



Design and fabrication of field-deployable microbial biosensing devices

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Biosensors could enable a wide range of applications in environmental monitoring, pathogen detection, and biomarker diagnostics. While conventional diagnostic platforms like chemical sensors and PCR-based assays are capable of highly sensitive detection in laboratory conditions, their configurations, production cost, and operational requirements are not suitable for applications beyond the laboratory. Recent advances in synthetic biology, bioelectronics, and materials sciences have paved the way for the creation of novel microbial biosensing devices, which integrate core synthetic biosensors with state-of-the-art deployment platforms to create unique biosensor products. Here, we review the latest developments in microbial biosensing devices and discuss challenges and perspectives towards realizing their broad applications in real-world settings.

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Current Opinion in Biotechnology 2022, 76:102731

This review comes from a themed issue on **Analytical Biotechnology**

Edited by **Peng Xu** and **Kang Zhou**

For complete overview of the section, please refer to the article collection, "[Analytical Biotechnology](#)"

Available online 12th May 2022

<https://doi.org/10.1016/j.copbio.2022.102731>

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Introduction

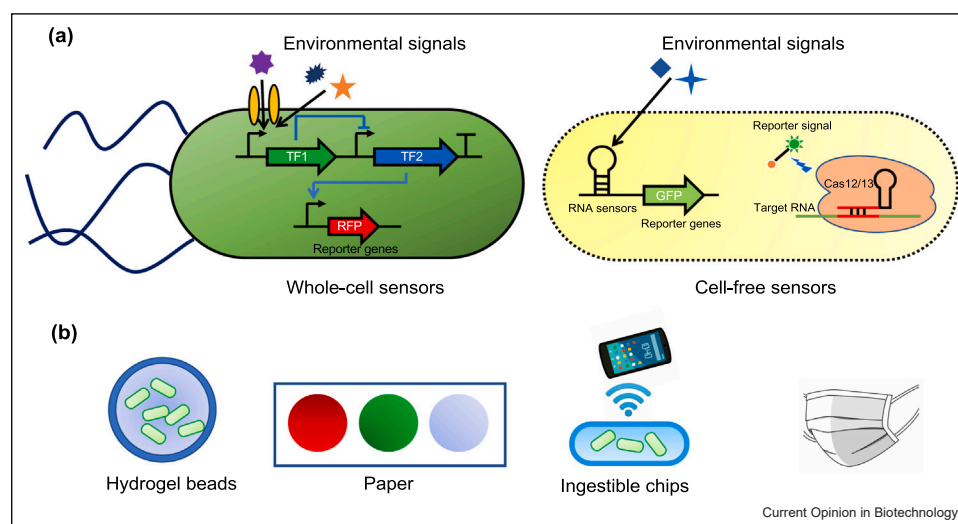
Microbes possess a rich repertoire of genetic elements responsible for sensing in diverse ecological niches, making them attractive resources for biosensor

development. In the last two decades, significant knowledge has been established in employing microbial cells and their biological components to design and construct high-performance whole-cell sensors (WCSs) and cell-free sensors (CFSs) that can detect a wide range of chemicals [1,2]. WCSs operate as living cells that generate detectable outputs upon their exposure to target chemicals. WCSs are amenable to large-scale production at a low cost by taking advantage of rapid growth and existing cultivation technologies [3,4]. However, challenges associated with their biohazard risks and requirement for viability maintenance need to be resolved to expedite the use of WCSs for practical applications. Meanwhile, CFSs are nonliving mixtures containing bioactive components that enable target detection and output generation. By removing the physical constraints of cell membranes, CFSs could facilitate the detection of cytotoxic targets, while reducing detection time and bypassing the need for live-cell maintenance and containment. Current efforts for CFSs development focus on expanding sensing targets, improving batch-to-batch consistency, and optimizing reaction costs to enable large-scale manufacturing [5,6]. Most WCSs and CFSs reported in recent years have shown promising performance in the laboratory but have yet to be broadly adapted in real-world diagnostic applications. One key challenge is to fabricate these sensors into shelf-stable products for containment, distribution, storage, transport, and utilization. There has been a strong emphasis on integrating high-performance synthetic biosensors with various deployment technologies to mitigate bio-hazards, facilitate rapid sampling, and enable data analysis beyond the laboratory. In this review, we discuss recent development, challenges, and perspectives of these innovative biosensing devices for applications even outside typical laboratory settings, specifically in environmental monitoring, pathogen detection, and biomarker diagnostics (Figure 1).

Design and fabrication of biosensing devices for environmental monitoring

The capacity to continuously monitor hazardous chemicals such as heavy metals, toxins, and antibiotics in food and water supply is essential for public healthcare. Accordingly, there has been steady growth in the number of WCSs-based biosensing devices developed for environmental monitoring. For example, Wan et al.

Figure 1



Design and fabrication of microbial biosensing devices for applications beyond the laboratory. **(a)** Strategies for microbial biosensor design. Whole-cell sensors can be designed from engineered intracellular transcription factors, two-component systems, RNA-based regulatory elements, or a combination of these biological tools to enable the biosensing of a wide range of chemical targets. Cell-free sensors can be designed from RNA parts or CRISPR-Cas complexes to enable the biosensing of chemicals or nucleic acids from viral targets. **(b)** Platform technologies for deploying whole-cell and cell-free sensors in various applications. Hydrogel beads are stringent biocontainment platforms that deploy live cells for environmental sensing applications. Paper is used to provide a lightweight, flexible, and stable platform for freeze-dried sensors that can be re-activated at the point of use. Ingestible chips provide versatile electronic interfaces for transmitting biological signals detected by live bacterial sensors to handheld devices, enabling their deployment in biological or environmental niches inaccessible via traditional sensing. Wearable biosensors provide real-time monitoring of biomarkers excreted by human users. RFP, red fluorescent protein; GFP, green fluorescent protein; TF, transcription factor.

successfully engineered *Escherichia coli* (*E. coli*) cells into highly sensitive WCSs capable of reporting the presence of arsenic (0.3 part-per-billion (ppb)) and mercury (2 ppb) in groundwater samples [7•]. Notably, their genetic design featured a core modular signal-amplification cascade based on an intracellular receptor (*hrpR*) and an activator (*hrpS*), which could be used to fine-tune similar transcription factor-based WCSs. They further fabricated a microbial sensor array based on the agarose hydrogel entrapment and microfluidic encapsulation of sensing cells, which could generate fluorescence signals detectable by a smartphone camera after 24-hour exposure to groundwater samples containing arsenic. However, the array's response time is relatively long, and its reproducibility after long-term storage is uncertain. Therefore, further characterization and optimization are required for such a prototype device before field deployment. In another study, Lopreside et al. engineered and deployed mercury-sensing *E. coli* strains, alongside other components as controls, on disposable paper to fabricate a three-leaf biosensor—enabling the smartphone-based analysis of mercury in water samples within 2 hours [8]. On the other hand, Liu et al. focused on detecting mercury from soil samples. They engineered mercury-sensing *E. coli* cells to produce ethylene (C_2H_4) gas as an output, which in turn, can be analyzed by a handheld C_2H_4 reader [9]. The use of a gas reporter overcame the limitations associated with

using conventional fluorescence reporters in opaque samples, such as soil-containing samples. Besides monitoring hazards in the water supply, the Belkin group developed WCSs-based sensing devices for the remote monitoring of explosives in landmines to mitigate humanitarian risks. They first engineered *E. coli* cells to detect and emit fluorescent signals in response to explosives such as 2,4,6-trinitrotoluene and its degradation product, 2,4-dinitrotoluene [10,11]. These sensing strains were then encased into alginate beads to enable trace amounts of such explosives to diffuse while maintaining cell viability within a short operational period. By combining bead-encapsulated cells with a laser-based optoelectronic system, they successfully created a system that allowed for the remote monitoring of antipersonnel mines in a field trial [12••]. Recently, they further optimized the system to make it more amenable for use beyond the laboratory, such as changing the fluorescence-based reporter to one based on bioluminescence, modifying the encapsulation matrix, and redesigning the optoelectronic circuit [13,14]. While WCSs have shown promising sensing performance, concerns regarding the escape risk of these genetically modified organisms into the environment still hinder their applications. Tang et al. tackled this issue by developing a deployable physical containment strategy (DEPCOS) that mitigates the escape risk for WCSs-based biosensing devices. The tough core-shell

hydrogel design of DEPCOS provides stringent containment of the engineered cells and their DNA, while still allowing the diffusion of nutrients and chemicals for cell survival and sensing functions [15••]. Regardless, the long-term sensing capacity and viability of the encapsulated cells require further investigation.

The development of CFSs-based biosensing devices for environmental monitoring is also accelerating. Typically, CFSs can be lyophilized on paper or in test tubes, and functionally rehydrated at the point of use, reducing the need for sophisticated fabrication methods. Transcription factors and RNA-based elements that are functionally stable in *in vitro* environment have been extensively exploited to develop CFSs. Such CFSs can detect essential chemical contaminants, such as arsenite, fluoride, cadmium, and cyanuric acid [16–20]. Jung *et al.* recently developed a CFS platform named RNA Output Sensors Activated by Ligand Induction (ROSALIND), using allosteric transcription factors (aTFs) as the key biosensing elements to control the phage polymerase-driven transcription of fluorescence-activating RNA aptamers output in response to the presence of target chemicals. ROSALIND can detect a wide range of water contaminants, including macrolides and heavy metal ions [21••,22]. Given the availability of diverse aTFs in nature, ROSALIND could be employed to develop a wide range of new CFSs for detecting other target compounds in the future.

Design and fabrication of biosensing devices for pathogen detection

Pathogens pose both immediate and long-term risks to human health. Pathogen outbreaks such as the COVID-19 pandemic could significantly impact the global population, reinforcing the need to develop diagnostic devices as potential countermeasures. In the past years, synthetic biology has seen tremendous efforts in the development of sensitive, low-cost, and user-friendly microbial biosensing devices that can rapidly detect pathogens with minimal equipment. For instance, microbial cells could be engineered to detect signature analytes that indicate the presence of target pathogens in clinical samples. These analytes include cholera autoinducer-1 from *Vibrio cholerae*, auto-inducer I from *Staphylococcus aureus*, and hydroxyphenylacetic acid from *Candida albicans* [23–25]. Recently, Wu *et al.* engineered *E. coli* cells to detect N-acylhomoserine lactone to sense and report the presence of *Pseudomonas aeruginosa* and *Burkholderia pseudomallei*. The sensing cells were immobilized on paper to create a device, enabling the production of lycopene as a visualizable output after exposure to the filtered culture of target pathogens for 8 hours [26]. By detecting analytes, WCSs do not require steps like sample preparation and nucleic acid amplification as compared to PCR assays or nucleic acid-based CFSs for pathogen detection, greatly simplifying the sensing workflow. However, cell growth

must be improved, and signal-generating time must be shortened to enhance WCSs' competitiveness for pathogen diagnostics.

CFSs-based pathogen sensors primarily focus on nucleic acid-based detection, taking advantage of the understanding that pathogens and their mutants could be identified and differentiated through their unique genetic sequences. Pardee *et al.* demonstrated the feasibility of designing toehold switches that recognize mRNA sequences unique to Ebola and Zika viruses at a femtomolar level and correspondingly trigger transcriptional events to produce outputs in paper-embedded cell-free mixtures [27•,28]. Building on this approach, Takahashi *et al.* developed CFSs capable of recognizing and distinguishing gut bacteria based on their 16S ribosomal RNA signatures, enabling the ultrasensitive identification of high toxin-producing *Clostridium difficile* in complex stool samples [29]. Recently, many studies have exploited the CRISPR-Cas system's programmable DNA recognition and cleavage activities to create a wide range of highly sensitive nucleic acid sensors for pathogen detection [30,31]. Gootenberg *et al.* created the first Specific High-Sensitivity Enzymatic Reporter UnLOCKing (SHERLOCK) platform, which utilizes the Cas13a protein to recognize target RNA sequences. The Cas13a protein exhibits collateral activity that triggers the cleavage of quenched fluorescent RNA reporters to release output signals [32••]. Intriguingly, SHERLOCK allows for the attomole-level detection and differentiation of targets with a single-base-pair resolution. Subsequently, they created SHERLOCK version 2 (SHERLOCKv2), which synergistically combined Cas13 and its associated enzyme Csm6 for signal amplification. SHERLOCK v2 enabled the sensitive detection of single-stranded DNA from dengue or Zika virus and their mutations in patient liquid biopsy samples [33]. During the COVID-19 pandemic, SHERLOCK promoted the rapid development of a series of innovative biosensing devices for SARS-CoV-2 detection. For example, Arizti-Sanz *et al.* developed the Streamlined Highlighting of Infections to Navigate Epidemics (SHINE), an optimized SHERLOCK-based assay for the rapid detection of SARS-CoV-2 RNA from unextracted samples [34••]. SHINE employed heating unextracted diagnostic samples to obliterate nucleases to rapidly inactivate nucleases and lyse viral particles, followed by single-step RNA amplification and Cas13-based detection. By incorporating a smartphone-friendly in-tube fluorescence readout procedure, SHINE enabled rapid detection (1 hour) without human exposure to pathogenic samples [34••,35]. Furthermore, Welch *et al.* deployed SHERLOCK-based sensors on a microfluidic device to create mCARMEN, enabling the high-throughput surveillance of a virus panel, including SARS-CoV-2 variants Delta and Omicron [36]. Interestingly, Nguyen *et al.* creatively fabricated a paper-based facemask embedded with the SHERLOCK sensors to enable the real-time

detection of SARS-CoV-2 particles resulting from the wearer's respiration [37•]. Chen et al. also developed a DNA endonuclease-targeted CRISPR trans reporter (DETECR) to detect viral DNA in human samples at the attomolar level. In contrast to SHERLOCK, DETECR exploits a Cas12a enzyme that collaterally cleaves fluorescent-quenched single-stranded DNA reporter molecules upon the detection of target DNA sequences [38•]. Building on DETECR, Boughton et al. developed an immunoassay to detect SARS-CoV-2 at a clinically relevant level in respiratory swab specimens within 1 hour [39••].

Design and fabrication of biosensing devices for biomarker diagnostics

Microbial sensors could enable a wide range of biomarker sensing applications both *in vitro* and *in vivo*. For instance, Chang et al. developed a unique synthetic receptor platform known as Engineered Modularized Receptors Activated via Ligand-induced Dimerization (EMERALD), which allows diverse ligand-binding domains to be fused to a synthetic receptor scaffold derived from *E. coli*. The developed sensors can detect pathological bile salts as biomarkers in human serum samples with high sensitivity and specificity within 2 hours [40,41••]. Meanwhile, McNerney et al. harnessed zinc-responsive transcription elements and isopropyl β -D-1-thiogalactopyranoside-inducible elements in *E. coli* to create two-input zinc-sensing WCSs that could generate colored pigments in response to zinc at different concentrations [42•]. The authors further demonstrated that the sensing cells could maintain robust performance upon lyophilization and rehydrating in human serum samples, enabling the quantification of zinc concentration at the point of use in 12 hours. At the same time, microbial sensors and microbial sensing devices offer the unique capacity to monitor biomarkers in hard-to-access body niches, including the gastrointestinal (GI) tract. Early works in the field have demonstrated how engineered cells could be deployed as live diagnostics that could eventually become a stable member of the human microbiome and report relevant biomarkers present in the GI tract, such as tetrathionate and nitrate [43–45]. Chien et al. recently introduced a multiplex biosensing capacity into probiotic cells, enabling the simultaneous detection of signals like pH, lactate, and oxygen [46•]. Such a platform could someday be useful for programming cells to localize and deliver drugs at desired niches in the GI tract. Another notable work comes from Mimeo et al., whose team created a unique miniaturized ingestible micro-bio-electronic device (IMBED) which embedded core bacteria sensors with an ingestible electronic chip. IMBED can transmit wireless signals from the mammalian gut upon exposure to heme at elevated concentrations, allowing the standoff monitoring of insults to internal organs [47••]. By offering a

unique solution for both biocontainment and remote detection, IMBED could inspire many novel *in vivo* biosensing applications in the future.

Conclusions, challenges, and perspectives of microbial biosensing devices

As highlighted in this review, microbial biosensing devices have the potential to enable a wide range of novel biosensing applications. Given the increasing number of microbial biosensing devices in development, the emergence of their commercial products is imminent. However, there are several key challenges that should be addressed in future developments to satisfy regulatory and large-scale production requirements.

Whole-cell sensors-based biosensing devices

Synthetic biologists have established a solid foundation for the design and optimization of WCSs performance. Nonetheless, the number of field-deployable WCSs-based devices remains limited due to modest target diversity and biocontainment issues. To expand target diversity, focus should remain on genomic mining to discover novel biosensing elements capable of detecting diverse molecules. In addition, rational redesign and directed evolution approaches could be wielded to alter the biochemistries of existing biosensing scaffolds to detect noncognate molecules, as exemplified by the development of EMERALD. With regards to biocontainment, continued innovations in new deployment platforms, such as DEPCOS and IMBED, are essential in creating WCSs-based biosensing products that pose minimal biohazard risks. On the other hand, auxotrophic strains can also provide another layer of biocontainment [48]. We opine that the development of these strains into high-performance WCSs, combined with their integration into compatible deployment platforms, would lead to a wide range of novel WCSs-based sensing devices that fulfill stringent regulatory requirements.

Cell-free sensors-based biosensing devices

Compared with WCSs, CFSs are arguably friendlier for regulatory approval and are more amenable for rapid development in response to urgent diagnostic needs. However, it is challenging to maintain performance consistency while reducing manufacturing costs of CFSs. The output of CFSs could vary between production batches, sampling, and detection instruments at point of use, and among human operators [49]. As the field evolves, the establishment of standardized practices would help reduce the variability of these contributing factors. Currently, the estimated cost of cell-free reaction is US\$5/mL, which might hinder their large-scale manufacturing. Optimizing active ingredients, such as finding replacements for expensive energy substrates and cofactors, could help eventually bring down the manufacturing cost to less than US\$1/mL [6].

Furthermore, new approaches for developing cell-free reactions from the lysates of diverse microbial strains other than *E. coli* could lead to the discovery of novel biosensing mechanisms, which could facilitate the detection of novel chemical targets in the future.

CRedit authorship contribution statement

HLP wrote the manuscript. HL and MWC commented and edited the manuscript. All authors have read and agreed to the published version of the manuscript.

Conflict of interest statement

The authors declare that there are no commercial or financial relationships that could be construed as a potential conflict of interest.

Acknowledgements

We gratefully acknowledge the financial supports from NUS Medicine Synthetic Biology Translational Research Programme (NUHSRO/2020/077/MS/02/SB), the Summit Research Programme of the National University Health System (NUHSRO/2016/053/SRP/05), the Synthetic Biology Initiative of the National University of Singapore (DPRT/943/09/14), the Synthetic Biology R&D Programme of the National Research Foundation of Singapore (SBP-P2, SBP-P7, SBP-P9), the Industry Alignment Fund-Industry Collaboration Project of the Agency for Science, Technology and Research (A*STAR) of Singapore (ICP1600012, I2001E0068), the United States Army (ARO/2019/74459LS), and the Ministry of Education of Singapore (MOE/2014/T2/2/128, and NUHSRO/2020/046/T1/3). We thank Kamila Isabelle Alabado Navarro for the comments made to the manuscript.

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