

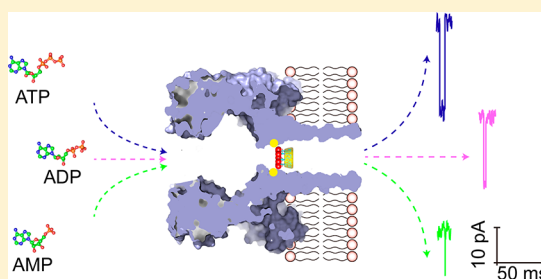
Simultaneous High-Resolution Detection of Bioenergetic Molecules using Biomimetic-Receptor Nanopore

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Supporting Information

ABSTRACT: A novel artificial receptor, heptakis-[6-deoxy-6-(2-hydroxy-3-trimethylammonium-propyl) amino]- β -cyclomaltoheptaose, with similar functions of mitochondrial ADP/ATP carrier protein, was synthesized and harbored in the engineered α -HL (M113R)₇ nanopore, forming a single-molecule biosensor for sensing bioenergetic molecules and their transformations. The strategy significantly elevates both selectivity and signal-to-noise, which enables simultaneous recognition and detection of ATP, ADP, and AMP by real-time single-molecule measurement.



Single-molecule analysis has unique advantages over ensemble or bulk-measurement in detecting species, which can simultaneously provide fingerprint information on not only a single molecule but also many different single molecules by molecular counting.¹ Such ability to capture the characteristic detail of sample heterogeneity is very important on biological applications, especially in the detections of complex biofluid and/or those components with minor differences. For example, adenosine-5'-triphosphate (ATP), adenosine-5'-diphosphate (ADP), and adenosine-5'-monophosphate (AMP) (referred to as adenosine phosphates, APs) that are relevant to biological energy storage and signal transduction² have recently also been designated as non-invasive diagnostic and prognostic biomarkers for many diseases including Alzheimer's, Parkinson's, and those involving the heart and blood vessels.^{3–5} To obtain insight into the important and complex cell energy-relevant biological processes and to meet clinical needs, there is a growing demand to simultaneously detect them, but it is an extreme challenge because of similar structures, fast and reversible conversion between them under specific catalysis of enzymes,⁶ as well as wider distribution (ATP level for healthy cell: 0.28 pM–11 pM per cell).⁷

Among many various single-molecule methods available at present, nanopore technology has emerged as a powerful tool to treat biological problems due to simplicity, label-free, solution-based detection and easy operation.^{8–13} The technology mainly relies on the changes in nanopore current produced by analyte-translocating events. Therefore, protein nanopore, unlike with solid nanopore, should have a top priority in sensing small molecules because of comparable dimensions. But, in recognizing and capturing small biomolecules, effective nanopore including the most commonly used α -hemolysin (α -HL) has remained remarkably unpredictable, which could result from the fast transport through the nanopore¹⁴ and its

own properties of lacking selectivity.¹⁵ Some efforts have addressed the above limitations by (1) functionalizing the nanopore surface with hydrophobic¹⁶ and positively¹⁷ or negatively¹⁸ charged residues; and (2) modifying¹⁹ or carrying analyte.^{20–22} These strategies are cumbersome, require careful optimization, yet frequently are ineffective. It is still an essential challenge to develop reliable nanopore that is able to distinguish and detect directly specific molecules such as ATP, ADP, and AMP, with high selectivity and sensitivity. For this purpose, a bioinspired strategy could be a perfect solution. Herein, we display that such biomimetic receptor (BR)-equipped protein nanopore can be obtained by two-step processes: (1) designing and synthesizing a new artificial receptor that resembles mitochondrial ADP/ATP carrier protein in the shape and the vital functional residues; (2) followed by binding it in the engineered α -HL (M113R)₇ to form a single-molecule sensing element. We demonstrate its excellent performance through the molecular simulation and the single-molecule electronic measurements in both recognizing APs simultaneously and real-time enzyme-catalyzing transformation kinetics and thermodynamics. Furthermore, the ability at the single-phosphate resolution has also great promise in synthetic DNA sequencing.²³

EXPERIMENTAL SECTION

Reagents and Materials. Adenosine-5'-triphosphate (ATP, 99%), adenosine-5'-diphosphate (ADP, 99%), and adenosine-5'-monophosphate (AMP, 99%), 2,3-epoxypropyl trimethylammonium chloride (95%), and calf intestinal alkaline phosphatase (CIAP, EC 3.1. 3.1) were purchased from Sigma-Aldrich. 1,2-Diphytanoyl-*sn*-glycero-3-phospho-

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choline was obtained from Avanti Polar Lipids. The thickness of Teflon film (Goodfellow) was 25 μm .

Single-Channel Recording and Data Analysis. 2-Diphtanoylphosphatidylcholine (DPhPC) bilayer was formed over a 130–150 μm aperture in a Teflon septum that divided a planar bilayer chamber into cis and trans parts. Both solutions were 1 M KCl and buffered with 10 mM Tris (pH 7.5). (M113R)₇, ATP, ADP, AMP, and enzyme CIALP were added to the cis compartment that was connected to the ground. BR was added to the trans side that was connected to the head-stage of the amplifier. The final concentration of the (M113R)₇ proteins was 0.08–0.18 ng/mL. Currents were recorded with a patch clamp amplifier (Axopatch 200B, Molecular Devices, Sunnyvale, CA), filtered with a four-pole Bessel filter at 5 kHz, sampled at 100 kHz by a computer equipped with a Digidata 1550 A/D converter (Molecular Devices), and acquired with Clampex 10.4 software (Molecular Devices). Single-channel events were analyzed using Clampfit 10.5 (Molecular Devices) and origin 9.0 (Microcal, Northampton, MA) software. Mean dwell time values were obtained from the dwell histograms that were fitted to single exponential functions. The blockades were plotted as residual current histograms, and the distributions were fitted to Gaussian functions.

RESULTS AND DISCUSSION

Design and Synthesis of Biomimetic Receptor. The key of mitochondrial ADP/ATP carrier protein to recognize and transport ADP/ATP is the five positively charged arginine (R) residues (R79, R137, R234, R235, and R279) in its funnel-shaped cavity, forming a high-density charge cluster (Figure 1a).²⁴ Inspired by the specific structure, we designed and synthesized a biomimetic receptor (BR), (heptakis-[6-deoxy-6-(2-hydroxy-3-trimethylammonio-propyl)amino]- β -cyclomaltoheptaose) (Figure 1b), containing a cluster of positively charged quaternary ammoniums that is permanently charged and independent of the solution pH.²⁵ Cyclomaltoheptaose is a bowl-like hollow molecule with 6.0–6.5 Å in diameter.²⁶ The cavity size is comparable with the size of the mitochondrial ADP/ATP carrier (about 8 Å in diameter)²⁴ and well matches ATP/ADP/AMP molecules (maximum size 6 Å).²⁷ The BR was prepared by four-step reactions: The first three-step reactions were to convert all the primary hydroxyl groups of β -cyclomaltoheptaose to amino groups (SI 2 and Figure S1); the heptakis-(6-deoxy-6-amino)- β -cyclomaltoheptaose subsequently underwent the chemical reaction with 2, 3-epoxypropyl trimethylammonium chloride in triethylamine-HCl buffer solution (pH = 10) at 50 °C for 24 h (Figure 1c). The final BR product (yield: 51%) was characterized by ESI-MS (m/z): $[\text{M}]^{7+} = 277.1822$.

Interactions between BR and APs. As we previously reported, the quaternary ammonium cation is distinctive for binding DNA derivatives,^{12,28} so the ring of high-density quaternary ammonium cations located in the funnel bottom of the BR could be utilized as a molecular trap to catch adenosine phosphate derivatives. The predefined property was demonstrated by forming BR-APs complexes in bulk solution (for details see SI Figure S4a–f, Table S1–4 and S9). Through the measurements of UV–visible absorbance (ΔA) of APs at 260 nm, we observed the obvious differences of three complexes in the formation constant (K_f) and the standard free energy (ΔG°): K_f (BR-ATP) = $1.02 \times 10^4 \text{ M}^{-1}$, K_f (BR-ADP) = $2.18 \times 10^4 \text{ M}^{-1}$, K_f (BR-AMP) = $6.87 \times 10^4 \text{ M}^{-1}$, ΔG° (BR-ATP) = $-27.11 \text{ kJ mol}^{-1}$, ΔG° (BR-ADP) = $-24.34 \text{ kJ mol}^{-1}$, and

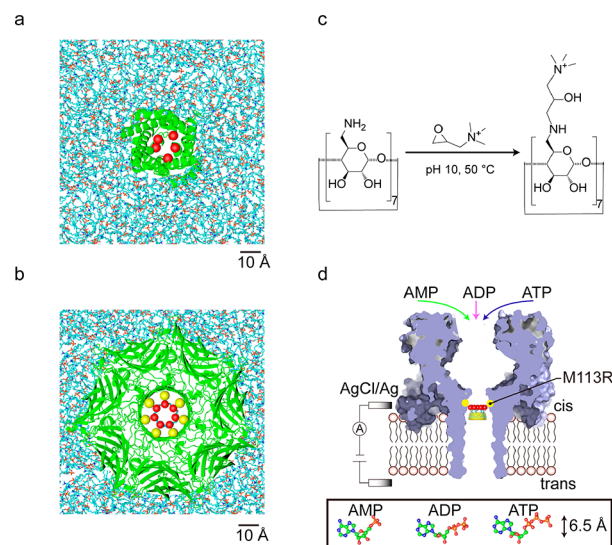


Figure 1. Construction of biomimetic receptor-equipped protein nanopore. (a) Top view of the mitochondrial ADP/ATP carrier inserted into the lipid bilayer (POPC, 110 Å $\times$ 110 Å). The cationic cluster consisting of five arginine residents (R79, R137, R234, R235, R279) in the ADP/ATP carrier is represented by red balls. (b) Molecular model of biomimetic receptor-equipped (M113R)₇ nanopore in the lipid bilayer (POPC, 110 Å $\times$ 110 Å). BR is located in the barrel of a mutated M113R α -HL pore (R is labeled by yellow color). The quaternary ammonium of BR is represented by red color. (c) Synthesis of heptakis-[6-deoxy-6-(2-hydroxy-3-trimethylammonio-n-propyl)amino]-cyclomaltoheptaose (BR) from heptakis-(6-deoxy-6-amino)-cyclomaltoheptaose, which was treated with 2,3-epoxypropyl trimethylammonium chloride in triethylamine-HCl buffer solution (pH = 10) at 50 °C for 24 h. (d) Schematic representation of the APs detection system using BR-equipped (M113R)₇ α -HL pore. BR was added into the trans side and APs to the cis side. Structural models of mitochondrial ADP/ATP carrier and α -HL were produced by PDB 2C3E and PDB 7AHL. BR, APs, and POPC lipids were constructed and then rendered by VMD and PyMOL software.

ΔG° (BR-AMP) = $-22.46 \text{ kJ mol}^{-1}$ at 20 °C, which should be ascribed to both various phosphate number and chain length (see SI 3).

We further investigated the interaction of BR and APs using molecular docking simulation analysis (for details see SI 4). The results of semiflexible docking approaches revealed that ATP, ADP, and AMP as guest molecule all exhibited high affinity with host molecule BR (SI, Figure S5). However, the number of salt bridge between ammonium groups and phosphates (SI, Table S5–7) was gradually reduced in these 1:1 complexes: 5 (ATP-BR), 4 (ADP-BR), and 3 (AMP-BR), while the number of hydrogen bonds was also reduced: 7 (ATP-BR), 5 (ADP-BR), and 4 (AMP-BR).

Single-Molecule Recognition and Detection of APs. We prepared genetically engineered α -hemolysin protein pore, (M113R)₇ and mounted BR molecule at 113 binding sites, forming single-molecule recognition and detection device (Figure 1d). The (M113R)₇ pore produced a stable opening current. When +140 mV voltage was applied, single-channel current was $140 \pm 5 \text{ pA}$ ($n = 24$) in 1 M KCl (Figure 2a). For the bound-BR (M113R)₇ pore, (M113R)₇-BR, only a $36 \pm 2 \text{ pA}$ ($n = 15$) current level was observed at +140 mV (Figure 2b). The mutants of the (M113R)₇ pore that bind the BR molecule are $\sim 10^3$ times more tightly bound than the wild-type pore that binds cyclomaltoheptaose molecule (SI Table

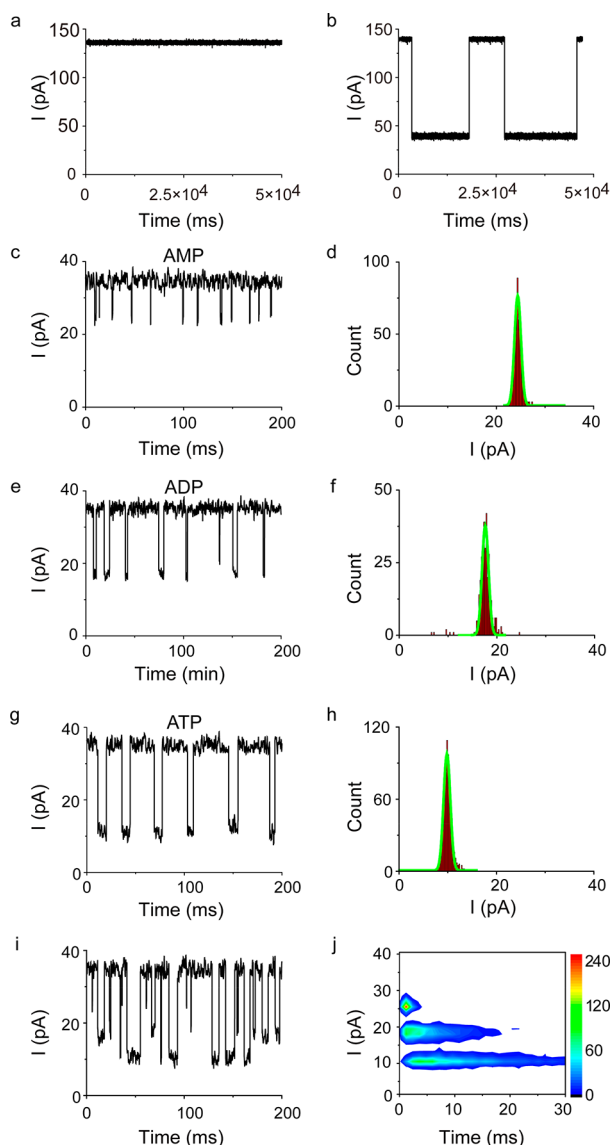


Figure 2. (M113R)₇-BR nanopore for sensing APs. Typical current traces recording at 140 mV with (a) (M113R)₇ pore, (b) (M113R)₇-BR pore, and (M113R)₇-BR pore for (c) AMP, (e) ADP, (g) ATP, and (i) the mixture of ATP, ADP, and AMP. The residual current histograms: AMP (d), ADP (f), and ATP (h). (j) 2D contour plot of the APs mixture. The concentration of APs (cis side): ATP (1.78 μ M), ADP (5.35 μ M), and AMP (7.12 μ M). The concentration of BR is 60 μ M (trans side). The experiment temperature is 20 $^{\circ}$ C.

S8). Next, we tested the recognizing ability of the (M113R)₇-BR pore for APs by single-channel recording. After adding to the cis side (on the opposite side of the BR), ATP, ADP, and AMP exhibited three distinct current-blocking levels: 10.38 ± 1.35 pA ($n = 26$) for ATP, 18.68 ± 1.58 pA ($n = 20$) for ADP, and 24.76 ± 1.69 pA ($n = 19$) for AMP, at +140 mV, respectively (Figure 2c–h). Despite only one phosphate difference, the current value varies greatly at least 6.08 pA. Such a huge difference is especially important for quickly distinguishing them through direct readout. We also note that two differences in current between ATP-ADP and ADP-AMP (6.08 pA and 8.3 pA) are not equal, which means that the current change resulted from APs in (M113R)₇-BR pore is not only size-exclusion effect, but also deals with different conformation of ATP, ADP, and AMP. This subtle difference

can also be observed in docking results. The mean dwell time (τ_{off}) values for dianion AMP with monophosphate, trianion ADP with biphosphate, or tetraanion ATP with triphosphate were 0.64 ± 0.03 ms ($n = 26$), 3.87 ± 0.36 ms ($n = 21$), and 7.34 ± 0.90 ms ($n = 19$), respectively. The longer dwell time reflects the stronger binding. These results demonstrated that the interaction between APs and (M113R)₇-BR is highly dependent on the number of their charges and number of hydrogen bonds. To evaluate the distinguishing ability in mixture, the mixture of ATP, ADP, and AMP was added to the cis side and three current levels quickly arose in the current traces, which is clearly visible with the naked eye (Figure 2i). As shown in the 2D-contour plot (Figure 2j), the current values and the dwell time of them in the mixture are the same as that in the individual substance. However, the mixture of ATP, ADP, and AMP for (M113R)₇ was unable to be discriminated. APs could not introduce any signal for WT α -hemolysin (see SI Figure S8).

Enthalpy-Driven Binding of APs in the Confined Nanopore. The binding of APs in the (M113R)₇-BR pore is voltage-dependent. The rate constants at different voltages were obtained and analyzed as previously described.²⁹ Although both the association constant k_{on} ($1/c \cdot \tau_{\text{on}}$) and the dissociation constant k_{off} ($1/\tau_{\text{off}}$) of APs in the (M113R)₇-BR pore exponentially increase with increasing voltage (Figure 3a,b), the standard free energy ΔG° ($\Delta G^{\circ} = -RT \ln((k_{\text{on}})/$

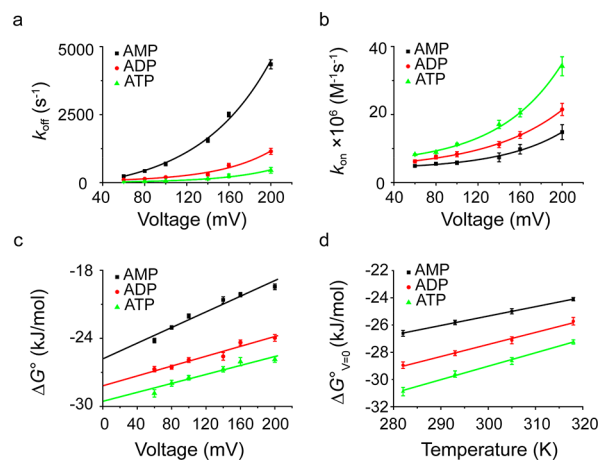


Figure 3. Interactions between APs and (M113R)₇-BR. (a–b) Plots of the $k_{\text{off}} \sim V$ and $k_{\text{on}} \sim V$. (c) Voltage (V) dependence of the standard free energy (ΔG°). (d) Variation of standard free energy (ΔG°) at different temperatures. APs: AMP (black), ADP (red), and ATP (green).

(k_{off})) linearly increases (Figure 3c), suggesting the decrease in the stability of (M113R)₇-BR-APs complexes or the reduction of the binding frequency with increasing voltage. By extrapolating the linear relationship between ΔG° and the voltage, the standard free energy ($\Delta G^{\circ}_{V=0}$) values at 0 mV are gained: -25.81 kJ mol^{−1} for AMP, -28.07 kJ mol^{−1} for ADP and -29.6 kJ mol^{−1} for ATP, respectively. The $\Delta G^{\circ}_{V=0}$ values decrease linearly as the temperature increases (Figure 3d). The values of ΔH° and ΔS° obtained by linear fitting of $\Delta G^{\circ}_{V=0}$ and temperature (T) are -46.41 ± 0.42 kJ mol^{−1} and -70.27 ± 1.46 J mol^{−1} for AMP, -53.99 ± 1.47 kJ mol^{−1} and -88.55 ± 2.32 J mol^{−1} for ADP, as well as -58.63 ± 1.26 kJ mol^{−1} and -98.69 ± 4.11 J mol^{−1} for ATP. Both ΔH° and ΔS° are negative. However, the huge enthalpy change (ΔH°) that can

completely offset the small change in $T\Delta S^\circ$ produces a larger negative value of $\Delta G^\circ_{V=0}$, thus making the binding of APs proceed spontaneously and favorably. The overall exothermic binding in the confined space is mainly an enthalpy-driven process. Interestingly, $\Delta G^\circ_{V=0}$ in the (M113R)₇-BR nanopore is more negative in comparison with ΔG° in the bulk solution (SI Table S9). For ATP, ADP, and AMP, the difference in the standard free energy is $\Delta\Delta G^\circ_{ATP} = -2.49 \text{ kJ mol}^{-1}$, $\Delta\Delta G^\circ_{ADP} = -3.73 \text{ kJ mol}^{-1}$, and $\Delta\Delta G^\circ_{AMP} = -3.35 \text{ kJ mol}^{-1}$, respectively, demonstrating that the binding in the (M113R)₇-BR nanopore is more favorable. The $\Delta\Delta G^\circ$ should be ascribed to the space effect in confined nanopore.

Real-Time Monitoring Enzyme-Catalyzing Transformation. Based on the method above, the process of the ATP hydrolysis catalyzed by calf intestinal alkaline phosphatase (CIALP, EC 3.1. 3.1) was monitored (Figure 4a). In the absence of CIALP, ATP produced only the events with $10.38 \pm 1.35 \text{ pA}$ level at 140 mV voltage (Figure 4b, 4g). After adding CIALP in the ATP solution, the ADP and AMP signals ($18.68 \pm 1.58 \text{ pA}$ level and $24.76 \pm 1.69 \text{ pA}$ level) accompanied by the ATP signal were generated in 2 h of continuous recording (Figure 4c–f and 4h–j). The frequency of events (f) or the event number of unit time for each substance changed over time is proportional to its concentration (C), $C = k_{on}^{-1} \cdot f$. By fitting the scatter plot by the kinetic equation, the time-resolved change in the concentration of ATP, ADP, and AMP was directly obtained by monitoring ATP, ADP, and AMP signals (Figure 4k). Upon adding CIALP, ATP concentration drops sharply from $7.4 \mu\text{M}$ to nearly $2 \mu\text{M}$ within 30 min and followed a slow process to zero, while ADP and AMP increase first and then decrease, with the maximum peaks at $2.8 \pm 0.3 \mu\text{M}/25 \text{ min}$ and $1.9 \pm 0.2 \mu\text{M}/50 \text{ min}$, respectively, and finally convert to adenosine by a sigmoid relationship, which does not produce any current-blocking response. The fitted apparent hydrolysis rate constants of ATP, ADP, and AMP were 0.047 min^{-1} , 0.050 min^{-1} , and 0.063 min^{-1} , respectively (see SI 6), indicating the hydrolysis ability of CIALP for APs: $\text{AMP} > \text{ADP} > \text{ATP}$. This sequence is in accordance with alkaline phosphatase from other sources.³⁰ Figure 4l is the scatter plot of all events during whole enzyme-catalyzing transformation. We clearly observed (i) three kinetic phases by simultaneously monitoring ATP, ADP, and AMP using biomimetic-receptor nanopore; (ii) that three kinetic phases take place in a time sequential fashion; and (iii) different point density (or blackness) in the time-course of ATP hydrolysis, which represents their concentrations.

CONCLUSIONS

The BR-nanopore assay here described is a single-molecule approach to detect bioenergetic molecules and their transformations, which has many potential advantages: (i) the high selectivity of BR allows BR-nanopore to effectively capture and identify ATP, ADP, and AMP; (ii) it is label-free, has no amplification, and has no modification and thus does not suffer from other interference; (iii) the high-resolution real-time signals for ATP, ADP, and AMP enable us to directly read out their information; (iv) the ability for simultaneous rapid monitoring of ATP, ADP, and AMP is hard to achieve by other methods. Although simultaneously analyzing bioenergy-related molecules and their transformation dynamics has been demonstrated, the BR-nanopore strategy is broadly useful to any involved-phosphate biological processes and applications,

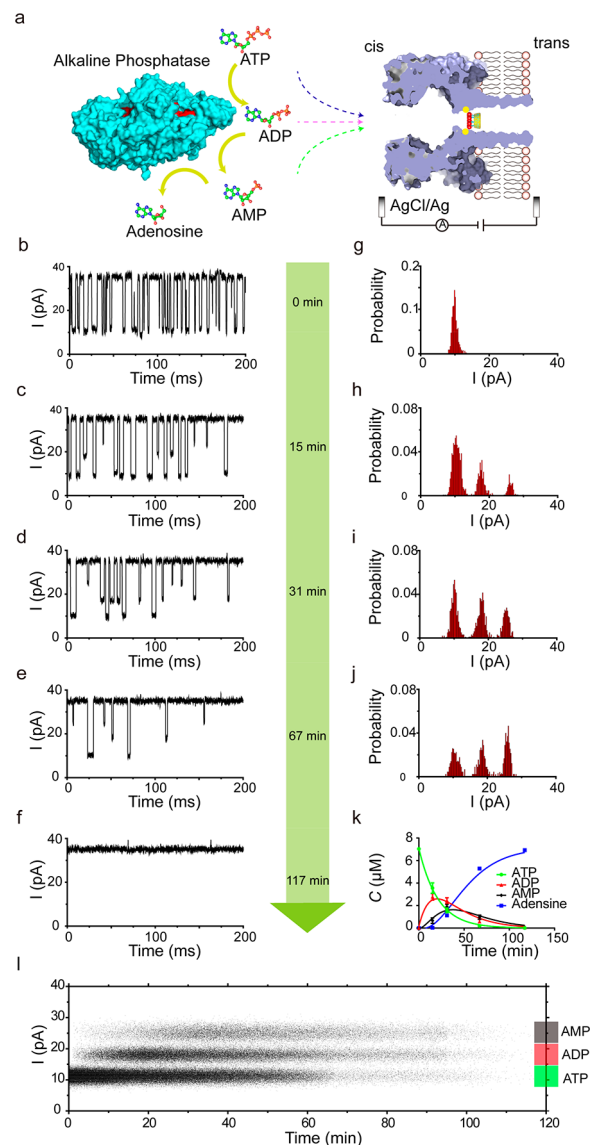


Figure 4. ATP hydrolysis kinetics and analysis. (a) Schematic representation of detecting ATP hydrolysis process. ATP hydrolysis was catalyzed by enzyme calf intestinal alkaline phosphatase (CIALP, EC 3.1.3.1). The structure of alkaline phosphatase is from PDB 1B8J, and active sites are represented by red. (b–f) Representative current–time traces at 0, 15 min, 31 min, 67 min, and 117 min, respectively. The hydrolysis of ATP ($7.4 \mu\text{M}$) was conducted by adding CIALP (0.89 unit/mL activated by 25 nM Mg^{2+} and 2.5 nM Zn^{2+}) to the cis side. (g–j) Normalized histogram plots of the residual current at different times. (k) Concentration variations of APs and adenosine during the hydrolysis process. Averaged adenosine concentration was calculated by the formula: $7.04 - ([\text{ATP}] + [\text{ADP}] + [\text{AMP}])$. (l) Scatter plot of all events during enzyme-catalyzing transformation. The hydrolysis was conducted in a solution of 1 M KCl , 10 mM Tris-HCl , $\text{pH} = 7.5$, at 20°C . The applied voltage was 140 mV .

for example, synthetic DNA sequencing method^{23,31} and detecting phosphorylation of DNA/RNA and protein.^{32–34}

ASSOCIATED CONTENT

Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: [10.1021/acs.analchem.9b04268](https://doi.org/10.1021/acs.analchem.9b04268).

Experimental details describing the synthesis, characterization, detailed information on molecular simulation, and analysis on hydrolysis kinetics, as well as additional figures (PDF)

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Notes

The authors declare no competing financial interest.

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