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**Peroxidase mimetic activity of Fe₃O₄ nanoparticle prepared
based on magnetic hydrogels for hydrogen peroxide and
glucose detection**

Shasha Song,^{*a} Yang Liu,^a Aixin Song,^b Zengdian Zhao,^a Hongsheng Lu^c and
Jingcheng Hao^b

^aSchool of Chemical Engineering, Shandong University of Technology, Zibo, 255000,
P. R. China

^bKey Laboratory of Colloid and Interface Chemistry & Key Laboratory of Special
Aggregated Materials, Shandong University, Ministry of Education, Jinan, 250100, P.
R. China

^cOil & Gas Field Applied Chemistry Key Laboratory of Sichuan Province, Southwest
Petroleum University, Chengdu, 610500, P. R. China

* To whom correspondence should be addressed.

S.S., e-mail: songshasha@sdut.edu.cn.

ABSTRACT: Stimuli-response magnetic hydrogels were prepared in the mixtures of magnetic surfactants, (C_n TAFB(C), $n = 12, 14, 16$), and chiral amphiphiles, sodium cholate (SC). The gelation behavior of C_n TAFB(C)/SC were studied in detail. The results proved that the hydrophobicity of surfactants and the hydration radius (R_h) of anions played a vital role in the gelation process. The microstructure of the hydrogels were determined to be three-dimensional network of fibrous aggregates. The formation of the hydrogel fibrils was considered to be mainly driven by a delicate balance of multiple non-covalent interactions including hydrophobic interaction, electrostatic interaction, hydrogen bonding, van der Waals force, and the steric effect of SC molecule. Rheological measurements demonstrated that the hydrogels are high mechanical strength materials (the yield stress exceeding 2000 Pa). The mechanical strength of the hydrogels is dependent on the fiber density, which can be regulated by changing the proportion of the two compounds, the total concentration and the chain length of the surfactants. The magnetic hydrogels of C_{12} TAFB/SC mixtures served as the precursors for preparing cubic Fe_3O_4 nanoparticles with the diameter of 7.2 nm. The as-prepared Fe_3O_4 nanoparticles exhibit excellent ferromagnetic characteristic and high peroxidase-like activity and can be used as biosensor for hydrogen peroxide (H_2O_2) and glucose detection. We developed a convenient and green method for preparing Fe_3O_4 nanoparticles, which can be used as a promising candidate biosensor for glucose detection.

KEYWORDS: *hydrogels, biosensor, peroxidase mimetic activity, Fe_3O_4 nanoparticles, glucose detection*

1. Introduction

Gels are commonplace household materials, which have permeated our daily life in various kinds of forms such as hair gel, shampoo, toothpaste, and other cosmetic [1]. Among various gels, hydrogels formed by functional surfactant molecules aroused tremendous interest, owing to their potential applications in the fields of biology, material, environment and biomedicine science. The main driving forces for the formation of surfactant hydrogels are noncovalent interactions (including hydrogen bonding, hydrophobic interaction, electrostatic interaction, π - π interaction, etc.) [2-8]. The weak and reversible nature of the non-covalent interactions endow the surfactant hydrogels respond to external stimulus, such as temperature, pH, light, and redox reactions [2,9]. Moreover, surfactant hydrogels are green soft materials, composed of large amounts of water (> 95 wt%) and small part of organic species, which can be used to imitate the physical properties of soft tissues (such as cartilage, muscle, and eyeball), and can be applied to diapers, contact lenses, and drug reservoirs [10]. Nowadays, one of the challenge for surfactant hydrogels is the design of novel surfactants with special functional groups for constructing hydrogels with fascinating structures to achieve functional applications [11].

The biocompatibility of hydrogels is crucial for biologically directed applications and environmental considerations [1]. Bile salts, the end product of the metabolism of cholesterol with several chiral centers and a rigid hydrophobic steroid nucleus, are produced by liver and stored in gallbladder [12-14]. The particular role and specific molecular structure render bile salts and its derivatives novel and abundant self-assembly behavior, which has been gradually investigated in recent decades [1,15]. The tubular structures as a thermal stable state were found in alkaline solutions of sodium or ammonium salts of lithocholic acid (LCA) [13,14,16-18]. In addition,

hydrogels were observed by mixing LCA with metal ions or organic amines [4,8,19,20].

Peroxidase activity is very important for many biochemical assays, due to their wide application in biomedical and environmental monitoring [21]. Currently, most of the peroxidase enzyme used for assays is horse radish peroxidase (HRP). Although HRP have high catalysis efficiency under very mild and friendly conditions, its applications is restricted due to its intrinsic properties such as sensitivity of catalytic activity to environmental condition and relatively low stability (denaturation and digestion) [22-24]. Therefore, tremendous efforts have been expended to construct enzyme mimetics [25,26,27]. Over the past few decades, a series of nanomaterials, such as graphene oxide (GO) [28], carbon nanotubes [29], carbon dots [30], bimetallic alloy nanostructures [31], nanoceria [32], FeS [33], and gold nanoparticles [34], have been found to exhibit unexpected peroxidase enzyme-like activity [35]. Among the nanomaterials, Fe₃O₄ magnetic nanoparticles (MNPs) have been considered as the most important peroxidase-like nanozyme and received the most attention, due to their high chemical stability, feasible surface modification, and excellent chemically and biologically inert [36,37]. However, the preparation of morphology controllable Fe₃O₄ MNPs is still a challenge. Current methods for fabricating morphology controllable Fe₃O₄ MNPs, including a hydrothermal process, solvothermal process and thermal decomposition [38,39], involve toxic sources (organic solvents) and rigorous conditions (e.g., a high reaction temperature, high pressure), preventing the large-scale production and widespread practical applications. Therefore, nontoxic, water-based approaches are urgently needed to prepare morphology controllable Fe₃O₄ MNPs.

Herein, we developed a convenient, water-based approach for the preparation of

Fe₃O₄ MNPs based on magnetic hydrogels to study their peroxidase mimetic activity and explore their applications in biocatalysis and biosensing. The magnetic hydrogels were obtained by mixing C_nTAFB and SC in water. The gelation behavior of C_nTAFB(C)/SC system demonstrated that the hydrophobicity of surfactant and hydration radius (R_h) of anions play crucial role in the gelation. The hydrogels were formed by fibrils with the uniform diameter of 30 nm. Rheological results demonstrated that the hydrogels are high mechanical strength materials, which can be regulated by changing the proportion of the two compounds, the total concentration and the hydrophobic chain length of surfactants. The hydrogels can serve as the precursors to prepare cubic Fe₃O₄ MNPs with the diameter of 7.2 nm. The as-prepared Fe₃O₄ MNPs exhibited excellent ferromagnetic property and higher catalytic activity, which can be used as biosensor for H₂O₂ and glucose detection.

2. Experimental section

2.1. Chemicals and materials

The cationic surfactant, CH₃(CH₂)_{n-2}CH₂N(CH₃)₃[FeCl₄]⁻ (C_nTAFB, n = 12, 14, and 16) and CH₃(CH₂)_{n-2}CH₂N(CH₃)₃[FeBrCl₃]⁻ (C_nTAFB, n = 12, 14, and 16), were synthesized according to the literature [40-42] by mixing equal molar amount of cationic surfactant, CH₃(CH₂)_{n-2}CH₂N(CH₃)₃Cl (C_nTAC, n = 12, 14, and 16) and CH₃(CH₂)_{n-2}CH₂N(CH₃)₃Br (C_nTAB, n = 12, 14, and 16), with iron trichloride (FeCl₃) in methanol and stirring overnight at room temperature. The solvent was then removed and the product dried at reduced pressure at 80 °C overnight yield brown/red solid. After the reaction, the Cl⁻ or Br⁻ can be converted to [FeCl₄]⁻ or [FeCl₃Br]⁻. C_nTAB (n= 12, 14, 16), FeCl₃, sodium hydroxide (NaOH), hydrogen peroxide (H₂O₂, 30 wt %), sodium acetate, and acetic acid were purchased from Sinopharm Chemical

Reagent Co. Ltd. (Shanghai, China). C_n TAC ($n = 12, 14, 16$), sodium cholate (SC, >98%), sodium deoxycholate (SDC, >98%), and glucose oxidase (GOx) were purchased from J&K Chemical Company, Ltd. (Beijing, China). Horseradish peroxidase (HRP) was purchased from Sigma–Aldrich. All the chemicals were used without further purification. Ultrapure water with a resistivity of $18.25 \text{ m}\Omega\cdot\text{cm}$ was obtained using a UPH-IV ultrapure water purifier (Chengdu Ultrapure Technology Co. Ltd., China).

2.2. Gelation behavior study

The samples were prepared by mixing appropriate amounts of SC (SDC or SLC) and C_n T AFC ($n = 12, 14, 16$) or C_n T AFB ($n = 12, 14, 16$) in water, and followed by stirring at 40°C . Then, the samples were equilibrated at $T = 25.0 \pm 0.1^\circ\text{C}$ for at least 4 weeks before the gelation behavior was inspected.

2.3. Methods and characterizations

For transmission electron microscopy (TEM) observation, small volume of gel sample was placed on TEM grids (copper grid, 3.02 mm, 200 meshes, coated with formvar film) and the excess sample was wiped away with a filter paper. The copper grids were frozen in a vacuum extractor at -55°C for several days. Then the copper grids were observed on a JEOL JEM-1400 TEM operating at 120 kV. The images were recorded on a Gatan multiscan CCD and processed with digital micrograph. Fe_3O_4 MNPs were observed through a JEOL JEM-2010 high-resolution TEM (Japan) at an acceleration voltage of 200 kV.

Rheological measurements were performed on a HAAKE RS6000 rheometer with a cone-plate system (C35/1° Ti L07116 at $25.0 \pm 0.1^\circ\text{C}$, diameter: 35 mm, cone angle: 1°). The viscoelastic properties of the hydrogels were determined by using oscillatory

measurements with an amplitude sweep in the frequency range of 0.01 to 10 Hz. Prior to the frequency sweep, the linear viscoelastic region was determined by stress-sweep measurements.

Phase transition temperature was obtained from DSC8500 (PerkinElmer, USA). The heating rate was set as $2.5\text{ }^{\circ}\text{C}\cdot\text{min}^{-1}$.

The XRD patterns were recorded using a Rigaku D/Max 2200-PC diffractometer with Cu K α radiation ($\lambda = 0.15418\text{ nm}$) and a graphite monochromator. The samples were measured at room temperature in the 2θ scan mode ($2.5^{\circ}\text{ min}^{-1}$).

The FT-IR spectra over the range of $4000 - 400\text{ cm}^{-1}$ were obtained on a VERTEX-70/70v FT-IR spectrometer (Bruker Optics, Germany) by taking 64 scans with a final resolution of 4 cm^{-1} . Spectral manipulation was performed by using the OPUS 6.5 software package (Bruker Optics, Germany). The sample was mixed with KBr and pressed into a plate for the measurements.

2.4. Fe_3O_4 magnetic nanoparticles (MNPs) preparation

As-prepared hydrogel was immersed in an aqueous solution of iron ions with a molar ratio of $[\text{Fe}^{2+}]/[\text{Fe}^{3+}] = 11:1$ for 12 h. The hydrogels loaded with iron ions were subsequently transferred into sodium hydroxide (NaOH) aqueous solution ($0.5\text{ mol}\cdot\text{L}^{-1}$) and kept at $50\text{ }^{\circ}\text{C}$ in water bath for 12 h, resulting in the precipitation of Fe_3O_4 MNPs.

2.5. Mimetic peroxidase activity assays

HRP-like activity was examined using TMB as a chromogenic substrate. Catalytic assays experiments were carried out using $50\text{ }\mu\text{g}\text{ Fe}_3\text{O}_4$ MNPs or 1 ng HRP in acetate buffer (8 mL , $0.2\text{ mol}\cdot\text{L}^{-1}$, $\text{pH} = 4.0$) in the presence of $530\text{ mmol}\cdot\text{L}^{-1}\text{ H}_2\text{O}_2$ for Fe_3O_4 MNPs and $8.8\text{ mmol}\cdot\text{L}^{-1}$ for HRP, using $816\text{ }\mu\text{mol}\cdot\text{L}^{-1}$ TMB as the substrate at $40\text{ }^{\circ}\text{C}$

for 1 h [27]. After the reactions, the color formation was monitored at 652 nm using a HITACHI-4100 spectrophotometer with the scan rate of $600 \text{ nm} \cdot \text{min}^{-1}$.

The reaction kinetics for the catalytic oxidation of TMB was carried out by recording the absorption spectra at 652 nm. The apparent kinetic parameters were calculated based on the Michaelis equation: $v = V_{\max} \times [S] / (K_m + [S])$ (1),

where v is the initial velocity, $V_{\max}$ is the maximal reaction velocity, $[S]$ is the concentration of substrate and K_m is the Michaelis constant. K_m and $V_{\max}$ were obtained by the Lineweaver-Burk plot method. To investigate the mechanism, assays were carried out under standard reaction conditions as described above by varying concentrations of TMB at a fixed concentration of H_2O_2 or vice versa.

2.6. H_2O_2 and glucose detection

H_2O_2 detection was performed using the Fe_3O_4 MNPs in substrate solution with various H_2O_2 concentrations ($0.01 \text{ } \mu\text{mol} \cdot \text{L}^{-1}$ – $1 \text{ mol} \cdot \text{L}^{-1}$). After the reactions, the substrate solutions were monitored at 652 nm using HITACHI-4100 spectrophotometer with the scan rate of $600 \text{ nm} \cdot \text{min}^{-1}$.

Glucose detection was performed as follows: (i) 0.1 mL GOx ($1 \text{ mg} \cdot \text{mL}^{-1}$) and 0.1 mL different concentrations of glucose in $10 \text{ mmol} \cdot \text{L}^{-1}$ acetate buffer ($\text{pH} = 7.0$) were incubated at 37°C for 30 min; (ii) 0.25 mL TMB ($1 \text{ mmol} \cdot \text{L}^{-1}$), 0.1 mL Fe_3O_4 MNPs ($175 \text{ mg} \cdot \text{L}^{-1}$), and 3.95 mL acetate buffer ($0.2 \text{ mol} \cdot \text{L}^{-1}$, $\text{pH} = 4.0$) were added into the glucose reaction solution; (iii) the mixture solution was incubated in 40°C water bath for 20 min, and the final reaction solution was used to perform the adsorption spectroscopy measurement at 652 nm. In control experiments, $10 \text{ mmol} \cdot \text{L}^{-1}$ maltose, $10 \text{ mmol} \cdot \text{L}^{-1}$ lactose, and $10 \text{ mmol} \cdot \text{L}^{-1}$ fructose were used instead of glucose, under conditions identical to those reported above.

3. Results and discussion

3.1. Gelation behavior

Magnetic hydrogels (the magnetic property of hydrogels was shown in Figure S1) was obtained by heating the mixtures of magnetic surfactant, $C_n\text{TAFB}(\text{C})$ ($n = 12, 14, 16$), and SC to 40 °C and cooling the mixtures to room temperature (R.T). In order to explore the influence of hydrophobicity of surfactant and hydration radius (R_h) of anions on the gelation, the gelation behavior of SC/ $C_n\text{TAFB}(\text{C})$ system was investigated in detail. The remarkable differences in gelation behaviors of the mixtures were listed in Table 1. From Table 1, one can see that the CGC and gelation time decrease with the increase in hydrophobic chain length of $C_n\text{TAFB}(\text{C})$, which is attributed to the increment of hydrophobic interaction facilitate the assembly of gelators to form gel [43,44]. The hydrophobic interaction in the mixtures can also be regulated by changing the number of hydroxyl in steroid nucleus of sodium salts of bile acid. As the number of hydroxyl group reduces, the hydrophobicity of gelator increases, causing the decrease of CGC. The gelation process is a balance between crystallization and solubilization, and the hydrogel is the results of a delicate balance between hydrophobicity and hydrophilicity [45,46]. Thus, SLC can not form hydrogel with $C_n\text{TAFB}(\text{C})$ due to the too high hydrophobicity, and only precipitates obtained. The hydration of anions also has a pronounced effect on the gelator assembly [47,48]. Cl^- is well hydrated anion, ascribed to kosmotrope, and Br^- is poorly hydrated anions, being referred as chaotropes [49]. Thus, $C_n\text{TAFB}$ was easier to aggregate to form gels with SC than $C_n\text{T AFC}$, presenting lower CGC and higher gelation ability. In the present work, we mainly focused on $C_n\text{TAFB}/\text{SC}$ system, and studied their gelation

properties and self-assembly process.

Table 1 Gelation behavior of C_n TAFB(C) and sodium salts of bile acid systems in aqueous solutions at 25 °C

	Chain length (nm) [50]	Aggregates			CGC ^a (wt %)			Gelation time			Gelation number ^b		
		SC	SDC	SLC	SC	SDC	SLC	SC	SDC	SLC	SC	SDC	SLC
C_{12} TAFB	1.672	G ^c	G	P ^d	0.329	0.282		48 h	96 h		7936	9259	
C_{12} TAFC	1.672	G	G	P	0.320	0.270		72 h	108 h		7407	8547	
C_{14} TAFB	1.925	G	G	P	0.249	0.224		36 h	48 h		11111	12345	
C_{14} TAFC	1.925	G	G	P	0.250	0.227		40 h	54 h		10101	11111	
C_{16} TAFB	2.178	G	G	P	0.211	0.184		30 h	36 h		13888	14873	
C_{16} TAFC	2.178	G	G	P	0.217	0.193		36 h	48 h		12345	13888	

^aCGC: critical gelation concentration; ^bGelation number: the maximum number of solvent molecules immobilized by gelator molecules [44]; ^cG: Gels; ^dP: precipitates.

Fig. 1 shows the phase diagram of C_n TAFB/SC system, which is certified by inverted tube observations. Hydrogels can form at the gelator concentration lower than 0.5 wt%, and the typical sample images are shown in Fig. 1. At a fixed SC concentration, phase transition from precipitates (P) to gels (G) then to P occurs with increasing amounts of C_n TAFB. With the addition of C_n TAFB, the hydrophobicity of the mixtures increases, weakening the gelation of the system and causing precipitates formation. As shown in Fig. 1, with an increase in hydrophobic chain length of C_n TAFB, the gel region decreases. C_n TAFC/SC system exhibits the same tendency (Fig. S2). For further detailed study, two series of sample were selected. One was at a fixed SC concentration of 50 mmol·L⁻¹ with different amounts of C_n TAFB, whereas another was at a fixed molar ratio of SC to C_n TAFB being 2:1 with various total surfactant concentrations. The rheological properties, self-assembly process and

stimuli-response properties of the gels were illustrated by C_{12} TAFB/SC system.

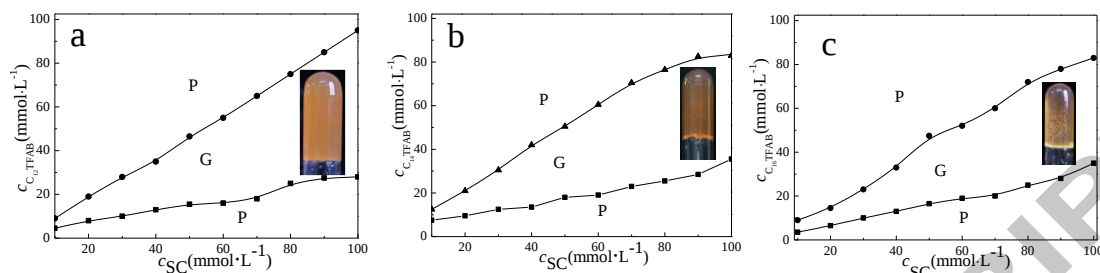


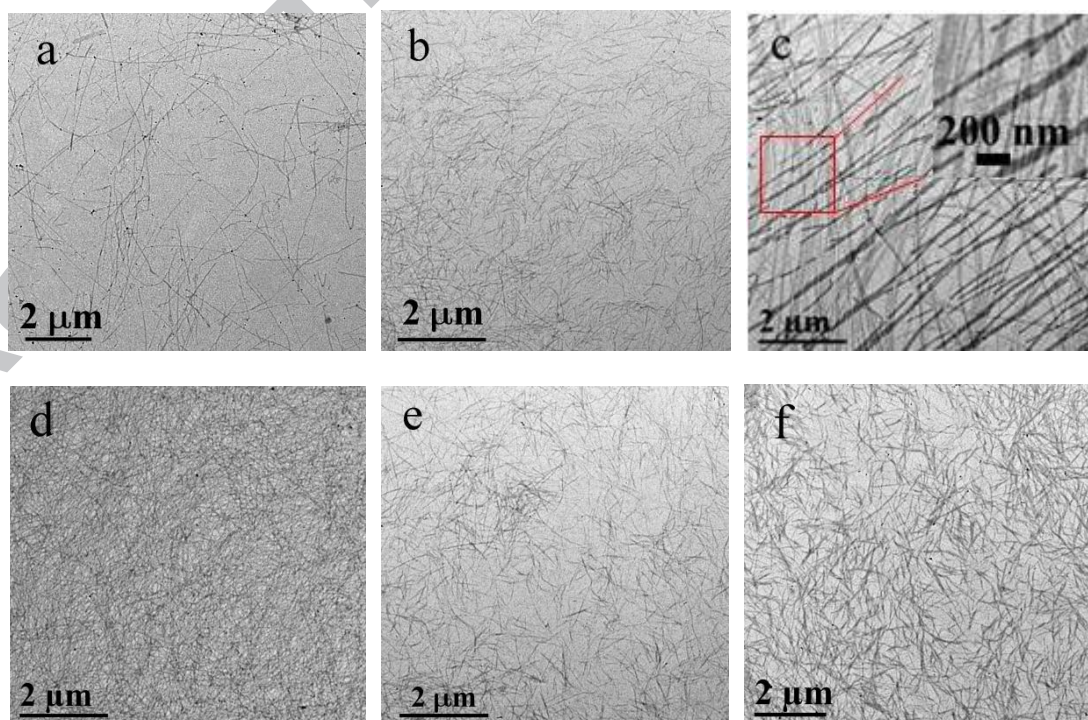
Fig. 1. Phase diagram of C_{12} TAFB/SC (a), C_{14} TAFB/SC (b), and C_{16} TAFB/SC (c) systems at 25.0 ± 0.1 °C.

3.2. Microstructure of hydrogels

TEM was employed to determine the microstructure in C_n TAFB/SC hydrogels. For TEM observations, a small amount of gels sample (without staining) was mounted onto the copper grid, and then freeze-dried for several days. From Fig. 2, a number of intertwined fibers with a width of 30 nm and the length of tens of micrometers were observed. These long fibers entangled with each other to form cross-linking networks, which immobilized water molecules through solvation and surface tension, resulting in the gelation [1]. At a fixed molar ratio of SC to C_{12} TAFB of 2:1, with the increase in total concentration, the diameter of the fibrils has no obvious change (Fig. 2a-d). With careful observation of Fig. 2c and d, one can find that with the increase in total concentration, a few bundles of fibrils are formed due to the increase in fibril density, which might be the reason of the opacity of the hydrogels at high concentration. Because the network of gels become more and more dense, and the structure are hardly observed, thus we do not give the microscopic images of the hydrogels at high gelator concentration.

The microstructure transition of another series of samples at a fixed SC concentration of $50 \text{ mmol} \cdot \text{L}^{-1}$ with different amounts of C_{12} TAFB was shown in Fig. 2c, e, f, and g. When the concentration of C_{12} TAFB is $20 \text{ mmol} \cdot \text{L}^{-1}$, cross-linked

network fibrils with the diameter of about 30 nm can be found in Fig. 2e. With the increasing concentration of C_{12} TAFB, the density of fibril becomes more and more dense, leading to the formation of bundles of fibrils. When C_{12} TAFB concentration reaches $35 \text{ mmol}\cdot\text{L}^{-1}$, lots of bundles of fibers are found, and the density of the fibers reaches a maximum value (Fig. 2f). When the concentration of C_{12} TAFB is above $35 \text{ mmol}\cdot\text{L}^{-1}$, the density of fibers decreases. The probable reason may be that the continuously increasing of C_{12} TAFB concentration leads to the increase in the hydrophobicity of the mixtures, weakening the gelation and decreasing the density of fibers in gels. When the concentration is higher than $40 \text{ mmol}\cdot\text{L}^{-1}$, only precipitates obtained. For C_{14} TAFB/SC and C_{16} TAFB/SC systems, the microstructure of the gels presents the similar tendency with that of C_{12} TAFB/SC system (Fig. S3 and S4), i.e., the density of fibers increases with increasing gelator concentration, and reaches a maximum value at the concentration of C_{14} TAFB (C_{16} TAFB) being $35 \text{ mmol}\cdot\text{L}^{-1}$, then decreases with increasing of C_{14} TAFB (C_{16} TAFB) concentration.



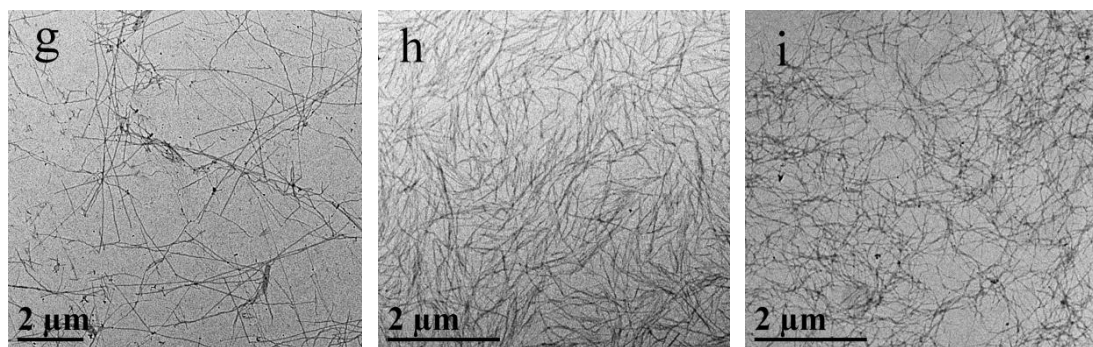


Fig. 2. TEM images of freeze-dried hydrogels formed by 20 $\text{mmol}\cdot\text{L}^{-1}$ SC/10 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (a), 40 $\text{mmol}\cdot\text{L}^{-1}$ SC/20 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (b), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/25 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (c), 60 $\text{mmol}\cdot\text{L}^{-1}$ SC/30 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (d), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/20 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (e), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/35 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (f), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/40 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB (g), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/25 $\text{mmol}\cdot\text{L}^{-1}$ C_{14}TAFB (h), and 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/25 $\text{mmol}\cdot\text{L}^{-1}$ C_{16}TAFB (i). An enlargement TEM image of hydrogels formed by 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/25 $\text{mmol}\cdot\text{L}^{-1}$ C_{12}TAFB was inserted in (c).

3.3. Rheological property

To study the rheological property of hydrogels (e.g., viscoelasticity and mechanical strength) can not only provide parameters of materials to guide the applications but also supply different models to speculate the microstructures of materials [10]. The solid-like network structure of gels, when being sheared under an increasing stress, will break suddenly at a critical shear stress, τ^* , beyond which a Newtonian-like flow occurs [1,51]. The critical shear stress (τ^*) was called “yield stress”, reflecting the strength of the network structures. We studied the influence of different factors on the mechanical strength of the hydrogels (Fig. 3). We firstly investigated the effect of the total concentration on the mechanical strength. At a fixed molar ratio of SC to C_{12}TAFB of 2:1, with the increase in total concentration, the yield stress increases gradually from 7 to 2000 Pa, which is ascribed to the more rigid network structure

induced by increasing of fibril density (Fig. 3a and e). For the sample of $100 \text{ mmol}\cdot\text{L}^{-1}$ SC/ $50 \text{ mmol}\cdot\text{L}^{-1}$ C₁₂TAFB (6.6 wt %), the yield stress can reach 2000 Pa, demonstrating the characteristic of soft viscoelastic solid [52,53]. The plateau value of the storage modulus (G') in the stress sweep can also be used to evaluate the mechanical strength of hydrogels. One can find that the G' value of the sample also rises with the total concentration, indicating the improvement of mechanical strength (Fig. 3e). The influence of C₁₂TAFB concentration on the mechanical strength was shown in Fig. 3b and f. At $c_{\text{SC}} = 50 \text{ mmol}\cdot\text{L}^{-1}$, with the increase in C₁₂TAFB concentration from 20 to $35 \text{ mmol}\cdot\text{L}^{-1}$, the yield stress increases from 25 to 100 Pa, owing to the increase of fibril density. With further increase in C₁₂TAFB concentration, the yield stress decreases, indicating the decreasing in fibril density. One can find that the hydrogel formed at the concentration proportion of $50 \text{ mmol}\cdot\text{L}^{-1}$ SC to $35 \text{ mmol}\cdot\text{L}^{-1}$ C₁₂TAFB exhibit the highest mechanical strength, which illustrates that at this proportion the hydrogel possesses the densest fibers (Fig. 2f). The hydrophobic chain length of C_nTAFB has little influence on the mechanical strength of the gels. At the same concentration, C₁₂TAFB, C₁₄TAFB, and C₁₆TAFB systems almost have the same yield stress of about 100 Pa (Fig. 3c). Finally, the influence of anions on the mechanical strength was shown in Figure 3d. At the same concentration, the yield stress of C₁₂TAFB/SC system is much higher than that of C₁₂TAFC/SC system due to its higher gelation capability. Thus, we can conclude that the mechanical strength of the hydrogels can be regulated by changing the proportion of the two compounds, the concentration of the surfactants, and the sorts of anions.

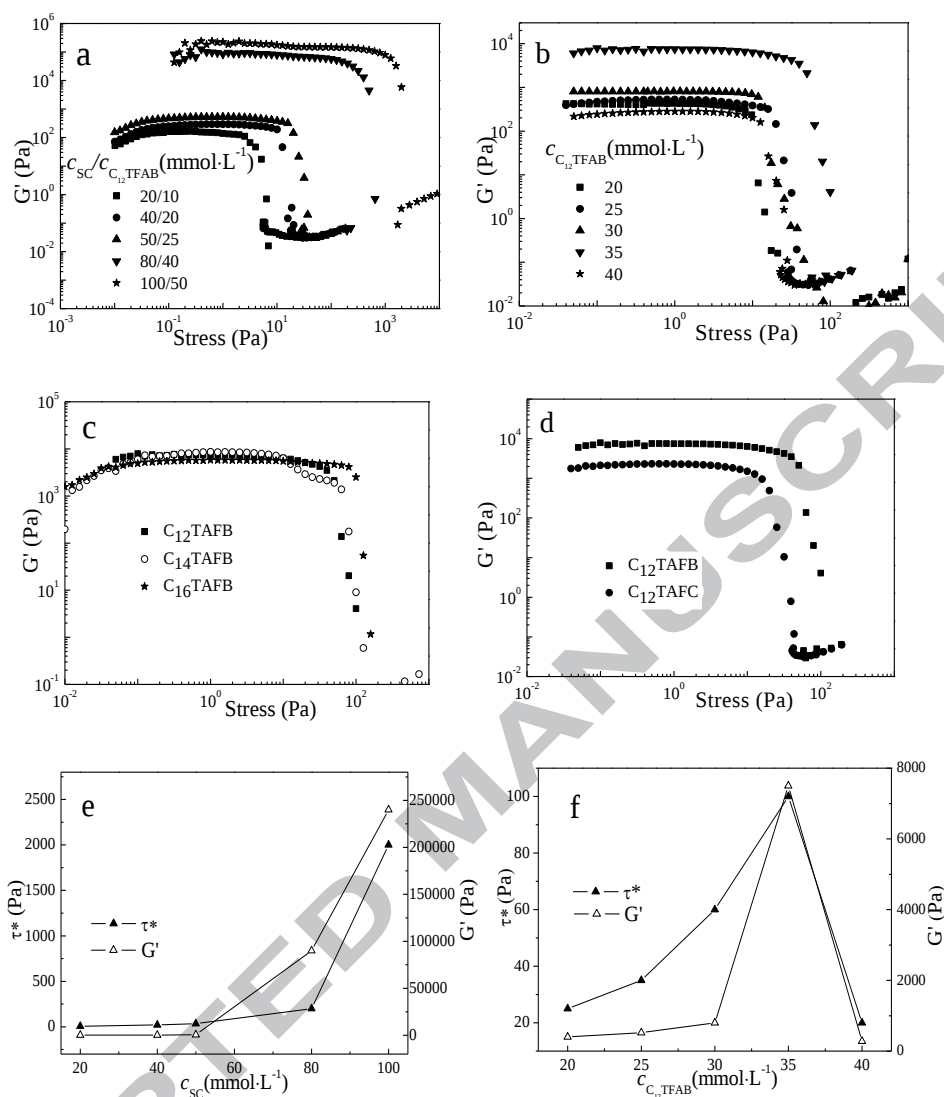


Fig. 3. G' as a function of oscillatory stress of hydrogels formed (a) at the molar ratio of SC to C_{12} TAFB of 2:1 with different total concentrations, (b) at $c_{SC} = 50$ mmol·L⁻¹ with different amounts of C_{12} TAFB, (c) at the different chain length (50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C_n TAFB), and (d) at 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C_{12} TAFB (C). (e) G' and τ^* as the function of total concentration at the molar ratio of SC to C_{12} TAFB of 2:1, (f) G' and τ^* as the function of C_{12} TAFB concentration.

Gels are viscoelastic soft solid-like materials that simultaneously store and display energy [4,53]. The viscoelasticity of gels can be characterized by two dynamic moduli: storage modulus (G'), which can estimate the degree of materials resistance against

mechanical disturbance, and loss modulus (G''), which measures the tendency of materials to flow under stress. Dynamic rheology was carried out to measure the viscoelasticity of C_{12} TAFB/SC hydrogels (Fig. 4). G' and G'' are almost independent of the frequency over the studied frequency region and show an elastic dominant property, demonstrating a solid-like rheological behavior [54]. Expectedly, the absolute value of G' increases with the increase in total concentration at a fixed molar ratio of SC to C_{12} TAFB of 2:1 (Fig. 4a and b). At a fixed SC concentration of 50 $\text{mmol}\cdot\text{L}^{-1}$, with an increase in C_{12} TAFB concentration, G' and G'' increase firstly and then decrease (Fig. 4c and d). The stiffness/rigidity values of the hydrogels, i.e., the ratio of the dynamic moduli, G' and G'' , are found to be 4 to 10 (Tables S1 and S2), which further proved that with the increasing of total concentration, the fibers arranged more tightly, causing much higher mechanical strength.

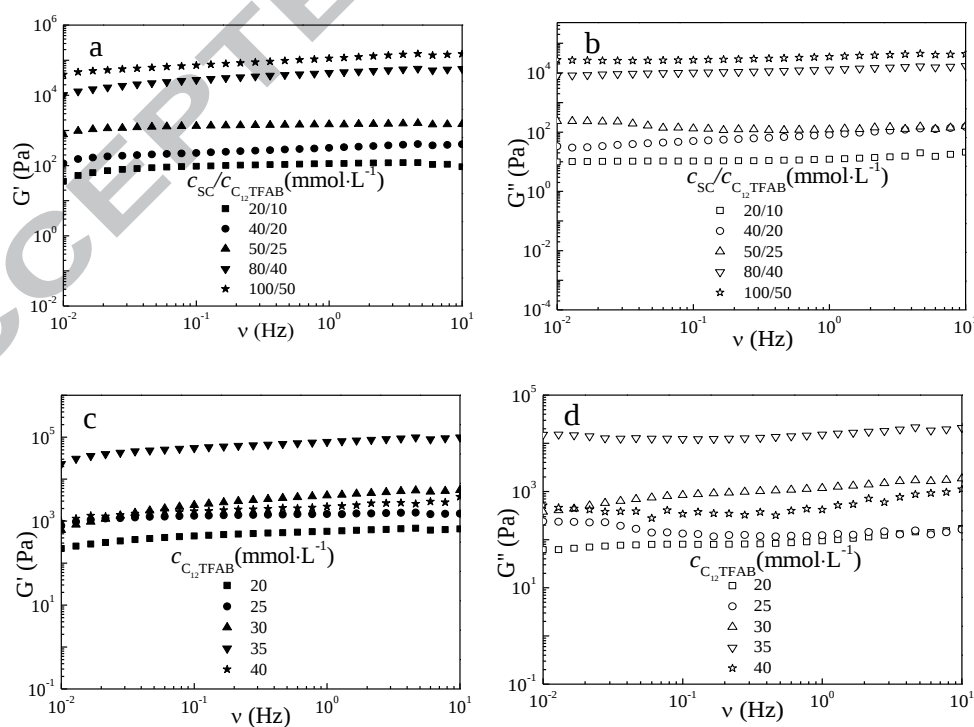


Fig. 4. G' (a) and G'' (b) as a function of frequency for the molar ratio of SC to

C_{12} TAFB of 2:1 with different total concentrations; G' (c) and G'' (d) as a function of frequency for $50 \text{ mmol}\cdot\text{L}^{-1}$ SC with different amounts of C_{12} TAFB.

3.4. Stimuli-responsive property

Hydrogels usually undergoes a gel-sol phase transition when temperature increases, which is accompanied by a reduction in the mechanical strength. For SC/ C_{12} TAFB system, when extra energy (temperature or shearing force) was introduced, the hydrogels would experience a reversible gel-sol transition. As shown in Fig. S5, when being heated, the hydrogels can be converted into solution (sol) and the sol can be turned back to hydrogels upon cooling to R.T. for several hours. Moreover, the hydrogels can also be destroyed by shaking the sample vigorously to give a solution, and which can be recovered to hydrogels after being rested for 1 hour.

Differential scanning calorimetry (DSC) experiments were performed to detect the gel-sol transition temperature ($T_{\text{gel-sol}}$). An endothermic peak can be found in the heating curve, which indicates a positive enthalpy from gel to sol, as shown in Fig. 5. At a fixed molar ratio of SC to C_{12} TAFB of 2:1, with the increasing of total concentration, the endothermic peak shifts to a higher temperature, owing to the much denser network requires more energy to destroy the hydrogels (Fig. 5a and c). At $c_{\text{SC}} = 50 \text{ mmol}\cdot\text{L}^{-1}$, with the increasing C_{12} TAFB concentration from 20 to $35 \text{ mmol}\cdot\text{L}^{-1}$, the $T_{\text{gel-sol}}$ increases from 31.86 to 72.73 °C firstly. With further increase in C_{12} TAFB amounts, $T_{\text{gel-sol}}$ decreases gradually. The $T_{\text{gel-sol}}$ variation tendency is consistent with the variation of mechanical strength of hydrogels.

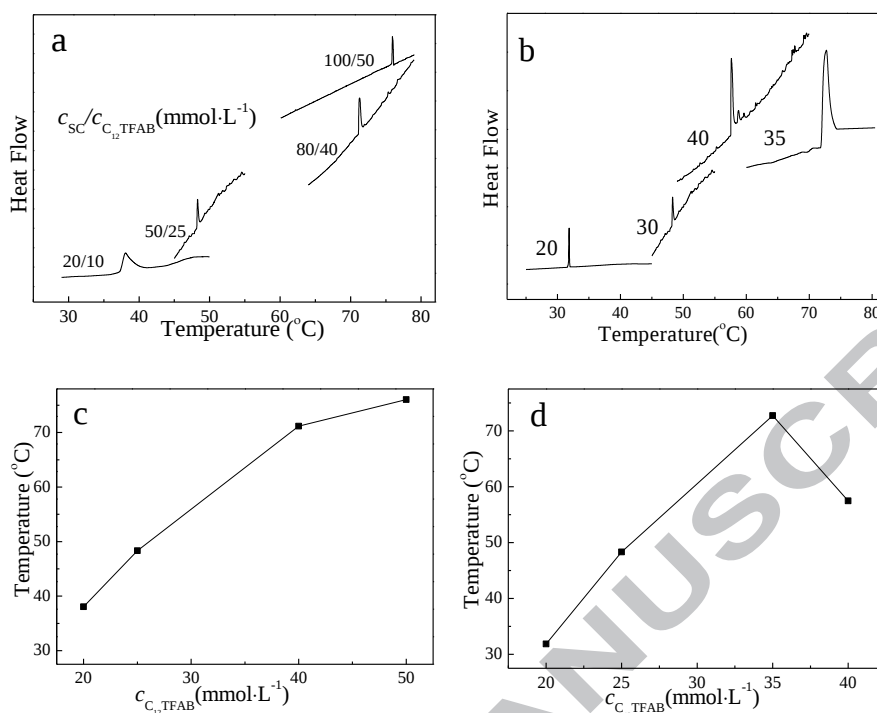
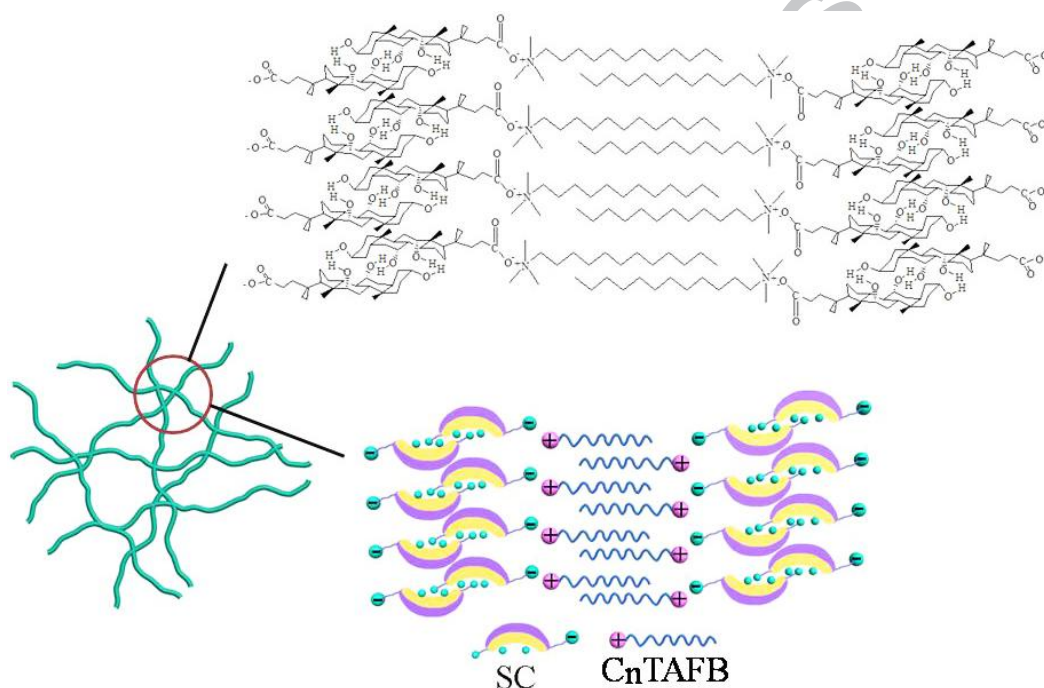


Fig. 5. (a) DSC curves of hydrogels formed by the molar ratio of SC to C₁₂TAFB of 2:1 with different total concentrations, (b) DSC curves of hydrogels formed by 50 mmol·L⁻¹ SC with different amounts of C₁₂TAFB, (c) T_{gel-sol} as a function of the total concentration, and (d) T_{gel-sol} as a function of the concentration of C₁₂TAFB at c_{SC} = 50 mmol·L⁻¹.

3.5. Discussion

A proposal for the interaction between SC and C₁₂TAFB for the formation of fibrous structures in hydrogels was shown in Scheme 1. When SC was added to C₁₂TAFB solution, C₁₂TA⁺...cholate ion pairs would be formed due to the electrostatic interaction. SC is a facial amphiphile with several chiral centers and a rigid steroid skeleton. Three hydroxyl groups and a carboxyl group are oriented to the concave side of the rigid steroid ring, being rendered hydrophilic, while the convex side is hydrophobic [12]. As shown in Scheme 1, hydrogen bonding exists between

the two reversed SC hydroxyl groups. Each SC molecule connects with another reversed SC molecule through hydrogen bonding and a C_n TAFB molecule through electrostatic interaction. Driven by hydrophobic interaction, electrostatic interaction, hydrogen bonding, and van der Waals force, the arrays combine with each other. Due to the rigid steroid skeleton and the chiral structure of SC molecules, the arrays cannot extend in linearity, but tilt to induce the formation of fibers.



Scheme 1. Proposed mechanism of fibrils formed in SC/ C_n TAFB hydrogels.

FT-IR and small-angle X-ray diffraction (SAXRD) experiments were performed to support the proposed mechanism of the formation of fibrils in hydrogels. The FT-IR spectra in Fig. S6 (curves b - d) within the wavelength region of 3000–4000 cm^{-1} demonstrated the hydrogen bonding between the hydroxyl groups of two reversed SC molecules. The arrangement of C_n TAFB and SC molecules in hydrogels was revealed by SAXRD patterns (Fig. 6). According to Bragg's law, the three well-resolved reflection peaks at 3.35, 4.56, and 7.65 $^\circ$ were calculated corresponding to the d

spacing of 2.65, 1.94, and 1.15 nm, respectively, which were considered to relate to some cycled units of the arrangements formed by SC and C₁₂TAFB. The d value of 2.65 nm is just a little less than the twice of the chain length of C₁₂TAFB molecule (1.672 nm) [50], belonging to the combination of two C₁₂TAFB molecules through hydrophobic interaction in each unit of the arrays. The d value of 1.93 nm is just a little longer than a cholate backbone length (1.5 nm), which might be ascribed to the elongation induced by the side-by-side connection of two reversed SC molecules in each unit through intermolecular hydrogen bonding [54-58]. The distance of 1.15 nm is comparable with twice the thickness of cholate skeleton (0.6 nm × 2) [54]. The position of the reflection peaks was almost unchanged with the variation of concentration or proportion of SC and C₁₂TAFB, demonstrating the same molecular arrangement in the fibers of hydrogel.

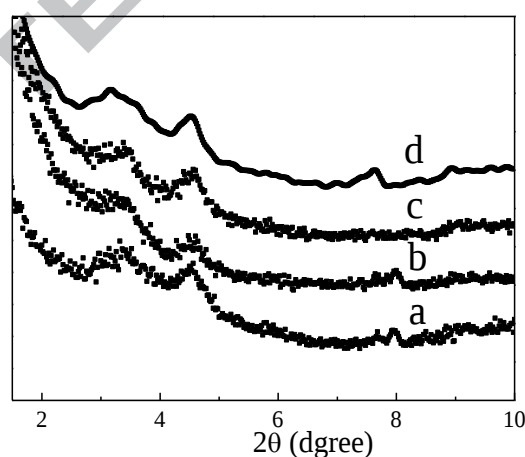


Fig. 6. SAXRD patterns of dried hydrogels formed by (a) 20 mmol·L⁻¹ SC/10 mmol·L⁻¹ C₁₂TAFB, (b) 50 mmol·L⁻¹ SC/20 mmol·L⁻¹ C₁₂TAFB, (c) 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₂TAFB, and (d) 50 mmol·L⁻¹ SC/35 mmol·L⁻¹ C₁₂TAFB.

3.6. Hydrogel as precursors for producing Fe₃O₄ MNPs

As a representative demonstration, the preparation of Fe₃O₄ MNPs based on

SC/C₁₂TAFB hydrogels with NaOH as the precipitator will be discussed in detail. Cationic surfactant (C₁₂TAFB) has larger anion, [FeCl₃Br]⁻, which can gradually release Fe³⁺. SC/C₁₂TAFB hydrogels loaded with Fe²⁺ were added into NaOH aqueous solution. After being kept at 50 °C in water bath for 12 h, black Fe₃O₄ precipitates were obtained. The XRD pattern of the obtained Fe₃O₄ precipitates (Fig. 7a) could be indexed to cubic phase (space group Fd3m, no.227), which was in good accordance with the ICPS file of Fe₃O₄ (JCPDS NO.65-3107). From the TEM image in Fig. 7b, it is clearly observed that the obtained Fe₃O₄ possess cubic geometrical morphology with an average edge length of 7.2 nm. The selected-area electron diffraction (SAED) pattern (Fig. 7c) is consistent with the XRD pattern. Well resolved 2D lattice fringes with a lattice spacing of 0.245 nm are observed in the high-resolution transmission electron microscopy (HR-TEM) image (Fig. 7d), which is in compliance with the (2,2,2) crystalline plane of the cubic Fe₃O₄. The magnetic properties of the cubic Fe₃O₄ were studied with a superconducting quantum interferometer device (SQUID) magnetometer from Quantum Design. The hysteresis loop of cubic Fe₃O₄ in low field from -400 Oe to 400 Oe exhibits clear ferromagnetic characteristics with saturation magnetization, remanent magnetization and coercivity of 62 emug·g⁻¹, 0.85 emug·g⁻¹ and 17 Oe, respectively (Fig. 7e). Owing to the excellent viscoelastic of hydrogels and the existence of [FeCl₃Br]⁻, SC/C₁₂TAFB hydrogel is a good precursor for preparing Fe₃O₄MNPs. The simple method was carried out under mild conditions in aqueous solution, eliminating the use of complex and toxic organometallic reactants as well as the complicated process and high

temperature required in common Fe_3O_4 preparation [37].

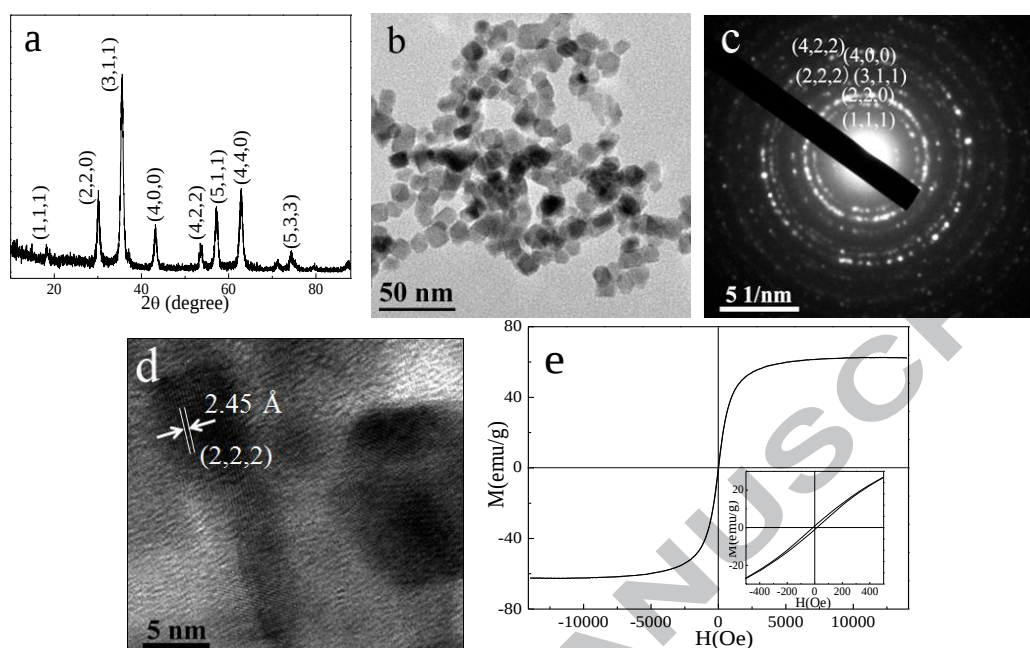


Fig. 7. a) XRD pattern, b) TEM image, c) SAED pattern, d) HR-TEM image, e) SQUID magnetometry of Fe_3O_4 MNPs prepared from SC/ C_{12} TAFB hydrogels.

3.7. Fe_3O_4 MNPs catalyses the oxidation of peroxidase substrates

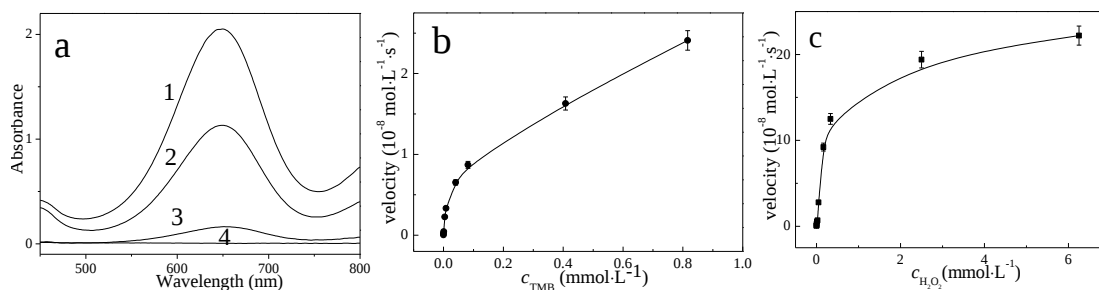
Fe_3O_4 MNPs are usually considered chemically and biologically inert, which has been widely used for bioanalysis, bioelectrocatalysis, drug delivery, bacteria inactivation, etc [59,60]. According to the literature, Fe_3O_4 MNPs within the size range of 5-7 nm have a greater surface-to-volume ratio to interact with substrates and exhibit higher peroxidase-like activity [59,60]. To investigate the catalytic activity of Fe_3O_4 MNPs, the catalytic oxidation process of the peroxidase substrate, 3,3',5,5'-tetramethylbenzidine (TMB), in the presence of H_2O_2 was tested. As shown in Fig. 8a (curve 1), Fe_3O_4 MNPs can catalyze the oxidation of TMB in the presence of H_2O_2 to produce a blue color reaction, which exhibits a maximum absorbance at 652 nm. In the absence of Fe_3O_4 MNPs or TMB, the colorless solution showed a negligible absorption in the range of 450 to 800 nm (curves 3 and 4). Notably, the obtained Fe_3O_4 MNPs with the average size of 7.2 nm present much higher catalytic

activity than HRP at the same condition (curves 1 and 2) due to its higher surface-to-volume ratio.

In order to interpret the reaction mechanism of the peroxidase activity of the Fe_3O_4 MNPs, the apparent steady-state kinetic parameters for the reaction were measured. Typical Michaelis-Menten curves were observed for Fe_3O_4 MNPs with TMB or H_2O_2 as substrates (Fig. 8b and c). The Lineweaver-Burk plot method was used to investigate whether the catalytic reaction of Fe_3O_4 MNPs followed the Michaelis-Menten behavior. As shown in Figure 8d and e, the reciprocal of the initial rate was directly proportional to the substrate concentration. The double reciprocal plots of the Michaelis-Menten equation were applied to obtain the catalytic parameters, as shown in Table 2. The apparent K_m value of the obtained Fe_3O_4 MNPs was significantly lower than that for HRP towards H_2O_2 and TMB [27,36], indicating that the obtained Fe_3O_4 MNPs had a higher affinity to TMB and H_2O_2 than HRP. Compared with the reported nanomaterial with peroxidase-like activities such as FeS, ZnFe_2O_4 , and Au-Pt, the obtained Fe_3O_4 MNPs had the smallest K_m value, which should be attributed to its small size and unique cubic structure [31-34].

Table 2 Michaelis constant (K_m) and maximal reaction rate (V_{max}) of Fe_3O_4 MNPs.

catalyst	substrate	$K_m(\text{mmol}\cdot\text{L}^{-1})$	$V_{max} (10^{-8} \text{ mol}\cdot\text{L}^{-1}\cdot\text{s}^{-1})$
Fe_3O_4	TMB	0.091	5.18
MNPs	H_2O_2	0.01957	1.26
HRP	TMB [27]	0.434	10.0
	H_2O_2 [27]	3.70	8.71



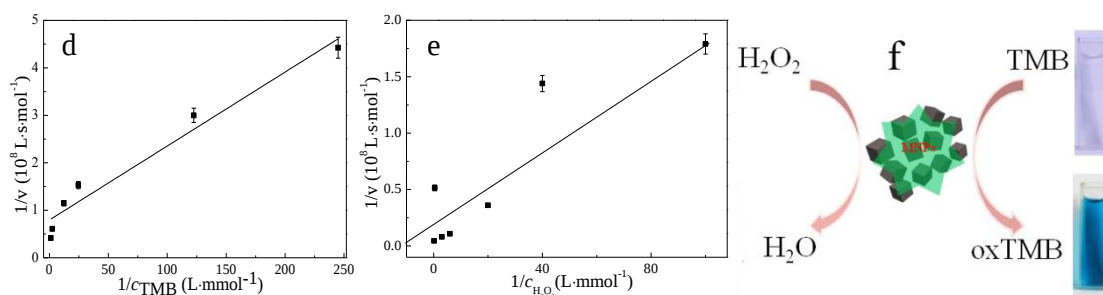


Fig. 8. (a) Typical absorption spectra of aqueous suspensions of the corresponding reactions incubated at 40 °C in acetate buffer (8 mL, 0.2 mol·L⁻¹, pH = 4.0), curve 1: 50 µg Fe₃O₄ MNPs with 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂; curve 2: 1 ng HRP with 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂; curve 3: 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂ without Fe₃O₄ MNPs; and curve 4: 50 µg Fe₃O₄ MNPs and 10 mmol·L⁻¹ H₂O₂ without TMB. (b-e) Steady-state kinetic assay and catalytic mechanism of Fe₃O₄ MNPs. The velocity (v) of the reaction was measured using 50 µg Fe₃O₄ MNPs in acetate buffer (8 mL, 0.2 mol·L⁻¹, pH = 4.0) at 40 °C (b,c). The concentration of H₂O₂ was 10 mmol·L⁻¹ and the TMB concentration was varied (b,d). The concentration of TMB was 816 µmol·L⁻¹ and the H₂O₂ concentration was varied (c,e). Schematic illustration of colorimetric determination of H₂O₂ using Fe₃O₄ MNPs catalyzed reactions (f).

As shown in Fig. S7a and b, the peroxidase-like activity of the Fe₃O₄ MNPs is inhibited at higher H₂O₂ concentrations. However, within the concentration range of H₂O₂ from 1 to 10 µmol·L⁻¹, the absorbance at 652 nm versus the concentration of H₂O₂ presents good linearity with a correlation coefficient of 0.99954 (Fig. 9a and b), which indicates that the change of the absorbance at 652 nm can be used for H₂O₂ detection. The detection limit for H₂O₂ is calculated to be 0.1 µmol·L⁻¹ (3σ/K), being better than that of other Fe₃O₄ and Au nanoparticles [36,37,60]. The images of color reaction of TMB with different concentrations of H₂O₂ were shown in Fig. S7c.

3.8. Glucose detection

Since H_2O_2 is the product of glucose oxidation reaction by glucose oxidase (GOx), we established a colorimetric biosensor for glucose detection when Fe_3O_4 MNPs was coupled with the glucose catalytic reaction (Fig. 9f). Fig. 9c and d show the calibration curve for glucose detection under conventional condition. The linear response ($R = 0.9998$) of the absorbance at 652 nm versus glucose concentration is within the range of $1.0 - 40 \mu\text{mol}\cdot\text{L}^{-1}$. The detection limit of glucose is $0.37 \mu\text{mol}\cdot\text{L}^{-1}$ ($3\sigma/K$). To examine the selectivity of glucose detection, control experiments were carried out using $10 \text{ mmol}\cdot\text{L}^{-1}$ lactose, $10 \text{ mmol}\cdot\text{L}^{-1}$ fructose, and $10 \text{ mmol}\cdot\text{L}^{-1}$ maltose in replacement of glucose ($38.5 \mu\text{mol}\cdot\text{L}^{-1}$). No detectable signals were observed (Fig. 9e). Thus, the proposed biosensor system is highly sensitive for glucose detection. Due to the observable change from colorless to blue by naked eyes, the visual detection can be realized without any instruments or complicated designs, which hopefully to be a novel candidate glucose sensor for glucose detection.

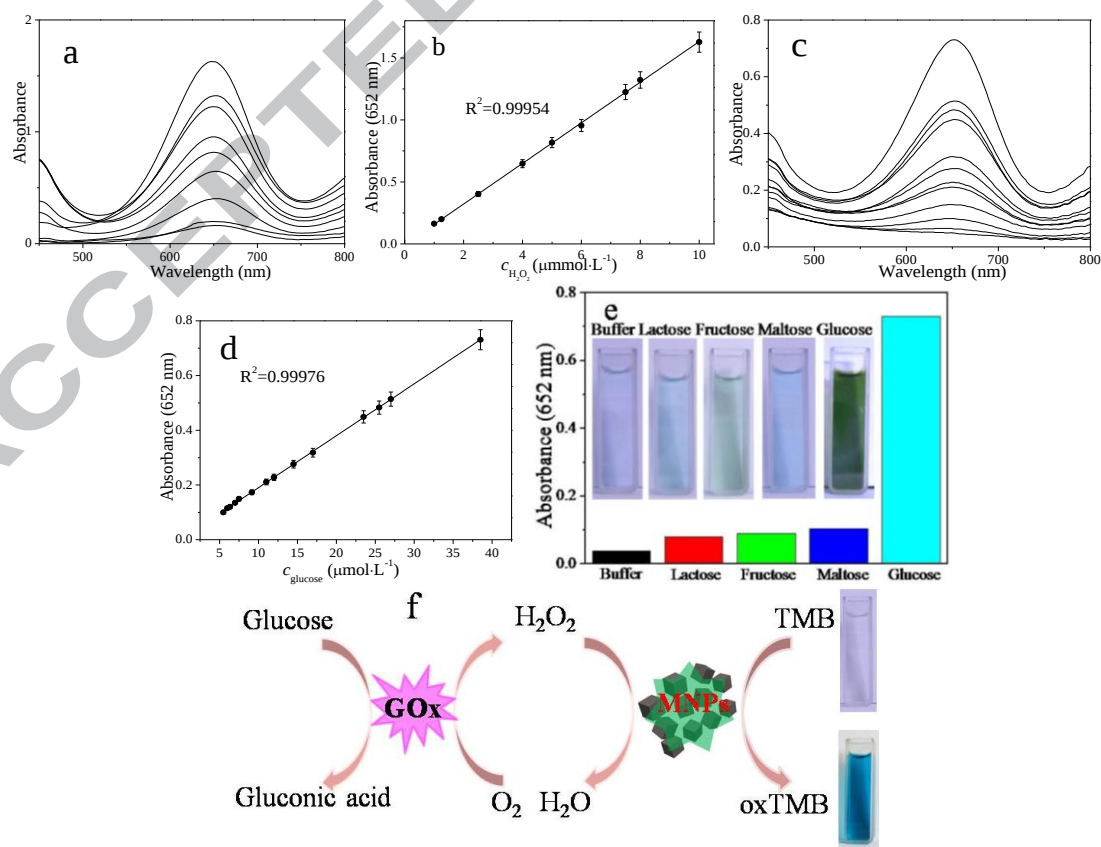


Fig. 9. H_2O_2 and glucose detection based on Fe_3O_4 MNPs. The UV-vis spectra of (a)

H₂O₂ solution and (c) glucose solution with Fe₃O₄ MNPs and 816 $\mu\text{mol}\cdot\text{L}^{-1}$ TMB in acetate buffer (pH = 4.0). The concentration of H₂O₂ ($\mu\text{mol}\cdot\text{L}^{-1}$) in (a) from top to bottom is 10, 8, 7.5, 6, 5, 4, 2.5, 1.25, and 1. The concentration of glucose ($\mu\text{mol}\cdot\text{L}^{-1}$) in (c) from top to bottom is 38.5, 27, 25.5, 23.5, 17, 14.5, 12, 11, 7.5, 5.5, 0.00143, and 0.00016. The linear calibration plot for H₂O₂ (b) and glucose (d). Selectivity analysis for glucose detection by monitoring the absorbance at 652 nm (e), the analyte concentration were as follows: 10 $\text{mmol}\cdot\text{L}^{-1}$ lactose, 10 $\text{mmol}\cdot\text{L}^{-1}$ fructose, 10 $\text{mmol}\cdot\text{L}^{-1}$ maltose, and 38.5 $\mu\text{mol}\cdot\text{L}^{-1}$ glucose, inset: the color change with the different solutions. Schematic illustration of colorimetric determination of glucose using glucose (GOx) and Fe₃O₄ MNPs catalyzed reactions (f).

4. Conclusions

In summary, stimuli-response magnetic hydrogels with excellent mechanical strength were obtained by mixing the magnetic surfactant, C_nTAFB(C) (n = 12, 14, 16), and SC in water. The gelation behavior of C_nTAFB(C)/SC systems indicated that the hydrophobic interaction and R_n of anions play significant roles in gelation process. The microstructure of hydrogels was observed to be nanofibrils with a width of 30 nm and the length of tens of micrometers. The increase in total concentration triggered the increase in the density of the fibers, corresponding to the mechanical strength enhancement and the T_{gel-sol} elevating. C₁₂TAFB/SC hydrogels served as the precursor for preparing cubic Fe₃O₄ nanoparticles with excellent ferromagnetic characteristics and higher peroxidase-like activity, which could be used as biosensor for H₂O₂ and glucose detection, expanding the range of biosensor platform used for biological assay. We hope our results will promote the further theoretical study on designing amphiphiles hydrogels, and provide a wide range of applications for Fe₃O₄ nanoparticles mimetic enzyme systems in bio-detection, catalysis, and clinical

diagnostics.

Acknowledgements

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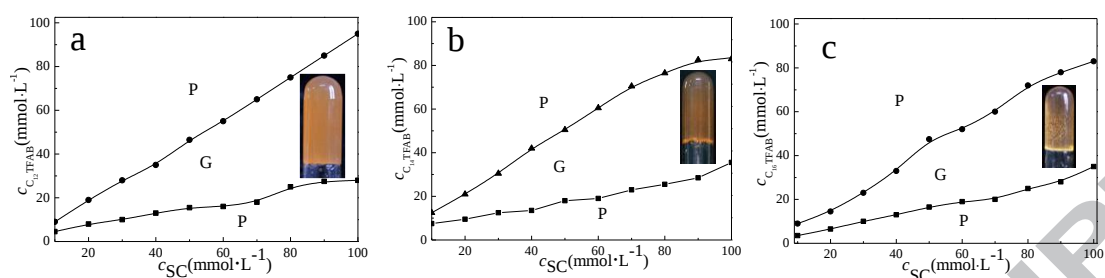


Fig. 1. Phase diagram of C_{12} TAFB/SC (a), C_{14} TAFB/SC (b), and C_{16} TAFB/SC (c) systems at 25.0 ± 0.1 °C.

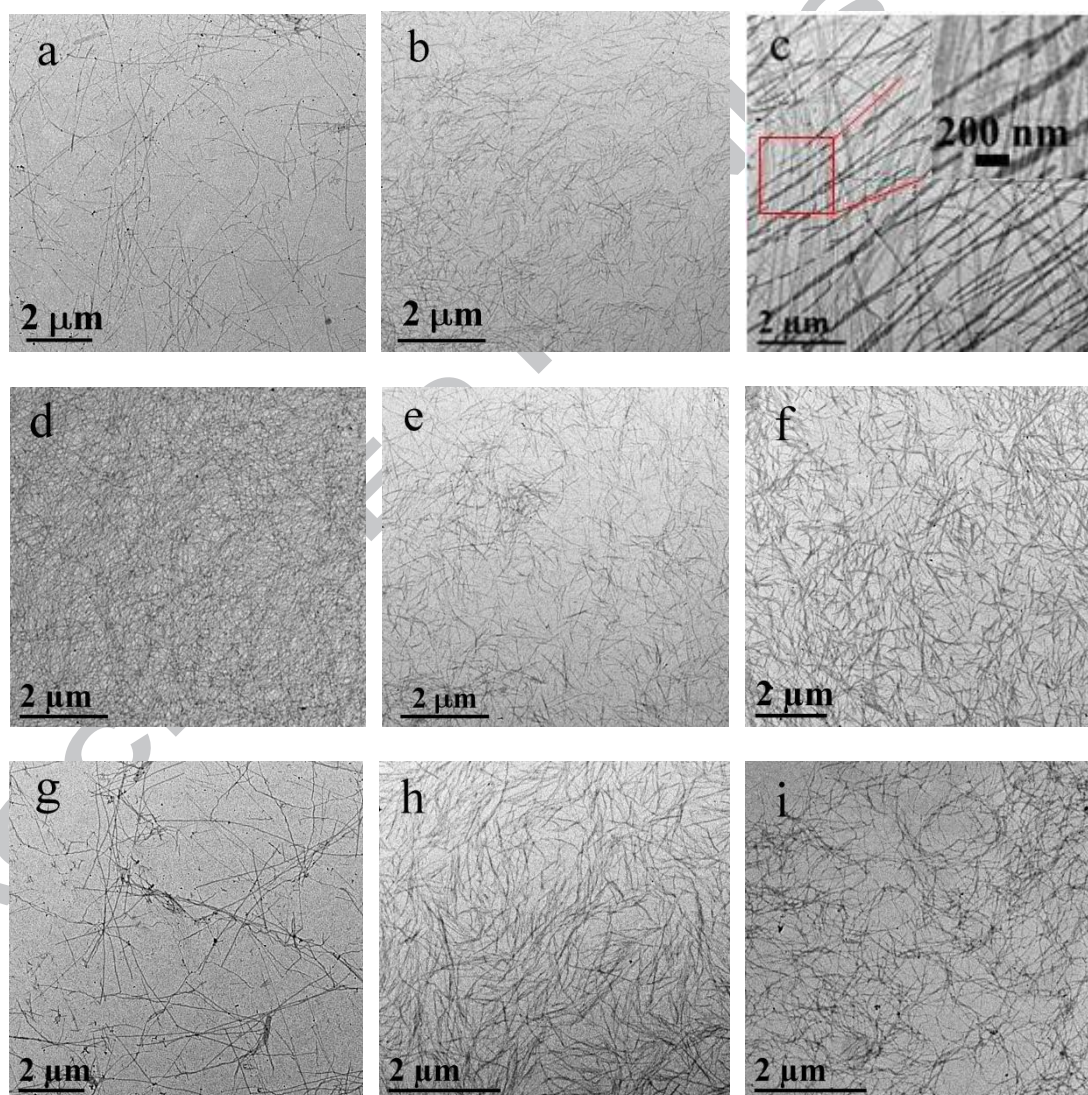


Fig. 2. TEM images of freeze-dried hydrogels formed by $20 \text{ mmol}\cdot\text{L}^{-1}$ SC/ $10 \text{ mmol}\cdot\text{L}^{-1}$ C_{12} TAFB (a), $40 \text{ mmol}\cdot\text{L}^{-1}$ SC/ $20 \text{ mmol}\cdot\text{L}^{-1}$ C_{12} TAFB (b), $50 \text{ mmol}\cdot\text{L}^{-1}$ SC/ $25 \text{ mmol}\cdot\text{L}^{-1}$ C_{12} TAFB (c), $60 \text{ mmol}\cdot\text{L}^{-1}$ SC/ $30 \text{ mmol}\cdot\text{L}^{-1}$ C_{12} TAFB (d), 50

mmol·L⁻¹ SC/20 mmol·L⁻¹ C₁₂TAFB (e), 50 mmol·L⁻¹ SC/35 mmol·L⁻¹ C₁₂TAFB (f), 50 mmol·L⁻¹ SC/40 mmol·L⁻¹ C₁₂TAFB (g), 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₄TAFB (h), and 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₆TAFB (i). An enlargement TEM image of hydrogels formed by 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₂TAFB was inserted in (c).

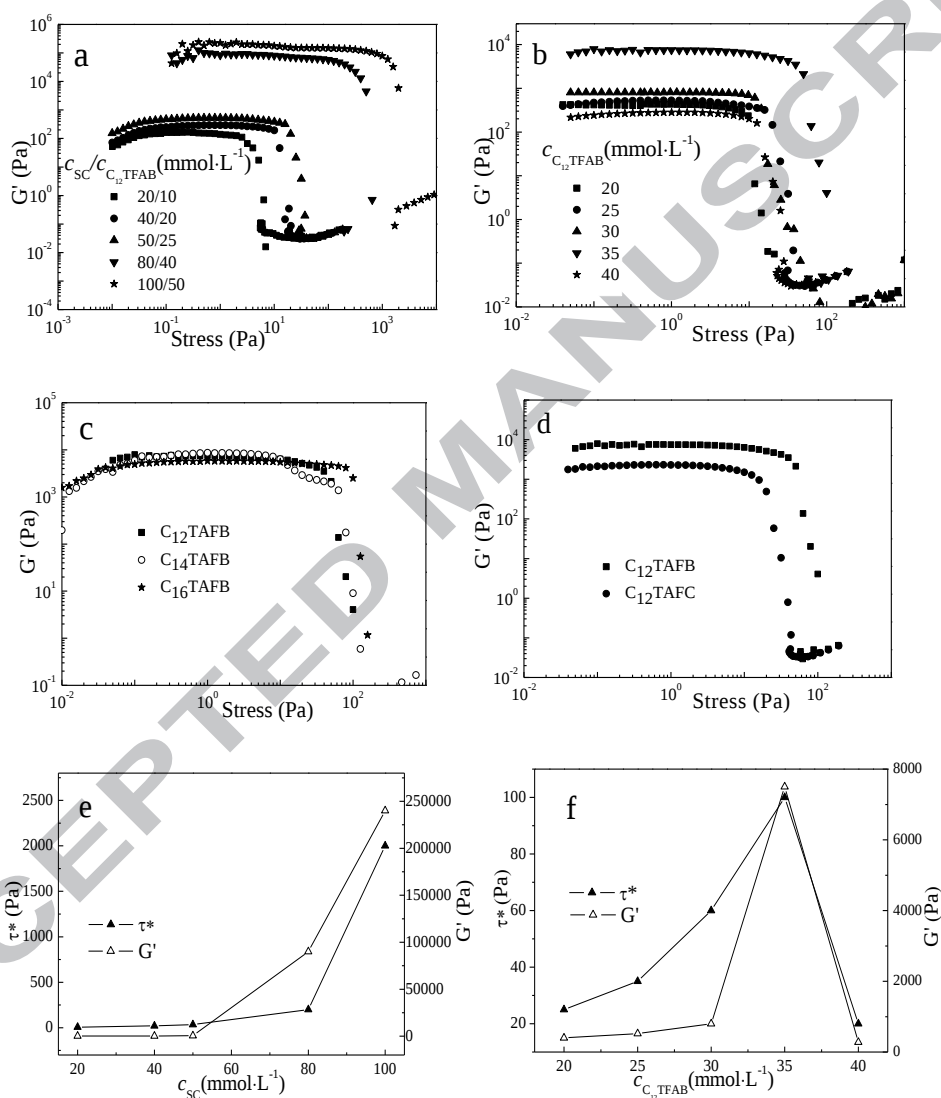


Fig. 3. G' as a function of oscillatory stress of hydrogels formed (a) at the molar ratio of SC to C₁₂TAFB of 2:1 with different total concentrations, (b) at $c_{SC} = 50$ mmol·L⁻¹ with different amounts of C₁₂TAFB, (c) at the different chain length (50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C_nTAFB), and (d) at 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₂TAFB (C). (e) G' and τ^* as the function of total concentration at the molar ratio of SC to C₁₂TAFB of

2:1, (f) G' and τ^* as the function of C_{12} TAFB concentration.

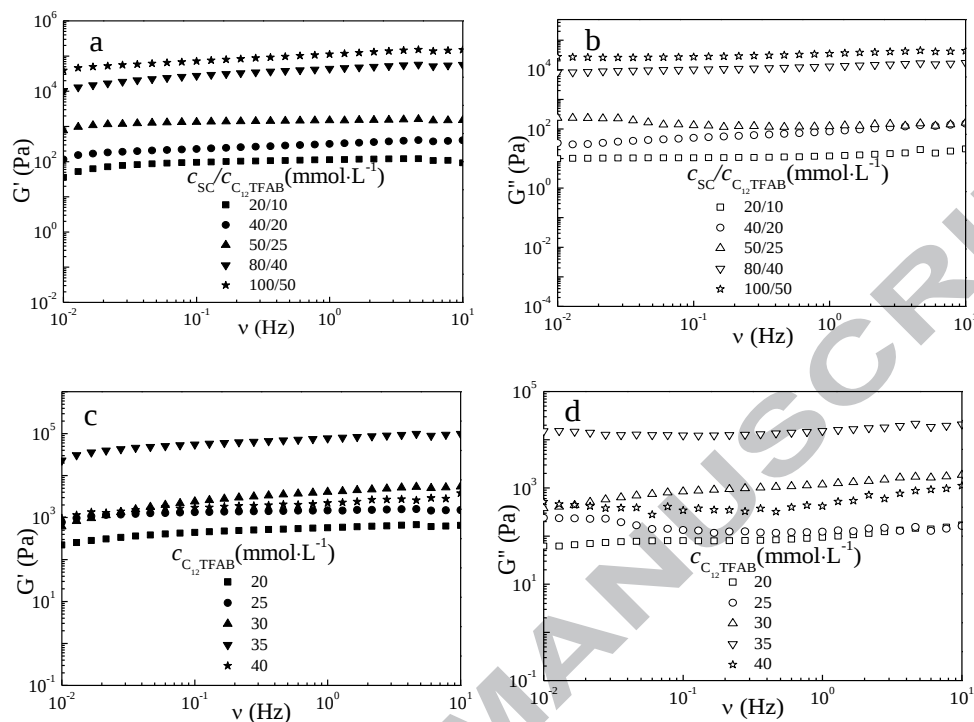


Fig. 4. G' (a) and G'' (b) as a function of frequency for the molar ratio of SC to C_{12} TAFB of 2:1 with different total concentrations; G' (c) and G'' (d) as a function of frequency for 50 mmol·L⁻¹SC with different amounts of C_{12} TAFB.

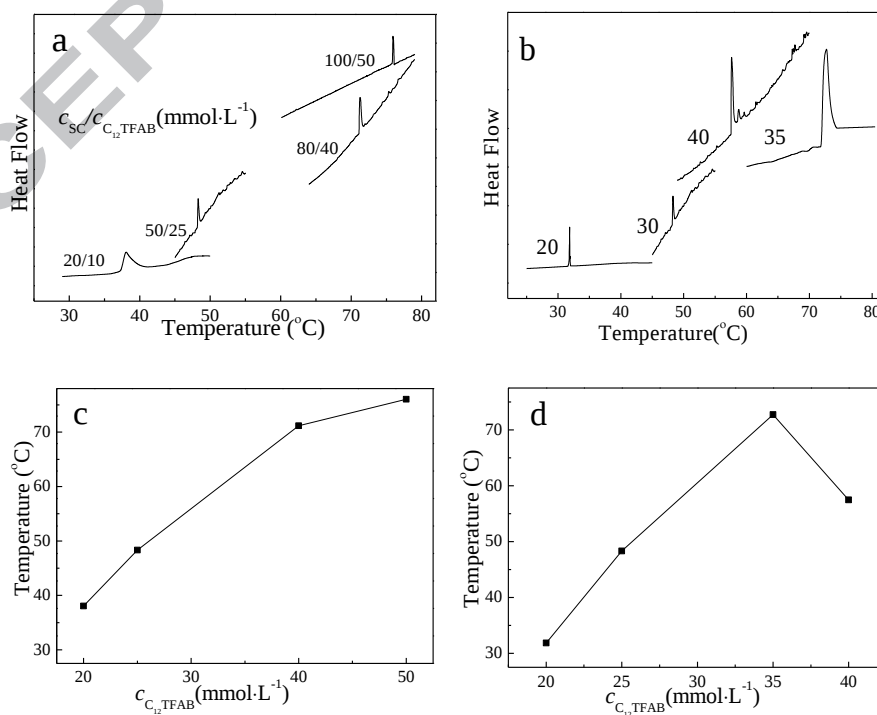
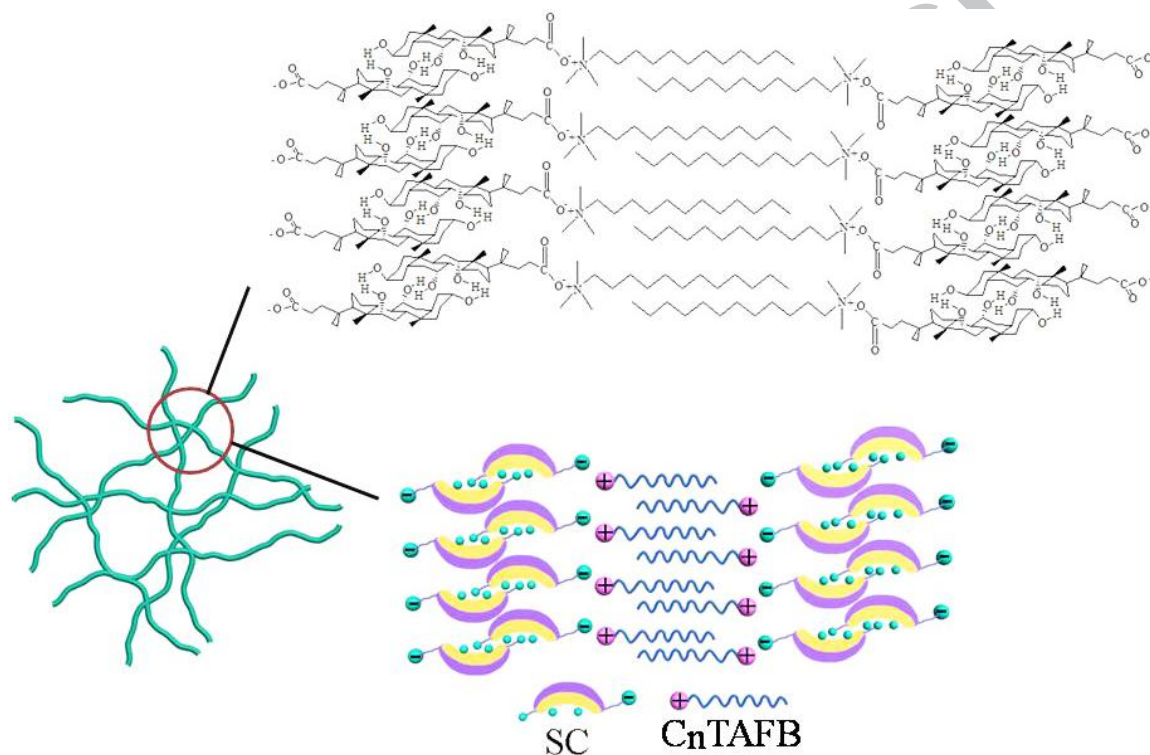


Fig. 5. (a) DSC curves of hydrogels formed by the molar ratio of SC to C₁₂TAFB of 2:1 with different total concentrations, (b) DSC curves of hydrogels formed by 50 mmol·L⁻¹ SC with different amounts of C₁₂TAFB, (c) T_{gel-sol} as a function of the total concentration, and (d) T_{gel-sol} as a function of the concentration of C₁₂TAFB at c_{SC} = 50 mmol·L⁻¹.



Scheme 1. Mechanism of the formation of fibers in SC/C_nTAFB hydrogels.

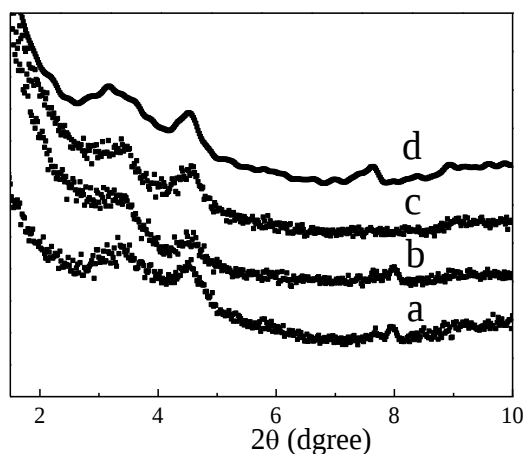


Fig. 6. SAXRD patterns of dried hydrogels formed by (a) 20 mmol·L⁻¹ SC/10 mmol·L⁻¹ C₁₂TAFB, (b) 50 mmol·L⁻¹ SC/20 mmol·L⁻¹ C₁₂TAFB, (c) 50 mmol·L⁻¹ SC/25

mmol·L⁻¹ C₁₂TAFB, and (d) 50 mmol·L⁻¹ SC/35 mmol·L⁻¹ C₁₂TAFB.

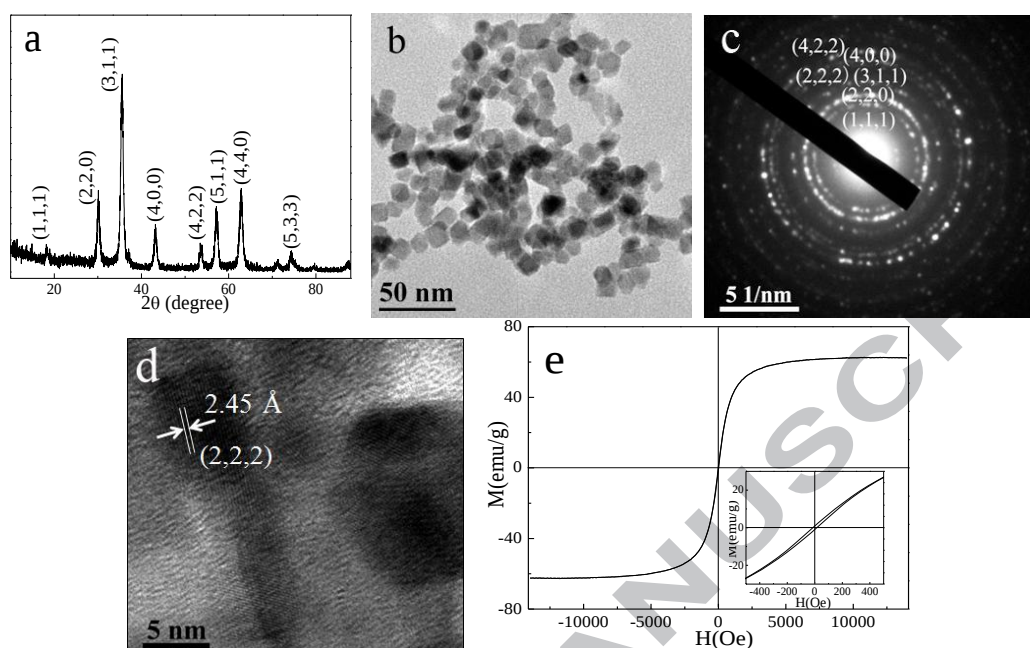


Fig. 7. a) XRD pattern, b) TEM image, c) SAED pattern, d) HR-TEM image, e)

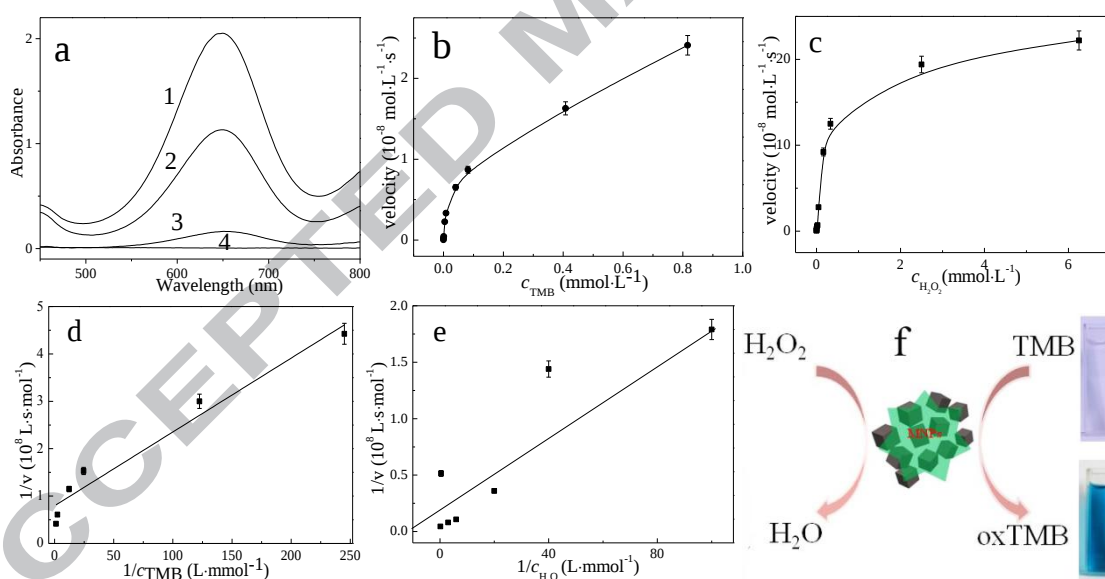


Fig. 8. (a) Typical absorption spectra of aqueous suspensions of the corresponding reactions incubated at 40 °C in acetate buffer (8 mL, 0.2 mol·L⁻¹, pH = 4.0), curve 1: 50 µg Fe₃O₄ MNPs with 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂; curve 2: 1 ng HRP with 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂; curve 3: 816 µmol·L⁻¹ TMB and 10 mmol·L⁻¹ H₂O₂ without Fe₃O₄ MNPs; and curve 4: 50 µg Fe₃O₄ MNPs and 10 mmol·L⁻¹ H₂O₂ without TMB. (b-e) Steady-state kinetic assay and catalytic

mechanism of Fe_3O_4 MNPs. The velocity (v) of the reaction was measured using 50 μg Fe_3O_4 MNPs in acetate buffer (8 mL, 0.2 $\text{mol}\cdot\text{L}^{-1}$, pH = 4.0) at 40 $^\circ\text{C}$ (b,c). The concentration of H_2O_2 was 10 $\text{mmol}\cdot\text{L}^{-1}$ and the TMB concentration was varied (b,d). The concentration of TMB was 816 $\mu\text{mol}\cdot\text{L}^{-1}$ and the H_2O_2 concentration was varied (c,e). Schematic illustration of colorimetric determination of H_2O_2 using Fe_3O_4 MNPs catalyzed reactions (f).

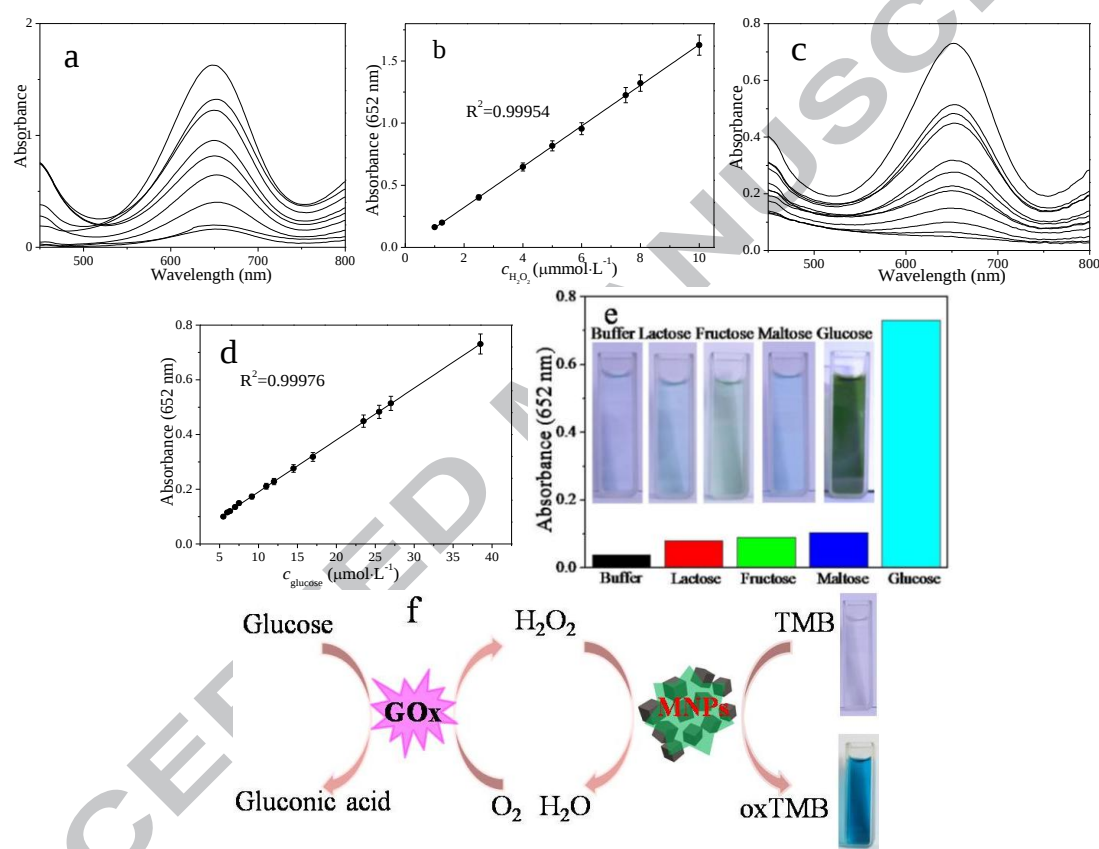


Fig. 9. H_2O_2 and glucose detection based on Fe_3O_4 MNPs. The UV-vis spectra of (a) H_2O_2 solution and (c) glucose solution with Fe_3O_4 MNPs and 816 $\mu\text{mol}\cdot\text{L}^{-1}$ TMB in acetate buffer (pH = 4.0). The concentration of H_2O_2 ($\mu\text{mol}\cdot\text{L}^{-1}$) in (a) from top to bottom is 10, 8, 7.5, 6, 5, 4, 2.5, 1.25, and 1. The concentration of glucose ($\mu\text{mol}\cdot\text{L}^{-1}$) in (c) from top to bottom is 38.5, 27, 25.5, 23.5, 17, 14.5, 12, 11, 7.5, 5.5, 0.00143, and 0.00016. The linear calibration plot for H_2O_2 (b) and glucose (d). Selectivity analysis for glucose detection by monitoring the absorbance at 652 nm (e), the analyte concentration were as follows: 10 $\text{mmol}\cdot\text{L}^{-1}$ lactose, 10 $\text{mmol}\cdot\text{L}^{-1}$ fructose, 10

mmol·L⁻¹ maltose, and 38.5 μmol·L⁻¹ glucose, inset: the color change with the different solutions. Schematic illustration of colorimetric determination of glucose using glucose (GOx) and Fe₃O₄ MNPs catalyzed reactions (f).

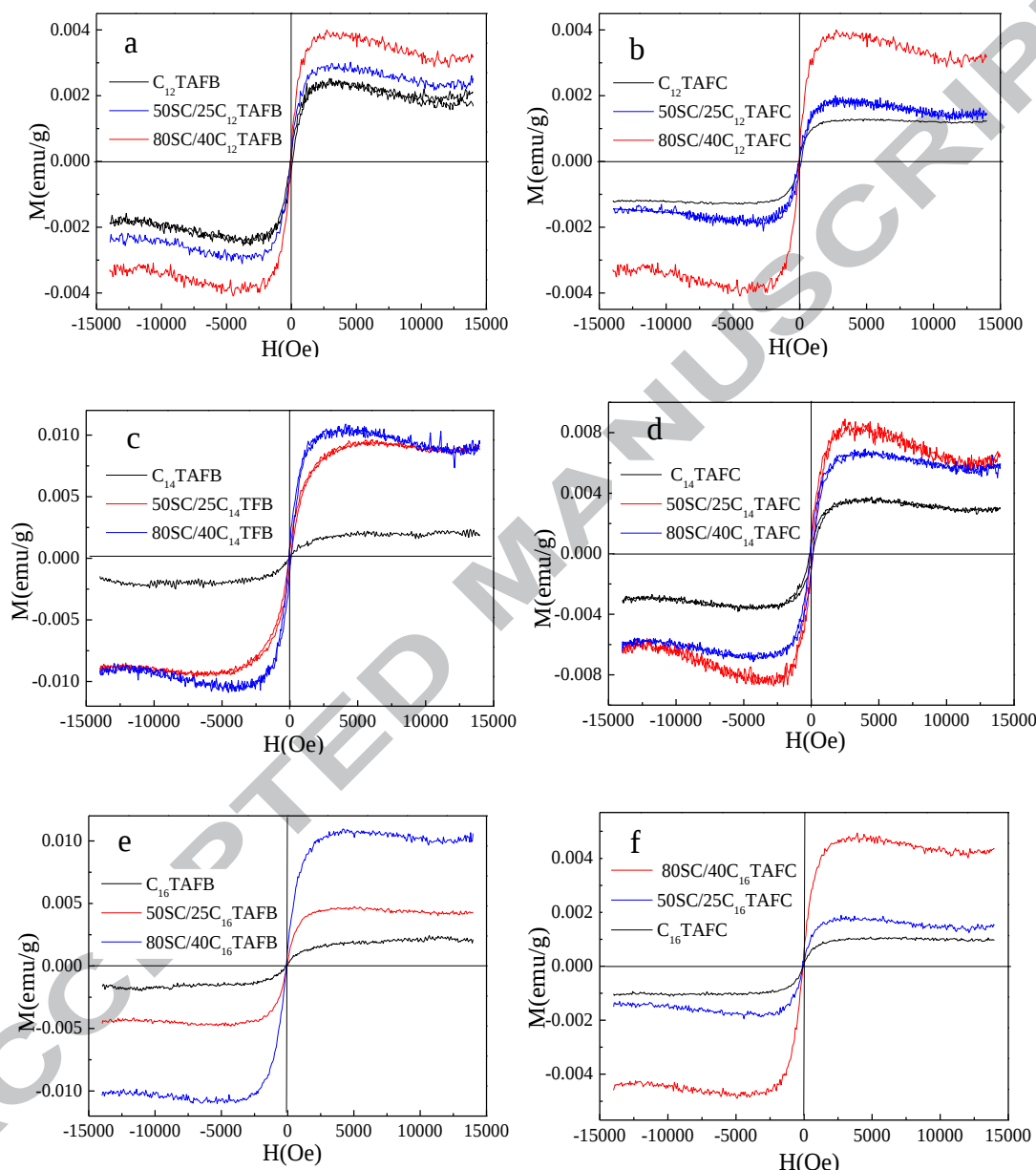


Fig. S1. Superconducting quantum interference device (SQUID) magnetometry of the magnetic surfactants, C_nTAFB (C) (n = 12, 14, 16), and the ferromagnetic C_nTAFB (C)/SC hydrogels: (a) C₁₂TAFB and C₁₂TAFB/SC hydrogels, (b) C₁₂TAFC and C₁₂TAFC/SC hydrogels, (c) C₁₄TAFB and C₁₄TAFB/SC hydrogels, (d) C₁₄TAFC and C₁₄TAFC/SC hydrogels, (e) C₁₆TAFB and C₁₆TAFB/SC hydrogels,

and (f) C_{16} TAFB and C_{16} TAFB/SC hydrogels. the concentration ($\text{mmol}\cdot\text{L}^{-1}$) of the hydrogels was inserted.

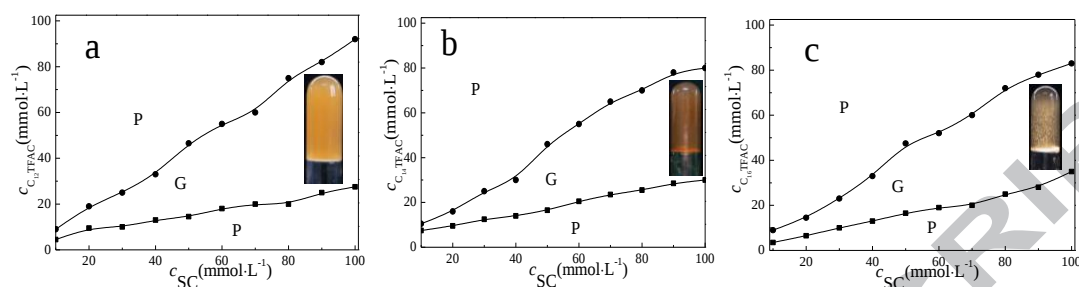


Fig. S2. Phase diagram of C_{12} TAFB/SC, C_{14} TAFB/SC, C_{16} TAFB/SC systems at $T = 25.0 \pm 0.1$ °C.

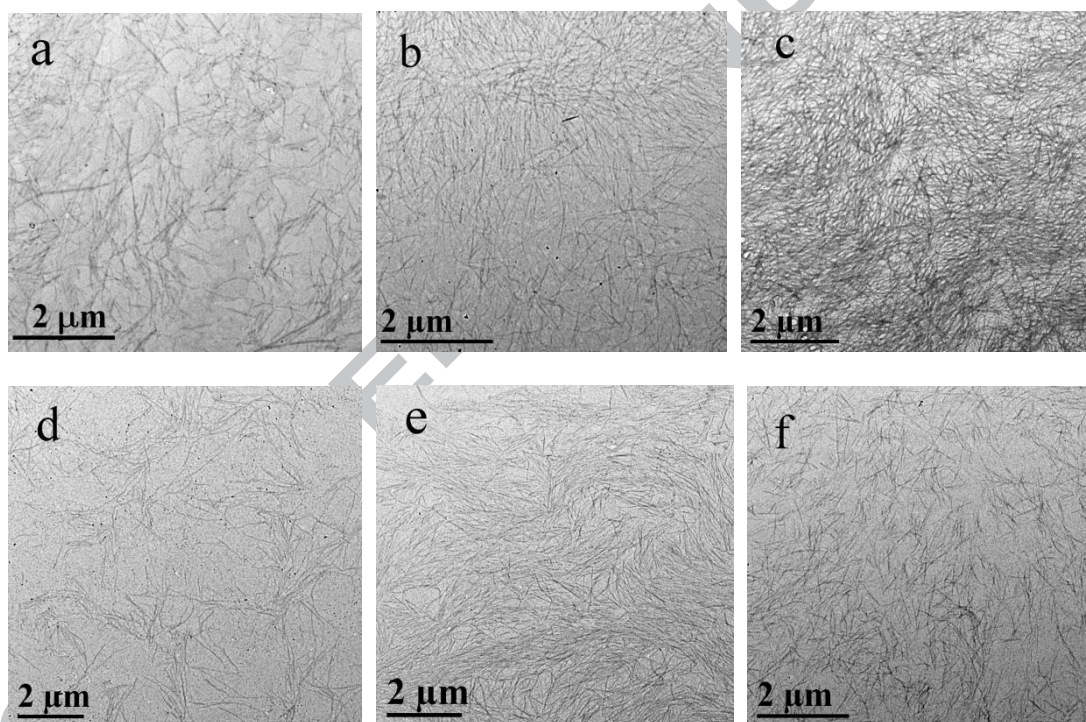


Fig. S3. TEM images of freeze-dried hydrogels formed by 20 $\text{mmol}\cdot\text{L}^{-1}$ SC/10 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (a), 40 $\text{mmol}\cdot\text{L}^{-1}$ SC/20 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (b), 60 $\text{mmol}\cdot\text{L}^{-1}$ SC/30 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (c), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/20 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (d), 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/35 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (e), and 50 $\text{mmol}\cdot\text{L}^{-1}$ SC/40 $\text{mmol}\cdot\text{L}^{-1}$ C_{14} TAFB (f).

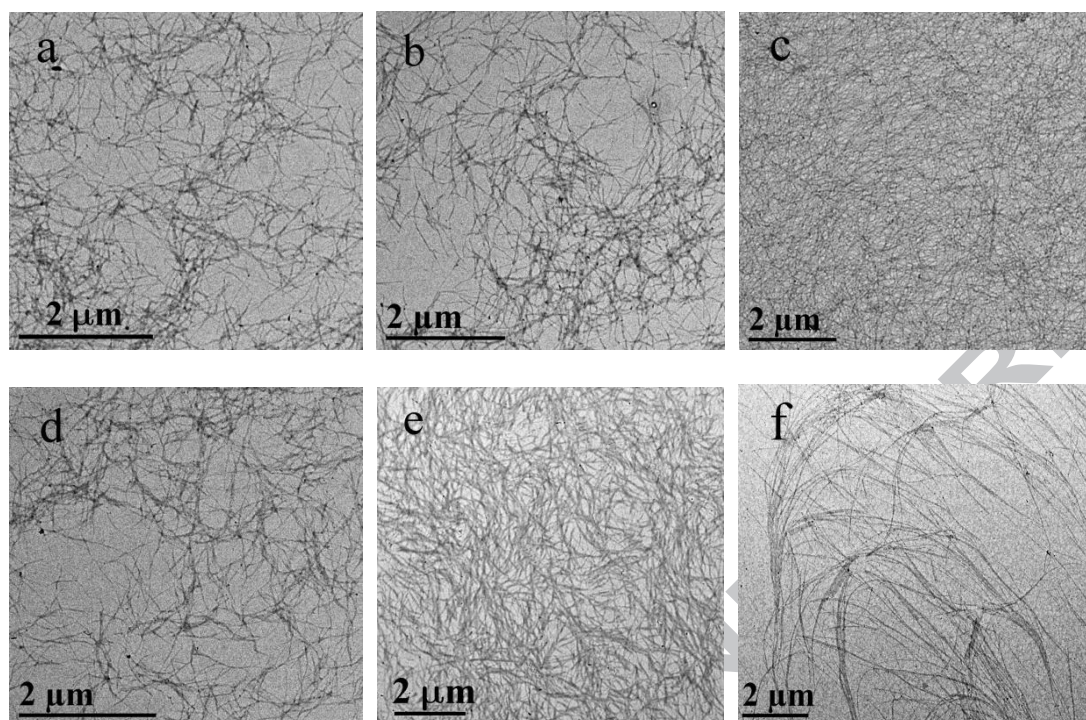


Fig. S4. TEM images of dried hydrogels formed by 20 mmol·L⁻¹ SC/10 mmol·L⁻¹ C₁₆TAFB (a), 40 mmol·L⁻¹ SC/20 mmol·L⁻¹ C₁₆TAFB (b), 60 mmol·L⁻¹ SC/30 mmol·L⁻¹ C₁₆TAFB (c), 50 mmol·L⁻¹ SC/20 mmol·L⁻¹ C₁₆TAFB (d), 50 mmol·L⁻¹ SC/35 mmol·L⁻¹ C₁₆TAFB (e), and 50 mmol·L⁻¹ SC/40 mmol·L⁻¹ C₁₆TAFB (f).



Fig. S5. Reversible stimuli-responsive transition of hydrogels (50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₂TAFB) triggered by shearing force and temperature.

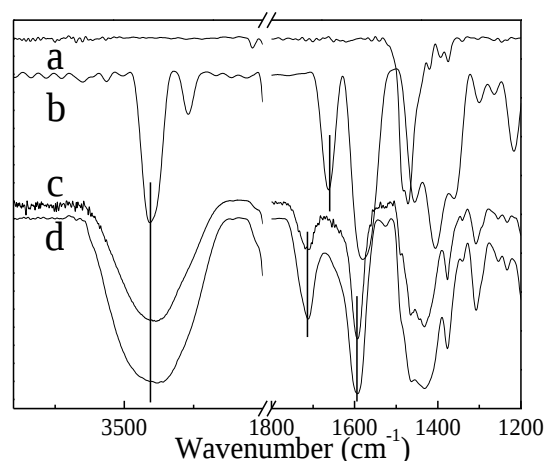


Fig. S6. FT-IR spectra of C₁₂TAFB (a), SC (b), xerogels formed by 50 mmol·L⁻¹ SC/25 mmol·L⁻¹ C₁₂TAFB (c) and 100 mmol·L⁻¹ SC/50 mmol·L⁻¹ C₁₂TAFB (d).

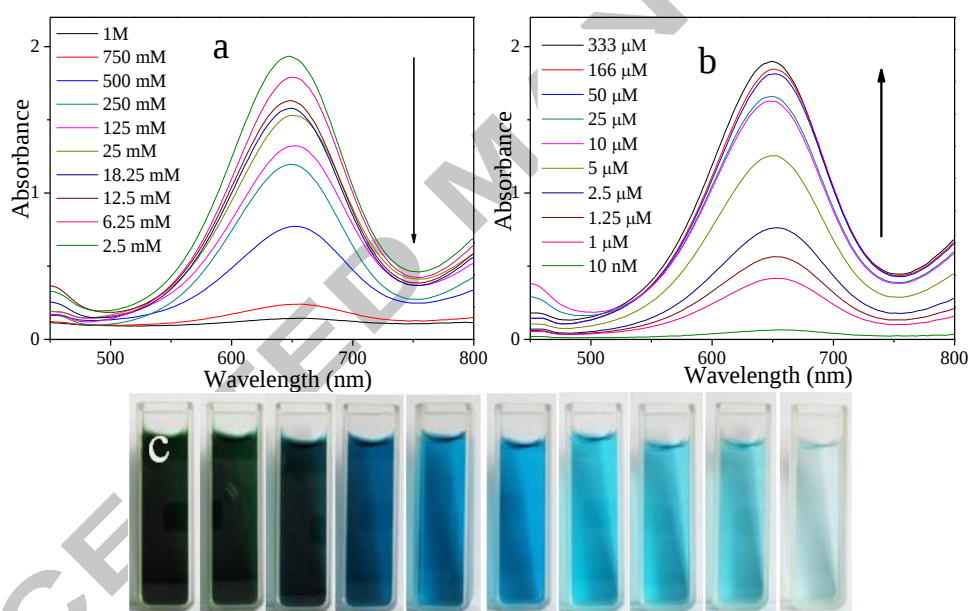


Fig. S7. H₂O₂ detection based on peroxidase-like Fe₃O₄ MNPs. The UV-vis spectra of H₂O₂ solution with Fe₃O₄ MNPs and 816 μmol·L⁻¹ TMB in acetate buffer (a, b). The images of color reaction of TMB with different concentrations of H₂O₂, the concentration of H₂O₂ (μmol·L⁻¹) from left to right is 1000, 500, 100, 50, 10, 5, 2.5, 1.25, 1, 0.01 (c).

Table 1 Gelation behavior of C_n TAFB (C) and sodium salts of bile acid systems in aqueous solutions at 25 °C

	Chain length (nm)[50]	Aggregates			CGC ^a (wt %)			Gelation time			Gelation number ^b		
		SC	SDC	SLC	SC	SDC	SLC	SC	SDC	SLC	SC	SDC	SLC
C ₁₂ TAFB	1.672	G ^c	G	P ^d	0.329	0.282		48 h	96 h		7936	9259	
C ₁₂ TAFC	1.672	G	G	P	0.320	0.270		72 h	108 h		7407	8547	
C ₁₄ TAFB	1.925	G	G	P	0.249	0.224		36 h	48 h		11111	12345	
C ₁₄ TAFC	1.925	G	G	P	0.250	0.227		40 h	54 h		10101	11111	
C ₁₆ TAFB	2.178	G	G	P	0.211	0.184		30 h	36 h		13888	14873	
C ₁₆ TAFC	2.178	G	G	P	0.217	0.193		36 h	48 h		12345	13888	

^aCGC: critical gelation concentration; ^bGelation number: the maximum number of solvent molecules immobilized by gelator molecules;⁴⁴ ^cG: Gels; ^dP: precipitates. SQUID magnetometry of Fe₃O₄ MNPs prepared from SC/C₁₂TAFB hydrogel.

Table 2 Michaelis constant (K_m) and maximal reaction rate (V_{max}) of Fe₃O₄ MNPs.

catalyst	substrate	K_m (mmol·L ⁻¹)	V_{max} (10 ⁻⁸ mol·L ⁻¹ ·s ⁻¹)
Fe ₃ O ₄ MNPs	TMB	0.091	5.18
	H ₂ O ₂	0.01957	1.26
HRP	TMB ^[27]	0.434	10.0
	H ₂ O ₂ ^[27]	3.70	8.71

Table S1 Dynamic rheology of SC/C₁₂TAFB hydrogels. The G' and G'' values were obtained from frequency sweep experiments

SC /C ₁₂ TAFB (mmol·L ⁻¹)	Storage modulus, G' (Pa)	Loss modulus, G'' (Pa)	Stiffness, (G'/G'')
20/10	120	12	10
40/20	360	60	6
50/25	1500	120	12.5
80/40	45000	10000	4.5
100/50	130000	30000	4.3

Table S2 Dynamic rheology of 50 mmol·L⁻¹ SC/C₁₂TAFB hydrogels. The G' and G'' values were obtained from frequency sweep experiments

50 mmol·L ⁻¹ SC/C ₁₂ TAFB (mmol·L ⁻¹)	Storage modulus, G' (Pa)	Loss modulus, G'' (Pa)	Stiffness, (G'/G'')
20	600	80	7.5
25	1500	150	10
30	4500	900	5
35	80000	15000	5.3
40	2000	400	5

Graphical abstract:



Fe_3O_4 nanoparticle prepared based on $\text{C}_{12}\text{TAFB/SC}$ hydrogels acted as a biosensor for H_2O_2 and glucose detection.