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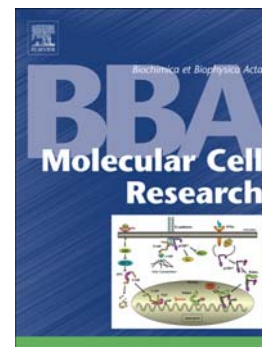
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Measuring Ca^{2+} inside intracellular organelles with luminescent and fluorescent aequorin-based sensors

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Abbreviations: GAP, GFP-Aequorin Protein; ER, endoplasmic reticulum; SR, sarcoplasmic reticulum; SERCA, sarco-endoplasmic reticulum Ca^{2+} ATPase; TBH, tert-butyl-hidroquinone; GECl, genetically encoded calcium indicator; GFP, green fluorescent protein; $[\text{Ca}^{2+}]_{\text{C}}$, $[\text{Ca}^{2+}]_{\text{ER}}$, $[\text{Ca}^{2+}]_{\text{SR}}$, $[\text{Ca}^{2+}]_{\text{GO}}$, Ca^{2+} concentrations in cytosol, ER, SR or Golgi apparatus, respectively; CICR, Ca^{2+} -induced Ca^{2+} -release; Cz, coelenterazine.

ABSTRACT

GFP-Aequorin Protein (GAP) can be used to measure $[Ca^{2+}]$ inside intracellular organelles, both by luminescence and by fluorescence. The low-affinity variant GAP3 is adequate for ratiometric imaging in the endoplasmic reticulum and Golgi apparatus, and it can be combined with conventional synthetic indicators for simultaneous measurements of cytosolic Ca^{2+} . GAP is bioorthogonal as it does not have mammalian homologues, and it is robust and functionally expressed in transgenic flies and mice, where it can be used for Ca^{2+} measurements *ex vivo* and *in vivo* to explore animal models of health and disease.

KEYWORDS: biosensor, calcium, organelles, GFP, aequorin, GECl, endoplasmic reticulum, Golgi apparatus.

Highlights

- GFP-Aequorin fusion proteins (GAP) are a new family of Ca^{2+} sensors.
- They are suitable for ratiometric Ca^{2+} imaging in cytoplasmic organelles.
- Low Ca^{2+} affinity can be engineered for high Ca^{2+} organelles such as ER or Golgi.
- GAPs are bioorthogonal and transgenic animals show normal phenotype.
- *Ex vivo* and *in vivo* measurements are possible in transgenic mice and flies.

1. INTRODUCTION

Calcium signalling is the trigger of many biological processes in animal cells [1]. Emphasis was traditionally focused on cytosolic Ca^{2+} ($[\text{Ca}^{2+}]_c$), but much attention has been drawn in recent years to Ca^{2+} inside intracellular organelles such as nucleus [2], mitochondria [3] or endoplasmic reticulum (ER) [4]. The ER, and its muscle counterpart the sarcoplasmic reticulum (SR), is the main Ca^{2+} storage organelle in eukaryotic cells. In addition, most of the organelles of the secretory pathway, from the Golgi apparatus [5] to the lysosome [6], have been shown to participate in both uptake and release of calcium. The luminal Ca^{2+} concentration in the ER ($[\text{Ca}^{2+}]_{\text{ER}}$) or the Golgi apparatus ($[\text{Ca}^{2+}]_{\text{GO}}$) is maintained in the 200-2000 μM range, three to four orders of magnitude above $[\text{Ca}^{2+}]_c$. These high Ca^{2+} concentrations are essential for proper functioning, and disturbances cause stress and “unfolded protein response” in the ER [7] and defects in protein segregation and cargo sorting in the Golgi apparatus [8].

Although some synthetic Ca^{2+} indicators such as rhod-2, rhod-5N, magfura-2 or magfluo-3 have been used to measure organellar Ca^{2+} content (**Table 1**), the selectivity of these probes is poor, and measurements have many drawbacks [9]. In contrast, genetically encoded calcium indicators (GECI) can be precisely targeted to intraluminal locations within the selected organelle [10]. The photoluminescent protein aequorin, extracted from the jellyfish *Aequorea victoria* [11], was originally injected into cells to follow the $[\text{Ca}^{2+}]_c$ transients associated with action potentials [12]. After cloning of its gene, recombinant aequorins were used to monitor Ca^{2+} transients in mitochondria [13], ER [14], Golgi [15] or secretory vesicles [16]. Aequorins are useful, clean and reliable probes to follow Ca^{2+} signals and they provided invaluable insight into many biological issues. However, limited

light output makes single cell imaging a difficult task, although Ca^{2+} oscillations in mitochondria or nucleus have been recorded [17].

Fluorescent GECIs show stronger light output than bioluminescent probes and, therefore, are more suitable for Ca^{2+} imaging. They consist of a Ca^{2+} -sensing protein, either calmodulin (CaM) [18] or troponin C (TnC) [19]. They are classified into two main families: those based on Förster resonance energy transfer (FRET), composed of two fluorescent proteins, such as the cameleons; and those based on a single fluorescent protein, such as the GCaMPs. In the first family, the binding of Ca^{2+} to CaM in cameleons [20] or TnC in TnC-sensors [21] increases FRET, leading to a change in the signal, with increased fluorescence at the longer wavelength and decreased fluorescence at the shorter one.

The second class of indicators consists of a single fluorescent protein, often circularly permuted (cp), fused to an N-terminal M13 peptide and a C-terminal CaM domain. The Ca^{2+} -dependent interaction of CaM with M13 modifies the environment of the chromophore in the fluorescent protein in such a way that the signal increases. Two GCaMP derivative families include the variants of distinct hues, GECOs [22] and low-affinity CEPIAs [23]. The CatchER family of indicators consists of a single EF-hand motif inserted in GFP [24]. A selection of the low affinity GECIs with their main characteristics are listed in **Table 1**. Previous reviews cover different aspects of GECIs [21, 25, 26]). Here we focus on the development and applications of a new class of low affinity Ca^{2+} indicators containing aequorin fused to GFP (GFP-Aequorin Protein, GAP), or other fluorescent proteins, and which can be used either as luminescent or fluorescent Ca^{2+} sensors.

2. RESULTS AND DISCUSSION

2.1. Modified aequorins

Besides the wild type aequorin, which emits blue luminescence in the presence of Ca^{2+} and the cofactor coelenterazine, modified aequorins emitting at different wavelenghts have been generated by fusion to different fluorescent proteins, green (GFP), red (mRFP) or tandem dimer tomato (tdT) [27-30]. Red aequorins provide the advantage that emission can be detected across the skin and other tissues, permitting *in vivo* measurements [30]. In addition, targeting of red and green aequorins to different subcellular compartments enables simultaneous monitoring of Ca^{2+} levels in two organelles [29].

Further useful modifications of aequorins include engineering for optimizing its affinity for Ca^{2+} to the Ca^{2+} concentration range found in the organelles to be measured. For example, the Ca^{2+} concentration expected in the lumen of the ER or the Golgi apparatus ranges from 200 to 2000 μM . The higher Ca^{2+} concentrations would provoke a complete consumption of the aequorin with cessation of luminescence in a few seconds [31]. Hence, several substitutions in the EF hands of the aequorin have been introduced in order to reduce the affinity for Ca^{2+} . In addition, various modified coelenterazines can also be used to modify the Ca^{2+} affinity [32].

Aequorins with different Ca^{2+} affinities are compared in **Figure 1A**. The wild type aequorin (named 1 in **Figure 1A**) enables measurements at around 10^{-6} M [Ca^{2+}], but at 5 μM the rate of consumption would be about 1 % per second, leading to consumption of most of the aequorin within a few minutes. Wild type aequorin in conjunction with coelenterazine n (2 in the **Figure 1A**) allows accurate [Ca^{2+}] quantification within the 2-20 μM range, and

can be applied to measure moderate Ca^{2+} overloads in the mitochondria [33]. Measuring $[\text{Ca}^{2+}]$ in the lumen of the ER was first achieved by combining a D119A (aspartic acid in position 119 exchanged by alanine) substitution in apoaequorin together with coelenterazine n [34]. This mixture (3 in **Figure 1A**) gives reliable estimations in the 20-1000 μM range, and is suitable for measurements in the ER, the Golgi apparatus and the overloaded mitochondria [33-35]. The fusion of the mutated aequorin to GFP (GFP-aequorin, mutGA in **Figure 1A**) produced minor effects on the affinity for Ca^{2+} [29].

The classical low affinity aequorin system (3 and ermutGA in **Figure 1A**) gets quickly consumed at high Ca^{2+} levels (near 1% per second at 10^{-3} M), and that prevents accurate measurements during experiments lasting for more than a few minutes. At 37 °C the problem is even worse as consumption is accelerated further (1b in **Figure 1A**). In order to overcome these limitations, two extra-low affinity aequorins have been recently developed. The new indicator GAP1 is a GFP-Aequorin Protein fusion (GAP, see section 2.2), where three substitutions, D117A, D119A and D163A, have been introduced in the aequorin moiety. Combining this indicator with coelenterazine n allows comfortable measurements in the 100-2000 μM range [36] (GAP1 in **Figure 1A**). Even lower affinity is achieved by the double mutated D119A and N28L aequorin reconstituted with coelenterazine i (er2mutA in **Figure 1A**) [37], that increases the range of $[\text{Ca}^{2+}]$ measurements up to 10000 μM . The use of this extra low affinity aequorin permits detection of ER subcompartments with Ca^{2+} concentrations as high as 2000 μM , which cannot be detected with other systems because of rapid burning of the aequorin [37].

2.2. GAP, a new family of fluorescent Ca^{2+} sensors for intracellular organelles

We realized recently that some of the GFP-Aequorin fusion Proteins (GAP) we developed for bioluminescence measurements also exhibited a Ca^{2+} -dependent fluorescence, with changes in the excitation spectrum of the green fluorescence. Coelenterazine was not required, indicating that the phenomenon is due to the interaction between the two moieties, GFP and aequorin, and this is not related to the luminescence reaction [38]. Upon Ca^{2+} binding, the fluorescence excited at 470 nm increases with a parallel decrease of the fluorescence excited at 405 nm. This enables ratiometric measurements that provide a more reliable quantification and are less prone to imaging artifacts. In addition, GAP indicators can be used in combination with synthetic probes such as fura or rhod dyes for simultaneous cytosolic and intraorganelle Ca^{2+} measurements.

The dynamic range of GAP, determined as the maximum change in the F_{470}/F_{405} ratio, is 3-4. The Ca^{2+} calibration curve follows the Hill function $y/y_{\max} = [\text{Ca}^{2+}]^n / (K_D^n + [\text{Ca}^{2+}]^n)$, where $y = (R - R_{\min}) / (R_{\max} - R_{\min})$ and the Hill coefficient (n) is 1 (**Figure 1B**). This makes the calibration easier and increases the useful concentration range of the probe (more than one order of magnitude for R values from 0.2 to 0.8). The K_D for Ca^{2+} is 0.2 μM , suitable for measurements of $[\text{Ca}^{2+}]_c$, and it can be modified by genetic engineering of the three aequorin EF hands (see below). Importantly, this indicator is insensitive to Mg^{2+} in the 100-5000 μM range and to H^+ in the 6.5-8.5 pH range. The probe was successfully targeted to cytosol (excluding the intracellular organelles), nucleus, mitochondria, ER or Golgi apparatus [38]. In contrast to most of the GECIs, which are based in calmodulin or troponin, the Ca^{2+} -responsive element of GAP is the photoprotein apoaequorin [38]. This makes of GAP a unique dual calcium sensor, able to function either as a fluorescent or as a bioluminescent indicator (**Figure 1C**).

GFP and aequorin, the two proteins from *Aequorea victoria* in which GAP is based, do not have mammalian homologues. As a consequence, the possibility of interaction between GAP and endogenous partners is minimized, in contrast to other indicators with calcium-binding elements coming from mammalian proteins. Consistently, transgenic mice expressing GAP ubiquitously were viable and did not show phenotypic anomalies, even though expression was specially prominent in neural tissues [38].

2.3. Low affinity GAPs

As mentioned above, adequate affinity of the indicator is essential for accurate measurement in the selected organellar environment. Thereupon, much effort was dedicated to generate low affinity GAPs that conform to the high $[Ca^{2+}]$ -organelles (**Figure 1B**). The first successful derivative, named GAP1, displayed a K_D of 17 μM and preserved all the other beneficial properties of the original GAP. It is adequate for measurements in mitochondria at submaximal Ca^{2+} overloads or in one of the subcompartments of trans-Golgi network with $[Ca^{2+}]_{GO} = 50 \mu M$ [35]. However, the affinity is too high for reliable measurements in the ER lumen, where $[Ca^{2+}]$ approaches 1000 μM . Consistently, although GAP1 is able to detect large decreases in the ER Ca^{2+} effected by massive Ca^{2+} release, it was not sensitive enough to detect moderate fluctuations in the ER Ca^{2+} content [38]. Further optimization of GAP for use in ER led to GAP2, that contains the mutations D119A and D24N, and has a K_D for Ca^{2+} of 400-500 μM (**Figure 1B**). This affinity is optimal for measurements in the ER, where $[Ca^{2+}]$ values of 200-1000 μM have been reported [39-42]. Finally, we developed a GAP2 derivative, named GAP3, by optimizing the codon usage for mammalian expression and re-engineering several residues (L15Q, I167V, S175G and D180Y) in the GFP moiety, to increase its fluorescence intensity. The

K_D and dynamic range of GAP3 were not dissimilar to those of GAP2, so GAP3 should be generally chosen for measurements in the ER or the Golgi apparatus (**Figure 1B**) [43].

2.4. GAP3 is optimal for monitoring $[Ca^{2+}]_{ER}$ and $[Ca^{2+}]_{Go}$

We have recently described functional results obtained in model cell lines and in primary cultures of cells expressing GAP3 in the ER [43]. The indicator successfully reported $[Ca^{2+}]_{ER}$ dynamics and was sensitive enough to follow luminal Ca^{2+} oscillations inside the ER of astrocytes. Moreover, we have generated transgenic animals (mice and flies) expressing ER-targeted GAP3 (erGAP3). No phenotypic alterations were detected in these animals, which were used to provide proofs of concept for the suitability of the probe to monitor $[Ca^{2+}]_{ER}$ under conditions close to the physiological ones. For example, we performed a functional mapping of acetylcholine receptors in acute isolated hippocampal slices by studying, at low magnification, agonist-induced Ca^{2+} release from the ER through direct monitoring of changes of $[Ca^{2+}]_{ER}$ (**Figure 2A**). At high magnification we observed that neurons expressed much more GAP3 than glia, so that the signal should represent mainly changes of $[Ca^{2+}]_{ER}$ in neurons. We found that only the CA1 region responded to acetylcholine with Ca^{2+} release from the ER, in agreement with the reported expression of the muscarinic acetylcholine receptors in this area [44, 45]. Mapping of ER release with other agonists resulted in different maps (results not show).

We simultaneously imaged ER- and cytosolic- Ca^{2+} dynamics using the erGAP3 (**Figure 2A**) and rhod-3 signals, respectively. Interestingly, we found that the $[Ca^{2+}]_C$ peak preceded maximal ER release. This result evidences the continuous clearance of the cytosolic Ca^{2+} by homeostatic mechanisms. We have shown in chromaffin cells that the relative contribution of different mechanism to the cytosolic Ca^{2+} clearance depends on

$[Ca^{2+}]_c$ [41]. At low $[Ca^{2+}]_c$, the high affinity Ca^{2+} pumps, the sarco-endoplasmic reticulum Ca^{2+} ATPase (SERCA) and the plasma membrane Ca^{2+} -ATPase (PMCA), predominate. On the contrary, at high $[Ca^{2+}]_c$, the low-affinity mitochondrial Ca^{2+} uniporter predominates, and Ca^{2+} is taken up into mitochondria. If the rate of mitochondrial uptake exceeds ER exit, then $[Ca^{2+}]_c$ decreases, as seen here. Note that $[Ca^{2+}]_c$ at the ER-mitochondria junction microdomains may very much exceed the mean $[Ca^{2+}]_c$ reported by the cytosolic Ca^{2+} probe. For example, cytosolic Ca^{2+} microdomains as high as 50-100 μ M have been postulated to exist in chromaffin cells near the functional triads constituted by the plasma membrane Ca^{2+} channels, the ER release sites and the subplasmalemmal mitochondria [33]. In non-excitable cells the $[Ca^{2+}]_c$ peak produced by stimulation of ER Ca^{2+} release by inositol-trisphosphate-producing agonists does also precede the peak of the $[Ca^{2+}]_{ER}$ decrease [43] and a part of the released Ca^{2+} is taken up by mitochondria [38].

In order to demonstrate the feasibility of *in vivo* measurements with the new Ca^{2+} sensors, we genetically engineered *Drosophila* to express erGAP3 specifically in the sarcoplasmic reticulum of striated muscles and then recorded the fluorescence signal in the easily accessible thoracic muscles [43]. These muscles can be stimulated through the giant fiber system, which activates all the motor neurones simultaneously [46]. **Figure 3** illustrates the results of one of such experiments in which stimulation was performed at different frequencies (from 0.25 up to 16 Hz), and fluorescence images were collected every 100 ms. At the lowest frequency (0.25 Hz) the unitary release events, with sudden decrease of $[Ca^{2+}]_{ER}$, can be perfectly distinguished every 4 s (**Figure 3A**). Release was very fast, as the decrease of $[Ca^{2+}]_{ER}$ had been completed within 100 ms, and was followed by a slower reuptake, with $t_{1/2}$ close to 1 s. At higher frequencies (4 and 16 Hz) the individual release events fused together leading to a larger $[Ca^{2+}]_{ER}$ drop. $[Ca^{2+}]_{ER}$ decreased during the first 1-1.5 s and then the ER began to refill even though the electric stimulation continued for 4

s. This decrease of $[Ca^{2+}]_{ER}$ release may be due to synaptic fatigue at the neuromuscular junction. When the electric stimulation ceased, the rate of SR refilling increased (**Figure 3A**). **Figure 3B** shows pseudo-colour coded GAP3 fluorescence images of the fly thorax normalized as R/R_0 . Note that the decrease in fluorescence was homogeneous in all the thorax muscles.

In **Figure 3C** the time courses of $[Ca^{2+}]_{ER}$ during stimulation at the three different frequencies has been superimposed for comparing amplitudes and rates. It is notable that prior to fatigue, the elementary events tend to have the same amplitude, about 0.01 scale units. The initial rate of $[Ca^{2+}]_{ER}$ decrease is also similar in all the cases. At 4 Hz stimulation (1 stimulus each 0.25 s vs sampling at 1 image every 0.10 s) the expected saw-tooth-like aspect was observed due to alternation between decrease and increase of the fluorescence signal in two consecutive time points.

In conclusion, we review here a new family of Ca^{2+} probes named GAP, that are GFP-Aequorin fusion Proteins. They can be used either as luminescent or as fluorescent probes and can be targeted to cytoplasmic organelles. The low Ca^{2+} affinity variants, adequate for measurements in high- Ca^{2+} environments such as the ER or the Golgi apparatus, are particularly addressed to. In luminescent mode GAP allows to perform long term measurements (up to 1 hour) in minimally perturbed tissues. In fluorescence mode GAP permits ratiometric imaging, and it can be combined with conventional synthetic indicators for simultaneous measurements of the cytosolic Ca^{2+} . Calibration of GAP is uncomplicated as the Hill coefficient is 1. As the building blocks of GAP do not have mammalian homologues, no interferences with endogenous proteins should be expected, so that the sensor is, in contrast to other precedent indicators, bioorthogonal. Transgenic flies and mice, with robust functional expression in different areas, including the central nervous

system, show a normal phenotype and can be used for Ca^{2+} measurements *ex vivo* and *in vivo*.

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FIGURE CAPTIONS

Figure 1. Ca^{2+} calibration of aequorins (A) and GAPs (B).

(A) Except when otherwise stated, all the calibrations are at 22 °C. **1.** Wild-type (wt) aequorin (AEQ) with native coelenterazine. **1b.** Same as 1, but at 37 °C. **2.** wt-AEQ with Cz n. **3.** ^{D119A}AEQ with Cz n. **ermutGA**, er-targeted GFP-^{D119A}AEQ with Cz n. **GAP1**, GFP-^{D117A, D119A, D163A}AEQ with Cz n. **er2mutAEQ**, ^{N28L, D119A}AEQ with Cz i at 37°C. Data in ordinate are counts/total counts (s^{-1}). Note double logarithmic scales. Data taken from [29, 33, 34, 36, 37]. **(B)** Calibration of GAPs. Adjusted to $y/y_{\max} = ([\text{Ca}^{2+}]^n) / (K_D^n + [\text{Ca}^{2+}]^n)$, where $y = ((R - R_{\min}) / (R_{\max} - R_{\min}))$, with $n = 1$. The values of K_D (μM) were: GAP, 0.2; GAP1, 17; GAP3, 450-500. The affinities of GAP2 and GAP3 were undistinguishable. Data taken from [38, 43]. **(C)** Model comparing the action of GAP as luminescent (left) and fluorescent probe (right). Ca^{2+} is the trigger in both cases. For luminescence emission combination of AEQ with the cofactor, Cz, is necessary. In contrast, Cz is not required nor does it modify fluorescence emission. Modified from [36].

Figure 2. Functional mapping of ER Ca^{2+} release induced by acetylcholine (ACh) erGAP3 in mice hippocampus.

(A) Frame sequence during stimulation with acetylcholine (ACh; 200 μM , 30 s) in acute hippocampal slices from erGAP3 transgenic mice (line 10; P7). Cornus ammonis regions (CA) and the upper blade of dentate gyrus are visible. Measurements of ER- (erGAP3) and cytosolic Ca^{2+} (rhod-3) were performed simultaneously. Frames were acquired every 10 s. Upper row: ER Ca^{2+} release, evidenced by the decrease of the GAP signal in CA1,

during ACh stimulation. Calibration bar, 200 μm . Lower row, coordinated increase of rhod-3 fluorescence, indicating the increase of $[\text{Ca}^{2+}]_{\text{C}}$ by release from the ER. **(B)** Detailed kinetics of regions of interest (ROIs) shown in (A). Each graph symbol corresponds to 10 s. Note that the peak increase of $[\text{Ca}^{2+}]_{\text{C}}$ occurs 10 s after the application of ACh, whereas maximum $[\text{Ca}^{2+}]_{\text{ER}}$ decrease required more than 30 s. The relaxation of the $[\text{Ca}^{2+}]_{\text{C}}$ peak is also faster than the one of the $[\text{Ca}^{2+}]_{\text{ER}}$ peak. Reproduced with permission from [43].

Figure 3. Stimulation of motor neurones promotes Ca^{2+} release from muscle sarcoplasmic reticulum.

Experiment performed in adult erGAP3-expressing transgenic *Drosophila melanogaster* *in vivo*. **(A)** The motor neurons were stimulated through the giant fiber system [46] with square 6 V/30 ms pulses at 0.25, 4 or 16 Hz, as shown. Images of F_{470} were captured every 100 ms (circles). Excitation ratioing is not feasible at this high acquisition rate. **(B)** The first image (F_{470}) shows the green fluorescence of the thoracic muscles seen from the top. Calibration bar, 500 μm . The region of interest where the measurements were taken is also shown (white square). The rest of the images (**a-d**) were normalized as the ratio F/F_0 and coded in pseudocolor (scale at right). The exact moment at which each image was taken is shown at (A). **(C)** Superimposition of the responses to the three stimuli at an expanded time scale. The arrowheads denote two successive stimuli of the 0.25 Hz series. Note that the stimulation periods last for longer than the time shown and that the sampling period for imaging is of 1 image every 0.1 s.

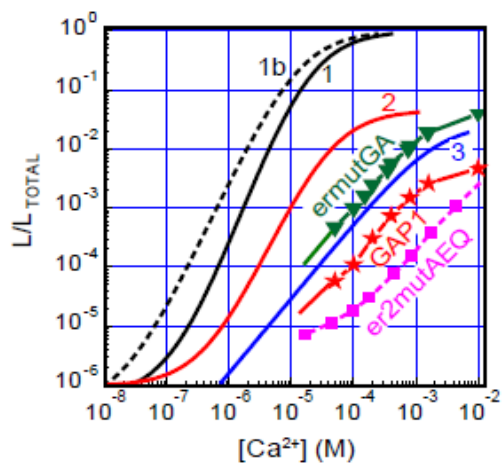
Table 1. Low affinity Ca²⁺ indicators.

Name	Type	K _d (μM)	n	Dynamic range	λ (nm)		Ref.
					Ex.	Em.	
Synthetic probes							
Mag-Fura-2	Ex. ratiometric	53	1	1.7	350 385	510	[47]
Mag-Indo-2	Em. ratiometric	30	1	20	355	400 480	[48]
Rhod-5N	Intensiometric	320	1	50	551	575	[9]
CaGF	Intensiometric	60	1	2.5	488	530	[49]
GECIs							
YC4er	Em. ratiometric	0.08 700	1.5 0.87	1.5	440	485 535	[18]
D1ER	Em. ratiometric	0.8 60	1.18 1.63	1.5	440	485 535	[50]
D4cpv	Em. ratiometric	80	1.35	3.8	440	485 535	[20]
Split-YC7.3er	Em. ratiometric	130	1.4	2.6	440	485 535	[51]
CatchER	Intensiometric	180	0.94	1.5	490	510	[24]
Twitch	Em. ratiometric	253		4.4	432	475 527	[52]
G-CEPIA1er	Intensiometric	672	1.95	4.7	472	520	[23]
R-CEPIA1er	Intensiometric	565	1.7	8.8	562	641	[23]
GEM-CEPIA1er	Em. ratiometric	558	1.37	21.7	377	466 520	[23]
D1ERCmR2	Em. ratiometric	220	0.5	1.1	480	510 560	[53]
GCaMPer	Intensiometric	238	0.93	2	490	540	[54]
LAR-GECO1	Intensiometric	24	1.3	10	559	647	[55]
erGAP1	Ex. ratiometric	16	1	4	405 470	520	[38]
erGAP3	Ex. ratiometric	489	0.9	3	405 470	520	[43]

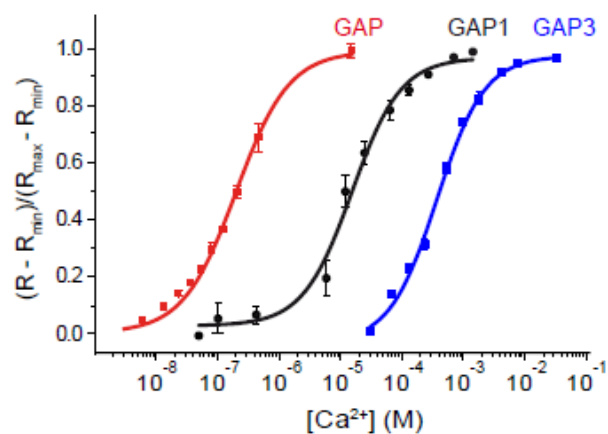
cp, circularly permuted; n, Hill coefficient; Ex., excitation; Em., emission.

Fig. 1

A. AEQUORINS



B. GAPs



C. GAP model

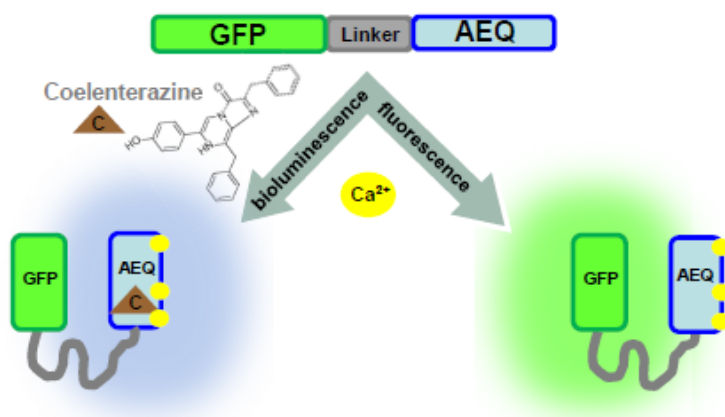


Fig. 2

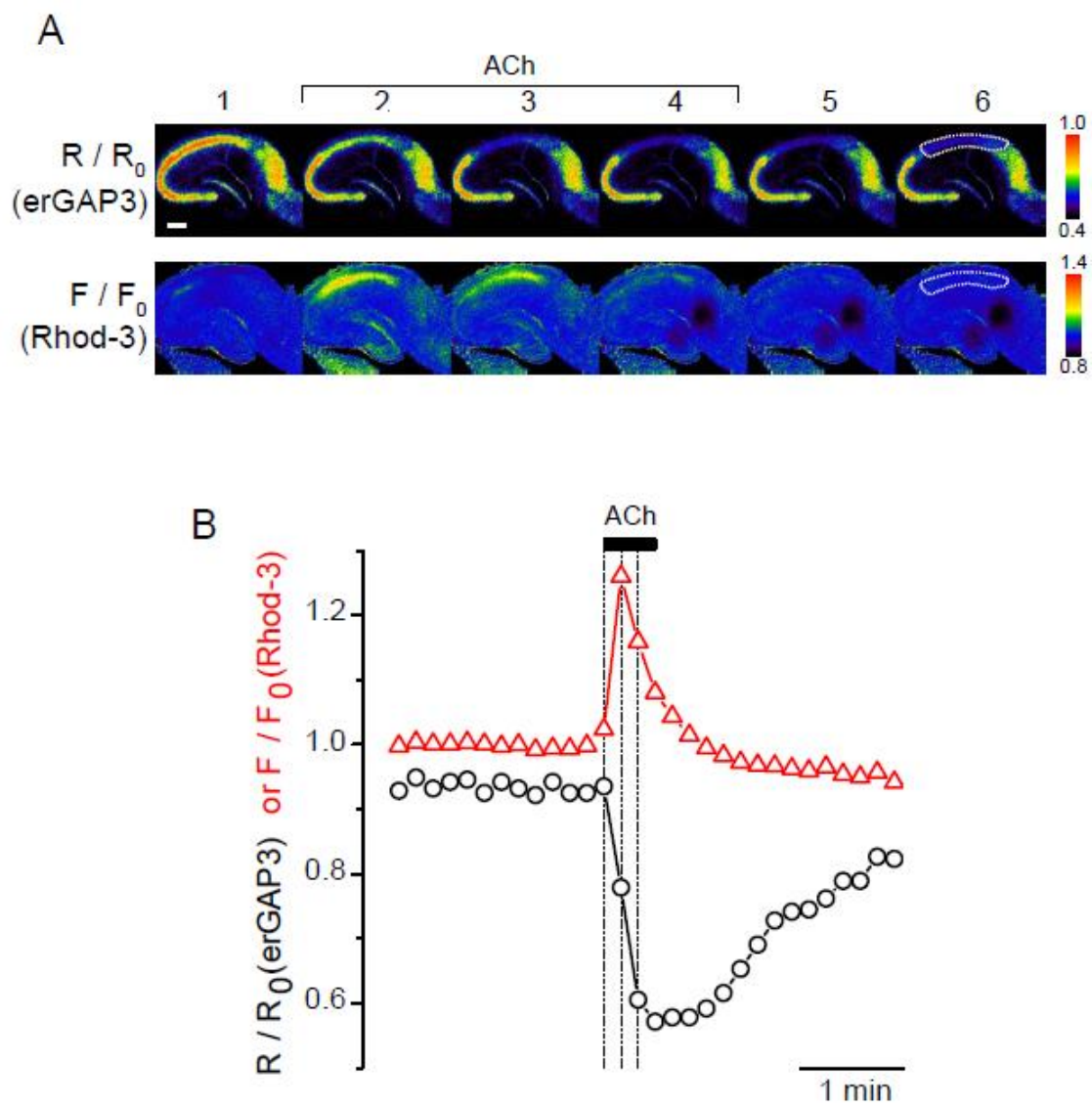


Fig. 3

