

# CdTe QD–CeO<sub>2</sub> Complex as a Strong Photoelectrochemical Signal Indicator for the Ultrasensitive microRNA Assay

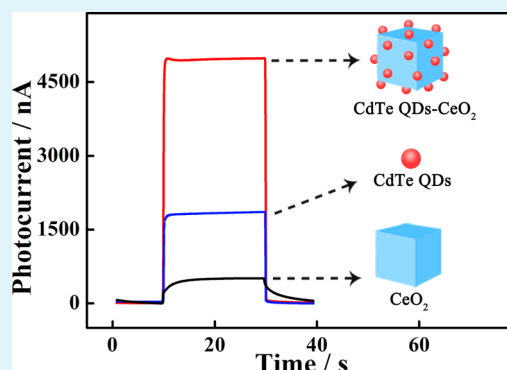
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## Supporting Information

**ABSTRACT:** The photoelectrochemical (PEC) signal can be enhanced by constructing sensitization structures containing photoactive materials and appropriate sensitizers. However, usually, the photoactive materials and sensitizers were separated in independent nanostructures, thereby producing long electron-transfer path and large energy loss, which could further result in limited photoelectric conversion efficiency and PEC signals. Herein, we designed a novel sensitization nanostructure simultaneously containing the photoactive material cerium dioxide (CeO<sub>2</sub>) and its sensitizer CdTe quantum dots (QDs) as the strong PEC signal indicator (CdTe QD–CeO<sub>2</sub> complex), which prominently enhanced photoelectric conversion efficiency because of the shortened electron-transfer path and reduced energy loss. The proposed CdTe QD–CeO<sub>2</sub> complex was used to construct a PEC biosensor for achieving ultrasensitive determination of microRNA-141 (miRNA-141) coupling with target converting amplification and DNA supersandwich structure amplification. The designed PEC biosensor demonstrated a wide linear range from 0.5 fM to 5 nM with a detection limit of 0.17 fM for miRNA-141. Impressively, this work provided a new and strong PEC signal indicator for the construction of PEC sensing platform and would extend the application of PEC sensors in bioanalysis and early disease diagnosis.

**KEYWORDS:** photoelectrochemical sensing, CdTe QD–CeO<sub>2</sub> complex, signal indicator, dual signal amplification, microRNA assay



## INTRODUCTION

Photoelectrochemical (PEC) analysis, as a newly budding and exceedingly promising analytical method, employs light as the excitation source and current as the detection readout, and thus, it presents superior features of high sensitivity, reduced background noise, and excellent stability compared with conventional optical and electrochemical methods.<sup>1–5</sup> In recent years, great effort has been made on constructing sensitization structures containing photoactive materials and appropriate sensitizers to promote light-harvesting capability, enhance charge carrier separation, and depress electron–hole recombination, thereby improving the photoelectric conversion efficiency prominently.<sup>6–10</sup> For instance, Ju and Wen reported an efficient sensitization structure of CdTe quantum dots (QDs)/CdS QDs/TiO<sub>2</sub> nanoparticles for the construction of a protein detection platform.<sup>8</sup> Zhu and co-workers have proposed a PEC immunosensing platform for ultrasensitive carcinoembryonic antigen detection based on CdSeTe@CdS:Mn core–shell QD-sensitized TiO<sub>2</sub> nanoparticles.<sup>9</sup> Although these works can increase the photoelectric conversion efficiency to some extent, the PEC signals are still restricted because the photoactive materials and sensitizers are separated in independent nanostructures, leading to long electron-transfer path and large energy loss. Thus, it is expected to control the photoactive material and sensitizer

within one nanostructure, which may greatly shorten electron-transfer path and reduce energy loss, thus further enhancing the photoelectric conversion efficiency and the PEC signal considerably.

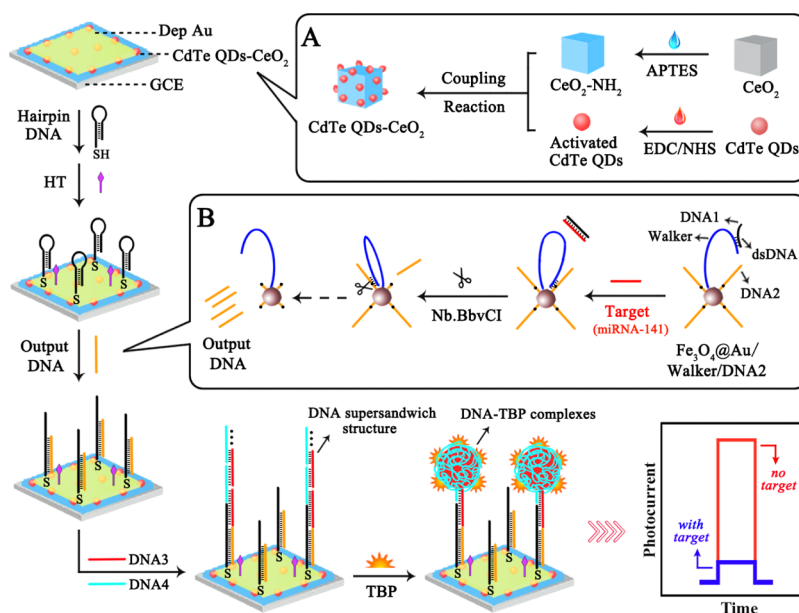
Cerium dioxide (CeO<sub>2</sub>), an attractive and typical semiconductor metal oxide, has been proverbially applied in the fields of catalysis, UV blocking, and PEC water splitting because of its advantages of steady physical and chemical properties as well as excellent photocatalytic activity.<sup>11–13</sup> Nevertheless, CeO<sub>2</sub> was rarely used in PEC sensing field owing to its wide band gap of 2.5 eV,<sup>14</sup> which seriously restricted the photoelectric conversion efficiency. This limitation might be lifted by combining the wide band gap CeO<sub>2</sub> and a narrower band gap semiconductor to construct an efficient sensitization structure. As a classic inorganic semiconductor, CdTe QDs possess ideal characteristics, such as tunable size, broad excitation, and high light-harvesting capability.<sup>15–18</sup> More importantly, the band gap of CdTe QDs is 1.8 eV,<sup>19</sup> which matches well with that of CeO<sub>2</sub> (2.5 eV), making CdTe QDs a promising sensitizer toward CeO<sub>2</sub>. Considering these challenges and opportunities, we here attempted to synthesize a

Received: February 1, 2019

Accepted: March 11, 2019

Published: March 11, 2019

**Scheme 1. Schematic Diagrams of the Proposed PEC Biosensor for miRNA-141 Detection; (A) Preparation of the CdTe QD–CeO<sub>2</sub> Complex; (B) Target Converting Amplification Procedure**



novel CdTe QD–CeO<sub>2</sub> complex by cross-linking –NH<sub>2</sub>-functionalized CeO<sub>2</sub> and 3-mercaptopropionic acid (MPA)-capped CdTe QDs, in which the photoactive material CeO<sub>2</sub> and its sensitizer CdTe QDs were controlled in one nanostructure. In consequence, the CdTe QD–CeO<sub>2</sub> complex exhibited excellent photoelectric performances and could be employed as a strong PEC signal indicator, which was ascribed to the fact that CeO<sub>2</sub> and CdTe QDs were controlled in one nanostructure, leading to shortened electron-transfer path, reduced energy loss, and improved photoelectric conversion efficiency.

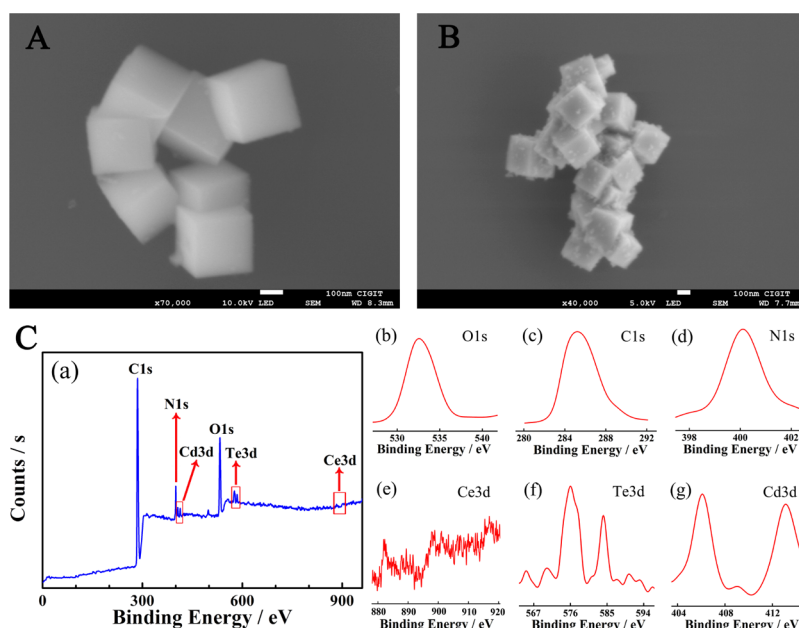
Herein, a PEC biosensor with the CdTe QD–CeO<sub>2</sub> complex as the PEC signal indicator was designed for ultrasensitive determination of miRNA-141 coupling with dual signal amplification strategy (Scheme 1). The successful synthesis of the CdTe QD–CeO<sub>2</sub> complex as a signal indicator could shorten the electron-transfer path and reduce the energy loss between CeO<sub>2</sub> and its sensitizer CdTe QDs, producing a strong PEC signal. Besides, the target converting amplification procedure based on DNA walker was adopted for achieving the conversion of small amounts of miRNA-141 to massive output DNA. These output DNAs could open hairpin DNA on the electrode surface and then trigger the generation of a DNA supersandwich structure containing numerous TATA sequences by the assistance of DNA3 and DNA4. With the addition of TATA-binding protein (TBP), the generated DNA supersandwich structure would specifically bind with TBP and bend at an 80° angle to form DNA–protein complexes,<sup>20–24</sup> which could effectively hinder the electron transfer, leading to a significantly reduced PEC signal for quantitative detection of miRNA-141. As expected, this work not only demonstrated the enormous potential of the CdTe QD–CeO<sub>2</sub> complex as a strong PEC signal indicator for sensing platform construction but also paved a new pathway for ultrasensitive detection of miRNA-141 in bioanalysis and early disease diagnosis.

## EXPERIMENTAL SECTION

**Synthesis of Fe<sub>3</sub>O<sub>4</sub>@Au, CdTe QDs, CeO<sub>2</sub>, and CdTe QD–CeO<sub>2</sub> Complex.** Fe<sub>3</sub>O<sub>4</sub>@Au and MPA-capped CdTe QDs were prepared based on the protocols reported previously.<sup>25,26</sup> CeO<sub>2</sub> was prepared using the method mentioned in the literature.<sup>14,27</sup> Briefly, 0.87 g of Ce(NO<sub>3</sub>)<sub>3</sub>·6H<sub>2</sub>O was added to 40 mL of 6 M NaOH aqueous solution. After stirring for 0.5 h, the mixture was transferred into a 50 mL Teflon bottle and reacted at 180 °C for 24 h. After washing with ultrapure water until pH = 7, the precipitate was dried at 60 °C for 14 h and then calcined at 450 °C for 3 h. The obtained CeO<sub>2</sub> was stored at 4 °C prior to the –NH<sub>2</sub> functionalization. For the preparation of –NH<sub>2</sub>-functionalized CeO<sub>2</sub> (CeO<sub>2</sub>–NH<sub>2</sub>), 2 mL of 3-aminopropyl triethoxysilane was dispersed in 20 mL of ethanol under stirring, followed by adjusting the pH to 5–8 with 3 M HCl. After that, 0.5 g of the as-prepared CeO<sub>2</sub> was added with constant stirring for 14 h. Finally, CeO<sub>2</sub>–NH<sub>2</sub> was acquired by centrifugal washing.

For the preparation of the CdTe QD–CeO<sub>2</sub> complex, the amide reaction was adopted to link MPA-capped CdTe QDs and CeO<sub>2</sub>–NH<sub>2</sub>. First, 4 mL of 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide/*N*-hydroxysuccinimide (10 mM/20 mM) solution was mixed with 2 mL of MPA-capped CdTe QDs for activation of –COOH groups. After washing by centrifugation, the activated MPA-capped CdTe QD was redispersed in 2 mL of ultrapure water, followed by adding 2 mL of CeO<sub>2</sub>–NH<sub>2</sub> aqueous solution for 2 h. Finally, the CdTe QD–CeO<sub>2</sub> complex was collected through centrifugation and washing.

**Target Converting Amplification Procedure.** The target converting amplification procedure based on DNA walker is illustrated in Scheme 1B. First, 2 μL of 2 μM DNA1 was mixed with 2 μL of 2 μM thiolated walker at 37 °C for 2 h to form a double-stranded DNA (dsDNA). Next, the dsDNA and 40 μL of 2 μM thiolated DNA2 were simultaneously added into 40 μL of Fe<sub>3</sub>O<sub>4</sub>@Au with stirring for 14 h, thus obtaining the Fe<sub>3</sub>O<sub>4</sub>@Au/walker/DNA1/DNA2 complex through Au–S bond. Afterward, 2 μL of miRNA-141 (target) was added for realizing hybridization with DNA1 and releasing walker via a toehold exchange mechanism. The released walker paired with DNA2 on the surface of Fe<sub>3</sub>O<sub>4</sub>@Au, leading to the generation of a cleavage site for nicking endonuclease (Nb.BbvCI). In the presence of 2 μL of 5 U Nb.BbvCI and 4 μL of NE buffer, DNA2 would be cut by Nb.BbvCI, producing output DNA. Simultaneously, walker would be released again for pairing with the next DNA2, which could achieve a further cutting and releasing process. In this way,



**Figure 1.** SEM images of (A) CeO<sub>2</sub> and (B) CdTe QD–CeO<sub>2</sub> complex. (C) XPS analysis of the (a) full region of the CdTe QD–CeO<sub>2</sub> complex, (b) O 1s region, (c) C 1s region, (d) N 1s region, (e) Ce 3d region, (f) Te 3d region, and (g) Cd 3d region.

numerous output DNA would be acquired *via* magnetic force and employed for opening hairpin DNA on the electrode surface.

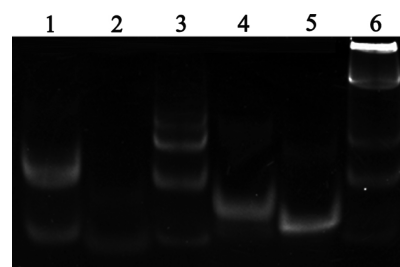
**Fabrication of the PEC Biosensor.** After being cleaned according to the method reported previously,<sup>28</sup> the glassy carbon electrode (GCE) was decorated with 15  $\mu$ L of the CdTe QD–CeO<sub>2</sub> complex and then dried at 37  $^{\circ}$ C. Next, the CdTe QD–CeO<sub>2</sub>-modified GCE was immersed in 1% HAuCl<sub>4</sub> solution for 10 s to acquire a gold nanoparticle layer by electrodeposition under  $-0.2$  V constant potential (DepAu), followed by dropping hairpin DNA (15  $\mu$ L, 2  $\mu$ M) and reacting for 14 h at 4  $^{\circ}$ C. After incubating hexanethiol (HT, 10  $\mu$ L, 0.1 mM) for 0.5 h, 15  $\mu$ L of output DNA was dropped on the electrode surface to hybridize with hairpin DNA. Subsequently, a DNA supersandwich structure was produced by adding DNA3 (10  $\mu$ L, 2  $\mu$ M) and DNA4 (10  $\mu$ L, 2  $\mu$ M), which possessed numerous TATA sequences and could specifically recognize TBP. Ultimately, the acquired electrode was incubated with 20  $\mu$ L of 1 ng/mL TBP for 1 h to bend DNA at an 80 $^{\circ}$  angle through the specific recognition between TBP and TATA sequences to form DNA–protein complexes. Scheme 1 presents the fabrication procedure of the PEC biosensor.

## RESULTS AND DISCUSSION

**Characterizations of Nanomaterials.** The morphologies of CeO<sub>2</sub> and the CdTe QD–CeO<sub>2</sub> complex were investigated *via* scanning electron microscopy (SEM). Figure 1A is the SEM image of CeO<sub>2</sub>, which presents a cubic structure with a uniform size of 250 nm. After reacting with CdTe QDs, as exhibited in Figure 1B, numerous CdTe QDs could be obviously observed on the surface of CeO<sub>2</sub> nanocubes. Furthermore, in order to confirm the successful synthesis of the CdTe QD–CeO<sub>2</sub> complex, the elemental analysis was obtained from the X-ray photoelectron spectroscopy (XPS). As illustrated in Figure 1C, XPS signals of O 1s, C 1s, and N 1s were found at binding energies of around 531.7, 284.8, and 399.4 eV, respectively, which demonstrated the presence of O, C, and N elements. These results were consistent with previous reports on O 1s, C 1s, and N 1s.<sup>14,29</sup> The Ce 3d binding energy peaks were investigated in detail in Figure S4 (Supporting Information). The peak was fitted into two peaks labeled as  $u''$  and  $v'$  to Ce<sup>3+</sup>, and the other six peaks labeled as  $u$ ,  $u'$ ,  $u'''$ ,  $v$ ,

$v''$ , and  $v'''$  to Ce<sup>4+</sup>, which tallied with the literature data.<sup>14,27</sup> Besides, the doublets located at 576 and 584 eV belonged to Te 3d (Te 3d<sub>5/2</sub> and Te 3d<sub>3/2</sub>), and two obvious peaks centered at 406 and 413 eV corresponded to Cd 3d (Cd 3d<sub>5/2</sub> and Cd 3d<sub>3/2</sub>), which tallied with the previous report<sup>30</sup> and implied the existence of CdTe QDs. These results revealed that CeO<sub>2</sub> and the CdTe QD–CeO<sub>2</sub> complex were prepared successfully. Moreover, the characteristic results of the synthesized CdTe QDs and Fe<sub>3</sub>O<sub>4</sub>@Au are presented in Figure S3 (Supporting Information).

**Gel Electrophoresis Analysis.** As observed from Figure 2, the generation of a DNA supersandwich structure was

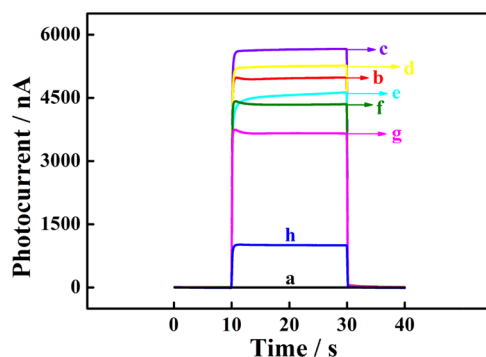


**Figure 2.** PAGE characterization: lane 1, hairpin DNA; lane 2, output DNA; lane 3, a mixture of hairpin DNA and output DNA; lane 4, DNA3; lane 5, DNA4; lane 6, a mixture of hairpin DNA, output DNA, DNA3, and DNA4.

characterized by polyacrylamide gel electrophoresis (PAGE). The result of hairpin DNA was shown in lane 1. Two bands could be obviously observed on lane 1 because the 3'-end of hairpin DNA was modified with thiol group and the formation of disulfide bond would lead to the increased molecular weight. Thus, the lower band on lane 1 represented hairpin DNA and the upper band on lane 1 indicated the formation of disulfide bonds. Compared with hairpin DNA (the lower band on lane 1), an increasing band shift was found from output DNA (lane 2) because of the reduced molecular weight. The result for hybridization of hairpin DNA with output DNA was shown in

lane 3, which presented a slower band shift (lane 3 vs 1, 2), indicating that the hybridization between hairpin DNA and output DNA was successful. DNA3 (lane 4) and DNA4 (lane 5) with different molecular weights exhibited different band shifts. When hairpin DNA, output DNA, DNA3, and DNA4 coexisted (lane 6), output DNA could open hairpin DNA and then trigger the generation of DNA supersandwich structures, leading to the formation of a long dsDNA molecule. Accordingly, a band shift with the slowest mobility was found (lane 6), suggesting the successful generation of DNA supersandwich structures.

**PEC Characterization of the Biosensor.** As presented in Figure 3, PEC analysis was employed to characterize the



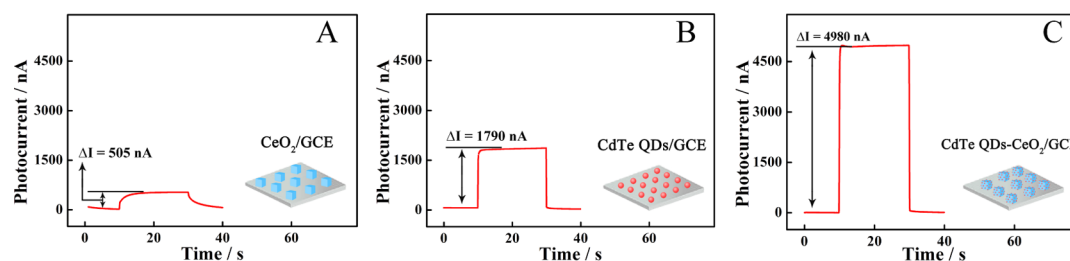
**Figure 3.** PEC responses of (a) bare GCE, (b) CdTe QD–CeO<sub>2</sub>/GCE, (c) DepAu/CdTe QD–CeO<sub>2</sub>/GCE, (d) hairpin DNA/DepAu/CdTe QD–CeO<sub>2</sub>/GCE, (e) HT/hairpin DNA/DepAu/CdTe QD–CeO<sub>2</sub>/GCE, (f) output DNA/HT/hairpin DNA/DepAu/CdTe QD–CeO<sub>2</sub>/GCE, (g) DNA3–DNA4/output DNA/HT/hairpin DNA/DepAu/CdTe QD–CeO<sub>2</sub>/GCE, and (h) TBP/DNA3–DNA4/output DNA/HT/hairpin DNA/DepAu/CdTe QD–CeO<sub>2</sub>/GCE in PBS containing 0.1 M AA.

modification process of this biosensor. The excitation light source with the wavelength of 460 nm and the radiant flux of 976 mW and the electrolyte solution of 5 mL phosphate-buffered solution (PBS) containing 0.1 M ascorbic acid (AA) were utilized during the PEC measurement. The PEC response of bare GCE was close to zero (curve a). After the CdTe QD–CeO<sub>2</sub> complex was modified on the surface of GCE, a greatly enhanced PEC response was observed (curve b) because of the excellent photoelectric activity of the CdTe QD–CeO<sub>2</sub> complex. Subsequent electrodeposition of gold nanoparticles caused a significantly increased PEC response (curve c) because of its excellent conductivity. The continuously decreased PEC responses were obtained (curves d–g) after successive assembly of hairpin DNA, nonconductive HT, output DNA, and DNA3–DNA4, owing to their poor charge transfer. Ultimately, a further decreased PEC response was

found with the addition of TBP (curve h) because the electron-transfer path between the CdTe QD–CeO<sub>2</sub> complex and electron donor could be impeded by the produced DNA–TBP complexes. The result implied that the modification process of the PEC biosensor was successful.

**Comparison of Different Photoactive Materials.** To explore the PEC efficiency of the CdTe QD–CeO<sub>2</sub> complex, two kinds of components including CeO<sub>2</sub> and CdTe QDs were selected for comparison under the same conditions. As illustrated in Figure 4, the PEC responses of CeO<sub>2</sub> and CdTe QDs were 505 and 1790 nA, respectively. A significantly enhanced PEC response (4980 nA) was obtained from the electrode surface modified with the CdTe QD–CeO<sub>2</sub> complex as the photoactive material (Figure 4C). In addition, the PEC responses of the CdTe QD–CeO<sub>2</sub> complex were 9.8-fold and 2.8-fold than those of pure CeO<sub>2</sub> and pure CdTe QDs, respectively. The key reasons for the PEC response enhancement were as follows: (a) the effective sensitization effect of CdTe QDs toward CeO<sub>2</sub> and (b) the prominently reduced electron-transfer distance between CeO<sub>2</sub> and CdTe QDs. The above results confirmed that the CdTe QD–CeO<sub>2</sub> complex with high PEC efficiency was a promising PEC signal indicator for application in PEC sensing platforms.

**PEC Mechanism of the Biosensor.** The PEC mechanisms of signal generating and quenching are shown in Figure 5. When the CdTe QD–CeO<sub>2</sub> complex was modified on the GCE surface, a strong PEC signal could be observed (Figure 5A), which might benefit from two reasons as follows. First, the effective band gap matching between CeO<sub>2</sub> and CdTe QDs could promote light-harvesting capability, facilitate charge separation, and depress electron–hole recombination, thus enhancing the photoelectric conversion efficiency. Second, CeO<sub>2</sub> and its sensitizer CdTe QDs controlled in one nanostructure could prominently reduce energy loss and enhance photoelectric conversion efficiency because of the shortened electron-transfer path. Concretely, under 460 nm illumination, electrons of CdTe QDs shifted from their valence band (VB) to their conduction band (CB) and then moved to the CB of CeO<sub>2</sub>. Simultaneously, electrons of CeO<sub>2</sub> also shifted from their VB to their CB. These photogenerated electrons located at the CB of CeO<sub>2</sub> eventually migrated to GCE and the continuous electron supply from the electrolyte solution containing 0.1 M AA also occurred immediately, thus producing a strong PEC signal. Besides, the output DNA obtained from the target converting amplification procedure could trigger the generation of DNA supersandwich structures by the assistance of DNA3 and DNA4. The resulted DNA supersandwich structure containing numerous TATA sequences would specifically bind TBP and bend at an 80° angle to form DNA–protein complexes. Thereby, a great steric hindrance immediately produced and significantly hindered



**Figure 4.** PEC responses of (A) CeO<sub>2</sub>, (B) CdTe QDs, and (C) CdTe QD–CeO<sub>2</sub> complex in PBS containing 0.1 M AA.

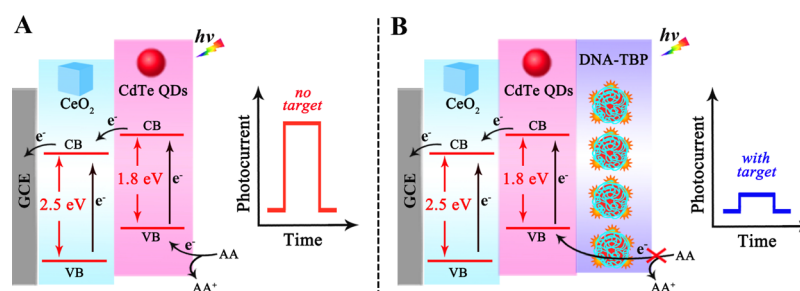


Figure 5. Mechanisms of (A) generation of PEC signal and (B) quenching of PEC signal.

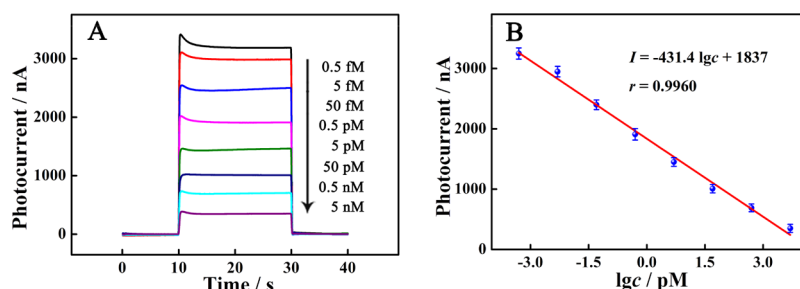


Figure 6. (A) PEC responses corresponding to different miRNA-141 levels. (B) Calibration curve for the miRNA-141 assay. Error bars represent standard deviations of three experiments.

the electron-transfer path between the CdTe QD–CeO<sub>2</sub> complex and electron donor (AA), resulting in a remarkably reduced PEC signal (Figure 5B).

**Detection of miRNA-141.** Under optimal conditions, the analytical characteristics of the developed biosensor were evaluated *via* quantitative detection of miRNA-141 with different concentrations. Figure 6A illustrated the PEC responses corresponding to different miRNA-141 levels, and the PEC response gradually decreased with the increasing miRNA-141 level from 0.5 fM to 5 nM. It could be obtained from Figure 6B that the PEC response was proportional to the logarithm of the miRNA-141 level, in which the linear equation was  $I = -431.4 \lg c + 1837$  with  $r = 0.9960$  ( $I$ : PEC response;  $c$ : miRNA-141 concentration;  $r$ : correlation coefficient). A detection limit of 0.17 fM was estimated based on the acknowledged calculation method,<sup>31–33</sup> and it was more sensitive compared with those of several published methodologies, which benefited from the introduction of dual signal amplification<sup>34–36</sup> and the efficient recognition of a detection probe to miRNA-141.<sup>37,38</sup> In addition, the specific comparison results for analytical characteristics between this developed biosensor and other assays reported previously are presented in Table 1.

#### Selectivity and Stability of the Proposed Biosensor.

Selectivity and stability were two key indexes in measuring the PEC performances of this proposed biosensor. Possible interfering species, such as miRNA-21, miRNA-199a, and thrombin, were utilized for the assessment of selectivity. As observed from Figure 7A, the PEC signal for blank measurement presented no significant difference compared with 5 nM miRNA-21, 5 nM miRNA-199a, and 5 nM thrombin. However, when 50 pM miRNA-141 was employed for determination, an obviously reduced PEC signal was obtained. These consequences revealed a high selectivity of the PEC biosensor for miRNA-141 assay. Besides, under consecutive “off–on–off” light for 10 times, the time-based PEC signal toward 50 pM miRNA-141 was recorded (Figure 7B). The

Table 1. Comparison of Different Methodologies for the miRNA Assay<sup>a</sup>

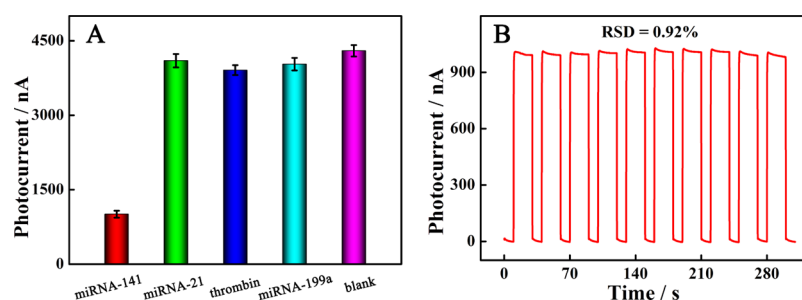
| analytical method | detection limit | linear range    | refs     |
|-------------------|-----------------|-----------------|----------|
| fluorescence      | 10 fM           | 1 pM to 10 nM   | 39       |
| electrochemistry  | 18 fM           | 50 fM to 500 nM | 40       |
| ECL               | 0.5 fM          | 1 fM to 1 nM    | 41       |
| SPR               | 1 fM            | 0–50 pM         | 42       |
| SERS              | 1 pM            | 1 pM to 100 nM  | 43       |
| CL                | 10 fM           | 20 fM to 5 pM   | 44       |
| PEC               | 153 fM          | 350 fM to 5 nM  | 45       |
| PEC               | 83 fM           | 100 fM to 3 nM  | 46       |
| PEC               | 0.31 pM         | 1 pM to 100 nM  | 34       |
| PEC               | 0.17 fM         | 0.5 fM to 5 nM  | our work |

<sup>a</sup>Abbreviations: electrochemiluminescence (ECL); surface plasmon resonance (SPR); surface-enhanced Raman spectroscopy (SERS); chemiluminescence (CL).

evident change of the PEC signal was not found with the light on, and the relative standard deviation was calculated as 0.92%, which implied that this biosensor possessed an excellent stability.

## CONCLUSIONS

In summary, a PEC biosensor with the CdTe QD–CeO<sub>2</sub> complex as the strong PEC signal indicator was successfully constructed for ultrasensitive assay of miRNA-141 coupling with dual signal amplification strategy. The proposed CdTe QD–CeO<sub>2</sub> complex possessed excellent photoelectric performances, and its PEC signal was 9.8-fold and 2.8-fold than those of pure CeO<sub>2</sub> and pure CdTe QDs, respectively, because the photoactive material CeO<sub>2</sub> and its sensitizer CdTe QDs were controlled in one nanostructure, leading to shortened electron-transfer path, reduced energy loss, and improved photoelectric conversion efficiency. Moreover, the introduction of dual signal amplification including target converting amplification and DNA supsandwich structure amplification



**Figure 7.** (A) Selectivity of the biosensor in the presence of different targets. (B) Stability of the biosensor. Error bars represent standard deviations of three experiments.

could effectively improve the detection sensitivity for miRNA-141 quantitative analysis. With the successful construction of the PEC sensing platform, this strategy not only offered a novel and promising PEC signal indicator but also revealed an efficient avenue for ultrasensitive miRNA estimation.

## ■ ASSOCIATED CONTENT

### Supporting Information

The Supporting Information is available free of charge on the ACS Publications website at DOI: 10.1021/acsami.9b02189.

Materials and reagents, apparatus, gel electrophoresis, PEC measurement, condition optimization, electrochemical characterization of the PEC biosensor, characterizations of CdTe QDs and Fe<sub>3</sub>O<sub>4</sub>@Au, and XPS analysis of the Ce 3d region (PDF)

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### Notes

The authors declare no competing financial interest.

## ■ ACKNOWLEDGMENTS

This work was financially supported by the NNSF of China (21575116, 21675129, and 21775124) and the Fundamental Research Funds for the Central Universities (XDJK2018AA003), China.

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