

# Efficient electrochemical biosensing of hydrogen peroxide on bimetallic $\text{Mo}_{1-x}\text{W}_x\text{S}_2$ nanoflowers

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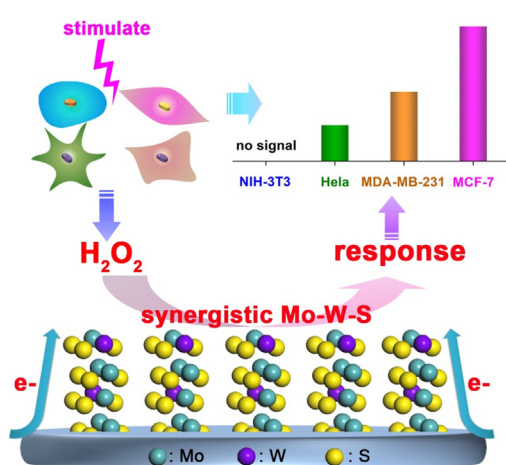
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## HIGHLIGHTS

- Bimetallic  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  identifies composition-dependent  $\text{H}_2\text{O}_2$  sensing associated with intermediate bindings.
- The optimal  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  accomplishes outstanding performance in  $\text{H}_2\text{O}_2$  sensing.
- The  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  distinguishes cancer cells via monitoring endogenous  $\text{H}_2\text{O}_2$ .

## GRAPHICAL ABSTRACT



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## ABSTRACT

Two-dimensional transition-metal dichalcogenides can serve as emerging biosensing platforms after rational structural optimization. Herein, we develop a series of  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  and investigate the composition-dependent sensing of hydrogen peroxide ( $\text{H}_2\text{O}_2$ ). Among them, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  affords high sensitivity ( $1290 \mu\text{A mM}^{-1} \text{cm}^{-2}$ ), good selectivity, and wide applicable concentration range ( $4 \times 10^{-1}$ – $1.0 \times 10^4 \mu\text{M}$ ). As indicated by theoretical investigations, such prominent performance stems from the bimetallic electronic configurations and the enhanced  $^*\text{OH}$  binding on surface. Moreover, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  is capable of monitoring trace amounts of  $\text{H}_2\text{O}_2$  released from normal cells and various cancer cells, which provides efficient cell detection for clinical diagnosis. In addition, the composition-dependence, as a result of electronic modulation on  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  surface, is further evidenced on electrocatalytic hydrogen evolution reaction, which highlights the promise in sensing and electrocatalysis that share similar electrochemical fundamentals.

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## 1. Introduction

Electrochemical detection of biomarkers (e.g. small molecules, DNA, proteins, cells, etc.) *in vitro* and *in vivo* is promising in real-time monitoring, clinical diagnosis and pathophysiology [1–4].

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They feature obvious advantages, including robustness, easy miniaturization, excellent detection limits, and also small analyte volumes, in comparison with other techniques (e.g., enzyme-linked immunosorbent assay, mass spectrometry, northern blot, etc.) that require technically complex equipment or time-consuming manipulation [5]. As a typical representative of reactive oxygen species (ROS) in biological systems, hydrogen peroxide ( $\text{H}_2\text{O}_2$ ) plays a key role in cell proliferation and death, response to chronic diseases, and intracellular signaling transduction [6–8]. For instance, the concentration of  $\text{H}_2\text{O}_2$  in tumor area is typically higher than that in normal tissue [9,10]. Thus rapid, accurate, and reliable determination of  $\text{H}_2\text{O}_2$  shows practical importance in biological analyses. In  $\text{H}_2\text{O}_2$  sensing, nanomaterials based non-enzymatic electrochemical biosensors can surmount the inherent problems of enzyme biosensors, such as rigorous storage conditions and short period of validity [11,12]. Rational structural optimization is anticipated to improve the sensing performance of non-enzymatic nanomaterials, regarding that  $\text{H}_2\text{O}_2$  sensing relies on the electrochemical redox processes of  $\text{H}_2\text{O}_2$  [13]. Non-enzymatic materials serve as electrocatalysts to boost the oxidation/reduction, thereby amplifying current response.

Two-dimensional (2D) transition-metal dichalcogenides (TMDs) have attracted attentions in biosensing due to their unique electronic/optical properties, versatile chemistry and easy surface-functionalization [14–17]. In particular, molybdenum disulfide ( $\text{MoS}_2$ ) based nanostructures are functional segments to detect proteins, DNA, cancer cells, cellular metabolism products, etc. [18–20]. In  $\text{H}_2\text{O}_2$  sensing, conventional  $\text{MoS}_2$  however suffers from low sensitivity on un-optimized surface. Therefore, many efforts in engineering particle size [21], edge-site exposure [22] and inter-layer structures [23] have been made. Besides, heteroatom doping is an alternative approach to promote sensing performance due to effective modification on electronic configurations. For instance, Ni [24,25], Cu [26], Ag [27] and N [28] are available dopants. However, such foreign elements with quite different atomic size and chemical properties from Mo or S usually destroy the parent lattices at high doping content, leading to unsatisfactory sensing response [29]. As congeners, W has the same valence electrons and chemical properties with Mo, and their disulfides share the similar layered structures. The solid-solution alloy phase of Mo-W-S will enable the precise and adequate electronic regulation toward optimal performance [30].

Recently, our work for the first time discovered that expanding the interlayer spacing of  $\text{MoS}_2$  can boost the electrochemical biosensing performance due to electronic regulation [23]. However, the effects of heteroatom doping and solid-solution-alloy have not been studied in this promising system, which are anticipated to bring further improvement in applications. Herein, we fabricate a series of  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  and investigate their composition-dependent sensing for  $\text{H}_2\text{O}_2$ . The  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  affords high sensitivity ( $1290 \mu\text{A mM}^{-1} \text{cm}^{-2}$ ), good selectivity, and wide applicable concentration range ( $4 \times 10^{-1}$ – $1.0 \times 10^4 \mu\text{M}$ ) for  $\text{H}_2\text{O}_2$  detection, superior to  $\text{MoS}_2$ ,  $\text{WS}_2$  and other counterparts with a high W content. As further confirmed by theoretical investigations, such performance stems from the enhanced  $^*\text{OH}$  binding on surface. However, further increasing W content in  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  ( $x > 0.50$ ) will lead to coarsened products that lose a large part of active edge-sites, which accounts for the prohibited performance. Furthermore, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  is capable of monitoring trace amounts of  $\text{H}_2\text{O}_2$  released from normal cells and different cancer cells, which provides efficient cell detection for clinical diagnosis. The above composition-dependence, as a result of the electronic modulation on  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$ , is also evidenced on electrocatalytic hydrogen evolution reaction (HER), highlighting the universal promotion in sensing and electrocatalysis that share similar electrochemical fundamentals.

## 2. Experimental section

### 2.1. Materials and reagents

Ammonium heptamolybdate tetrahydrate ( $(\text{NH}_4)_6\text{Mo}_7\text{O}_{24} \cdot 4\text{H}_2\text{O}$ , 99.5%, Aladdin), sodium tungstate dihydrate ( $\text{Na}_2\text{WO}_4 \cdot 2\text{H}_2\text{O}$ , 99%, Aladdin), thiourea (99%, Aladdin), *N,N*-dimethylformamide (DMF, 99.5%, Aladdin), hydrogen peroxide (30%, Guangzhou chemical reagent factory) and phosphate-buffered saline (PBS, 0.1 M, pH = 7.4, Gibco) were used for experiments as received. Phorbol 12-myristate 13-acetate (PMA, 98%), catalase ( $5000 \text{ U mg}^{-1}$ ) and Nafion solution (5 wt% in lower aliphatic alcohols and water) were purchased from Sigma-Aldrich. All chemicals were of analytical grade and used as received without further purification. All aqueous solutions were prepared using ultrapure water ( $>18 \text{ M}\Omega$ ).

### 2.2. Physical characterization

Scanning electronic microscopy (SEM) was taken on a ZEISS ULTRA55. Transition electronic microscopy (TEM), energy dispersive spectroscopy (EDS) and elemental mapping were conducted on a JEOL JEM 2100F. X-ray diffraction (XRD) was performed on Bruker D8 Advance diffractometer using  $\text{Cu K}\alpha$  radiation ( $\lambda = 1.54056 \text{ \AA}$ ). Raman spectra were recorded on a laser confocal Raman microspectrometer (HR-800, Horiba Jobin Yvon, Ltd.), with an excitation laser wavelength of 532 nm. X-ray photoelectron spectroscopy (XPS) was processed on a Thermo scientific (Escalab 250Xi), using C 1s ( $284.6 \text{ eV}$ ) as a reference.

### 2.3. Material synthesis

The synthesis of  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$ ,  $\text{MoS}_2$  and  $\text{WS}_2$  nanoflowers was conducted via a simple one-pot hydrothermal process. Typically, 5.0 mL of distilled water and 5.0 mL of DMF were mixed as a solvent. A varied amount of  $(\text{NH}_4)_6\text{Mo}_7\text{O}_{24} \cdot 4\text{H}_2\text{O}$  and  $\text{Na}_2\text{WO}_4 \cdot 2\text{H}_2\text{O}$  (total  $n_{\text{Mo+W}}$  is fixed as 2 mmol) and 1.525 g of thiourea (20 mmol) were dissolved into the above solvent, which was then stirred for 30 min to get a clean solution. The solution was transferred to a Teflon-lined stainless steel autoclave. After reaction at  $240^\circ\text{C}$  for 3 h, the product was collected by centrifugation, washed with ethanol and water at least 3 times, and dried at  $50^\circ\text{C}$  overnight.  $\text{MoS}_2$  or  $\text{WS}_2$  is obtained by adding only molybdenum or tungsten sources, respectively.

### 2.4. Electrochemical measurement

Electrochemical test was conducted with a conventional three-electrode system on a CHI 650E electrochemical workstation (Chenhua Instruments Shanghai Co., Ltd, China). A Ag/AgCl (3 M KCl) electrode and a platinum wire were used as the reference and counter electrodes, respectively.

The preparation of working electrodes is as follow. Prior to modification, a bare rotating disk electrode (RDE) or glassy carbon electrode (GCE) was polished with 0.3 and  $0.03 \mu\text{m}$  alumina powder on a polishing cloth to obtain a mirror like surface. 4 mg of  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  and 40  $\mu\text{L}$  of 5 wt% Nafion solution were dispersed in 1 mL of 4:1 vol/vol deionized water–ethanol mixed solvent, which was vigorously sonicated for at least 30 min to generate a homogeneous ink. Then, 15  $\mu\text{L}$  (5  $\mu\text{L}$  in GCE case) of the ink was loaded onto a RDE (5 mm diameter,  $0.196 \text{ cm}^2$ ) or a GCE ( $0.07 \text{ cm}^2$ ), and dried naturally in air. Electrochemical sensing  $\text{H}_2\text{O}_2$  were performed at  $25^\circ\text{C}$  in 0.1 M PBS buffer, and electrochemical hydrogen evolution was performed in 0.5 M  $\text{H}_2\text{SO}_4$  solution.

## 2.5. Electrochemical determination of intracellular $H_2O_2$ released from living cells

MDA-MB-231 (human breast adenocarcinoma cell line), MCF-7 (human breast cancer cells) and Hela (human cervical cancer cells) were obtained from Southern Medical University (Guangzhou, China). MDA-MB-231 cells were incubated in the flask ( $75\text{ cm}^2$ ) in Roswell Park Memorial Institute (RPMI) Medium 1640 basic containing 10% FBS (fetal bovine serum) and 1% antibiotics overnight (penicillin streptomycin,  $1 \times 10^4\text{ U/mL}$ ), plated in a 5%  $CO_2$  and 95% air at  $37^\circ\text{C}$ . MCF-7 and Hela were cultured in Dulbecco's modified Eagle medium (DMEM) containing 10% FBS,  $100\text{ U mL}^{-1}$  penicillin, and  $100\text{ mg mL}^{-1}$  streptomycin at  $37^\circ\text{C}$  in a 5%  $CO_2$  environment. Cancer cells were digested with 0.25 wt% trypsin at  $37^\circ\text{C}$  for 120 s and separated from the culture medium by centrifugation (1000 rpm) for 5 min, then washed with PBS (0.01 M, pH 7.4) for three times, and finally suspended in PBS to  $5 \times 10^6$  cells  $\text{mL}^{-1}$ .

The 1 mL cancer cells were mixed with 49 mL 0.1 M PBS buffer to reach its concentration of  $1 \times 10^5$  cells  $\text{mL}^{-1}$ . PMA was employed as the stimulant for intracellular  $H_2O_2$  release. To detect  $H_2O_2$  released from cells, the response of amperometric current-time plot was performed on the  $Mo_{1-x}W_xS_2$ /RDEs.

## 2.6. Theoretical calculations

The OH adsorption energy ( $\Delta E_{OH}$ ) calculations on the edge of  $MoS_2$ ,  $Mo_{0.75}W_{0.25}S_2$  and  $Mo_{0.50}W_{0.50}S_2$  were carried out by using Cambridge Sequential Total Energy Package (CASTEP) module in Material Studio. And  $\Delta E_{OH}$  was calculated as:

$$\Delta E_{OH} = E_{(\text{slab}+\text{adsorbate})} - E_{(\text{slab})} - E_{(\text{adsorbate})}$$

where  $E_{(\text{slab}+\text{adsorbate})}$ ,  $E_{(\text{slab})}$  and  $E_{(\text{adsorbate})}$  were the total energy of slab with adsorbate, the energy of pure slab/facet and the energy of adsorbate (OH) in the gas phase, respectively.

The exchange correlation energy was described by the generalized gradient approximation (GGA) with the Perdew-Burke-Ernzerhof (PBE) functional [31,32]. The kinetic energy cutoff for the plane-waves expansion was 450 eV. The self-consistent field (SCF) tolerance was  $1 \times 10^{-6}$  eV. The Brillouin zone was sampled by  $3 \times 3 \times 1$  k-points.  $MoS_2$ ,  $Mo_{0.75}W_{0.25}S_2$  and  $Mo_{0.50}W_{0.50}S_2$  crystal structure with an expanded interlayer spacing of 9.4 Å adopts a hexagonal crystal structure, using  $2 \times 2 \times 1$  supercell. Vacuum thickness of 15 Å was chosen to simulate the surface properties.

## 3. Results and discussion

### 3.1. Characterization of $Mo_{1-x}W_xS_2$

A series of  $Mo_{1-x}W_xS_2$  is fabricated via a one-pot hydrothermal process with various feeding molar ratios of Mo/W. The Mo/W ratio in products determined by EDS is consistent with the feeding one. As depicted in the XRD patterns (Fig. 1a), all the  $Mo_{1-x}W_xS_2$  shows an obviously down-shifting (0 0 2) peak at  $2\theta = 9.35^\circ$  ( $d \approx 0.94\text{ nm}$ ), in comparison with hexagonal  $MoS_2$  (JCPDS No.: 37-1492) and  $WS_2$  (JCPDS No.: 08-0237), but retains other peaks such as (0 1 0) and (1 1 0) without shift. This indicates an interlayer expanded structure along the [0 0 2] direction. According to our and other groups' previous reports [23,33], the strong interactions between  $MoS_2$  monolayers and excessive thiourea or DMF derivatives will expand the typical (0 0 2) d-spacing (0.62 nm) of  $MoS_2$  to a large one (e.g., 0.94 nm). As the W content increases, the diffraction peaks become sharp and narrow, indicating the enlarged and thickened nanosheets. In Raman spectra (Fig. 1b), the  $MoS_2$  exhibits two distinct bands at  $379.7$  and  $402.9\text{ cm}^{-1}$ , corresponding to the  $E_{2g}^1$  (in-plane) and  $A_{1g}$  (out of plane) vibrations, respectively [34]. The peaks at  $349.5$ ,  $354.8$  and  $415.3\text{ cm}^{-1}$  are observed on  $WS_2$ , which can be ascribed to 2 LA(M) (the second-order mode of longitudinal acoustic phonon),  $E_{2g}^1$  (in-plane) and  $A_{1g}$  (out of plane), respectively [35]. With increasing W content, the  $E_{2g}^1$  band shifts to lower wavenumbers while  $A_{1g}$  mode to higher range. This variation is in accordance with the evidenced spectral evolution in previous reports, and probably due to strong interactions between Mo and W [29].

SEM investigation clearly reveals the flower-like samples consisting of stacked nanosheets (Fig. 2). The  $MoS_2$  nanoflowers present a small size ( $\sim 200\text{ nm}$ ), and the nanosheets are thin (Fig. 2a). By contrast, the  $WS_2$  assembled by thicker nanoplates is as large as several microns (Fig. 2f). This suggests the different growth of  $MoS_2$  and  $WS_2$  crystals. In the case of  $Mo_{1-x}W_xS_2$ , introducing a small amount of W has slight influences on the size (e.g.,  $Mo_{0.75}W_{0.25}S_2$  and  $Mo_{0.50}W_{0.50}S_2$ ), but high x in  $Mo_{0.33}W_{0.67}S_2$  and  $Mo_{0.20}W_{0.80}S_2$  leads to the coarsened products. Obviously, the formers will be beneficial for sensing application.

TEM observation shows that the flower-like  $Mo_{0.75}W_{0.25}S_2$ , as a model sample, consists of thin nanosheets (Fig. 3a). And the high-resolution TEM (HR-TEM) identifies the lattice fringes of 0.94 and 0.27 nm on the nanosheets (Fig. 3b). The former is ascribed to the expanded (0 0 2) interlayers, agreeing with that of XRD results (Fig. 1a). Such value keeps the same in single-component  $MoS_2$  and

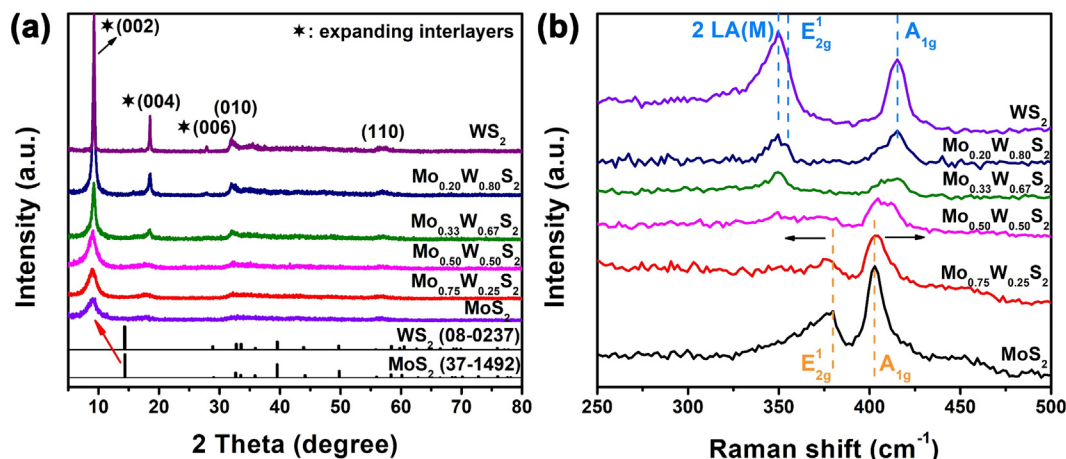
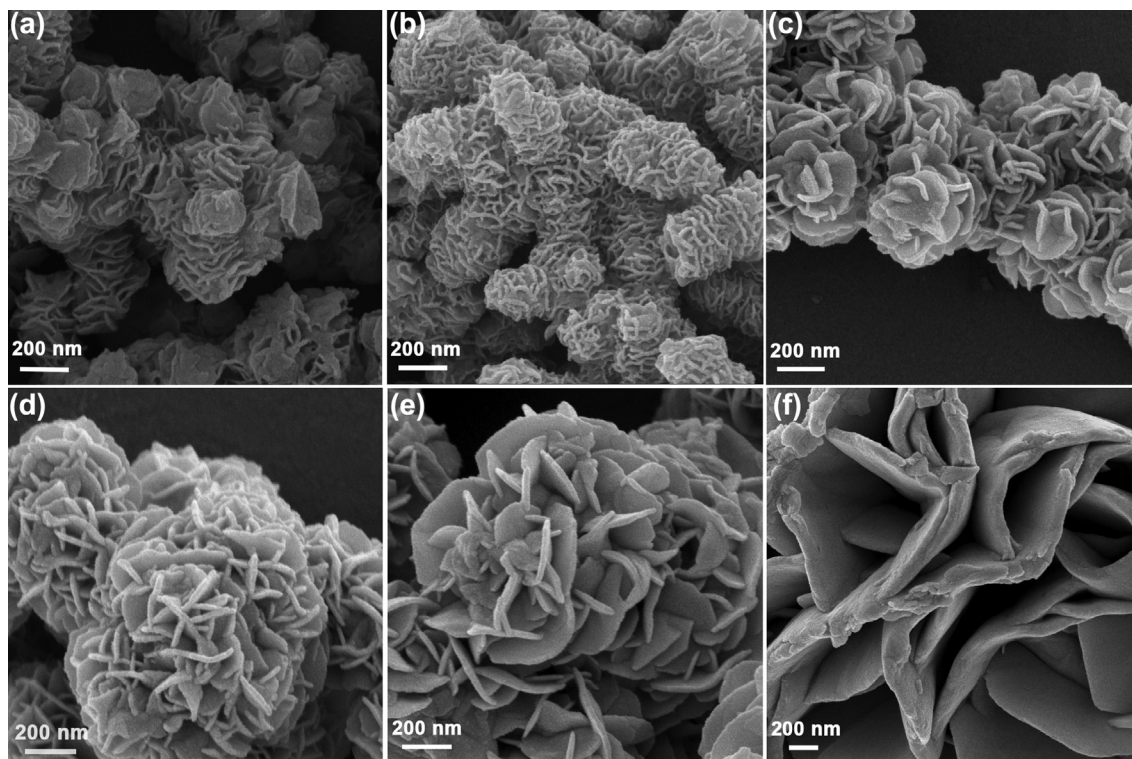
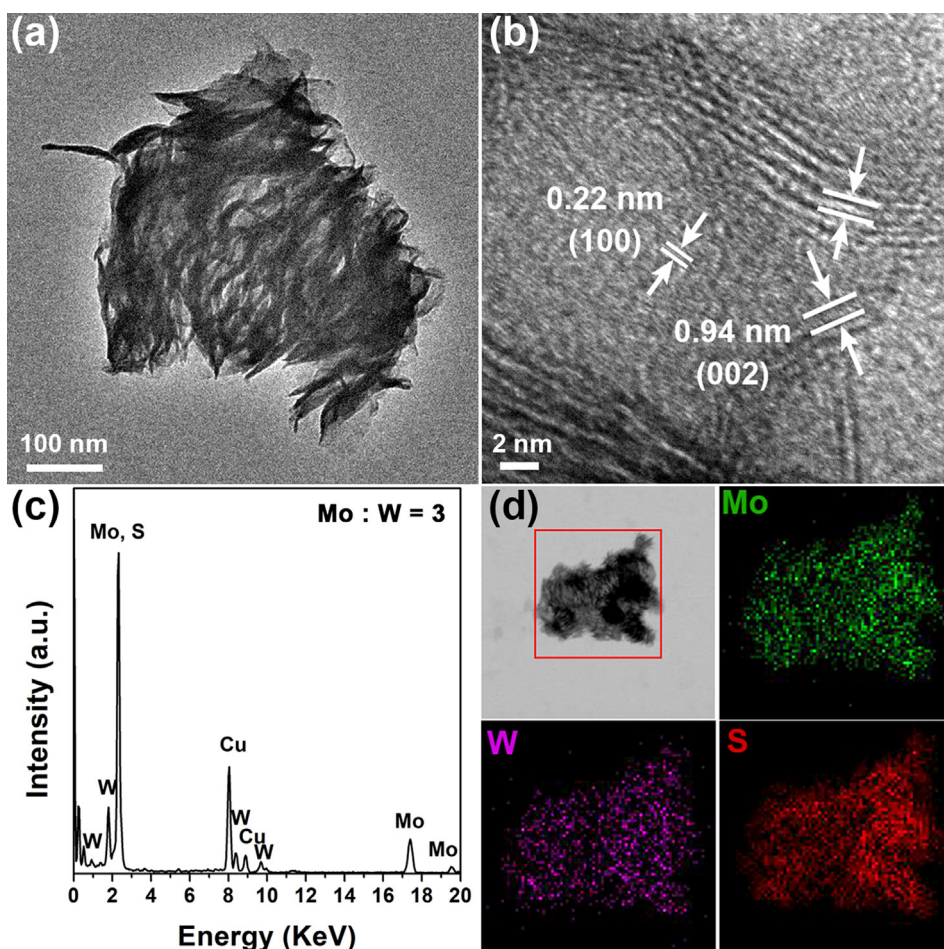


Fig. 1. (a) XRD patterns and (b) Raman spectra of  $MoS_2$ ,  $WS_2$  and  $Mo_{1-x}W_xS_2$ .



**Fig. 2.** SEM images of (a)  $\text{MoS}_2$ , (b)  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$ , (c)  $\text{Mo}_{0.50}\text{W}_{0.50}\text{S}_2$ , (d)  $\text{Mo}_{0.33}\text{W}_{0.67}\text{S}_2$ , (e)  $\text{Mo}_{0.20}\text{W}_{0.80}\text{S}_2$  and (f)  $\text{WS}_2$ .



**Fig. 3.** (a) TEM and (b) HR-TEM images, (c) EDS pattern and (d) corresponding elemental mapping of the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  nanoflowers.

WS<sub>2</sub> (Figs. S1 and S2 in Supplementary materials). And the latter can be assigned to the (0 1 0) of Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub>, which is non-affected in interlayer expanded sulfides. Moreover, the EDS attached on TEM shows the signals of Mo, W, S, C and N, and the additional peak for Cu is associated with the background of support grid (Fig. 3c). The Mo/W atomic ratio is confirmed as 3.0, in accordance with the feeding ratio. Elemental mapping further presents the uniform distribution of Mo, W and S on the nanosheets (Fig. 2d), indicating the uniform integration of W and Mo in Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>.

XPS survey spectra reveal the surface composition of MoS<sub>2</sub>, Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> and WS<sub>2</sub> (Fig. S3 in Supplementary materials). The elements of Mo, W and S are observed in Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>, while W is absent in MoS<sub>2</sub>, and Mo in WS<sub>2</sub>. The chemical states of the above elements are further analyzed. As showed in Fig. 4a, the Mo profile of MoS<sub>2</sub> can be deconvoluted into five peaks. The peak at 225.9 eV corresponds to the S 2s, and the ones at 228.7 and 232.1 eV are ascribed to the Mo 3d<sub>5/2</sub> and 3d<sub>3/2</sub> of Mo<sup>4+</sup> in MoS<sub>2</sub>, respectively [36,37]. The couple at 232.9 and 235.5 eV is ascribed to the small amount of Mo<sup>6+</sup> that is due to the slight oxidation of MoS<sub>2</sub> in air ambience. Such surface oxidation is depressed in bimetallic Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>, which is helpful to expose more surface active sites. When W proportion increases (Mo<sub>0.50</sub>W<sub>0.50</sub>S<sub>2</sub>, Mo<sub>0.33</sub>W<sub>0.67</sub>S<sub>2</sub> and Mo<sub>0.20</sub>W<sub>0.80</sub>S<sub>2</sub>), the binding energy of Mo<sup>4+</sup> affords a red-shift as compared with bare MoS<sub>2</sub>. Meanwhile, the W 4f profile of WS<sub>2</sub> can be deconvoluted into two couples (Fig. 4b). The ones at 31.8 and 33.9 eV are related to W<sup>4+</sup> in WS<sub>2</sub>, the other is associated with the W<sup>6+</sup> of surface oxides [38,39]. With the fixed values for W<sup>6+</sup>, the couple of W<sup>4+</sup> in Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> presents a blue-shift with increasing Mo, indicating rich electronic interactions between Mo and W. In addition, the profiles of S 2p keeps consistent in all the above samples (Fig. 4c).

### 3.2. Electrochemical H<sub>2</sub>O<sub>2</sub> sensing on Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>

In electrochemical H<sub>2</sub>O<sub>2</sub> sensing, the MoS<sub>2</sub>, WS<sub>2</sub> and Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> are modified onto RDEs to measure the electrochemical signals responding to H<sub>2</sub>O<sub>2</sub> injection (Fig. 5a). The Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> affords an obviously increased current in the presence of H<sub>2</sub>O<sub>2</sub>, and performs more sensitively than bare MoS<sub>2</sub> and WS<sub>2</sub>, indicating the promoted sensing due to W doping into MoS<sub>2</sub>. Such response is

also superior to that on other Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> with different compositions (Fig. S4 in Supplementary materials). More details for H<sub>2</sub>O<sub>2</sub> sensing were further assessed by amperometric *i*-*t* curves in response to H<sub>2</sub>O<sub>2</sub> concentration. The test was conducted by successively adding H<sub>2</sub>O<sub>2</sub> into a 0.1 M PBS solution, at a working potential of -0.6 V vs. Ag/AgCl (3 M KCl). As shown in Fig. 5b, the MoS<sub>2</sub>, WS<sub>2</sub> and Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> exhibit satisfactory reproducibility, and all the Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> delivers higher increase in response currents than the mono-metallic disulfides (MoS<sub>2</sub> and WS<sub>2</sub>), indicating the synergic enhancement by Mo and W components. Accordingly, Fig. 5c summarizes the average changes of currents responding to injecting H<sub>2</sub>O<sub>2</sub>. The changes on Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> are more sensitive than that on MoS<sub>2</sub> and WS<sub>2</sub>. And the Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> reaches a maximum increase, indicating the most sensitive response due to the optimal composition. In addition, the sensitive response on the Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> is also confirmed at a work potential from -0.05 to -0.70 V (Fig. S5 in Supplementary materials).

According to previous reports, the cathodic H<sub>2</sub>O<sub>2</sub> sensing proceeds via H<sub>2</sub>O<sub>2</sub> reduction to H<sub>2</sub>O [13,32]. And the rate-determining step of electrochemical H<sub>2</sub>O<sub>2</sub> reduction is the cleavage of O—O bond to form adsorbed \*OH, which is correlated with the \*OH binding on material surface. In this regard, density functional theoretical (DFT) calculations were conducted to reveal the varied binding energy. The high proportion of W obviously leads to the enlarged size of Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> (e.g., Mo<sub>0.33</sub>W<sub>0.67</sub>S<sub>2</sub> and Mo<sub>0.20</sub>W<sub>0.80</sub>S<sub>2</sub>), and thus other impacts beyond electronic effects emerge on sensing. Thereby, only the MoS<sub>2</sub>, Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> and Mo<sub>0.50</sub>W<sub>0.50</sub>S<sub>2</sub> with consistent particle sizes are taken into account. Fig. 5d presents the chemisorption configuration and the binding energy of \*OH on the edge (1 0 0). The value on the Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> is -3.7 eV, more negative than that on MoS<sub>2</sub> and Mo<sub>0.50</sub>W<sub>0.50</sub>S<sub>2</sub>, indicating the stronger binding. This is beneficial for the cleavage of O—O bond during H<sub>2</sub>O<sub>2</sub> reduction, and responsible for the sensitive response in H<sub>2</sub>O<sub>2</sub> detection.

Fig. 6a shows the *i*-*t* curve of a Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> modified RDE upon continuously injecting H<sub>2</sub>O<sub>2</sub> at a holding potential of -0.6 V (vs. 3 M Ag/AgCl). The electrode responds quickly and achieves a steady current within 3 s. Moreover, in order to investigate the stability of Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> in H<sub>2</sub>O<sub>2</sub> condition, the instrument is turn off for 250 s, and then turn on again. The current signal returns to its original level in a short time. The quick and steady

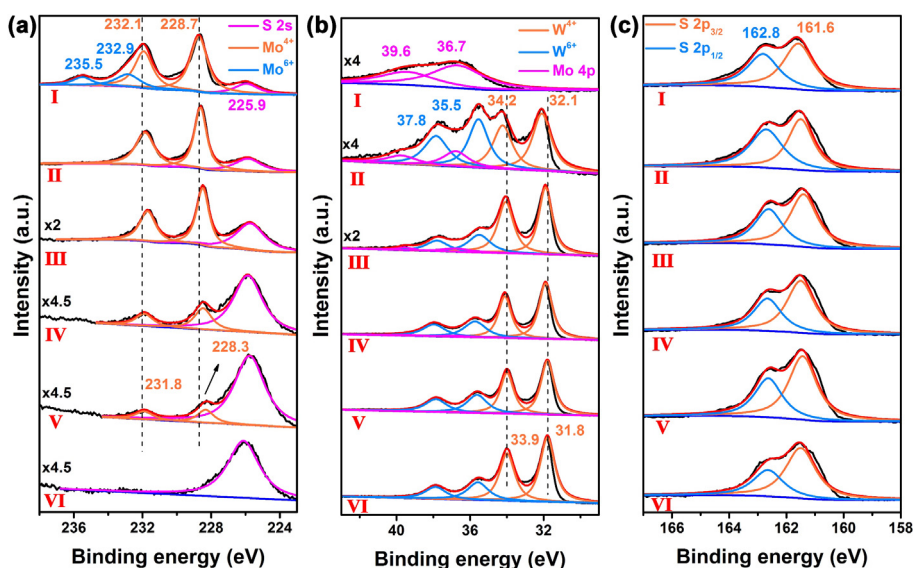
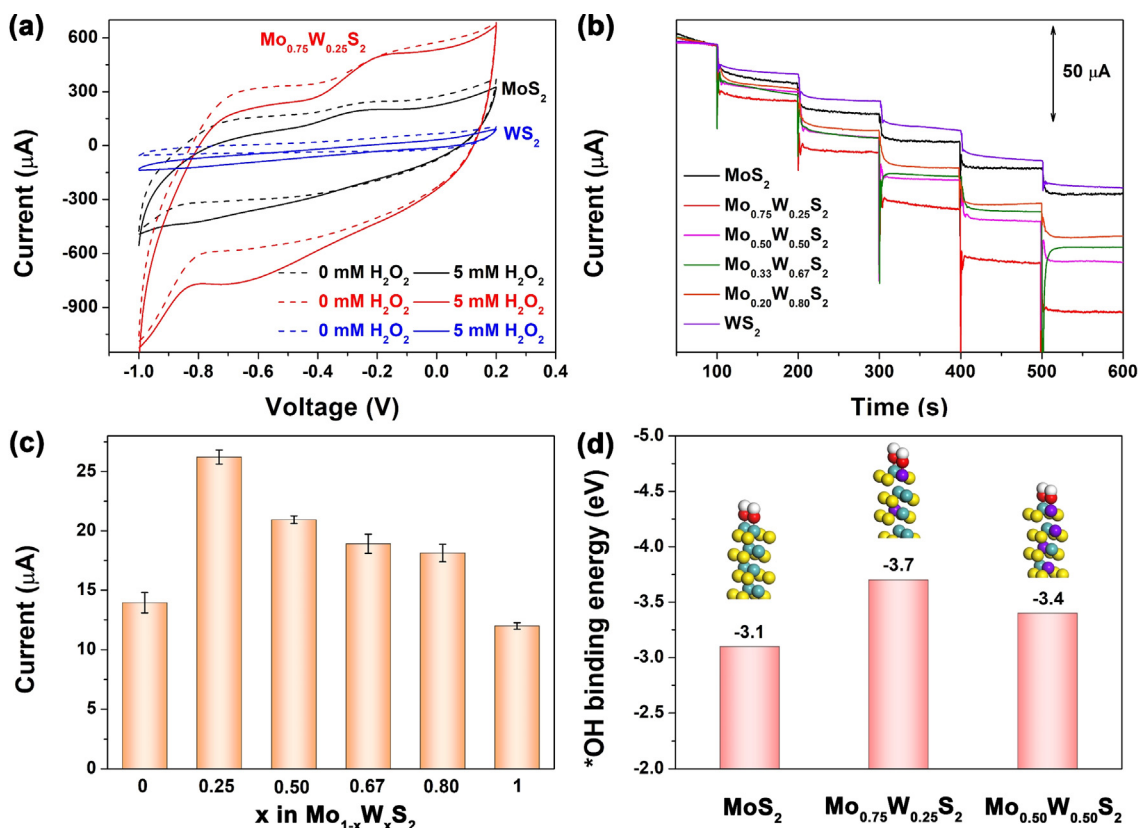
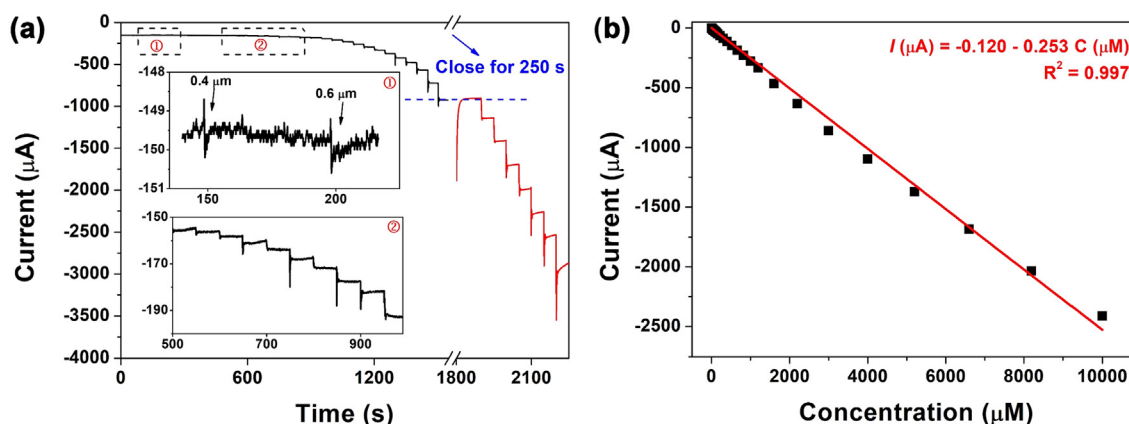


Fig. 4. XPS spectra of (a) Mo 3d, (b) W 4f and (c) S 2p in Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub> nanoflowers (I: MoS<sub>2</sub>, II: Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub>, III: Mo<sub>0.50</sub>W<sub>0.50</sub>S<sub>2</sub>, IV: Mo<sub>0.33</sub>W<sub>0.67</sub>S<sub>2</sub>, V: Mo<sub>0.20</sub>W<sub>0.80</sub>S<sub>2</sub> and VI: WS<sub>2</sub>).



**Fig. 5.** (a) CVs responses of MoS<sub>2</sub>/RDE, WS<sub>2</sub>/RDE and Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub>/RDE in the absence and presence of 5 mM H<sub>2</sub>O<sub>2</sub>. (b) Amperometric *i-t* curves of Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>/RDE in response to the successive addition of 100 μM H<sub>2</sub>O<sub>2</sub>, and (c) the corresponding current variation associated with *x* in Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>. (d) Chemisorption configuration (S: yellow, Mo: wathet blue, W: purple, O: red, and H: white) and binding energy of \*OH on the edge of MoS<sub>2</sub>, Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> and Mo<sub>0.50</sub>W<sub>0.50</sub>S<sub>2</sub>. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)

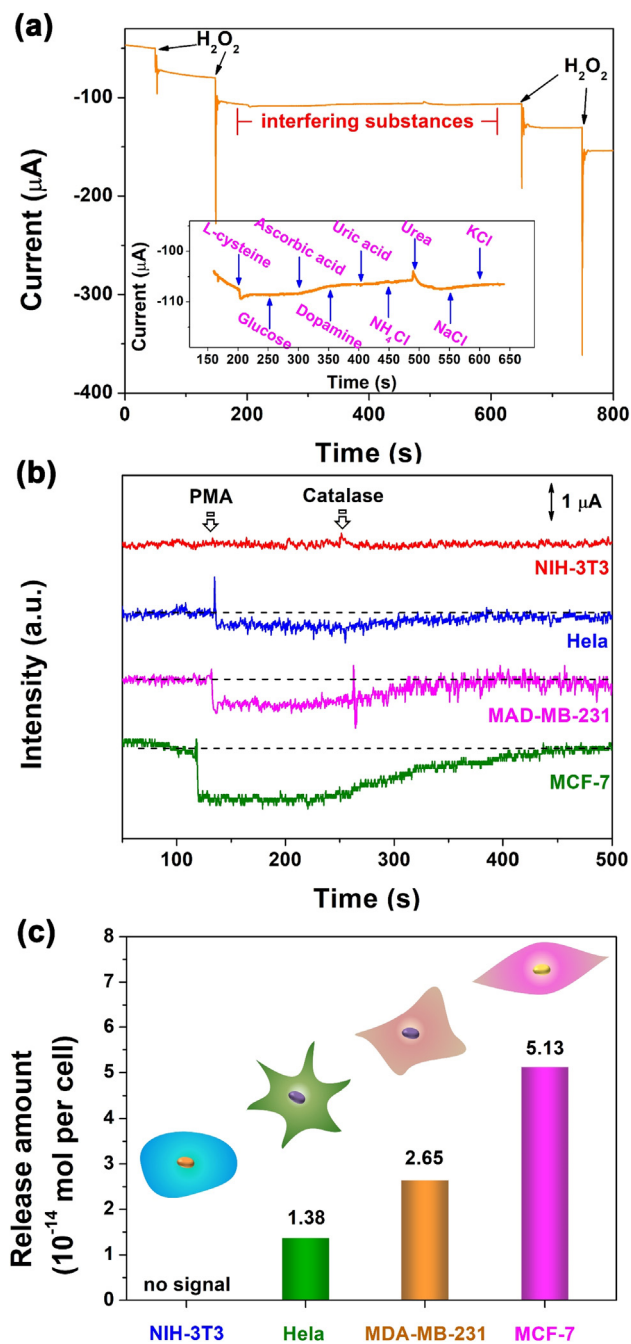


**Fig. 6.** (a) Amperometric response of a Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub>/RDE to dropwise adding H<sub>2</sub>O<sub>2</sub>, and (b) calibration curve of current vs. H<sub>2</sub>O<sub>2</sub> concentration.

response is possibly related to the fast H<sub>2</sub>O<sub>2</sub> reduction on the edge-sites of Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub>. The corresponding calibration curve between current response and H<sub>2</sub>O<sub>2</sub> concentration in Fig. 6b gives the regression equation of  $I (\mu A) = -0.253 C_{H_2O_2} (\mu M) - 0.120$  ( $R^2 = 0.997$ ) in a wide linear range of  $4 \times 10^{-1} - 1.0 \times 10^4 \mu M$ . Calculated from the slope of equation, the sensor shows a high sensitivity of  $1290 \mu A \text{ mM}^{-1} \text{ cm}^{-2}$ . The limit of detection (LOD) of this sensor is calculated as  $0.3 \mu M$  through the formula:  $\text{LOD} = 3S_b/S$  (Where  $S_b$  is standard deviation of blank signal, and  $S$  is sensitivity). Our previously developed MoS<sub>2</sub> with expanded interlayers could give higher sensitivity and lower LOD, but its sensitivity obviously decreased at high H<sub>2</sub>O<sub>2</sub> concentration [23], showing nar-

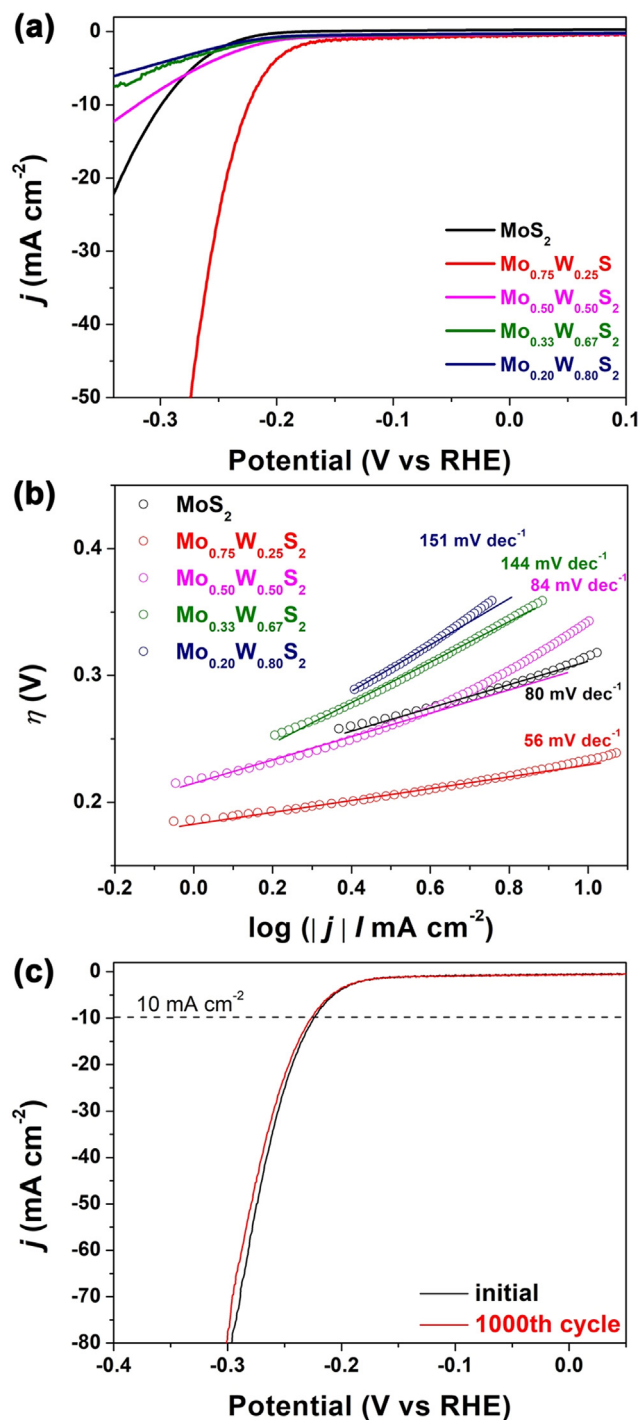
row applicable range in comparison with the Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> herein. This is possibly associated with the different conditions in hydrothermal synthesis. To study the composition-dependence of Mo<sub>1-x</sub>W<sub>x</sub>S<sub>2</sub>, reducible DMF was used as the reducing agent and co-solvent to ensure the formation of tungsten sulfides. In further comparison with recently reported materials, the Mo<sub>0.75</sub>W<sub>0.25</sub>S<sub>2</sub> performs at a high level (Table S1 in Supplementary materials). Its sensitivity or LOD outperforms those even involving enzymes or precious metals. As indicated, rational engineering on TMDs can reach the outstanding sensing performance even free from enzymes and precious metals, which will undoubtedly promote the cost-efficiency of sensing materials in practical use.

Before being applied to real samples, the sensing selectivity of the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  was concerned, because the capability of recognizing target molecules in complex biological environment is practically important. Possible interferences including L-cysteine, glucose, ascorbic acid, dopamine, uric acid and inorganic salt that usually co-exist with  $\text{H}_2\text{O}_2$  in body fluid are added sequentially during measuring the current response upon injecting  $\text{H}_2\text{O}_2$ . As shown in Fig. 7a, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  delivers negligible change, and the subsequent current response to  $\text{H}_2\text{O}_2$  keep the same intensity as the case free from interferences. This test confirms the good tolerance of  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  to various interferences.



**Fig. 7.** (a) *i-t* curves on a  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2/\text{RDE}$  responding to  $\text{H}_2\text{O}_2$  (100  $\mu\text{M}$ ) in the presence of various interfering substances (1000  $\mu\text{M}$ ). (b) Current response on  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2/\text{RDEs}$  to injecting PMA and catalase into 0.1 M PBS with various cells, and (c) the corresponding amount of  $\text{H}_2\text{O}_2$  released from cells.

$\text{H}_2\text{O}_2$  plays important roles in cellular processes, and the concentration of  $\text{H}_2\text{O}_2$  varies with the type and state of cells. For example, the concentration of  $\text{H}_2\text{O}_2$  is higher in tumor area than that in normal tissue, due to fast oxygen metabolism and unlimited proliferation of cancer cells [9]. Thereby, we can detect and monitor the change of  $\text{H}_2\text{O}_2$  concentration, and then distinguish these cells. PMA was introduced as stimulant for  $\text{H}_2\text{O}_2$  release, and the generated  $\text{H}_2\text{O}_2$  was then irreversibly decomposed after adding catalase. Herein, the optimal  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  is employed to detect  $\text{H}_2\text{O}_2$  level in living cancer cells, i.e., MCF-7 (human breast cancer cells), MB-MDA-231 (human breast cancer cells) and HeLa cells (human



**Fig. 8.** (a) Polarization curves and (b) corresponding Tafel plots of  $\text{MoS}_2$  and  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  modified GCEs in 0.5 M  $\text{H}_2\text{SO}_4$ . (c) Stability test of  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2/\text{GCE}$  in 0.5 M  $\text{H}_2\text{SO}_4$ .

cervical cancer cells). As shown in Fig. 7b, in the presence of the above cells, quick current responses are observed after injecting PMA, and the current decreases to a background level as catalase is introduced, because catalase can irreversibly decompose  $\text{H}_2\text{O}_2$  to  $\text{O}_2$  and  $\text{H}_2\text{O}$ . It's suggested that the current response is due to  $\text{H}_2\text{O}_2$  released from cancer cells. By contrast, non-cancerous NIH-3T3 cells (murine fibroblast cell line) show no obvious response after introducing PMA. Moreover, the amounts of  $\text{H}_2\text{O}_2$  released from different cells are calculated in Fig. 7c, and per HeLa, MDA-MB-231 and MCF-7 produces  $1.38 \times 10^{-14}$ ,  $2.65 \times 10^{-14}$  and  $5.13 \times 10^{-14}$  mol  $\text{H}_2\text{O}_2$ , respectively. MCF-7 cells exhibit the highest intracellular  $\text{H}_2\text{O}_2$  level, consistent with previous reports [40]. Obviously, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  based electrochemical biosensor can discriminate normal cells and different types of cancer cells according to their  $\text{H}_2\text{O}_2$  concentration, which is of great importance in biosensing or other biological fields.

### 3.3. Electrocatalytic HER on $\text{Mo}_{1-x}\text{W}_x\text{S}_2$

The  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  nanoflowers not only offer a sensitive platform for  $\text{H}_2\text{O}_2$  detection, but also can be used in a variety of electrochemical reactions, such as HER. The  $\text{MoS}_2$  and  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  were investigated in 0.5 M  $\text{H}_2\text{SO}_4$  (Fig. 8). The polarization curves identify that the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  only requires a overpotential ( $\eta_{10}$ ) of 224 mV to achieve a current density of  $-10 \text{ mA cm}^{-2}$  (Fig. 8a), which is lower than that of  $\text{MoS}_2$  and other  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$ . Accordingly, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  delivers a lower Tafel slope of  $56 \text{ mV dec}^{-1}$ , indicating rapidly increasing  $\text{H}_2$  generation rate with applied overpotential. This is consistent with its polarization curve (Fig. 8b). The higher slopes observed on the  $\text{MoS}_2$  and other  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  indicate the relatively slower kinetics. In further comparison with previously reported TMDs, e.g.,  $\text{rGO/WS}_2$  ( $\eta_{10}$ : 229 mV, Tafel slope:  $73 \text{ mV dec}^{-1}$ ) [41],  $\text{H}_2$ -annealed  $\text{MoS}_2$  ( $\eta_{10}$ : 357 mV, Tafel slope:  $75 \text{ mV dec}^{-1}$ ) [42], bimetallic Co-doped  $\text{MoS}_2$  nanofibers ( $\eta_{10}$ : 330 mV, Tafel slope:  $60 \text{ mV dec}^{-1}$ ) [43] and  $\text{W}_x\text{Co}_y\text{S}$  ( $\eta_{10}$ : 228 mV, Tafel slope:  $111 \text{ mV dec}^{-1}$ ) [44], the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  highlights the outstanding HER activity. The enhanced electrocatalytic performance should be ascribed to the engineered electronic configuration on edges. And the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  affords satisfactory stability for the HER in 0.5 M  $\text{H}_2\text{SO}_4$  (Fig. 8c). There is negligible degradation observed in final polarization curves after 1000 continuous scans.

## 4. Conclusions

A series of bimetallic  $\text{Mo}_{1-x}\text{W}_x\text{S}_2$  are fabricated and investigated as efficient electrochemical biosensors, with clearly evidenced composition-dependence on engineered electronic configurations and surface \*OH binding. The optimal  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  affords high sensitivity ( $1290 \mu\text{A mM}^{-1} \text{ cm}^{-2}$ ), good selectivity, and wide applicable concentration range ( $4 \times 10^{-1}$ – $1.0 \times 10^4 \mu\text{M}$ ), in comparison with single-component counterparts and even recently reported materials involving enzymes or precious metals. Owing the sensitive and specific  $\text{H}_2\text{O}_2$  detection, the  $\text{Mo}_{0.75}\text{W}_{0.25}\text{S}_2$  can distinguish normal cells and different cancer cells via monitoring the amount of endogenous  $\text{H}_2\text{O}_2$ . Moreover, it also accomplishes a high efficiency in electrocatalytic HER, highlighting the universal promotion in sensing and electrocatalysis that share similar electrochemical fundamentals. We believe that the more-precise manipulation on the composition and surface architecture of bimetallic TMDs will further boost their performance for both sensing and catalysis.

### CRedit authorship contribution statement

**Yijin Shu:** Methodology, Investigation, Writing – original draft.  
**Wenbiao Zhang:** Software, Investigation. **Xing Yin:** Formal analy-

sis. **Lingli Zhang:** Data curation. **Yang Yang:** Resources. **Dong Ma:** Writing – review & editing. **Qingsheng Gao:** Conceptualization, Supervision, Writing – review & editing.

### Declaration of Competing Interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this paper.

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### Appendix A. Supplementary material

Supplementary data to this article can be found online at <https://doi.org/10.1016/j.jcis.2020.01.083>.

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