



Fluorescent biosensors illuminate calcium levels within defined beta-cell endosome subpopulations

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ABSTRACT

Live cell imaging has revealed that calcium ions (Ca²⁺) pass in and out of many cellular organelles. However, technical hurdles have limited measurements of Ca²⁺ in acidic organelles, such as endosomes. Although evidence hints that endosomes play a role in Ca²⁺ signaling, direct measurements within endosomal lumina represent one of the final frontiers in organelle imaging. To measure Ca²⁺ in a TiVAMP-positive endosome sub-population, the pH-resistant ratiometric Ca²⁺ biosensor GEM-GECO1 and the ratiometric pH biosensor mKeima were used. A positive correlation between acidic endosomal pH and higher Ca²⁺ was observed within these Rab5a- and Rab7-positive compartments. Ca²⁺ concentration in most endosomes was estimated to be below 2 μM, lower than Ca²⁺ levels in several other intracellular stores, indicating that endosomes may take up Ca²⁺ during physiological stimulation. Indeed, endosomes accumulated Ca²⁺ during glucose-stimulation, a condition where endosomal pH did not change. Our biosensors permitted the first measurements revealing a role for endosomes in cellular Ca²⁺ homeostasis during physiological stimulation.

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1. Introduction

Calcium ions (Ca²⁺) play many essential roles in cellular signaling. The plasma membrane separates the low cytoplasmic Ca²⁺ concentration (<200 nM in a quiescent cell) from the much higher extracellular Ca²⁺ levels (>1 mM). Multiple organelles participate in global cellular Ca²⁺ homeostasis, while also signaling locally to regulate specific subcellular events [1–3]. Fluorescent protein-based biosensors enable direct measurements of Ca²⁺ dynamics within the lumina of defined Ca²⁺ handling organelles, and provide minimally invasive windows into their respective roles in cellular physiology [4]. Some organelles function primarily as Ca²⁺ stores, whereas other organelles are transient Ca²⁺ buffers that act to shape cellular Ca²⁺ signals and protect cells from excitotoxicity [1]. The endoplasmic reticulum (ER) is the most well characterized intracellular Ca²⁺ store, with Ca²⁺ levels

of 250–600 μM [5]. ER Ca²⁺ concentration is primarily regulated by Ca²⁺-importing pumps called sarco/endoplasmic reticulum Ca²⁺-ATPases (SERCAs), as well as Ca²⁺ release channels including the IP₃R and RyR [1,6]. The Golgi network also stores Ca²⁺ (100–300 μM) at levels that facilitate post-translational protein modifications [7,8]. On the other hand, direct measurements in living cells indicate that other organelles, such as the nucleus and mitochondria, rapidly take up Ca²⁺ but do not act as long-term stores for significant amounts of Ca²⁺ [1]. Roles in Ca²⁺ handling have been proposed for other organelles, particularly the acidic organelles of the endosomal and lysosomal systems [9], but direct and specific measurements of Ca²⁺ within those lumina have been challenging due to the disproportionate pH sensitivity of existing Ca²⁺ biosensors [10]. Thus, despite the fact that endosomes are important signaling organelles [11], the physiological role of endosomal Ca²⁺ fluxes remains poorly understood.

The highly acidic nature of endosomes dictates that biosensors with sufficient pH insensitivity are required for luminal Ca²⁺ imaging in this compartment. Although current Förster resonance energy transfer (FRET)-based ‘cameleon’ probes are acceptable for ER and other organelles [6,12,13], they are large (>70 kDa) and typically incorporate highly pH-sensitive fluorescent protein variants that are quenched in acidic environments. Single fluorescent protein Ca²⁺ biosensors (e.g. G-CaMP) [14,15] are smaller, but

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Table 1

The K_d , Hill coefficient n , R_{max} and R_{min} of GEM-GECO1 obtained from fitting at different pH values.

pH	K_d (mM)	n	R_{max}	R_{min}	Adjusted R^2
4.97	54.24	2.80	0.954	0.050	0.999
5.42	17.88	2.97	1.402	0.050	0.999
6.00	3.09	2.70	1.533	0.041	0.999
6.50	0.68	2.75	1.418	0.035	0.999
7.00	0.46	3.02	1.453	0.017	0.996
7.50	0.27	2.27	1.476	0.021	0.998

also typically employ pH-sensitive fluorescent proteins [14,16]. Recently, we developed an expanded series of Ca^{2+} indicators via directed evolution of G-CaMP3 [16]. One variant in this series, known as GEM-GECO1, exhibits a blue-green ratiometric emission, a K_d of 340 nM, an exceptionally high dynamic range (11,000% change *in vitro*), and is relatively pH insensitive [16]. Specifically, GEM-GECO1 still maintains 50% of its maximum dynamic range at the acidic pH of 6.1, and we therefore considered that it might be suitable for Ca^{2+} imaging in endosomes of living cells.

Here, we describe the combined use of GEM-GECO1 and a pH biosensor to achieve calibrated and pH-corrected, semi-quantitative Ca^{2+} measurements in the endosomal lumen. Using this novel approach, we estimated the baseline Ca^{2+} concentration of Rab5a- and Rab7-positive endosomes and imaged the kinetics of endosomal Ca^{2+} fluxes in glucose-stimulated beta-cells. Using this new tool, we discovered that endosomes take up Ca^{2+} in glucose-stimulated beta-cells.

2. Materials and methods

2.1. Cloning, plasmids and transfection

Synthetic DNA oligonucleotides used for cloning and library construction were purchased from Integrated DNA Technologies (Coralville, Iowa). The sequences of all oligonucleotides used in this work are provided in Table 2. Pfu polymerase (Fermentas, Waltham, MA) and Pfx polymerase (Life Technologies, Carlsbad, CA) were used for non-mutagenic PCR amplifications in the buffer supplied by the respective manufacturer. PCR products and products of restriction digests were routinely purified using preparative agarose gel electrophoresis followed by DNA isolation using the GeneJET Gel Extraction Kit (Fermentas) and MinElute Gel Extraction Kit (Qiagen, Hilden, Germany). Restriction endonucleases were purchased from Fermentas and New England Biolabs (Ipswich, MA) and were used according to the manufacturers' recommended protocol. Ligations were performed using T4 ligase in Ligation Buffer (Life Technologies, New England Biolabs). Small-scale isolation of plasmid DNA was performed using the GeneJET Miniprep Kit (Fermentas) and QIAprep Spin Miniprep Kit (Qiagen). Invitrogen's PureLink HiPure Plasmid Filter Maxiprep Kit was used for large scale DNA amplification.

MIN6 beta-cells were cultured in DMEM media containing 25 mM glucose (Sigma–Aldrich, St. Louis, MO) supplemented with 10% (v/v) FBS (Life Technologies) and penicillin/streptomycin (100 µg/ml; Life Technologies) at 37 °C and 5% CO₂ as described previously [6]. All constructs were transfected into MIN6 cells using the NEON Transfection system. 2 µg of plasmid DNA were used to electroporate 1 million MIN6 cells. Cells were electroporated with two 1200 V pulses with a pulse width of 20 ms.

Primary hand picked human islets from a healthy 11-year-old male donor were dispersed and electroporated using the NEON transfection system (2 µg DNA per 1 million cells, 1000 V, 2 pulses, 30 ms pulse width) and subsequently cultured in CMRL medium for 72 h prior imaging.

2.2. Microscopy and image analysis

Colocalization images were acquired using a widefield inverted Zeiss Axiovert 200M microscope equipped with a 100× 1.45NA objective. Image stacks were deconvolved using Slidebook Software to obtain confocal image planes. Object based colocalization studies were performed using the Fiji/ImageJ plugin JaCoP [17].

Live cell imaging of MIN6 and primary cells was performed on a wide-field microscope setup (Zeiss Axiovert 200M) with a mounted 40× Plan-Neofluar 1.3NA oil objective (Zeiss, Jena, Germany) [6]. Cells were cultured and imaged on poly-D-lysine coated No. 1.5 25 mm circular borosilicate coverslips (Electron Microscopy Sciences, Hatfield, PA) and were kept at 37 °C in a temperature controlled incubation chamber (Harvard Apparatus, Holliston, MA) during imaging. Images were acquired with a CoolSNAP HQ2 CCD camera (Photometrics, Tucson, AZ). GEM-GECO1 was excited with a selective bandpass filter (386/23 nm) and emissions were detected with selective bandpass filters (440/40 nm and 520/32 nm) using a single filter cube with a mounted dichroic mirror. The Sutter Lambda 10-2 emission filter wheel is capable of switching between different emission filters within 75 ms. Ratiometric mKeima imaging was performed by using selective excitation filters (430/25 nm and 575/50 nm) and a 632/60 nm emission filter. The excitation filters were mounted in a Sutter instruments DG4 light source enabling excitation switches in <2 ms. The exposure times for GEM-GECO1 and mKeima detection were kept at ≤1 s.

Sensor calibration imaging of purified GEM-GECO1 and mKeima protein was performed in a 96 well-plate with a No. 1.5 glass bottom. The calibration is detailed below. Time-lapse image sequences, as well as still images, were analyzed using Slidebook software (Intelligent Imaging Innovations, Denver, CO), Cell Profiler 2.0 [18], and the ImageJ distribution Fiji [19]. Local background subtraction was performed to correct for cellular autofluorescence [20]. Live-cell experiments were performed with preheated solutions and stable perfusion at 1 ml/min, and complete solution changes were achieved in <60 s. Live cells were imaged in Ringer's buffer (119 mM NaCl, 4.7 mM KCl, 25 mM NaHCO₃, 2.5 mM CaCl₂, 1.2 mM MgSO₄, 1.2 mM H₂PO₄) supplemented with glucose as indicated in the figures.

2.3. Protein purification and *in vitro* spectroscopy

To purify GEM-GECO1 for *in vitro* spectroscopic characterization, the pBAD plasmid harboring the gene for mKeima-GEM-GECO1 was first used to transform electrocompetent *E. coli* DH10B cells. Following selection on LB/ampicillin (200 mg/ml), single colonies were picked and used to inoculate 4 mL LB medium (200 mg/ml ampicillin, 0.2% L-arabinose). Bacterial cultures were shaken at 250 rpm and allowed to grow for 30 h at 30 °C. Bacteria were harvested by centrifugation (10,000 × g for 5 min), resuspended in 30 mM Tris–HCl buffer (pH 7.4), lysed by French press, and clarified by centrifugation at 13,000 × g for 45 min at 4 °C. Proteins were purified from the cell-free extract by Ni-NTA affinity chromatography (Agarose Bead Technologies, Tampa, FL). Purified proteins were dialyzed into either 30 mM Tris, 150 mM NaCl, pH 7.4 or 10 mM MOPS, 100 mM KCl, pH 7.2. Fluorescence spectra were recorded on a Safire2 plate reader (Tecan, Maennedorf, Switzerland). Since GEM-GECO1 and mKeima are ratiometric sensors, the response to Ca^{2+} or H^{+} is expressed as the fluorescent ratio R . For GEM-GECO1, $R = (I \text{ at } 453 \text{ nm}) / (I \text{ at } 513 \text{ nm})$, where I = fluorescence intensity when excited at 390 nm. For mKeima $R = (I \text{ with } 584 \text{ nm excitation}) / (I \text{ with } 448 \text{ nm excitation})$, where I = fluorescence intensity at 635 nm.

Table 2
Primers used in this study.

Primer name	Primer sequence (5'–3')
Fw_NcoI.6xhis.mKeima	GCGATGCCATGGGTGTCATCATCATCATCATCATGGTACAATGGTCGACTCTAGAATGGTGAGTGTGATCGCTAAACAAATGACC
Rv_mKeima_KpnI.HindIII	GCGAAAGCTTCTATCCGGTACCCATGGTACTTCCACCTGTGCCACC
Fw_KpnI.GEM	GCGAGGTACCACCATGGTCGACTCATCACGTC
Rv_GECO-Stop-HindIII	GCGATGAAGCTTCTACTTCGCTGTCATCATTTGTACAACTCTTCGTAGTTT
Fw_ApaI.TiVAMP	GGGGGCGCGCCGCGCATGGCGATTCTTTTGTGCTGTGTTG
Rv_TiVAMP_NotI	CGCGGCGCTTTCTTACACAGCTTGCCATG
Fw_EcoRI.GEM-GECO1	CGAATTCTAACGCCGCGAGCTGCGACTGCG
Rv_GEM-GECO1.HindIII	CAAGCTTCTACTTCGCTGTCATCATTTGTACAAAC
Fw_XbaI.mKeima	CCTCTAGAATGGTGAGTGTGATCGCTAAACAAATGACCTACAAGG
Rv_mKeima.HindIII	GGAAGCTTCTAACCGAGCAAAGAGTGGCGTGCAATGG
Fw_SacI.Rab5a	GGCGAGCTCAAATGGCTAGTCGAGGCGCAACAAG
Rv_Rab5a_BamHI	CGCGGATCCTTACAGATCCTCTCTGAGATGAGTTTC
Fw_SacI.Rab7	GGCGAGCTCAAATGGCGAGCGCGACCACTG
Rv_Rab7_BamHI	CGCGGATCCTTACAGATCCTCTCTGAGATGAGTTTC

2.4. Determination of K_d of mKeima as a pH indicator

mKeima was used as an organelle pH indicator. To achieve this, we needed to measure the apparent pK_a of mKeima using standard solutions with different pHs, prepared as follows. A solution containing 30 mM trisodium citrate and 30 mM borax was adjusted to pH 11.5 and HCl (12 M and 1 M) was then added drop-wise to provide solutions with pH values ranging from 11.5 to 3 in 0.5 pH unit intervals. In a 96-well plate, 1 μ l of concentrated mKeima protein solution in MOPS buffer (30 mM MOPS, 100 mM KCl, at pH 7.2) was added into a well containing 100 μ l of each of the standard solutions described above. The mKeima fluorescence in each pH condition was recorded using a Safire2 multiwell fluorescence plate reader, with three replicates. The results were fitted in the following Hill equation:

$$R_{\text{mKeima}} = 0.106 - \frac{3.18 \times [H^+]^{1.16}}{[H^+]^{1.16} + 1.89 \times 10^{-7}} \quad (1)$$

$$R^2 = 0.993$$

2.5. Determination of Ca^{2+} K_d of GEM-GECO1 at different pHs

The K_d of GEM-GECO1 as a function of the pH can be determined by Ca^{2+} titrations in a series of standard solutions at different pHs values. Ca^{2+} titrations were performed by dilution (1:100) of a concentrated protein solution of mKeima–GEM-GECO1 into a series of buffers which were prepared by mixing Ca^{2+} -saturated and Ca^{2+} -free buffers (30 mM MOPS, 100 mM KCl, 10 mM EGTA, either with or without 10 mM Ca^{2+}) in different ratios to provide a series of solutions with various free Ca^{2+} concentration at 20 °C [21].

To determine the K_d of GEM-GECO1 as a function of pH, we prepared a series of buffers with different pH values (pH 5, 5.5, 6.0, 6.5, 7.0 and 7.5). Each pH buffer was prepared as a Ca^{2+} -saturated and a Ca^{2+} -free solution. We then used these standard solutions to mix more buffers with various Ca^{2+} concentrations for each given pH. Since the K_d values of the Ca–EGTA complex in different conditions are known, we can calculate the free Ca^{2+} concentration in each buffer. Note that the pH and ionic strength of the buffer must be taken into account, as they influence the K_d of the Ca–EGTA complex. Free Ca^{2+} at different pHs, ionic strengths and different ratios of Ca–EGTA to EGTA can be conveniently calculated using Max-Chelator (<http://www.stanford.edu/~cpatton/maxc.html>) [22]. For a series of Ca^{2+} buffers at a given pH, the fluorescence ratio of GEM-GECO1 in each solution (Ca^{2+} -free and Ca^{2+} -saturated) was measured in the fluorescence plate reader and plotted as a function of Ca^{2+} concentration (Fig. 4A). Experiments were performed in triplicate and the averaged data from the three independent measurements was fit to the Hill equation to calculate effective K_d value of GEM-GECO1 at that given pH (Table 1). The K_d values

obtained from different pHs were then used to determine the K_d as the function of H^+ concentration was fit to a parabolic equation to obtain:

$$K_d(H^+) = 1.55 \times 10^{11} \times [H^+]^2 + 3.47 \times 10^6 \times [H^+] + 0.019 \quad (2)$$

$$R^2 = 0.98$$

Because the chromophore environment in Ca^{2+} -unbound and bound states of GEM-GECO1 is also influenced by the pH, the maximum and minimum ratios (R_{max} and R_{min}) of GEM-GECO1 are also dependent on the pH and require calibration. R_{max} and R_{min} from the fitted equations in different pHs were extracted and fit to the Hill equations in order to establish the relationship between R_{max} and R_{min} and pH. This procedure provided the following equations:

$$R_{\text{max}}(H^+) = 1.46 - \frac{1.36 \times [H^+]^{2.86}}{[H^+]^{2.86} + 9.93 \times 10^{-15}} \quad (3)$$

$$R^2 = 0.89$$

$$R_{\text{min}}(H^+) = 0.020 + \frac{0.031 \times [H^+]^{1.41}}{[H^+]^{1.41} + 1.53 \times 10^{-15}} \quad (4)$$

$$R^2 = 0.98$$

By substituting K_d , R_{max} and R_{min} using Eqs. (1), (3) and (4) respectively, the final calibration equation could be generalized as follows:

$$R_{\text{GEM-GECO1}}(H^+) = R_{\text{min}}(H^+) + [R_{\text{max}}(H^+) - R_{\text{min}}(H^+)] \times \frac{[Ca^{2+}]_{\text{free}}^{2.85}}{[K_E(H^+)]^{2.85} + [Ca^{2+}]_{\text{free}}^{2.85}} \quad (5)$$

where the Hill coefficient ($n = 2.85$) is the average of Hill coefficients of the fitted equations for pH 5.0–7.0. Eq. (5) can be further reordered into Eq. (6):

$$[Ca^{2+}]_{\text{free}} \approx K_d(H^+) \times \left[\frac{R_{\text{GEM-GECO1}}(H^+) - R_{\text{min}}(H^+)}{R_{\text{max}}(H^+) - R_{\text{GEM-GECO1}}(H^+)} \right]^{0.35} \quad (6)$$

Eq. (6) is the function for the 3-dimensional surface plot of the response of GEM-GECO1 as a function of Ca^{2+} concentration and pH *in vitro* shown in Fig. 4C).

2.6. Conversion of mKeima and GEM-GECO1 ratios into estimated pH and free Ca^{2+} level *in situ*

With Eq. (6) and the correlated R_{max} and R_{min} of mKeima and GEM-GECO1, the signals of mKeima and GEM-GECO1 obtained from *in situ* experiments were translated into the estimated pH and Ca^{2+} levels in endosomes. Briefly, the estimated pH was calculated based on the raw ratio of mKeima using Eq. (1). The estimated pH

was then used to determine the K_d , $R_{\max}$ and $R_{\min}$ of GEM-GECO1. Finally, the free Ca^{2+} concentration was calculated based on the raw ratio of GEM-GECO1, the calculated K_d , the calculated $R_{\max}$, and the calculated $R_{\min}$, by using Eq. (6). In these images, 33 out of 230 measured endosomes were below the minimum fluorescent GEM-GECO1 ratio ($R_{\min}$) due to an insufficient signal to noise ratio and were excluded from the following conversion.

After the conversion, we obtained (semi)quantitative information of Ca^{2+} levels of endosomes with different pHs which reveals a clear correlation between the Ca^{2+} level and the pH of endosomes. In contrast, the raw signal ratios of mKeima and GEM-GECO1 were poorly correlated (Fig. 5B). To address the reliability of our data, we estimated the upper and lower limit of quantification using the confidence band (95%) of the Ca^{2+} titration curves with different pHs according to literature [52]. Subsequently, we fit the upper and lower limit of quantification using equation $y = a \cdot b^{\text{pH}}$. The results are plotted in Fig. 5D. In addition, we also give the 95% confidence band for the fitted curves in Fig. 5D. As shown in Fig. 5D, red and blue lines indicate the upper and lower limit of quantification, the dash lines represent the 95% confidence band. These lines define the usable range for measuring Ca^{2+} concentration using GEM-GECO1 under different pHs. Within the endosomal pH (below 6.5), most of the data points and the regression curve fall within the valid region, which demonstrates that our measurements are statically valid.

2.7. Statistical analysis

Data are expressed as mean $\pm$ SEM. Statistical analysis throughout the study was performed by applying two-tailed student *t*-tests. Significance was defined at $p < 0.05$.

3. Results

3.1. TiVAMP–GEM–GECO1 is a luminal Ca^{2+} biosensor localized to early and late endosomes

To generate an endosomal lumen targeted Ca^{2+} biosensor, tetanus-insensitive vesicle-associated membrane protein (TiVAMP, also known as VAMP7) was used as a targeting protein. TiVAMP is a SNARE protein that drives endosomal fusion and is known to be localized to endosomes [23–25]. The functional domain responsible for membrane tethering is located at the cytoplasmic N-terminus of TiVAMP [26]. It has been previously reported that C-terminal tagging of TiVAMP leads to a functional protein with the tethered fusion partner localized to the endosomal lumen [26]. GEM-GECO1 was fused to the C-terminus of TiVAMP–GEM-GECO1 via a 61 amino acid linker that was included to mitigate functional interference with its fusion partners (Fig. 1A). Fluorescence imaging of MIN6 beta-cells transfected with a vector encoding TiVAMP–GEM-GECO1 revealed that the protein product localized to endosome-like structures and exhibited fluorescence emission that was much brighter than the background autofluorescence (Fig. 1B and C). To validate the proper localization of TiVAMP–GEM-GECO1, we co-expressed the sensor with markers of specific endolysosomal compartments. The endosomal calcium sensor colocalized with red fluorescent markers for early endosomes (TagRFP-Rab5a, Fig. 1D), late endosomes (TagRFP-Rab7, Fig. 1E) and LysoTracker, a tracer dye for acidic vesicles (Fig. 1F). By this colocalization analysis, we observed that ~70% of the TiVAMP–GEM-GECO1-positive endosomal population is marked by Rab5a (23%), Rab7 (24%) or LysoTracker (22%). The remaining minority of ~30% TiVAMP–GEM-GECO1 likely localized to endosomal compartments that are not labeled in this analysis (e.g. recycling endosomes). Taken together with the known cellular localization of TiVAMP, these data confirm that the Ca^{2+} biosensor

TiVAMP–GEM-GECO1 localizes to both early and late endosomes in beta-cells.

3.2. TiVAMP–GEM–GECO1 senses endosomal Ca^{2+} changes in the physiological range

We next examined the functionality of TiVAMP–GEM-GECO1. First, we simply modified endosomal Ca^{2+} by changing the Ca^{2+} content of the extracellular media entering MIN6 cells transfected with TiVAMP–GEM-GECO1. A switch from Ca^{2+} -free media to standard media containing 2 mM Ca^{2+} significantly increased the endosomal Ca^{2+} concentration detected with TiVAMP–GEM-GECO1. Conversely, endosomal Ca^{2+} was reduced by incubating cells in buffer containing 0 mM CaCl_2 or 1 mM of the Ca^{2+} chelator EGTA, compared with standard 2 mM CaCl_2 (Fig. 2A and B). These data suggest that TiVAMP–GEM-GECO1 can reflect changes in extracellular Ca^{2+} , possibly due to the simple fluid phase endocytosis of extracellular media.

Dynamic changes in endosomal Ca^{2+} were assessed with time-lapse imaging. TiVAMP–GEM-GECO1-transfected MIN6 cells were initially incubated in standard 2 mM CaCl_2 Ringer's solution, after which this baseline solution was replaced with a high Ca^{2+} (20 mM CaCl_2) Ringer's solution containing ionomycin to promote Ca^{2+} flux across membranes. As expected, endosomal Ca^{2+} levels increased significantly compared to baseline (Fig. 2C). Subsequently, the elevated endosomal Ca^{2+} was depleted by perfusion of the cells with Ca^{2+} free Ringer's solution containing ionomycin and 1 mM EGTA. The TiVAMP–GEM-GECO1 biosensor reflected this change with a change in the emission ratios, which corresponded to a lower relative Ca^{2+} concentration compared to baseline (Fig. 2C). Note that the baseline emission ratio for endosomal Ca^{2+} is between the maximum and minimum ratios obtained during this experiment. This maximum-minimum pattern of TiVAMP–GEM-GECO1 could be observed both in averages of all endosomes within a cell, as well as with analysis of populations of single endosomes (Fig. 2C and D). Taken together, these data suggest that TiVAMP–GEM-GECO1 dynamically reports luminal Ca^{2+} changes in endosomes and that it has adequate dynamic range to sense changes in luminal Ca^{2+} in these specific compartments.

3.3. Endosomes enrich Ca^{2+} during maturation

During the course of our experiments, we observed a remarkable heterogeneity in Ca^{2+} levels in the total pool of TiVAMP–GEM-GECO1 labeled endosomes (Fig. 2D). Single endosome population analysis of MIN6 cells bathed in standard 2 mM CaCl_2 buffer revealed that Ca^{2+} levels varied dramatically between endosomes within a single cell (Fig. 3A–D). While this heterogeneity can be caused to some degree by the movement of the vesicle between the acquisitions of the individual channels during ratiometric imaging, we still observed remarkable differences in fluorescent ratios by observing individual vesicles (Fig. 3D). We therefore tested the hypothesis that this heterogeneity in luminal Ca^{2+} levels was associated with the maturation of endosomes toward the lysosomal compartment [27]. Indeed, by analyzing only endosomes labeled with TagRFP-Rab5a and TiVAMP–GEM-GECO1, we found a lower relative endosomal Ca^{2+} concentration in early endosomes compared to late endosomes labeled by TagRFP-Rab7 and TiVAMP–GEM-GECO1 (Fig. 3E and F). The increase in luminal Ca^{2+} composition of endosomes as they mature and fuse with lysosomes is consistent with the process of endosomal acidification during the transport of the organelle to lysosomes, which is thought to increase the driving force for Ca^{2+} uptake [28]. Collectively, our data suggest that Ca^{2+} in TiVAMP-labeled endosomes increases

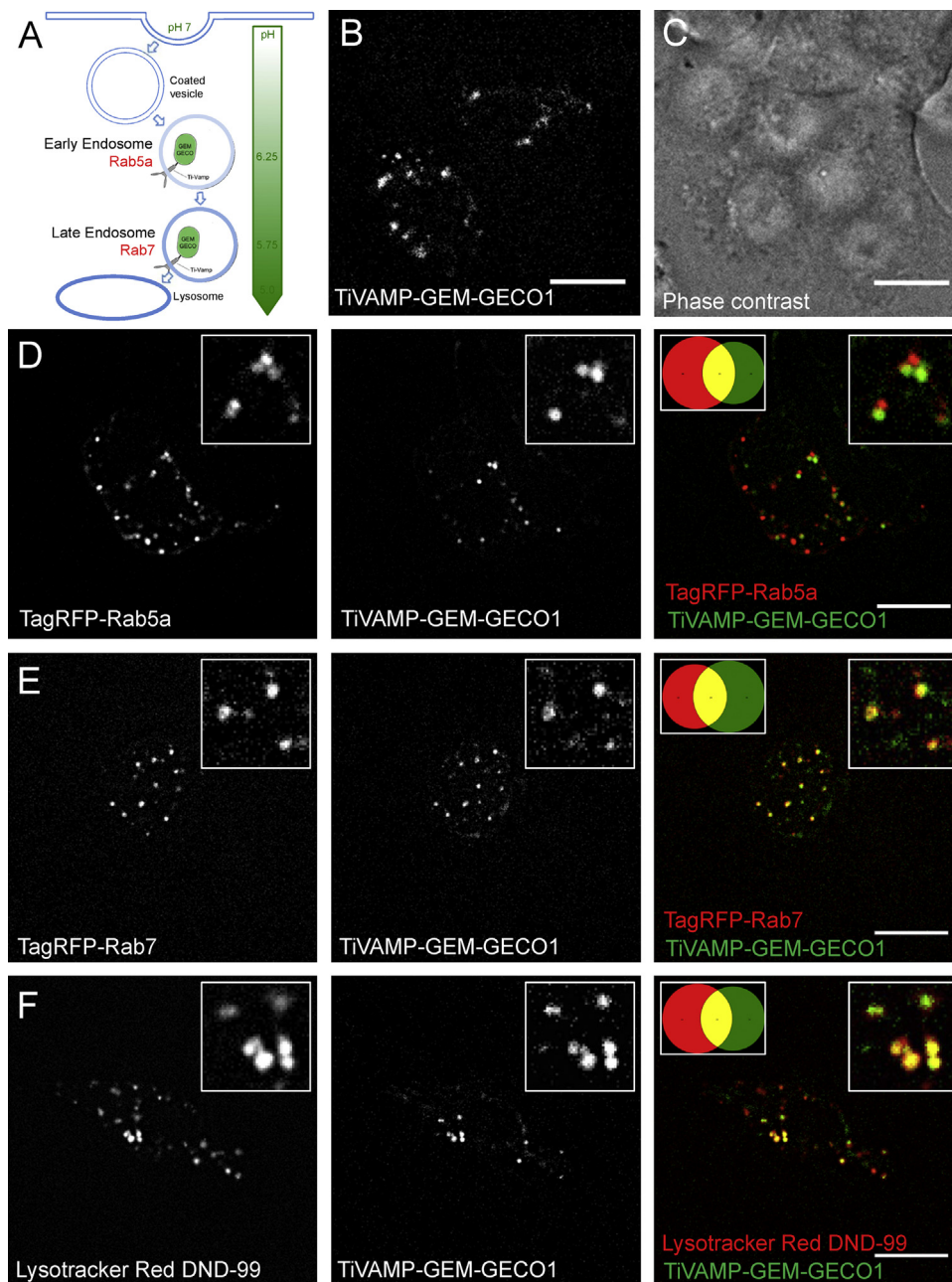


Fig. 1. TiVAMP localizes to early and late endosomes. (A) Schematic illustration of the specific targeting of GEM-GECO1 to the endosomal lumen, as well as the pH gradient along the endolysosomal pathway established from the literature. Note that the very earliest vesicle after endocytosis is not likely to be tagged with the Ca^{2+} or pH sensor probes. (B, C) Expression of TiVAMP-GEM-GECO1 in MIN6 cells, shown in fluorescence and phase contrast modes. (D) TiVAMP-GEM-GECO1 colocalizes with early endosomes labeled by TagRFP-Rab5a. (E) TiVAMP-GEM-GECO1 colocalizes with TagRFP-Rab7-positive late endosomes. (F) TiVAMP-GEM-GECO1 colocalizes to acidic vesicles labeled by the tracer dye Lysotracker Red DND-99. Representative images are shown. Scale bar equals 10 μm . Inset Venn diagrams visualize the degree of vesicle colocalization obtained by object based colocalization analysis ($n = 10$ cells for each condition).

during the maturation from Rab5a-positive ‘early’ endosomes to Rab7-positive ‘late’ endosomes.

3.4. Semi-quantitative Ca^{2+} measurements and *in vitro* calibration

From the above results, it was apparent that TiVAMP-GEM-GECO1 could qualitatively report on endosomal Ca^{2+} dynamics. However, to achieve semi-quantitative interpretation of the GEM-GECO1 emission ratio, we required a means of accounting for differences in both Ca^{2+} and pH in single endosomes. Endosomes are challenging organelles for semi-quantitative approaches since

their luminal composition is highly dynamic [28]. In addition, both the maximal fluorescence response and the Ca^{2+} dissociation constant (K_d) of GEM-GECO1 are dependent on pH (Fig. 4A), despite the improved pH resistance of this biosensor when compared to other Ca^{2+} sensors [16]. To achieve semi-quantitative pH measurements, we employed mKeima, a fluorescent protein that is known to have pH-dependent excitation peaks at 440 nm and 590 nm ($pK_a = 6.0$) [29,30], making it a suitable ratiometric pH biosensor. Indeed, *in vitro* measurements of the excitation ratio of mKeima at different pH values showed a strong dependence between pH values of 5 and 6 (Fig. 4B). To determine the apparent pK_a for mKeima, a series of pH buffers was prepared. The fluorescence of mKeima

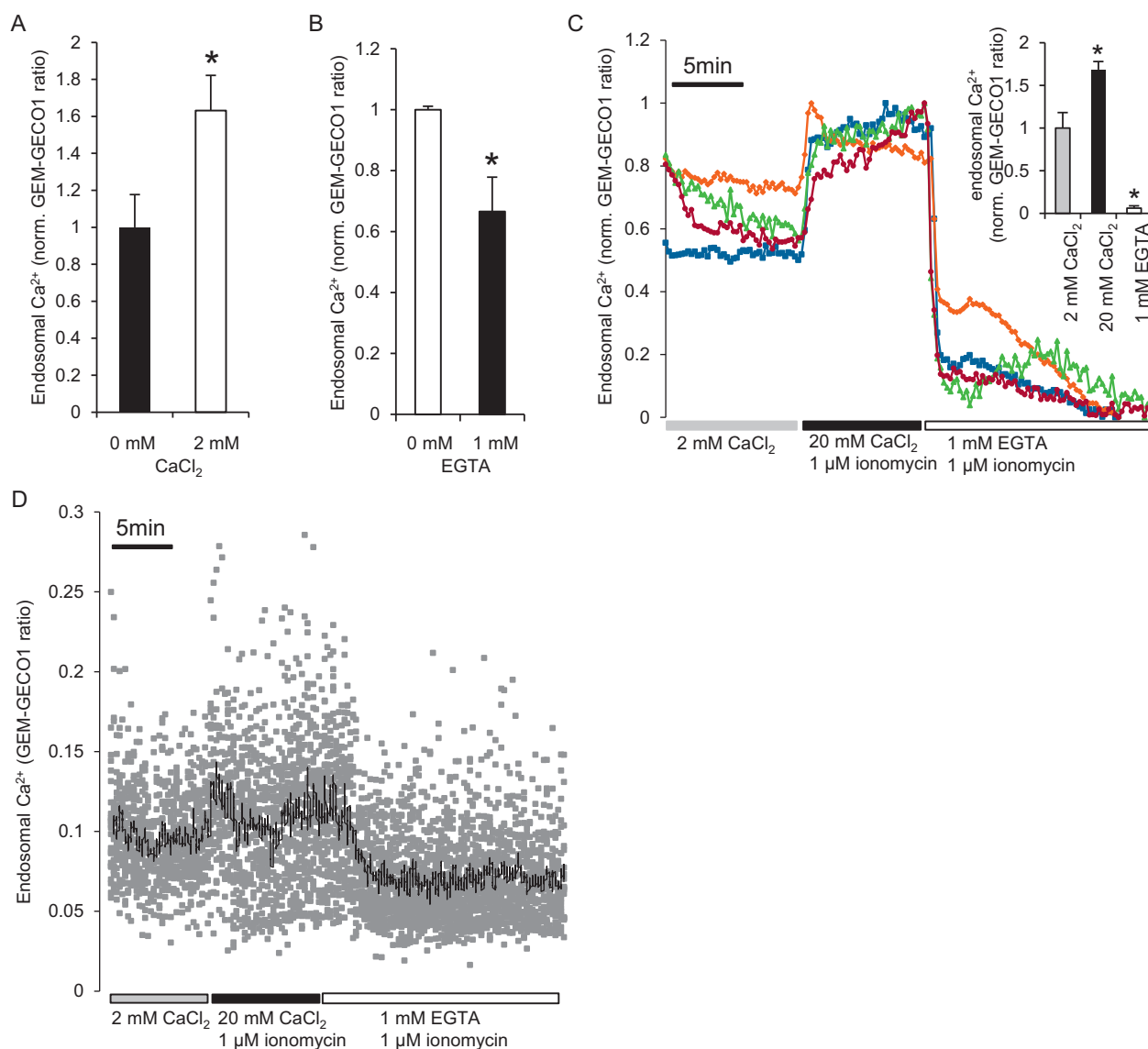


Fig. 2. TiVAMP-GEM-GECO1 senses changes in endosomal Ca^{2+} . (A, B) Endosomal Ca^{2+} was modified by fluid phase internalization of Ringer's buffer of different compositions. (A) MIN6 cells were incubated for 30 min with either CaCl_2 free or 2 mM CaCl_2 containing Ringer's. (B) Extracellular calcium of 2 mM CaCl_2 Ringer's was chelated by incubating cells for 30 min with 1 mM EGTA and compared to cells incubated in regular Ringer's media containing 2 mM CaCl_2 . The bar graphs represent averaged endosomal GEM-GECO1 ratios per cell ($n=4$). (C) Live-cell perfusion demonstrates the responsiveness and dynamic range of TiVAMP-GEM-GECO1 to induced changes in endosomal Ca^{2+} content (averaged per cell). Inset graph shows a 1-min average of endosomal GEM-GECO1 ratios at the end of each individual treatment as a fold change to the baseline to demonstrate the significant change in GEM-GECO1 ratios caused by the treatment ($n=4$). (D) GEM-GECO1 ratio analysis of the population of single endosomes per time point in one cell in response to indicated treatments in a live cell perfusion experiment. The black line represents the average endosomal Ca^{2+} content at each time point. * $p < 0.05$, error bars represent SEM.

in each buffer condition was recorded. The results were fit to a Hill equation to calculate the effective K_a of mKeima. The apparent pK_a of mKeima measured in our studies was 5.80.

It is not currently technically possible to simultaneously clamp both pH and Ca^{2+} within both endosomal and cytosolic compartments, which precluded attempts at *in situ* calibration. Thus, we employed an *in vitro* approach to calibrate the probe combination of GEM-GECO1 and mKeima. A tandem protein composed of GEM-GECO1 fused to mKeima via a 14 amino acid residue linker (GGTGGSTMGMVD) displayed the dynamic and spectral sensing properties of each of the single biosensors. Although it was not useful in living cells, it was ideal for generating a calibration curve essential for quantitative imaging of both Ca^{2+} and pH. To determine the K_d of GEM-GECO1 as a function of pH, we prepared a series of Ca^{2+} -saturated and Ca^{2+} -free buffers at different pH values. For a series of pHs, the fluorescence ratio of GEM-GECO1 in each

solution was determined using a multi-well plate reader, and plotted as a function of Ca^{2+} concentration (Fig. 4A). These data were fit to the Hill equation to calculate effective K_d value of GEM-GECO1 at that given pH (Table 1 and Fig. 4C). The fluorescence of these samples was also measured on the microscope stage using the same filter sets as used for cell imaging experiments. The maximum and minimum ratios of mKeima and GEM-GECO1 obtained in the microscope measurements were used to substitute for the corresponding parameters of the fitting equations (Fig. 4H–J). For the microscope calibration, we assumed that the K_d and Hill coefficient are identical to the previously measured values, and so the only parameters that needed to be adjusted were the maximum and minimum signal ratios ($R_{\max}$, $R_{\min}$) of mKeima and GEM-GECO1. To test this assumption, we analyzed the intensity ratios of pure mKeima protein in MOPS buffer measured *in vitro* and the data obtained from imaging the GEM-GECO1-mKeima solutions at the microscope. The fitting

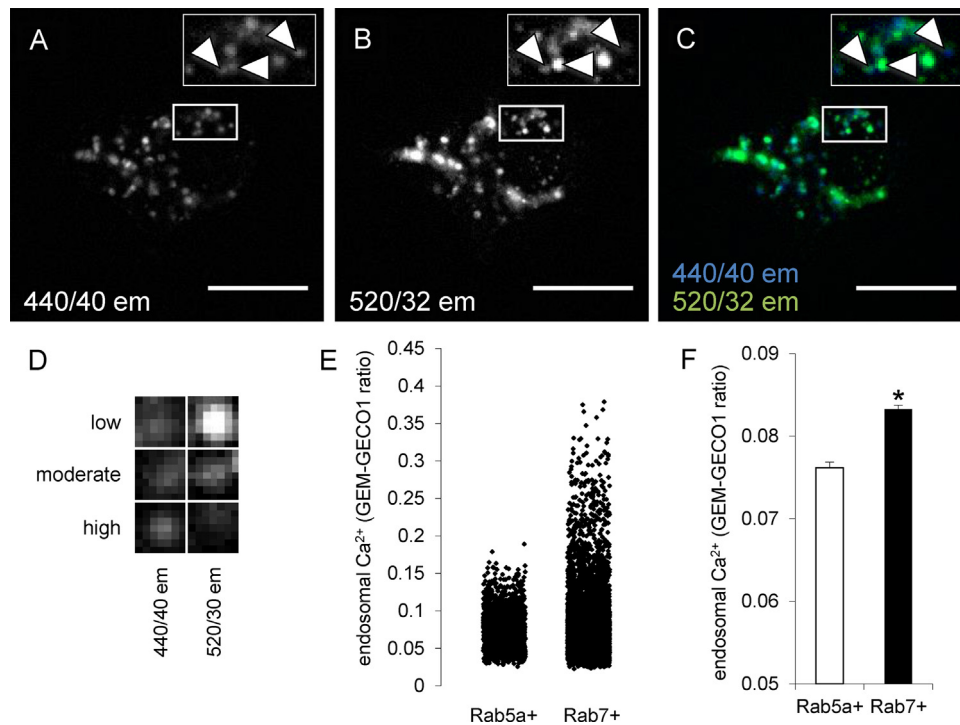


Fig. 3. Ca^{2+} enrichment of endosomes during maturation. (A–D) Heterogeneity in relative endosomal Ca^{2+} content in a MIN6 cell visualized with TiVAMP–GEM–GECO1. Arrowheads point to endosomes with different luminal Ca^{2+} contents. (E, F) Analysis of relative single endosome Ca^{2+} content of early, Rab5a labeled and late, Rab7 labeled endosomes (8 cells). * $p < 0.05$, error bars represent SEM, >1600 endosomes analyzed per population.

equations of all conditions were similar, with the primary difference between the experimental values of R_{max} and R_{min} (Fig. 4D–F). Moreover, the values for pK_a and Hill coefficients showed no significant difference between the calibrated measurements (Fig. 4E and F; $p > 0.1$). The calibration equations obtained through the procedure described above enabled the estimation of endosomal pH and Ca^{2+} using the emission ratios obtained from GEM–GECO1 and mKeima (Fig. 4G).

3.5. Semi-quantitative endosomal Ca^{2+} and pH measurement in living cells

To generate a probe for pH monitoring in endosomes, we fused mKeima to TiVAMP to enable endosomal pH measurements. TiVAMP–mKeima was co-expressed with TiVAMP–GEM–GECO1 for quantitative Ca^{2+} imaging in live cells (Fig. 5A). As expected, the biosensors TiVAMP–GEM–GECO1 and TiVAMP–mKeima colocalized in the same organelles (Fig. 5A). By co-expression of both biosensors, we were able to determine the mean intensity ratios for both mKeima and GEM–GECO1 within individual endosomes (Fig. 5B). To support our measurements, we modeled contour curves of fixed Ca^{2+} concentrations in the diagram (Fig. 5B). These lines indicate that our measurements are within the detection range of the sensor pair, since the GEM–GECO1 ratio is only robustly affected by changes within the endosomal pH range at rather high Ca^{2+} concentrations (Fig. 5C). However, to gain maximum accuracy in our estimates, we corrected the fluorescence ratios for the pH dependency of GEM–GECO1 (see Section 2.5 for details). After this calibration, we observed a strong correlation of mKeima and GEM–GECO1 fluorescence ratios (Fig. 5D, $R^2 = 0.85$) compared to the raw values (Fig. 5B, $R^2 = 0.22$). By employing the calibration curve (Fig. 4G), we determined that the luminal Ca^{2+} concentration of the majority of endosomes is below $2 \mu\text{M}$ (Fig. 5D). The median Ca^{2+} concentration was estimated to be $\sim 900 \text{ nM}$, though this and all of our measured values lower than approximately $1 \mu\text{M}$ should

be interpreted with caution as they are approaching the limits of quantification (LOQ) of the sensor pair as determined by *in vitro* calibration curves (Fig. 5D, Section 2)

While this analysis does reveal a high heterogeneity of endosomal Ca^{2+} concentrations, essentially all endosomes display luminal Ca^{2+} concentrations in the range between hundreds of nanomolar and $5 \mu\text{M}$. These concentrations are within the range of cytoplasmic concentrations in many cell types under stimulated conditions [31], including human pancreatic beta-cells [32]. Interestingly, we observed a high correlation between pH and Ca^{2+} content in the lumen of individual endosomes, with the endosomal Ca^{2+} content increasing exponentially with decreasing pH (Fig. 5D). These data are consistent with a similar correlation reported for luminal pH and Ca^{2+} in the lumen of lysosomes [33]. Thus, our genetically encoded biosensor pair enabled the first simultaneous semi-quantitative measurements of pH and Ca^{2+} concentration in single endosomes of living cells. This approach provides a template for similar analyses in other acidic Ca^{2+} handling organelles.

3.6. Ca^{2+} flux into endosomes in glucose-stimulated beta-cells

Having characterized the heterogeneity of endosomal Ca^{2+} under basal conditions, we next investigated the potential roles of endosomes in intracellular Ca^{2+} homeostasis under physiological stimulation conditions. Glucose-stimulated insulin release from pancreatic beta-cells is strongly dependent on the influx of intracellular Ca^{2+} through voltage-gated Ca^{2+} channels in the plasma membrane [34,35]. However, chronically elevated cytoplasmic Ca^{2+} can also induce cell death [36], making the control of these Ca^{2+} influx signals critical. We previously hypothesized that organelles close to the plasma membrane may buffer the influx of Ca^{2+} within beta-cells during glucose stimulation [37]. Our conclusion that Ca^{2+} concentrations within some endosomal lumina are not very far from the cytosolic concentrations, prompted us to test this hypothesis by measuring real-time changes in

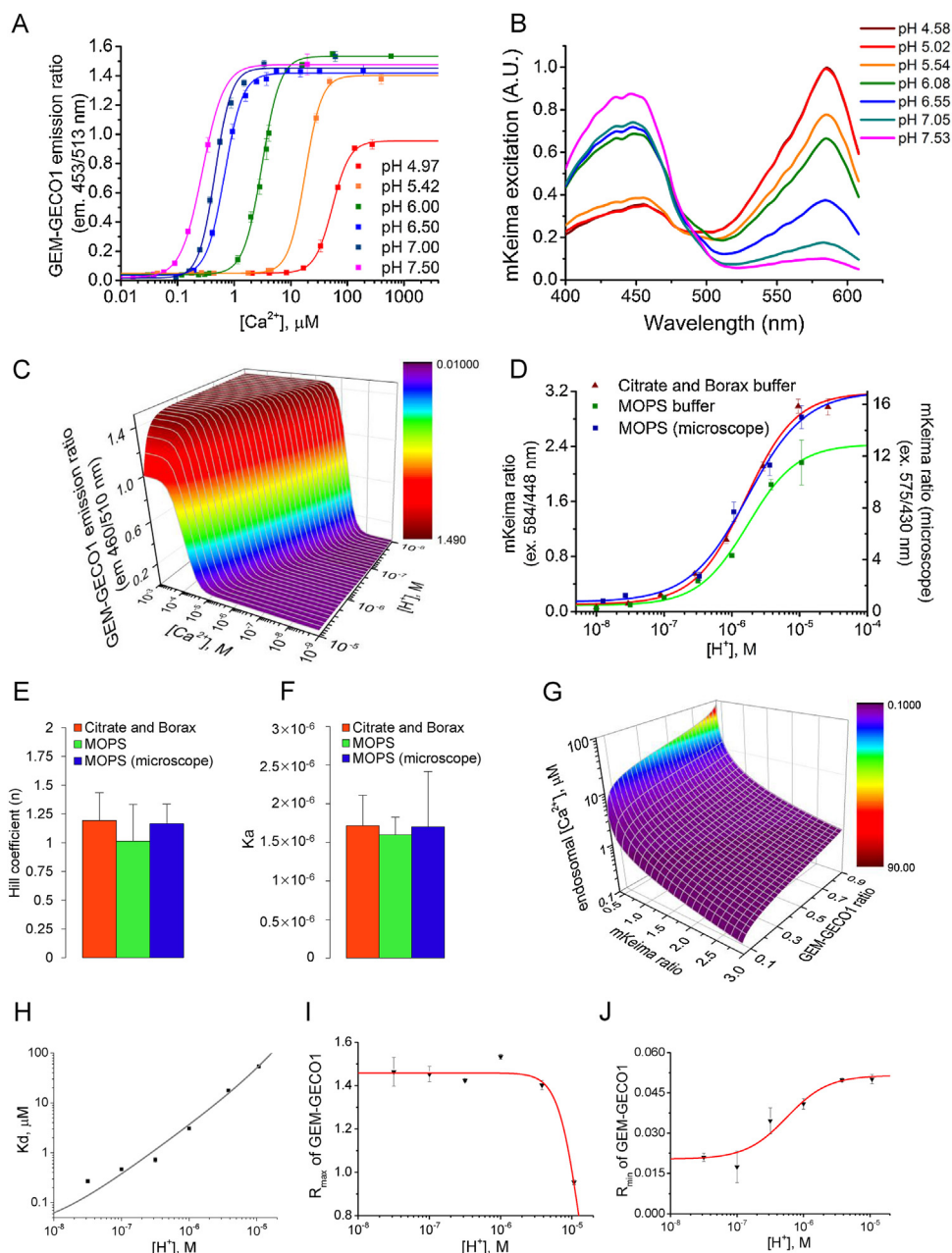


Fig. 4. Quantitative Ca^{2+} measurements and *in vitro* calibration. (A) Ratio of GEM-GECO1 as a function of the Ca^{2+} concentration in different pH conditions. (B) Excitation spectra of mKeima in as a function of the pH. (C) Ratio of GEM-GECO1 as a function of Ca^{2+} and H^{+} concentration. (D) Results of pH titration of mKeima. mKeima protein was reconstituted in citrate/borax buffer or MOPS buffer. mKeima ratios were measured with a plate reader or microscope. (E, F) Statistical analysis of apparent Hill coefficient and K_a of mKeima measured under different conditions. (G) Endosomal Ca^{2+} concentration as a function of the mKeima and GEM-GECO1 ratios based on ratiometric measurements with the microscope setup. (H–J) Coefficient curve fitting using GEM-GECO1 ratios obtained by microscope measurements. (H) K_d of GEM-GECO1 as a function of H^{+} concentration. (I) $R_{\max}$ of GEM-GECO1 as a function of H^{+} concentration; (J) the $R_{\min}$ of GEM-GECO1 as a function of H^{+} concentration. Error bars represent SEM ($n = 3$).

endosomal Ca^{2+} during glucose stimulation. Fluorescence imaging of TiVAMP–GEM-GECO1-positive endocytic vesicles after switching extracellular glucose from 3 mM to 20 mM revealed an elevation of Ca^{2+} within endosomes (Figs. 6A and B). To further characterize this phenomenon, we co-expressed TiVAMP–GEM-GECO1 and the early endosomal marker TagRFP-Rab5a. Early endosomes were identified in the TagRFP channel and the GEM-GECO1 intensity ratios for these objects were tracked to analyze relative early endosomal Ca^{2+} content. Ca^{2+} increases were measured in single Rab5a-positive early endosomes upon glucose stimulation (Fig. 6C). Indeed, the average early endosomal Ca^{2+} content increased under elevated glucose conditions. The change of

endosomal Ca^{2+} upon glucose stimulation was independent of the luminal pH, which remained constant while the endosomal Ca^{2+} concentration doubled under these acute high glucose conditions (Fig. 6D). Interestingly, the endosomal Ca^{2+} did not typically return to baseline immediately after the return to non-stimulatory glucose after stimulation, possibly supporting the concept that a sub-population of endosomes may act as relatively long-acting Ca^{2+} buffers. These data were supported by endosomal Ca^{2+} measurements in a single glucose-stimulated human beta-cell (Fig. 6E). Together, these data suggest that a population of endosomes may act as a previously unappreciated component of the beta-cell Ca^{2+} handling network during the glucose response.

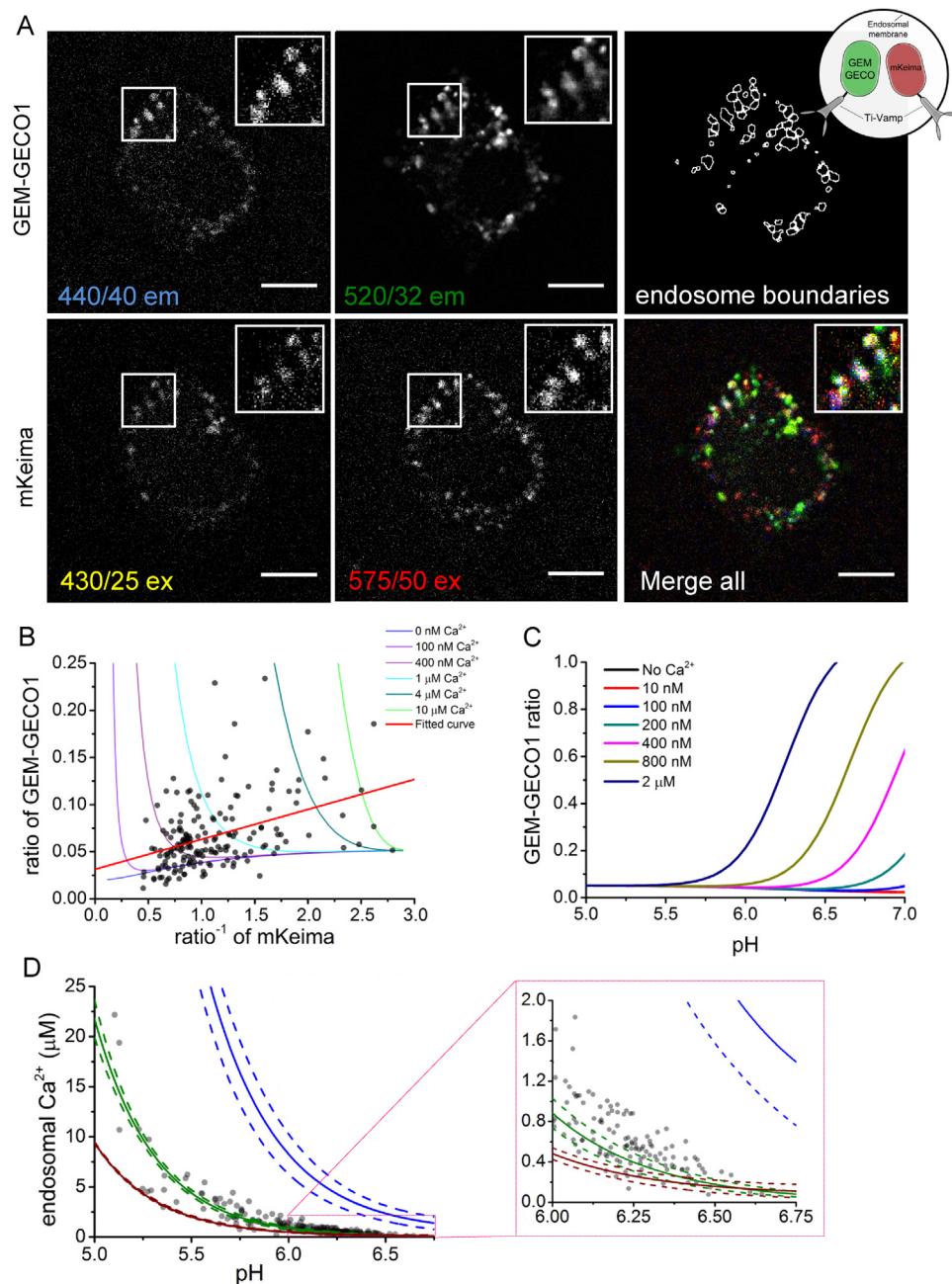


Fig. 5. Correlation between endosomal pH and Ca^{2+} . (A) Simultaneous imaging of mKeima and GEM-GECO1 targeted to the same population of endosomes. The merge panel shows the combined merge of 2 ratios (mKeima and GEM-GECO1) according to the 4 colors shown at the bottom of each panel. Inset is a schematic illustration of specific targeting of GEM-GECO1 and mKeima to the endosomal lumen for quantitative Ca^{2+} and pH measurement *in situ*. (B) Raw single endosomal mKeima and GEM-GECO1 fluorescence ratios (6 cells). (C) Theoretical change of GEM-GECO1 ratio at different pH values and given $[\text{Ca}^{2+}]$. (D) Data from (B) following conversion to pH and $[\text{Ca}^{2+}]$ based on *in vitro* calibration curves. Green line represents a fitted equation of the form $[\text{Ca}^{2+}]_{\text{free}} (\mu\text{M}) \approx 2 \times 10^{-6} \times 0.041^{\text{pH}}$, relating endosomal Ca^{2+} and pH ($R^2 = 0.833$). Red and blue lines indicate the upper and lower limit of quantification (LOQ), with dashed lines representing the 95% confidence band. Note that our fitted curve is close to the lower limit of quantification. The median endosomal $[\text{Ca}^{2+}]$ was estimated to be $\sim 0.9 \mu\text{M}$ and the average pH to be 6.05. Calculations are based on the analysis of 197 endosomes in 6 cells. Inset diagram shows enlarged area of the main diagram.

4. Discussion

The goal of the present study was to develop a pH-resistant Ca^{2+} biosensor to directly measure Ca^{2+} concentration in single endosomes and to determine whether endosomes play any role in pancreatic beta-cell Ca^{2+} homeostasis. To accomplish these goals, we paired the GEM-GECO1 fluorescent Ca^{2+} probe with the pH-sensitive mKeima fluorescent protein, and targeted both proteins to the luminal side of a defined sub-population of endosomes. Our

semi-quantitative estimations suggest that Ca^{2+} levels within the majority of endosomes are below $2 \mu\text{M}$, in the range of cytoplasmic Ca^{2+} levels observed in physiologically stimulated beta-cells, and orders of magnitude lower than what has previously been suggested from experiments using dyes taken up into endosomal compartments that were not molecularly defined [38]. We found endosomal Ca^{2+} was higher in more acidic Rab7-positive late endosomes when compared with Rab5a-positive early endosomes. Our results also identify Rab5a-positive early endosomes as an organelle

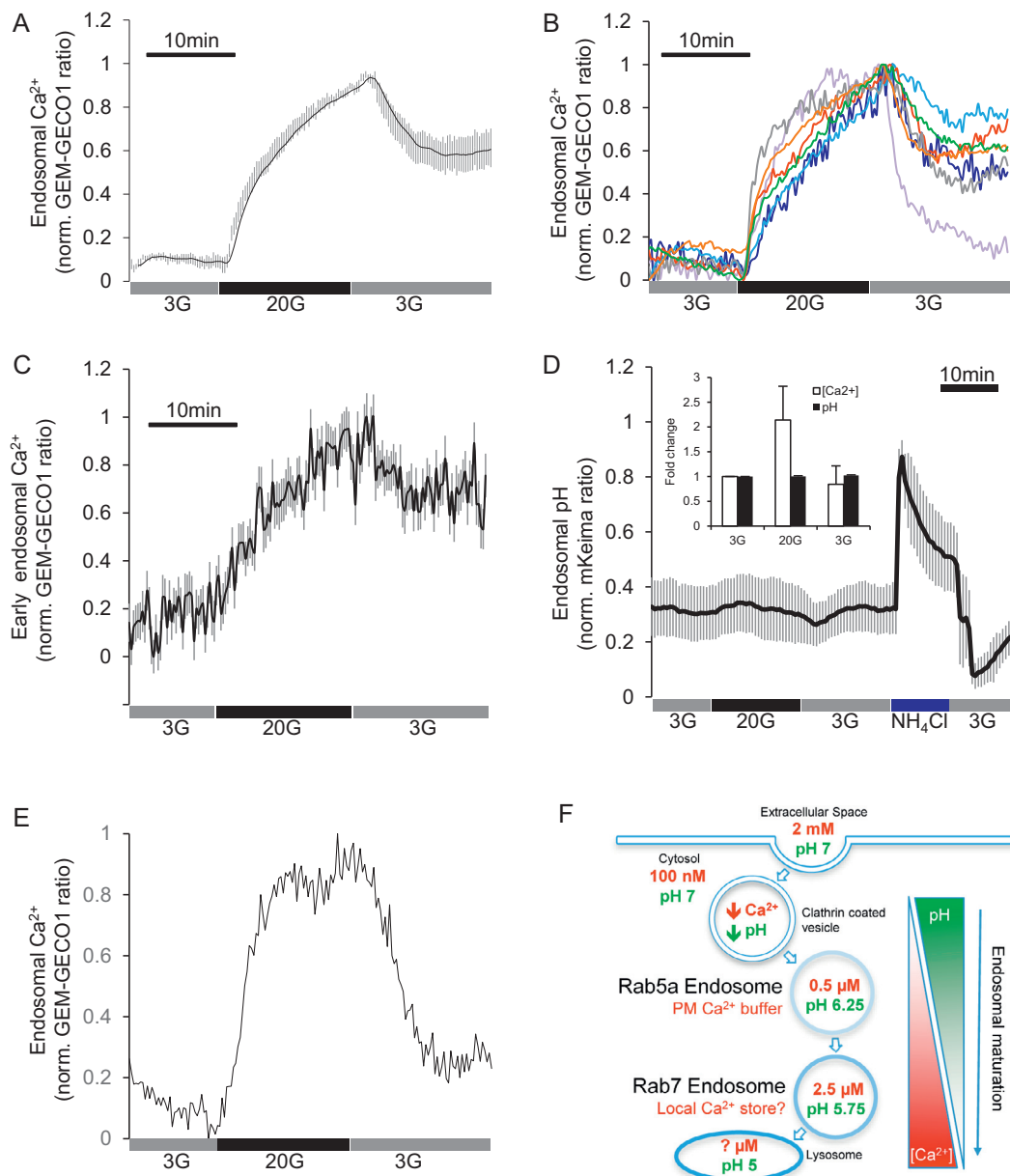


Fig. 6. Early endosomes enrich Ca^{2+} in glucose-stimulated beta-cells. (A, B) Average and individual whole-cell endosomal Ca^{2+} content in response to glucose ($n=8$). (C) Early, Rab5a-positive endosomes were analyzed for their relative Ca^{2+} content in response to glucose. (D) Average whole-cell endosomal pH in response to glucose. 20 mM NH_4Cl was perfused as a positive control for mKeima ($n=4$). (D, inset) Relation between endosomal pH and calcium content in the glucose response of a beta-cell ($n=3$). Error bars represent SEM. (E) Average whole-cell endosomal Ca^{2+} content in response to glucose in a human pancreatic beta-cell. (F) Working model of endosomal acidification and luminal Ca^{2+} accumulation during organelle maturation. Measurements are only available for vesicles containing TiVAMP, Rab5a or Rab7.

compartment that can actively enrich Ca^{2+} in glucose-stimulated beta-cells, demonstrating a previously unappreciated role for these organelles in intracellular Ca^{2+} handling in pancreatic beta-cells.

Specific and quantitative data describing the luminal Ca^{2+} concentrations within the endolysosomal organelle system has been hampered by a lack of appropriate molecular tools. Early pioneering work by Gerasimenko and colleagues relied on Oregon Green488 BAPTA-5 N taken up into cells from the extracellular media, to estimate a Ca^{2+} concentration of $\sim 28 \mu\text{M}$ in 'early' endosomes (defined as those imaged within 3 min after endocytosis). As the endosomes matured, the Ca^{2+} was seen to drop to $8.5 \mu\text{M}$ 5 min after endocytosis, and then $3 \mu\text{M}$ 20 min after endocytosis [38]. On the other hand, Christensen et al. reported Ca^{2+} levels of 400–600 μM in lysosome-like structures loaded with FFP18-AM, a dye reported to label cell membranes [33]. Previous work has addressed Ca^{2+} release from

isolated, artificially enlarged endolysosomal organelles [39,40], but whether this system approximates the situation in an intact cell remains unclear. The apparent lack of consensus between all of the described studies addressing the homeostasis of luminal endosomal Ca^{2+} in intact cells clearly highlights the requirement for new biological tools that are able to specifically quantify endosomal Ca^{2+} in living, fully functional cells. In the present study, we estimated Ca^{2+} and pH within a molecularly defined sub-population of endosomes in living cells for the first time using genetically encoded biosensors.

One drawback of our genetically encoded protein-based Ca^{2+} biosensor is that it was apparently unable to capture luminal Ca^{2+} fluxes immediately after the initial moment of endosome internalization, when Ca^{2+} would be equivalent to that in the bulk extracellular space. Our TiVAMP-targeted biosensor was unable to

capture this event, presumably due to the time required to recruit sufficient biosensor proteins to these nascent endosomes and/or due to the potential saturation of the Ca^{2+} sensor at extremely high Ca^{2+} concentrations. This property of our sensor contributes to an estimated average Ca^{2+} concentration in our measured sub-population of endosomes that is lower than that previously proposed for endosomes including the Ca^{2+} enriched nascent endosomes which are not included in our analysis. Approaches wherein Ca^{2+} sensitive dyes are internalized directly from the extracellular space would be expected to capture this event and its immediate sequelae, so it is not surprising that those methods estimated high Ca^{2+} .

We demonstrated that our biosensor pair of TiVAMP–GEM–GECO1 and TiVAMP–mKeima can be used simultaneously to quantify the pH and the absolute Ca^{2+} concentration in single endosomes. Control experiments demonstrated that TiVAMP–GEM–GECO1 responds primarily to Ca^{2+} and only to pH to a lesser degree. Using this biosensor pair, we identified a remarkable heterogeneity of endosomal Ca^{2+} content in beta-cells. We determined that this heterogeneity of endosomal Ca^{2+} is associated with organelle maturation and acidification. Specifically, later endosomes with lower luminal pH have higher endosomal Ca^{2+} concentrations (Fig. 6F). Interestingly, a correlation between Ca^{2+} and pH in endocytic vesicles mediated by a pH-sensitive Ca^{2+} channel has been suggested [41]. It was further shown by others that a disruption of endosomal Ca^{2+} homeostasis leads to a disruption of the endolysosomal transport system, supporting the concept of Ca^{2+} as a central regulator in membrane fusion and endosome acidification [41]. Together with work from other groups, our data suggest a strong interrelationship of Ca^{2+} and pH within the endolysosomal system [33], but further work is needed to firmly establish the causal relationship between Ca^{2+} flux and pH in these organelle lumina.

Live-cell, intra-organelle Ca^{2+} imaging is a powerful approach to understanding the fundamental biology of endosomes and other organelles [4]. The GEM–GECO1 probe has been extensively tested *in vitro* where it exhibits robust ratiometric Ca^{2+} sensing, with sufficient dynamic range and relative pH insensitivity [16]. GEM–GECO1 is significantly smaller than previous biosensors based on Ca^{2+} -dependent FRET between two fluorescent proteins. We propose that the combined use of endosome-targeted GEM–GECO1 and mKeima marks a significant improvement over alternate approaches. Together with this previous work [26], our data demonstrate that linking GEM–GECO1 to TiVAMP permits high localization specificity, to an extent that is not possible with dye-based approaches [42].

The imaging approach described in this work attempts to achieve the very challenging goal of simultaneously quantifying both endosomal pH and Ca^{2+} using the most appropriate combination of spectrally distinct genetically encoded sensors currently available. Relative to the use of dye-based indicators, genetically encoded biosensors have the advantage of being less invasive and also enabling the targeting of organelles with molecular specificity (i.e., Rab5a vs. Rab7 endosomes). However, the imaging approach used in this work also has a number of limitations that place constraints on the accuracy, temporal resolution, and the lower limit of quantification that can be achieved. A major challenge of this work is accounting for the fact that the GEM–GECO1 Ca^{2+} indicator has both a fluorescence response and a Ca^{2+} affinity that is still somewhat pH dependent. To correct for these dependencies, we projected an *in vitro* calibration onto a dataset of cellular measurements. This procedure required multiple assumptions – the most important of which was the assumption that the *in vitro* K_d is maintained in cells. It is not known whether our probe would have identical properties in an *in situ* calibration. Another challenge was related to the fact that individual endosomes are small structures that have relatively low signal-to-noise for single

measurements, and the fact that cellular autofluorescence at the wavelengths used for imaging was substantial and could only be corrected using a sophisticated local background subtraction technique. With respect to temporal resolution, our ratiometric sensor pair requires the acquisition of 4 fluorescence emission channels, and so our ability to image rapid endosomal Ca^{2+} and pH fluxes is limited by the exposure times and sensitivity of the imaging system. Taking these caveats into consideration, we are more confident about the upper range of our estimates of endosomal Ca^{2+} concentration than we are of the lower end of the range. However, we note that our measurements of endosomal Ca^{2+} and pH do fit within a range of concentrations proposed in previous studies [33,38]. We anticipate that combined use of GEM–GECO1 and mKeima will prove useful for simultaneous semi-quantitative measurements of Ca^{2+} and pH in the lumina of other organelles. For example, it should be feasible to link GEM–GECO1 and mKeima to SNARE proteins of the exocytotic machinery to study pH and Ca^{2+} dynamics within secretory granules, possibly providing new insight into the role of luminal Ca^{2+} in exocytotic events [43,44].

Our results provide an improved understanding of dynamic Ca^{2+} homeostasis in beta-cells and, as such, take a step toward further elucidating the physiological control of insulin secretion and other Ca^{2+} -dependent processes in this key endocrine cell type [2,6,32,45]. In response to elevated extracellular glucose levels, cytoplasmic Ca^{2+} levels increase to drive the docking and fusion of secretory insulin granules with the plasma membrane of the beta cell [35]. Interestingly, alterations in beta-cell Ca^{2+} homeostasis have been implicated in the development of type 2 diabetes [46]. Specifically, it has been proposed that excessive Ca^{2+} influx leads to an increased beta-cell death by apoptosis, a phenomenon associated with diabetes [47]. In this context, we previously speculated that endosomes might act as Ca^{2+} buffers in beta-cells responding to high glucose [37]. In the present work, we provided experimental data that are consistent with this model.

The degree to which endosomes contribute to the total Ca^{2+} buffering ability of intracellular organelles remains to be elucidated. Endosomes occupy a small volume of many cell types (0.65–2%), but this may be higher in beta-cells. We speculate that endosomes may play a role as physiologically relevant local Ca^{2+} buffers only near the plasma membrane, shaping Ca^{2+} signals that originate in close proximity. Unlike larger Ca^{2+} -handling organelles such as mitochondria (3.9% of the total beta-cell volume) or ER (20% of the total beta-cell volume) [48–50], endosomes may not play a primary role in shaping Ca^{2+} signals originating from within the cell. Our novel endosomal Ca^{2+} biosensor promises to shed light on the mechanisms involved in endosomal Ca^{2+} homeostasis in intact living cells and resolve current controversies around the nature of this important organelle [39,40,51].

Author contributions

Tobias Albrecht, Yongxin Zhao and Trang Hai Nguyen performed experiments. Tobias Albrecht, Yongxin Zhao, Robert E. Campbell and James D. Johnson designed experiments, analyzed data and wrote the manuscript. James D. Johnson is the guarantor of this work.

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