/(A - A_0)$  on the reciprocal amsacrine concentrations. According to the intercept to slope ratio obtained from the linear plot, binding constant of the amsacrine–DNA complex was found to be  $K = 1.55 \times 10^4/M$ . Furthermore, obtained  $K$  values were found comparable with the binding constant of well-known intercalators such as quercetin ( $3.19 \times 10^4/M$ ), proflavine ( $2.32 \times 10^4/M$ ), epirubicin ( $3.4 \times 10^4/M$ ) and lumazine ( $1.74 \times 10^4/M$ ) [30].



**Fig. 5.** UV–vis absorption spectra of ds DNA (15 μM) in the absence and presence of the amsacrine in the range of 5.0–25.0 μM. Inset:  $A_0/(A - A_0)$  vs.  $1/[Amsacrine]$  plot.

### 3.11. Docking examination

#### 3.11.1. Minor groove docking investigation

For studying the groove interaction, a canonical DNA (PDB code: 1BNA) has been chosen to position the docking in the minor groove (Fig. 6A) and the blind docking has been run on the DNA duplex [31] and the binding energy has been obtained  $-7.1$  kcal/mol. Studies indicated stabilization of amsacrine at the DNA minor groove (Fig. 6B). Moreover, the major contribution of hydrogen bonds has been demonstrated in interacting between amsacrine and DNA.

Hydrogen bonds included: Hydrogen (H) 3 and 22 of guanine 114 (DG114) interacted with oxygen (O) 27 from amsacrine (bond length:  $\text{N-H}\cdots\text{O}$  2.75 & 2.25 Å, bond angle:  $129.97^\circ$  &  $146.89^\circ$  respectively). Then, H 41 of amsacrine interacted with O 4' from guanine 116 (DG116) (bond length:  $\text{N-H}\cdots\text{O}$  2.06 Å; bond angle:  $\text{N-H}\cdots\text{O}$   $155.04^\circ$ ). H 40 of amsacrine and O'3 from guanine 116 (DG111) (bond length =  $\text{N-H}\cdots\text{O}$  2.14 Å, bond angle:  $\text{N-H}\cdots\text{O}$   $137.46^\circ$ ).

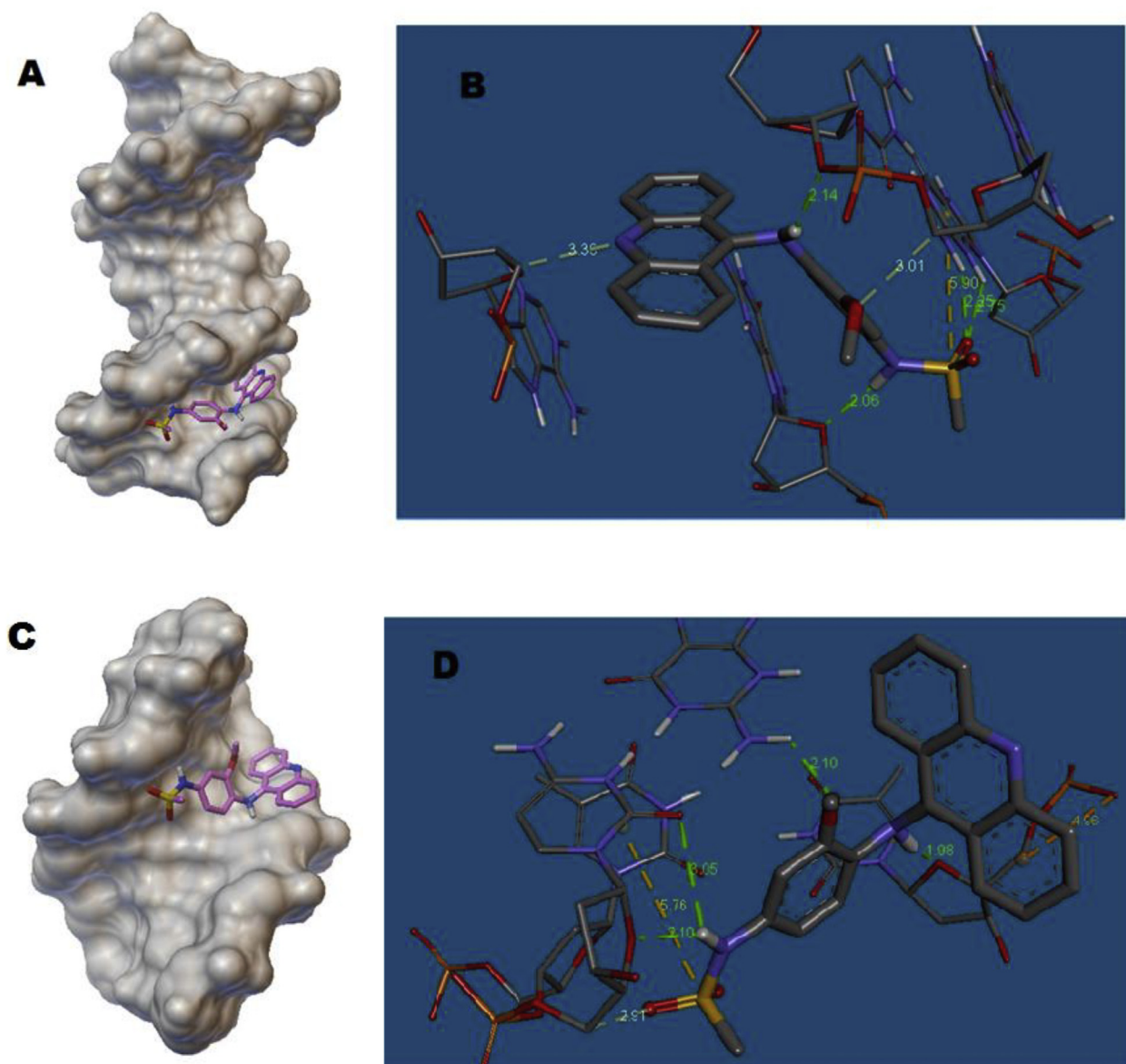
In addition, sulphur atom (25) of amsacrine exhibited a  $\pi$

interaction with aromatic ring of guanine 114 (DG 114) (bond length: 5.9 Å). C'5-H in DA111 and DG 112 established a hydrogen bond with N 7 and O 22 in amsacrine (bond length:  $\text{C-H}\cdots\text{N}$  &  $\text{C-H}\cdots\text{O}$  3.39, & 3.01 Å respectively).

According to the results of docking, amsacrine can interact effectively with bases in the minor groove of DNA.

#### 3.11.2. Intercalation docking investigation

In this stage, a conducted intercalation DNA complex (PDB code: 1Z3F) has been utilized to examine amsacrine-DNA interaction. It has been selected with regard to the published studies [32]. Therefore, the docking outputs showed stabilization of amsacrine in the intercalating location of DNA (major groove) across 2  $\pi$ -loan pair interactions and 5 hydrogen bonds with the nucleotides (Fig. 6C). Based on the result, the binding energy has been estimated to be  $-8.0$  kcal/mol. Interactions are presented here. H 41 of amsacrine interacted with O 4' and O 2 from cytosine 55 (DC55) (bond length:  $\text{N-H}\cdots\text{O}$  2.10 & 3.05 Å, bond angle:  $\text{N-H}\cdots\text{O}$   $122.79^\circ$  &



**Fig. 6.** (A) Amsacrine- DNA minor groove interaction. (B) Geometrical disposition of amsacrine in DNA minor groove (distances in Å). (C) Amsacrine- DNA major groove interaction. (D) Geometrical disposition of amsacrine in DNA intercalation (distances in Å).

126.0°, respectively). H 40 of amsacrine established a hydrogen bond with O 4' of thymine 44 (DT 44) (bond length: N-H...O 1.98 Å, bond angle: N-H...O 163.45°). In addition, H 22 of guanine 22 interacted with O 22 of amsacrine (bond length: N-H...O 2.10 Å, bond angle: N-H...O 149.58°). Finally, C5'-H showed a hydrogen bond with O 27 of amsacrine (bond length: C-H...O 1.91 Å, bond angle: C-H...O 151.26°). Moreover, two  $\pi$  interactions like the loan pair of S 25 of amsacrine and aromatic ring of thymine 44 (DT 44) and OP1 of thymine 44 and aromatic ring of amsacrine with bond length 5.76 and 4.96 Å have been observed respectively (Fig. 6D).

Therefore, amsacrine as an intercalator has the effective interaction with DNA at the major groove that  $\pi$  interactions play a key role. Also, the  $\Delta G$  for major groove binding is less than  $\Delta G$  for minor groove interaction of amsacrine and DNA, therefore possibility of intercalation at major groove is higher than minor groove.

#### 4. Conclusion

The present study examined amsacrine interaction with the ds-DNA using the electrochemical, UV–Vis spectrophotometry and docking techniques. The results indicated the effective interaction of amsacrine at minor and major groove of ds-DNA. In addition, the development of a selective electrochemical biosensor was conducted using Eu<sup>3+</sup>-doped NiO nanocomposite and ds-DNA to determine amsacrine in real specimen. Moreover, new biosensor showed acceptable repeatability and stability for detecting amsacrine with an extensive linear range from 0.1 to 100.0  $\mu$ M, low LOD (0.05  $\mu$ M, S/N = 3), and reasonable selectivity in presence of interferences. Based on the results, ds-DNA/Eu<sup>3+</sup>-doped NiO/CPE could be utilized to detect amsacrine in the biological samples.

#### CRediT authorship contribution statement

**Hamid Akbari Javar:** Supervision. **Zahra Garkani-Nejad:** Software. **Gholamreza Dehghan Noudeh:** Formal analysis. **Hadi Mahmoudi-Moghaddam:** Conceptualization, Methodology, Investigation, Resources, Writing - review & editing.

#### Declaration of competing interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

#### Appendix A. Supplementary data

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.aca.2020.07.071>.

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