



Geometry-dependent DNA-TiO₂ immobilization mechanism: A spectroscopic approach

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ABSTRACT

DNA nucleotides are used as a molecular recognition system on electrodes modified to be applied in the detection of various diseases, but immobilization mechanisms, as well as, charge transfers are not satisfactorily described in the literature. An electrochemical and spectroscopic study was carried out to characterize the molecular groups involved in the direct immobilization of DNA structures on the surface of nanostructured TiO₂ with the aim of evaluating the influence of the geometrical aspects. X-ray photoelectron spectroscopy at O1s and P2p core levels indicate that immobilization of DNA samples occurs through covalent (P—O—Ti) bonds. X-ray absorption spectra at the Ti2p edge reinforce this conclusion. A new species at 138.5 eV was reported from P2p XPS spectra analysis which plays an important role in DNA-TiO₂ immobilization. The P—O—Ti/O—Ti ratio showed that quantitatively the DNA immobilization mechanism is dependent on their geometry, becoming more efficient for plasmid ds-DNA structures than for PCR ds-DNA structures. The analysis of photoabsorption spectra at C1s edge revealed that the molecular groups that participate in the C1s → LUMO electronic transitions have different pathways in the charge transfer processes at the DNA-TiO₂ interface. Our results may contribute to additional studies of immobilization mechanisms understanding the influence of the geometry of different DNA molecules on nanostructured semiconductor and possible impact to the charge transfer processes with application in biosensors or aptamers.

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1. Introduction

DNA nucleotides are used as molecular recognition system, double stranded deoxyribonucleic acid (ds-DNA) is a well characterized system, a double helix formed when two single strands are paired by hydrogen bonds to form a long chain of nitrogenous base pairs, Adenine-Thymine and Cytosine-Guanine (A-T and C-G). A single strand DNA (ss-DNA) is formed by a polyanionic sugar-phosphate backbone connected to the nitrogenous bases, rich in π -bonds. This is a system that contains a stack of π -orbitals extending within the DNA, facilitating electron transfer, which is one of the reasons for the various applications of DNA structure in biosensors devices [1,2].

DNA-based biosensors consist of the immobilized DNA strand to detect the complementary nucleic acid sequence by DNA target hybridization. DNA immobilization on the surface of electrodes can be applied in

the detection of viral diseases [3–5]. These detection devices depend on the efficiency of charge-transfer processes (electric signal) occurring from the complementary and/or adjacent nucleobases of the triphosphate groups to the conductor or semiconductor substrate. Understanding the characteristics of the immobilization of different geometrical structures of DNA it is possible to deepen into the charge transfer mechanisms relevant for application in DNA-based biosensors. The interaction of biomolecule and the substrate surface involve covalent, ionic, hydrogen or van der Waals bonding that depends on the molecular structure, size and the nanostructured metal oxide properties (i.e. surface charges, energy, functional groups, etc.) [6,7].

TiO₂ is widely used as a semiconductor material functionalized with molecules due to its high biocompatibility, high stability, easy availability and low cost [8,9]. Connor et al. have demonstrated that the phosphate groups perform electrostatic interactions with TiO₂ using internal reflectance spectroscopy (IRS) [10], and Liu et al. studied the photo-oxidation of ds-DNA immobilized on TiO₂ films by cyclic voltammetry [11].

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This work aims to study chemical species involved in the mechanisms of direct immobilization of the *Escherichia coli* plasmid ds-DNA (pDNA) and PCR ds-DNA (PCR) on TiO_2 . For this purpose, a combination of electrochemical and core-level spectroscopic characterizations was performed. Our results showed that these DNA molecules are immobilized on TiO_2 surface through P—O—Ti bonds, and that immobilization efficiency depends on the DNA geometry. The charge transfer process between DNA molecules and TiO_2 substrate were elucidated by cyclic voltammetry and corroborated by C K-edge and Ti L-edge X-ray absorption.

2. Experimental

2.1. Materials and Methods

Titanium (IV) isopropoxide (97%), ethanol (99.5%) and hydrochloric acid (37%) were purchased from Sigma-Aldrich. ITO (Indium Tin Oxide) coated on glass ($75 \times 50 \times 0.7$ mm, surface resistivity $15 \Omega/\text{sq}$) was obtained from (Lumtech, Taiwan). Tris hydrochloride (Tris-HCl) solution, Ethylenedinitrilotetraacetic acid (EDTA) buffer, Tris-EDTA buffer solution, glucose solution, sodium hydroxide P.A., sodium dodecyl sulfate solution, sodium hypochlorite solution, potassium acetate, glacial acetic acid, chloroform, and isopropanol were purchased from Sigma-Aldrich. dNTP Set was acquired from Thermo Scientific and Platinum Taq DNA Polymerase were acquired from Invitrogen™.

2.2. dsDNA Samples (gDNA, pDNA and Amplicon)

The pCR™ 2.1-TOPO® (Invitrogen by Thermo) plasmid vector (pDNA) extraction was performed through the alkaline lysis method [12]. The 200 bp amplicon was obtained copying a known fragment of pDNA through the Polymerase Chain Reaction (PCR) method using the Taq DNA Polymerase Platinum kit (Invitrogen™ by Thermo Scientific) and M13 primers, following the manufacturer's recommendations. The sequence of nitrogenous bases from a plasmid strand and PCR-DNA are found in Supplementary material of this paper.

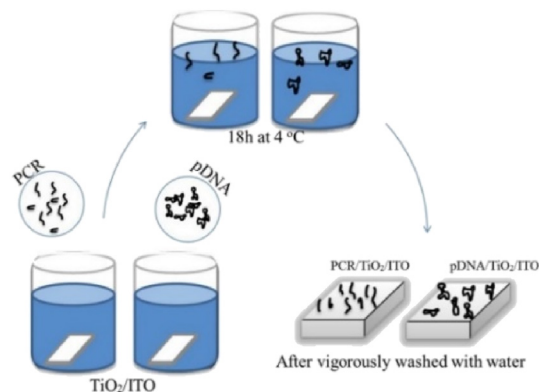
2.3. TiO_2 Films and Synthesis

The nanostructured TiO_2 was synthesized through the sol-gel method according to the literature [13]. A container containing 2.3 mL of Titanium (IV) isopropoxide, 7.6 mL of ethanol and 15.0 mL of hydrochloric acid was stirred for 6 h. The TiO_2 films were produced by adding an aliquot of the sol-gel of TiO_2 over ITO (Indium Tin Oxide)/glass substrates (15×15 mm) using the spin coating method at 3000 rpm by 60 s. Subsequently, the TiO_2 /ITO films were sintered in a muffle at 350°C for 45 min.

The surface morphology of the TiO_2 /ITO film was obtained with an AFM (Innova, Bruker) on an area of $(20 \times 20) \mu\text{m}^2$, operated in contact mode using silicon nitride cantilevers to scan the samples. They were performed with 512×512 pixels at a scan rate of 1.0 Hz. All measurements were performed at room temperature (296 ± 1 K) and $40 \pm 1\%$ relative humidity. The feedback control was adapted to the surface in order to obtain the best possible images, and they were analysed using the WSxM software [14] for determining the films surface roughness and thickness, as shown in Fig. S11 in Supplementary material. The films AFM images show a surface roughness of 1.02 nm and thickness of 15 nm, representative of a homogeneous surface.

2.4. DNA Immobilization

According to Scheme 1, the TiO_2 /ITO films were immersed in two containers containing 2.0 mL of deionized water, one with pDNA pellet, and another, with PCR pellet overnight at 4°C for DNA immobilization. The DNA solutions were kept in phosphate buffer of pH 4. Afterwards, the films were vigorously washed with deionized water to remove the



Scheme 1. DNA immobilization procedure on TiO_2 /ITO surfaces in aqueous solution.

excess of DNA or DNA samples that have done weak bonds on the TiO_2 film surface, and dried at room temperature. The films were taken to an oven for 30 min at a temperature of 70°C . The investigated samples will be labelled here as TiO_2 /ITO, pDNA/ TiO_2 /ITO and PCR/ TiO_2 /ITO for nanostructured TiO_2 and immobilized DNA- TiO_2 films, respectively.

2.5. Electrochemical Experiments

The DNA immobilization was characterized by cyclic voltammetry (CV) in a conventional three-electrode configuration using the AUTOLAB PGSTAT 302N potentiostat (Metrohm Autolab, Utrecht, The Netherlands) equipped with GPES 4.9 software. The reference electrode was Ag/AgCl (3 M KCl) and the auxiliary electrode was a platinum wound wire. The working electrodes used in the experiment contained a total area of 15×10 mm ITO/glass, and the samples of interest were deposited at 10×10 mm. In the CV assays, a solution of methylene blue of $2.0 \mu\text{mol} \cdot \text{L}^{-1}$ was used as electrolyte and intercalator at a scanning rate of 50 mV/s .

2.6. NEXAFS Experiments

Near edge X-ray absorption fine structure (NEXAFS) experiments were performed at the SGM beamline (250–1000 eV) at the Brazilian Synchrotron Light Source (LNLS), in Campinas, Brazil. Samples of TiO_2 /ITO, pDNA/ TiO_2 /ITO and PCR/ TiO_2 /ITO were fixed on the sample holder with a carbon conductive tape and introduced into the ultra-high vacuum chamber (10^{-8} mbar). NEXAFS spectra were obtained in the total electron yield (TEY) mode at carbon, K absorption edge and titanium L-edge, before and after pDNA and PCR-DNA immobilization on nanostructured TiO_2 . The spectra were normalized by the incident photon flux (I_0) measured with an Au mesh placed just upstream of the sample. Phenylalanine was used as standard reference for photon energy calibration of the NEXAFS spectra [15]. NEXAFS spectra shown in this work were background corrected by a linear pre-edge subtraction and linear regression beyond the edge.

2.7. XPS Experiments

X-ray photoelectron spectroscopy (XPS) measurements were performed at the ESCALAB 250Xi spectrometer (Thermo Scientific) equipped with an electron energy hemispherical analyzer using monochromatized Al K α line ($h\nu = 1486.6$ eV) excitation. The spectra were energy referenced to the C1s signal of aliphatic C atoms at binding energy of 285.00 eV. XPS spectra were collected using X-ray beam spot size = $650 \mu\text{m}$ and with emission angle of 0° with respect to the sample surface. Survey spectra were measured from 0 to 1300 eV with pass energy of 50 eV and high resolution spectra acquired with 25 eV pass energy at C1s, N1s, O1s, Ti2p and P2p core levels. Sensitivity factors were

used to determine the atomic concentrations of each element in the samples [16]. The spectra were collected at two different points of the sample surface for evaluated the chemical homogeneity of the films.

3. Results and Discussion

The electrochemical behavior of pDNA/TiO₂/ITO, PCR/TiO₂/ITO and TiO₂/ITO electrodes was studied using as electrolyte and intercalator a methylene blue solution. Fig. 1 shows comparative cyclic voltammograms in which it is possible to observe two significant differences: i) the anodic and cathodic peaks in the voltammograms of pDNA/TiO₂/ITO and PCR/TiO₂/ITO electrodes show a shift in relation to TiO₂/ITO electrode that implied different electrochemical responses and electrode modification. This shift is probably due to the methylene blue interaction with the cytosine and guanine sequences, intercalating the π -stacking [17–19].

The reduction of methylene blue can occur by two mechanisms: first, through DNA-mediated charge transfer (intercalation); second, through the direct reduction on the surface of TiO₂ [18,19]. An attenuation of the current signal of the PCR curve was observed when compared to the curve of the immobilized pDNA. The passivation of the PCR/TiO₂/ITO film may be related to the charge transport properties intrinsic to the base sequence that constitutes the molecular structure of the PCR. ii) the bigger current density present in electrodes DNA functionalized than TiO₂/ITO, indicating a greater binding capacity to produces a reversible redox couple via-charge transfer with methylene blue, as a reported by Pheeney and Barton [19].

This electrochemical performance can be explained by the two different geometries of the immobilized DNA structures that influence the charge mobility mechanism through the work electrode, these points are better exploited with spectroscopic techniques. In Fig. 2 (a) the XPS survey spectra for pDNA/TiO₂/ITO/glass, PCR/TiO₂/ITO/glass and TiO₂/ITO/glass films are presented. All characteristic peaks for TiO₂, ITO and DNA samples, as C1s, O1s, Ti2p, In3d and Sn3d core levels were identified. The presence of In3d, Sn3d and Ti2p core levels in the XPS survey spectra is evidence that TiO₂ ultrathin films were deposited onto ITO substrate and confirmed by AFM image analysis (see Fig. S11 in Supplementary material). On the other hand, the presence of C1s core level at pDNA/TiO₂/ITO/glass and PCR/TiO₂/ITO/glass XPS spectra is an indication that DNA molecules are adsorbed on the TiO₂ surface. N1s and P2p peaks were not directly observed in the survey spectra of DNA samples, probably due to the low photoionization cross-sections for these core levels using Al K α photon energy and also to the low concentration (very thin films) of DNA on the TiO₂

films. Then, the high-resolution N1s and P2p XPS spectra for pDNA and PCR samples were measured and are presented in Fig. 2(b) and (c), respectively.

The deconvolution of these spectra allowed us to carry out the assignments for the different chemical environments of nitrogen and phosphorus atoms. The high-resolution N1s spectra of the DNA-TiO₂ samples were deconvoluted using three contributions centred at 398.5, 399.8 and 401.5 eV for PCR and 398.1, 399.8 and 401.3 eV for pDNA, respectively. These contributions can be attributed to the imine (—N=), amine (—NH—) and amino (—NH_2) nitrogen species, respectively [20–24].

No significant changes are observed at the N1s spectra for both DNA samples analysed here and their profile are indeed very similar to DNA samples, which suggests lower participation of nitrogen species in DNA-TiO₂ immobilization. On the other hand, high resolution P2p spectra are characterized by two contributions: the first one appears at 133.4 eV, is labelled as 1 in Fig. 2(c) and assigned to phosphate backbone (PO₄) present in the DNA structure [21–24]; the other contribution, labelled as 2 in Fig. 2(c), appears at 138.5 eV and has never been reported before in DNA immobilization on semiconductor and conductor surfaces. The last contribution may be due to the interaction between DNA phosphate groups and the TiO₂ surface. Phosphorus species with binding energy close to 138.5 eV has been only reported by Yan et al. on gas phase volatile phosphorus compounds containing polarizable ligands [25]. However, recently, Taucher et al. showed that electrostatic effects can influence significantly the measured core-level binding energies [26]. Then, this P2p contribution at high binding energy could be influenced by electrostatic interaction between DNA and TiO₂.

The spin-orbit doublet 2p_{3/2} and 2p_{1/2} components with energy separation of 0.85 eV are clearly identified in both P2p spectra. A notable reduction of the phosphate group contribution due to covalent DNA-TiO₂ is clearly observed for pDNA/TiO₂/ITO sample. The new species at 138.5 eV labelled as 2 plays an important role in pDNA-TiO₂ immobilization. The origin of this species will be discussed below. The quantitative chemical analysis obtained from XPS survey and high resolution N1s and P2p spectra for both DNA samples are reported in Table 1.

High-resolution O1s XPS spectra for TiO₂/ITO, PCR/TiO₂/ITO and pDNA/TiO₂/ITO are illustrated in Fig. 3. O1s spectrum of TiO₂/ITO substrate was deconvoluted into two contributions appearing at 530.0 eV and 531.3 eV and ascribed to O²⁻ of titanium oxide and to weakly physical adsorbed oxygen species such as OH groups on the surface (Ti-OH), respectively [22,27]. Three contributions were used in the deconvolution of the O1s DNA spectra. Besides the two oxygen observed in TiO₂/ITO

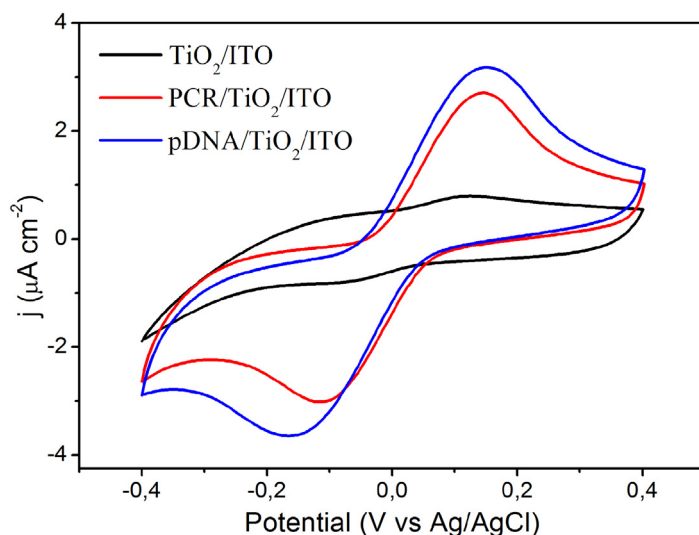


Fig. 1. Cyclic voltammogram of the TiO₂/ITO (black curve), PCR/TiO₂/ITO (red curve) and pDNA/TiO₂/ITO (blue curve) and in MB 2.0 $\mu\text{mol}\cdot\text{L}^{-1}$ solution. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)

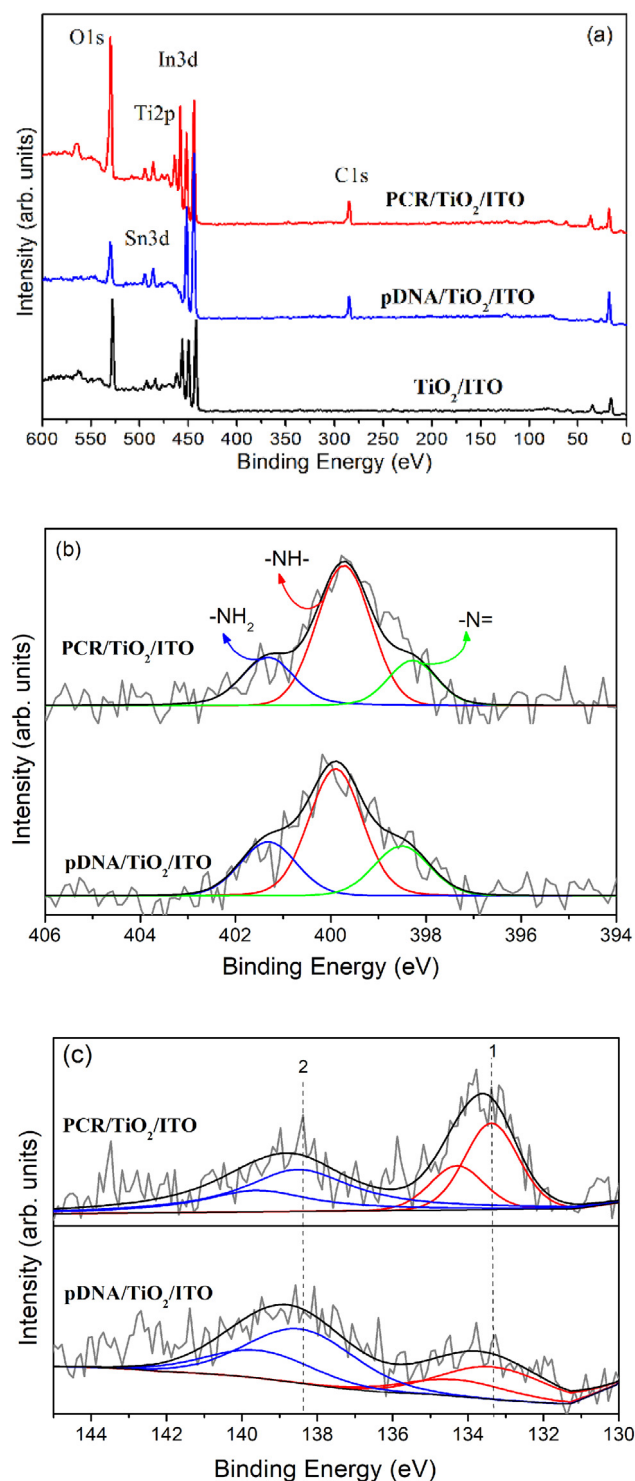


Fig. 2. XPS survey spectra of PCR/TiO₂/ITO, pDNA/TiO₂/ITO and TiO₂/ITO films (a). High-resolution N1s (b) and P2p (c) XPS spectra of PCR/TiO₂/ITO and pDNA/TiO₂/ITO.

Table 1

Elemental composition (at%) of pDNA/TiO₂/ITO and PCR/TiO₂/ITO films obtained from XPS spectra analysis. The P atomic % was divided into two components (1) and (2), corresponding to phosphate of the DNA backbone and P—O—Ti, respectively.

	Atomic percentage							
	C1s	O1s	N1s	P2p(1)	P2p(2)	Ti2p	In3d	Sn3d
PCR	22.7%	47.6%	0.9%	0.6%	0.8%	19.3%	7.0%	0.9%
pDNA	34.3%	32.2%	1.0%	0.2%	0.7%	18.9%	11.3%	1.4%

substrate, other oxygen species is found at binding energy of ≈ 532.7 eV in PCR and 532.6 eV in pDNA, respectively [28–30]. This species was attributed to O—C, O=C bonds in DNA molecules (nitrogenous bases and deoxyribose). The increase in component intensity at 531.2 eV was attributed to P—O—Ti bonding between the tris-phosphate group of the PCR and pDNA structure and TiO₂ surface [31,32]. However, according to quantitative analysis of the O1s, P2p and N1s core levels the most probable contribution in pDNA sample is P—O—Ti species.

Previous studies have shown that DNA immobilization on TiO₂ films occurs through tris-phosphate groups that, in aqueous solution, assume a negative charge density, while on TiO₂ surface they form positively charged layers [10,11]. Thus, on the DNA-TiO₂ interface in aqueous solution, the interactions are mainly of the electrostatic type. As already known, TiO₂ may present oxygen vacancies [33], and the negatively charged oxygen from the phosphate group can interact with empty 3d orbitals of titanium, forming covalent bonds producing a characteristic photoelectron peak at 531.2 eV binding energy [31,32] which could be evidenced by our XPS spectroscopy results. The fitting results are shown in Table 2. Peak areas were used to determine the atomic percentage of oxygen species in different chemical environments, specifically O—Ti, P—O—Ti, and O=C. The primary interest of this study is to determine the relative concentration of P—O—Ti/O—Ti species as an evidence of the DNA immobilization samples on the TiO₂ surface. The ratio between P—O—Ti/O—Ti oxygen species calculated from Table 2 was 0.17 and 0.24 for PCR/TiO₂/ITO and pDNA/TiO₂/ITO samples, respectively. A similar trend is observed for phosphorous species reported in Table 1, where the contribution labelled as 2 on P2p XPS spectra is higher than for pDNA/TiO₂ film.

This result allows us to associate this phosphorous species to P—O—Ti link. The combination of O1s and P2p results shows that the immobilization involving P—O—Ti species is more efficiently for pDNA/TiO₂/ITO sample. Some factors may be contributing to these quantitative results, as for example, the DNA molecule geometry and ordering. It is well known that plasmid DNA molecule presents a well-ordered structure compared to PCR. This together with circular geometry of the pDNA molecule can help to increase the contact area between the molecule and substrate [34]. Besides, PCR-DNA is a short and linear fragment with less contact area to anchoring to TiO₂ surface [35].

DNA immobilization on the TiO₂ films was also investigated by NEXAFS spectroscopy. This is a technique highly sensitive to chemical changes of material surfaces and, therefore, capable of determining the density of unoccupied electronic states in DNA/TiO₂ interface. Fig. 4 shows C K-edge NEXAFS spectra for the pDNA/TiO₂/ITO and PCR/TiO₂/ITO films. The main electronic transitions characterizing the C1s absorption spectra of DNA samples are C1s $\rightarrow \pi^*C=C$ (285.4 eV), C1s $\rightarrow \pi^*C=N$ (286.9 eV), C1s $\rightarrow \pi^*HNC=O$ (287.6 eV), C1s $\rightarrow \sigma^*C-C$ (294.0 eV) and a weak feature attributed to C1s $\rightarrow \sigma^*C-O$ (297.0 eV) [36–38].

NEXAFS spectra on the C K-edge showed different intensities and profiles. In the PCR spectrum it was observed that C1s $\rightarrow \pi^*C=N$ transitions are more intense than C1s $\rightarrow \pi^*C=O$ transitions, whereas in the pDNA spectra the intensities of these transitions are nearly similar. These results suggest that the charge transfer processes follow different pathways within the analysed DNA-TiO₂ system. The C1s XPS measurements corroborate this observation. In the inset of Fig. 4(a) and (b), the deconvoluted C1s XPS spectra show that C—N and C—O peaks have similar behavior to that observed in the C K-edge NEXAFS spectra.

The literature [39,40] reports that the number of neighbouring guanines of G-G and G-G-G types in same tape favours charge transfer process through π orbitals with the purine ring stacked along the chain. The greater presence of neighbouring guanines, the greater is the probability that the DNA structure behaves as a conductive material. The plasmid DNA has 7858 nitrogenous bases with GG = 330 and GGG = 93 neighbours, whereas the PCR has 400 nitrogenous bases with GG = 20 and GGG = 3 (as showed in the Table S1†). The ratio between the guanine bases shows qualitatively the conductive behavior of the DNA

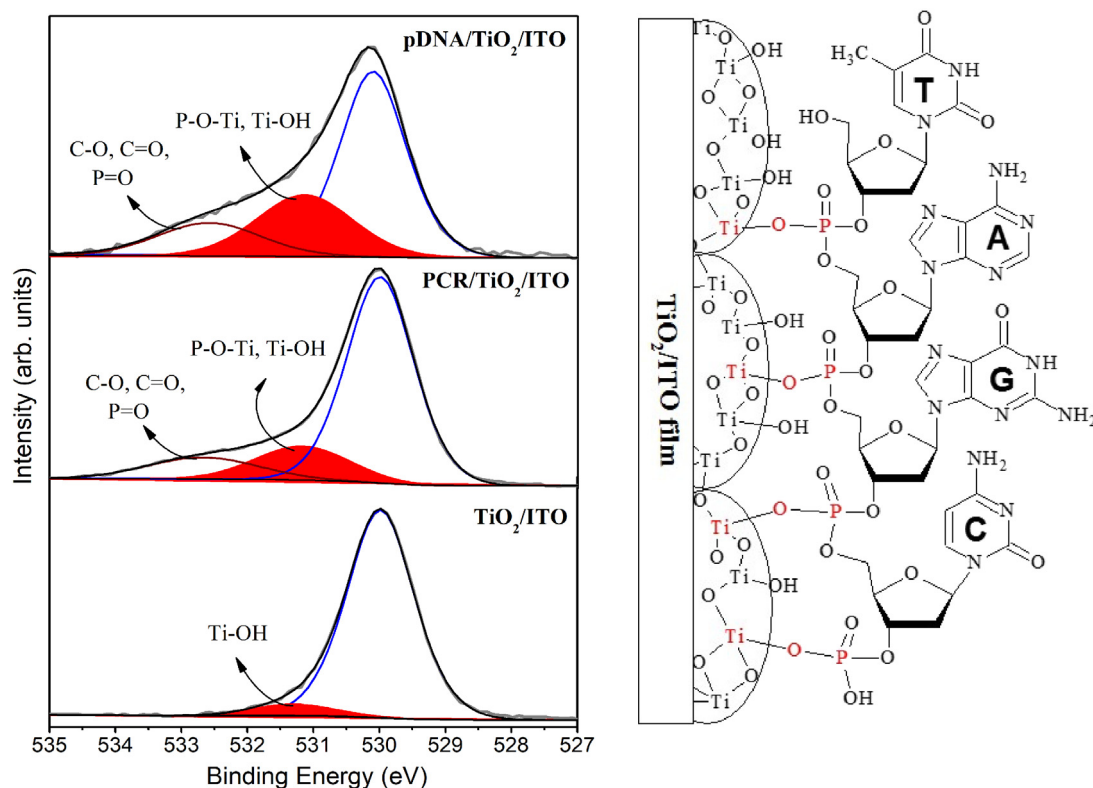


Fig. 3. Deconvolution of the O1s XPS spectra for pDNA/TiO₂/ITO, PCR/TiO₂/ITO, and TiO₂/ITO samples. In the inset, DNA immobilization on TiO₂/ITO through tri-phosphate groups.

samples. In this way, the GGG/GG ratio indicates that pDNA (0.28) is more conductive than PCR (0.15). Details are given of the complete plasmid DNA and PCR sequence is given in the Supplementary material. It was suggested in the literature [41] that the HOMO-LUMO gap of the ds-DNA is related to the phenomenon of charge drop with a band gap of 2.6 eV associated to a transition between the π and π^* orbitals. The qualitative comparison between the intensities of the C K-edge NEXAFS spectra showed that the PCR has more empty states than the plasmid DNA. Thus, the PCR has greater probability of receiving electrons in the unoccupied orbitals and, therefore, has a higher reactivity. So, we conclude that the plasmid DNA compared to the PCR presents greater stability.

Fig. 5 shows the Ti L-edge NEXAFS spectra for the TiO₂, PCR/TiO₂/ITO and pDNA/TiO₂/ITO films. Ti L-edge NEXAFS spectrum is characterized by a set of peaks associated to L₃ (a₁ and a₂) resulting from 2p_{3/2} transition to 3d_{5/2} final state and L₂ (b₁ and b₂) resulting from 2p_{1/2} transition to 3d_{3/2} final state. The character of these states is modified by the combined spin-orbit and crystal field interactions. The peak splits (L₃ and L₂) correspond to transitions involving t_{2g} (a₁ and b₁) and e_g (a₂ and b₂) orbitals in an octahedral symmetry slightly distorted TiO₂ structure [39,40,42]; the same pattern was observed for the NEXAFS spectra of PCR/TiO₂/ITO and pDNA/TiO₂/ITO in terms of peak splitting and symmetry. Remembering that in X-ray absorption spectroscopy, the core electron is excited to empty electronic states, the transitions are observed only if these states are unoccupied.

Table 2

Binding energy (BE) values and atomic percentage (at%) of molecular groups for TiO₂/ITO substrate and DNA samples from high-resolution O1s XPS measurements.

Samples	TiO ₂ /ITO		PCR		pDNA	
	BE (eV)	at%	BE (eV)	at%	BE (eV)	at%
O—Ti	530.0	93.9	530.0	34.3	530.1	19.3
P—O—Ti/Ti—OH	531.3	6.13	531.2	7.6	531.2	8.2
C=O/P=O	—	—	532.7	5.7	532.6	4.7

The intensity of the peaks can be used to estimate the density of unoccupied states, qualitatively. Both PCR and pDNA are immobilized on TiO₂ thin film, and the transitions to unoccupied states for the L₃ (e_g) and L₂ (e_g) do not vary in intensity, but for the L₃ (t_{2g}) and L₂ (t_{2g}) there is a significantly change relative to TiO₂/ITO [43]. The electrons in t_{2g} electronic states are concentrated in the space between the incoming ligand in TiO₂ octahedral coordination, while e_g orbital points straight at the incoming ligands. The t_{2g} orbitals have the incorrect symmetry to participate in sigma interactions with the ligands. However, they have the correct symmetry to participate in π -interactions with the ligands. This indicates that there is chemical interaction between the DNA samples and the TiO₂ surface through Ti t_{2g} electronic states with a π -character [44–46]. The π -symmetry of the electronic states involved in DNA anchoring results in high electron mobility between molecule and substrate which is an important point for a successful application in biomaterials.

4. Conclusions

This study aimed to investigate different aspects related to the influence of the geometry of the different DNA structures immobilized on TiO₂ and approach to the charge transfer mechanisms. Electrochemical experiments showed that the DNA molecule was successfully immobilized on the semiconductor, being possible to emphasize that the pDNA has more intercalation effects than PCR with methylene blue, as well as that the presence of DNA molecules decreases the charge transfer resistance of the TiO₂ film. New phosphorous specie at 138.5 eV was reported from P2p XPS spectra analysis which plays an important role in DNA-TiO₂ immobilization. This specie is associated to P—O—Ti bond between phosphate backbone (PO₄) present in the DNA structure and TiO₂ substrate surface. From the quantitative analysis of the O1s XPS spectra, the P—O—Ti/O—Ti ratio showed that immobilization through the tris-phosphate groups was higher for the plasmid ds-DNA (0.24) than for the PCR ds-DNA (0.17).

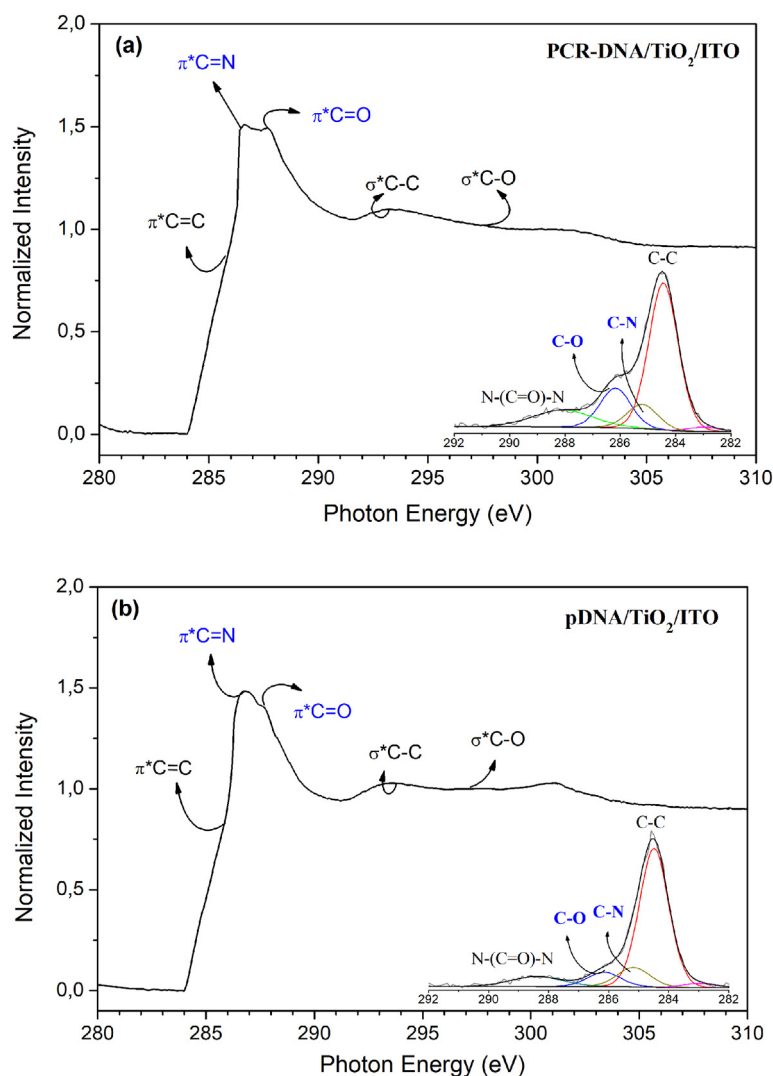


Fig. 4. C K-edge spectrum for PCR/TiO₂/ITO (a) and for pDNA/TiO₂/ITO (b). Inset, deconvolution of the C1s XPS spectra of PCR/TiO₂/ITO and pDNA/TiO₂/ITO samples.

The analysis of the C K-edge NEXAFS spectra showed that the charge transfer processes follow different pathways within the studied DNA/TiO₂ systems. The Ti L-edge NEXAFS spectra revealed that the

immobilization of DNA occurs through empty Ti 3d orbitals and O 2p orbitals of oxygen atoms from tri-phosphate groups, involving mainly Ti t_{2g} electronic states with a π -character.

These results contribute to better understanding the influence of the geometry of the different DNA molecules immobilized on nanostructured semiconductor and impact to the charge transfer processes in DNA molecules usually applied in electrochemical biosensors.

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Disclosure

The authors declare no competing financial interest.

Appendix A. Supplementary data

In Supporting information, we present the full sequence of bases of plasmid DNA and PCR. It is also shown the AFM image of TiO₂/ITO

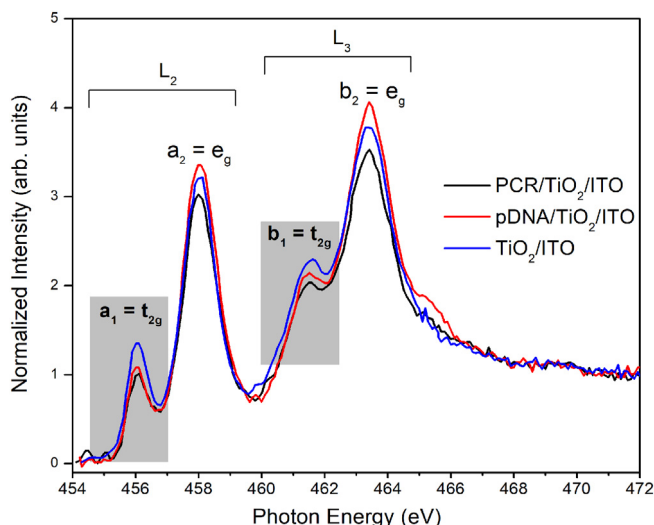


Fig. 5. Ti L-edge NEXAFS spectra for PCR/TiO₂/ITO, pDNA/TiO₂/ITO and TiO₂/ITO films.

substrate. Supplementary data to this article can be found online at <https://doi.org/10.1016/j.saa.2018.03.081>.

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