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Amperometric Detection of Lactose Using β-Galactosidase Immobilized in Layer-by-Layer films

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ABSTRACT: A direct, low cost method to determine the concentration of lactose is an important goal with possible impact in various types of industry. In this study, a biosensor is reported which exploits the specific interaction between lactose and the enzyme β-Galactosidase (β-Gal) normally employed to process lactose into glucose and galactose for lactose-intolerant people. The biosensor was made with β-Gal immobilized in layer-by-layer (LbL) films with the polyelectrolyte poly(ethylene imine) (PEI) on an indium tin oxide (ITO) electrode modified with a layer of Prussian Blue (PB). With an ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_{30}$ architecture, lactose could be determined with an amperometric method with sensitivity of 0.31 μA $mmol^{-1}$ cm^{-2} and detection limit of 1.13 mmol L^{-1}, which is sufficient for detecting lactose in milk and for clinical exams. Detection occurred via a cascade reaction involving glucose oxidase (GOx) titrated as electrolytic solution in the electrochemical cell, while PB allowed for operation at 0.0 V vs. saturated calomel electrode, thus avoiding effects from interfering species. Sum-Frequency Generation (SFG) spectroscopy data for the interface between the LbL film and a buffer containing lactose indicated that β-Gal lost order, which is the first demonstration of structural effects induced by the molecular recognition interaction with lactose.

KEYWORDS: *Lactose, amperometric detection, β-Galactosidase, Layer-by-Layer, sum-frequency generation*

INTRODUCTION

Lactose is a disaccharide found in milk and dairy products, being the only source of carbohydrates in milk with concentrations ranging from 4.4 to 5.2%.[1] It is hydrolysed by lactase in the digestive system to the monosaccharides glucose and galactose. For humans suffering

from lactose intolerance for the lack of lactase, the commercially available β-galactosidase may be used to hydrolyse lactose to be absorbed by the body. Lactose concentrations may be indicative of abnormalities and be used for clinical diagnosis. For instance, lactose in excess in the blood indicates gastrointestinal malignancy.[2] The quantitative determination of lactose is usually performed in specialized laboratories, and requires long analysis times and expensive instruments for methods such as spectrophotometry[3], infrared spectroscopy[4], titrimetry[5] and chromatography.[6,7]

The development of a low cost, fast method for monitoring lactose is therefore an important aim, which may be achieved with biosensors based on an enzymatic cascade reaction with ß-galactosidase (ß-Gal) in the presence of glucose oxidase (GOx).[8,9] In these biosensors ß-Gal catalyzes the hydrolysis of lactose producing glucose that is catalyzed by GOx, thus generating hydrogen peroxide (H_2O_2). Examples include an amperometric biosensor with ß-Gal, GOx, peroxidase (HRP) and the mediator tetrathiafulvalene (TTF) co-immobilized onto a gold electrode modified by a self-assembled monolayer (SAM).[2] Detection was carried out at 0.00 V (vs Ag/AgCl) with the signal being proportional to the lactose concentrationbetween1.5 and 120 $\mu mol.L^{-1}$. Another amperometric biosensor was prepared by immobilizing β-Gal and GOx with glutaraldehyde onto a glassy carbon electrode coated with a mercury thin film.[10]A spectrophotometric assay for quantifying lactose was developed with β-Gal, GOx, HRP and o-phenylenediamine (OPD) for the concentration range from 0.2 to 1.8 $mmol.L^{-1}$.[11]

In this study, we also exploit β-Galactosidase, but immobilized with the layer-by-layer (LbL) technique together with the polyelectrolyte PEI onto an ITO electrode modified with Prussian Blue (PB), which served as mediator for H_2O_2.[12] GOx was incorporated into the electrolyte solution. The design of this biosensor has advantages over those reported in the

literature, which include a suitable enzyme immobilization method,[13] only two enzymes are involved in the cascade reaction and the oxidation of H_2O_2 is carried out at 0.0V (vs SCE).[14] The choice of the LbL method was based on its suitability to immobilize enzymes with preserved activity.[15–19] PEI was selected because it has been proven more adequate than other polyelectrolytes for preserving enzyme activity[12,20,21]. We also performed sum-frequency generation (SFG) measurements in an attempt to correlate the detection of lactose with changes in the immobilized β-Galactosidase.

EXPERIMENTAL SECTION

Materials. The enzyme β-Galactosidase (β-Gal) (E.C. 3.2.1.23) from *Aspergillus Oryzae*, isoelectric point at pH4.6, optimal activity between pH 4.5 and 5[22] and 8 units/mg; Glucose Oxidase (GOx) from *Aspergillus Niger* (E.C. 1.1.3.4), isoelectric point at pH 4.2 [23], optimal activity between pH 3.5 and 6.5[24] and 138.8 units/mg; poly(ethylene imine) (PEI), poly (vinyl sufonate) (PVS),β-lactose, glucose and sucrose were purchased from Sigma Aldrich, while ascorbic acid was purchased from Cinética and uric acid was obtained from Fluka.

Substrate. The LbL films were assembled onto quartz slides and CaF_2 plates for spectroscopic investigations, and onto ITO-coated glass (indium–tin oxide, one-side coated on glass by Delta Technologies) for electrochemical measurements. The quartz plates were cleaned with $HCl/H_2O_2/H_2O$ (1:1:6) (v/v) and $NH_4OH/H_2O_2/H_2O$ (1:1:5) (v/v) hydrophilization solutions, both for 10 min at 80 °C, while CaF_2windows were cleaned with hydrogen peroxide and potassium permanganate. ITO was cleaned with chloroform, isopropanol (in a sonicator) and rinsed with ultrapure water (Milli-Q). ITO slides were previously modified with a Prussian Blue (PB) layer.[25]

Solutions. The solutions of PEI (1mg mL^{-1}) was prepared in ultrapure water with pH adjusted to 5.5 by adding HCl (1 mol L^{-1}). The solutions of PVS (4μL mL^{-1}), GOx (0.5mg mL^{-1}), β-Gal (5mg mL^{-1}), lactose (1mol L^{-1}), glucose (1mol L^{-1}), sucrose (1mol L^{-1}), ascorbic acid (1mol L^{-1}) and uric acid (10 mmol L^{-1}) were prepared in a sodium acetate buffer (0.05 mol L^{-1}, pH 5.5). The molecular weights were Mw = 200,000-350,000 for PVS and Mw = 750,000 for PEI.

LbL films. For fluorescence and optical absorption measurements, 2-bilayer $(PEI/PVS)_2$ LbL films were used as a cushion to reduce the influence of substrate morphology on film growth[26], while the amperometric measurements were made with 1-bilayer cushion of $(PEI/PVS)_1$. LbL films were assembled by dipping the substrate in PEI and β-Gal solutions, both for three minutes, interspersing the immersion in sodium acetate buffer during 30s for washing. This procedure was repeated until the desired number of bilayers was reached. Film growth was monitored by measuring the fluorescence spectrum at each bilayer deposited with a Thermo Scientific Shimadzu™ model RF-5301 PC spectrofluorimeter. The absorption spectra were taken with a Thermo Scientific Genesys 6 UV-vis spectrophotometer. All the films were assembled at room temperature. For FTIR and SFG spectroscopic measurements, a 2-bilayer cushion of $(PEI/PVS)_2$ was deposited onto the CaF_2 windows, on top of which one bilayer of $(PEI/β\text{-}Gal)_1$ was added, leaving the β-Gal exposed in the outermost layer.

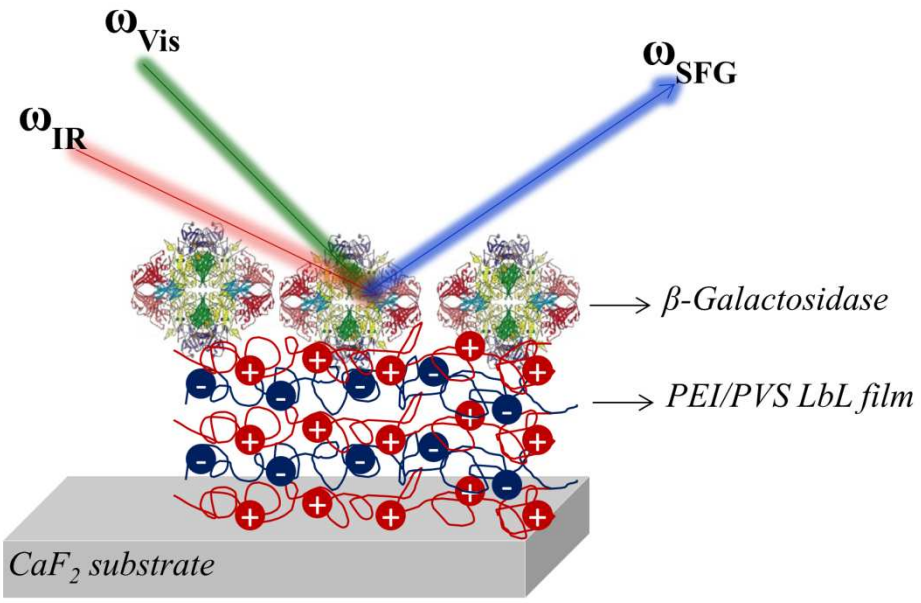
Electrochemical measurements. The PB film was potentiostatically deposited onto ITO at a potential of +0.40V (vs Ag/AgCl electrode) during 400s from aqueous 2×10^{-3}mol $L^{-1}K_3[Fe(CN)_6]$ + 2×10^{-3}mol L^{-1} $FeCl_3$ solutions in 0.1 mol L^{-1}KCl+ 0.01 mol L^{-1}HCl. After deposition, the modified electrodes were rinsed with Milli-Q water and immersed into a solution containing 0.1 mol L^{-1}KCl+ 0.01 mol L^{-1}HCl, where the electrode potential was cycled between

0.0 and 1.0 V (vs Ag/AgCl electrode) at a scan rate of 0.05 V s^{-1}, until a stable voltammetric response was obtained.[12] Amperometric measurements were performed at 0.0 V vs saturated calomel electrode (SCE) with an Autolab PGSTAT 30 using a conventional electrochemical cell (7 mL of sodium acetate buffer + 500μL of GOx), comprising an auxiliary electrode of platinum foil (1 cm^2) and the working electrodes being ITO modified with LbL films with a PB layer as follows: ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-}Gal)_{10}$ or ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-}Gal)_{30}$. The applied potential for each biosensor was kept at 0.0V allowing the background current to decay to a steady state value before the amperometric experiments in each addition of lactose (100 μL, 0.1 mol L^{-1}) under stirring. Usually, one min. elapsed before the measurements were taken, in order to get a stable signal. The effect from interferents and the stability of the biosensor were also studied.

FTIR and SFG spectroscopy studies. The FTIR spectra were acquired inN_2-purged atmosphere using a Nicolet 470 Nexus spectrometer. In the experiments with the enzyme powder, 0.5 % of β-Gal was dispersed in pellets in a KBr matrix. For the measurements on films, $(PEI/PVS)_3$ and $(PEI/PVS)_2$+$(PEI/\beta\text{-}Gal)_1$ LbL films were grown onto CaF_2 windows and then dried in a weak flow of N_2. All measurements were carried out in the transmission mode with a resolution of 6 cm^{-1}.

Sum-frequency generation (SFG) spectroscopy measurements were performed on the upper face of a CaF_2 plate at a film-air interface, on which LbL films were grown with the enzyme immobilized. The film architectures investigated were $(PEI/PVS)_3$ and $(PEI/PVS)_2$+$(PEI/\beta\text{-}Gal)_1$, which were exposed to buffer or lactose solutions, and then dried in a low flux of N_2 before the experiments. The setup consists of two laser beams, one in the visible range (ω_{vis}) and another, tunable in the infrared (ω_{IR}), both overlapping spatially and

temporally at the interface giving rise to a sum-frequency signal $\omega_{SFG} = \omega_{vis} + \omega_{IR}$. When the IR beam frequency matches a normal vibration mode, the intensity of the SFG signal increases. However, if the molecules at the interface have a null or random orientation, the SFG signal is zero. Therefore, even the molecules at the interface must have a net average orientation for a measurable SFG signal be obtained. Scheme 1 displays an idealized structure of the samples analyzed by SFG spectroscopy.



Scheme 1. Structure of a 2-bilayer $(PEI/PVS)_2$ LbL film on which the enzyme β-galactosidase was immobilized with a top $(PEI/β\text{-}Gal)_1$ bilayer. The laser beams ω_{vis} and ω_{IR} overlap spatially and temporally to generate the SFG signal $\omega_{SFG} = \omega_{vis} + \omega_{IR}$.

For the analysis of the vibrational spectrum, the intensity of the SFG signal may be expressed as

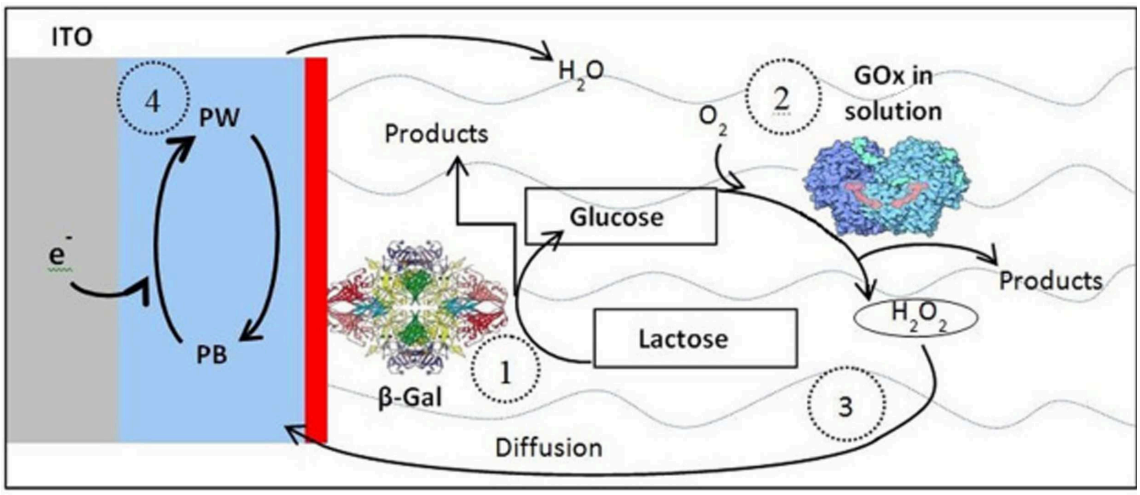
$$I_{SFG} \propto \left|\chi^{(2)}_{eff}\right|^2 = \left|\chi^{(2)}_{NR} + \chi^{(2)}_{R}\right|^2 = \left|\chi^{(2)}_{NR} + N_S \sum_q \frac{A_q}{\omega_{IR} - \omega_q + i\Gamma_q}\right|^2 \qquad (1)$$

where $\chi_{NR}^{(2)}$, $\chi_{R}^{(2)}$, N_s, A_q, ω_q, Γ_q are the nonresonant and resonant contributions to $\chi_{eff}^{(2)}$, the surface density of molecules and the oscillator strength, resonant frequency and linewidth of the q-*th* vibrational mode, respectively. From equation (1) one notes that when ω_{IR} is near the frequency of molecular vibrations ω_q, the SFG output is resonantly enhanced. Equation (1) also illustrates a feature of nonlinear spectroscopic methods which differ from their linear counterparts: there is *interference* of the resonant contribution, $\chi_{R}^{(2)}$, with the non-resonant background, $\chi_{NR}^{(2)}$, leading to changes in the spectral line shape depending on both the magnitude and phase of $\chi_{NR}^{(2)}$, and on the presence of nearby resonances. Therefore, a quantitative analysis of SFG spectra requires curve fitting to eq. (1) to obtain the amplitudes, frequencies and linewidths of the resonances. Further details on the SFG technique are available in.[27,28]

The SFG vibrational spectra were obtained with a commercial spectrometer (Ekspla, Lithuania) equipped with a pulsed Nd^{3+}:YAG laser that provides a fundamental beam at 1064 nm (28 ps pulse duration, 20 Hz repetition rate) with a harmonic unit generating second and third harmonics (532 and 355 nm, respectively). The third harmonic and fundamental beams pump an optical parametric amplifier with a difference frequency stage that generates an infrared (IR) beam tunable from 1000 to 4000 cm^{-1} with pulse energy ~ 30-200 μJ. The spot sizes and incidence angles for the IR and visible (532, 600 μJ) beams are 0.50 mm, 55º and 1.00 mm, 60º, respectively. The SFG signal is measured with a photomultiplier after spatial and spectral filtering, with data being collected for each scan with 100 shots data point, with a resolution of 3 cm^{-1}. The molecular-level information was obtained by analyzing the SFG measurements in *ppp* polarization combinations (*p*- sum-frequency generated beam, *p*- visible beam and *p*-infrared beam).

RESULTS AND DISCUSSION

Electrode preparation. Scheme 2 shows the idealized structure of an LbL film containing the immobilized enzyme onto ITO modified with a PB layer, also including the mechanisms for detection of lactose. This is carried out in the presence of GOx in the buffer solution, with generation of H_2O_2, as depicted in steps 1, 2, 3 and 4 in Scheme 2.



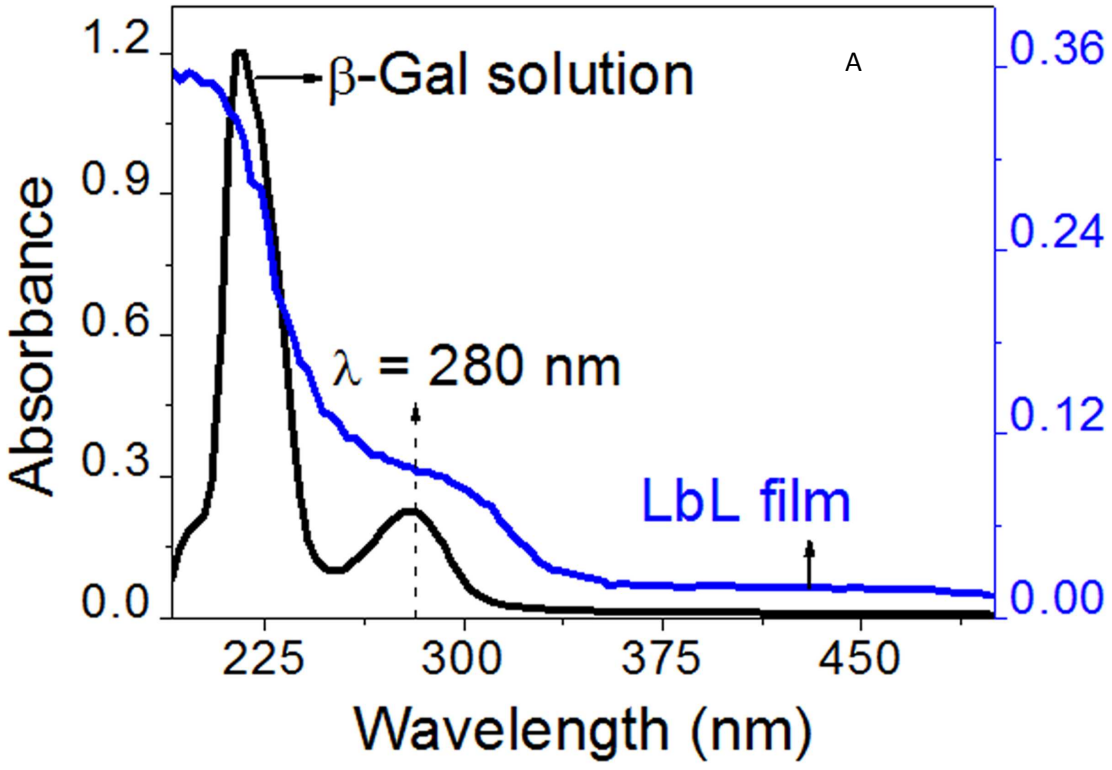
Scheme 2. The biosensor made with a (PEI/β-Gal)$_n$ LbL film operating at 0.0 V vs SCE.

PB films can be reduced to their colorless form, referred to as Prussian White (PW), according to Eq. (2):

$$KFe^{III}Fe^{II}(CN)_6 + e^- + K^+ \rightarrow K_2Fe^{II}Fe^{II}(CN)_6 \quad (2)$$

where Fe^{III} and Fe^{II} are the oxidation states of Fe atoms in the PB structure.[12,29] In subsidiary experiments we observed that bare ITO and ITO modified with PB used in amperometric measurements failed to detect lactose.

Film Growth. The absorbance spectra for β-Gal in solution and immobilized in a PEI/β-Gal8-bilayer LbL film in Figure 1A display absorption bands at λ = 215 nm and 280 nm, assigned to tryptophan, phenylalanine and tyrosine and peptide bonds, which confirm the enzyme immobilization. Film growth was successful with the same amount deposited in each deposition step, as indicated by the linear increase in the fluorescence intensity at 344 nm for $(PEI/PVS)_2(PEI/\beta\text{-Gal})_1$ LbL films in Figure 1B, with excitation at 280 nm. Emission at 344 nm is attributed to phenylalanine, tyrosine and tryptophan chromophores in the enzyme.[30] Absorption spectra shown in the Supporting Information confirmed the success of the LbL deposition.



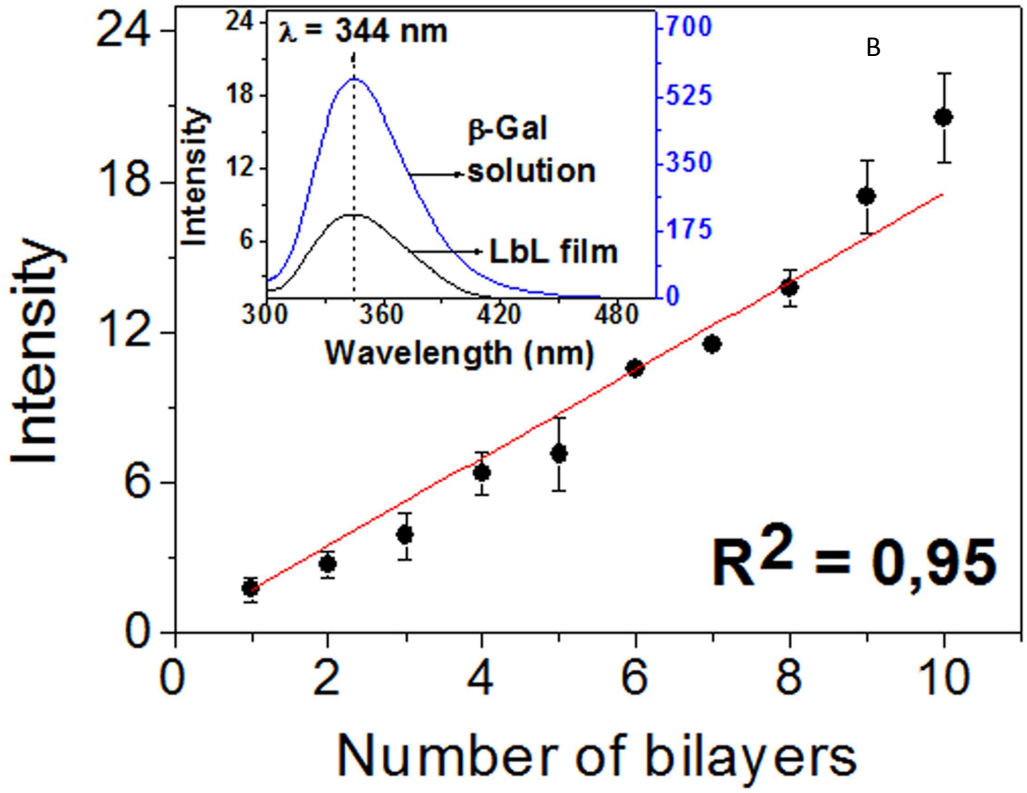


Figure 1.(1A) Absorption spectrum for β-Gal in sodium acetate buffer at pH 5.5 and in LbL films.(1B) Fluorescence intensity vs. number of bilayers for a $(PEI/PVS)_{2(}PEI/\beta\text{-Gal})_{10}$ LbL film at 344 nm, and with excitation at 280 nm. The inset shows the emission spectra for β-Gal in sodium acetate buffer at pH 5.5 and in an LbL film.

FTIR and SFG. The FTIR spectrum for β-Gal dispersed in a KBr matrix in Figure 2 exhibits the main bands of the enzyme, consistent with the literature.[31] The bands at 1650 and 1540 cm^{-1} are assigned to the amides I and II, respectively.[32,33,34, 35] The doublet at 1644 and 1660 cm^{-1} in the amide I region allows one to probe the enzyme structure, since the former is associated with *β-sheets* or *random coils* while the latter at 1660 cm^{-1} is related to *α-helices.*[31,34,36,37]

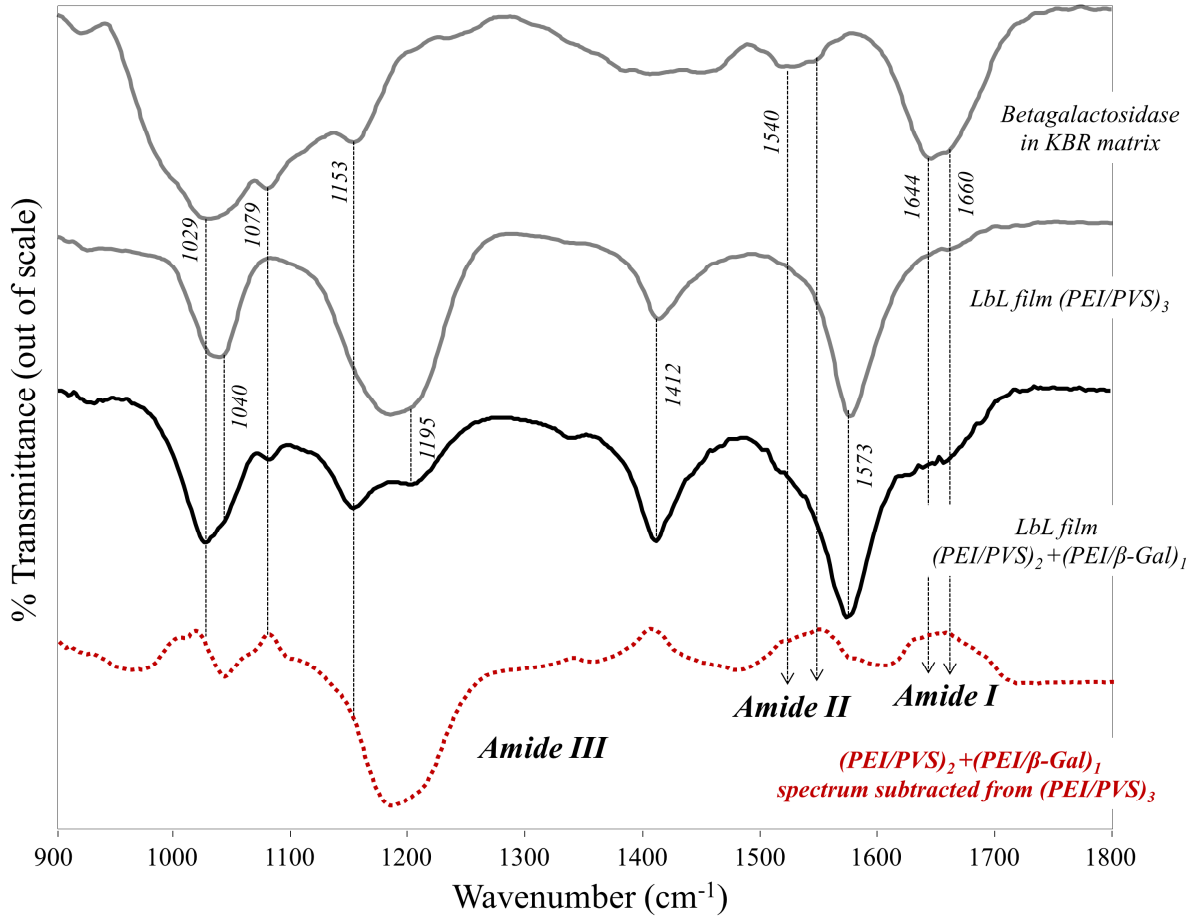


Figure 2.FTIR absorption spectra for β-Gal in KBr pellet, and for LbL films of $(PEI/PVS)_3$ and $(PEI/PVS)_2$+$(PEI/β\text{-}gal)_1$. The red dotted spectrum was obtained by subtracting the $(PEI/PVS)_2$+$(PEI/β\text{-}gal)_1$ spectrum from that of$(PEI/PVS)_3$, which reveals the main bands of the enzyme immobilized in the film. The LbL films were grown onto a CaF_2 plate up to 3 bilayers.

The main bands for $(PEI/PVS)_3$ LbL films in Figure 2 appear at 1040, 1195, 1412 and 1573 cm^{-1}, assigned to the symmetric and asymmetric stretching of SO groups, angular deformations of CH (bending) in the polymer chains and angular deformation of NH groups, respectively.[38,39,40] Since SO and NH groups are related to PVS and PEI, respectively, the spectra confirm the presence of these two polyelectrolytes in the $(PEI/PVS)_3$ LbL films. The spectrum for the $(PEI/PVS)_2$+$(PEI/β\text{-}Gal)_1$ LbL film exhibited the same bands observed for β-Gal and

PEI/PVS film, with no band shifts or appearance of additional bands. The main bands of β-Gal, namely amides I and II and III, are inferred in the LbL film from spectral subtraction of $PEI/PVS)_3$ and $(PEI/PVS)_2$+$(PEI/\beta\text{-Gal})_1$, especially for amide III band that is overlapped by the $(PEI+PVS)_3$ bands at ca. 1200 cm^{-1}. Therefore, there is no strong molecular-level interaction between the film components, in spite of the high stability of the enzyme in the film when exposed to aqueous media. This stability should be governed by electrostatic interactions and H-bonding between the PEI/PVS film and β-Gal, which are usually the main driving forces for film growth .[41,42]

Molecular organization in the $(PEI/PVS)_3$ LbL film after being immersed into the buffer solution is weak according to the SFG spectrum in Figure 3A, where only a broad, low-intensity band appeared between 1600 and 1650 cm^{-1}, assigned to the angular deformation of NH^{2+} group as an ionized form of the polymer when in the water.[39,43] When this $(PEI/PVS)_3$ LbL film was immersed in a lactose solution, even the weak signal practically disappeared as indicated in figure 3B.

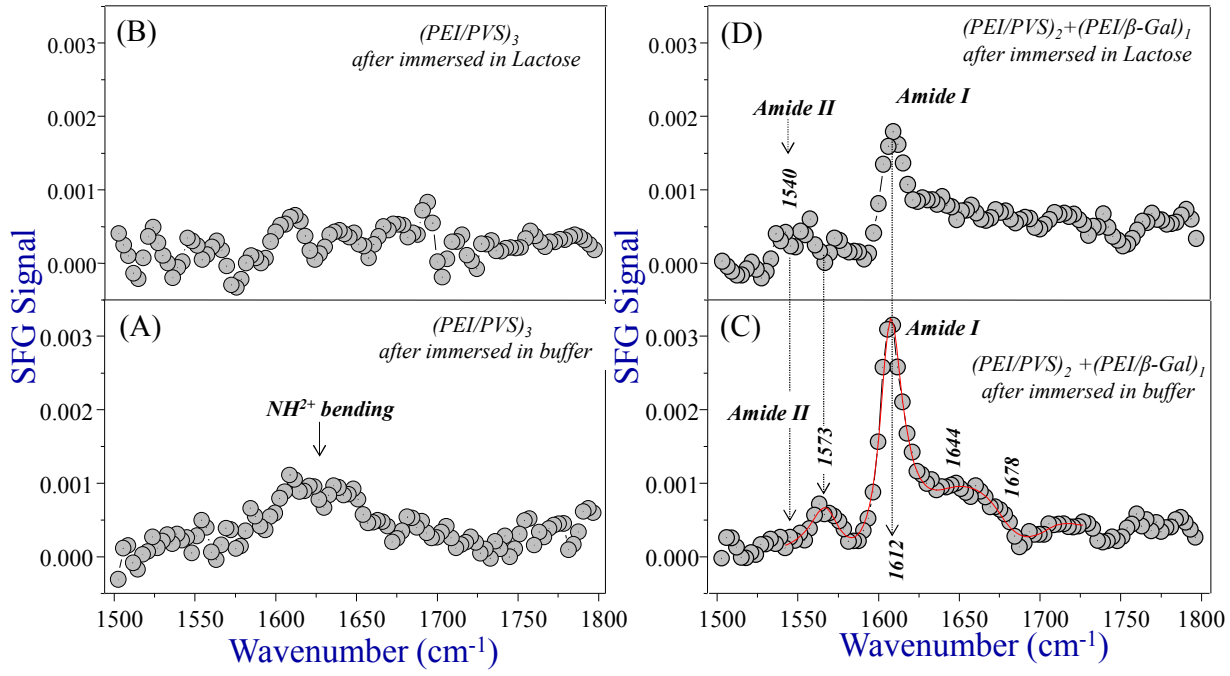


Figure 3. SFG spectra for the samples $(PEI/PVS)_3$ (A) after contact with buffer solution and (B) lactose solutions, and $(PEI/PVS)_2$+$(PEI/\beta\text{-Gal})_1$ (C) after contact with buffer solution and (D) lactose solution. The measurements were performed in a PPP polarization configuration. The spectrum in figure (C) is fitted to Eq. (1), illustrated by a red line, and the bands are highlighted.

The adsorption of an enzyme layer brought considerable molecular organization, as it is clear from the spectrum in Figure 3C for the $(PEI/PVS)_2$+$(PEI/\beta\text{-Gal})_1$ LbL film after being immersed in the buffer solution. Four bands could be identified when the spectrum was fitted to Equation (1), at 1573, 1612, 1644 and 1678 cm^{-1}. The peak at 1573 cm^{-1} is assigned to a PEI vibrational mode, and was also observed in the FTIR results. Since this mode was not present in the spectrum for the $(PEI/PVS)_3$ film, one infers that it becomes active in SFG owing to interactions with the enzyme, thus adopting a net orientation in the outer polymer layer. The bands at 1644 and 1678 cm^{-1} are attributed to *β-sheets* and *β-turns* of the enzyme, respectively.[36,31,34] The most intense peak at 1612 cm^{-1} is also assigned to the enzyme; according to the literature it can either be due to *aggregate strands* or *β-sheets* induced by intermolecular enzyme interactions.[44,45,34] The conformation inferred for the enzyme does not coincide with that

found via FTIR measurements (KBr pellet), which could be due to two main reasons: in the KBr pellet the enzyme would adopt a different conformation, and/or the enzyme structure was modified upon immobilization on the LbL film. However, CD measurements (see Supporting Information file) indicate only a small conformational change of the enzyme upon immobilization onto the PEI layer. This suggests that the conformation dominant in the SFG spectrum is not the most abundant in the protein, but rather the most well oriented in the adsorbed enzyme.

The effect from exposing the $(PEI/PVS)_2$+$(PEI/\beta\text{-Gal})_1$ LbL film to lactose was considerable, as shown in Figure 3D. The decrease in the band intensities points to a much less ordered film than when exposed to the buffer only (no lactose). Therefore, lactose appears to have a disordering effect on the LbL films. This applies to the neat $(PEI/PVS)_3$ film, but especially for the film containing the enzyme, as is seen for the amide I band. To our knowledge, this is the first observation of such disordering effect caused by lactose. We do not know whether this is specific for the lactose-galactosidase interaction, since the initial order of LbL films can also be altered by other factors such as a flux of air,[46] heating[46] or exposure to specific vapours.[48]

Amperometric measurements. The amperometric response of LbL films containing β-Gal was tested, whose results are shown in Figures 4 and 5 for biosensors with the architecture ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_n$ with 10 and 30 bilayers ($_n$ is the number of PEI/β-Gal bilayers), respectively, operating at 0.0V (vs. SCE) in a sodium acetate buffer and GOx solution at pH 5.5. The biofunctionality of β-Gal/PEI LbL structure as well as the feasibility of the method for biosensing are demonstrated by the increase in reduction current upon addition of successive aliquots of lactose. Each addition corresponds to an increase of 100 μL of $1x10^{-1}$mol L^{-1} lactose in 7 mL sodium acetate buffer of supporting electrolyte.

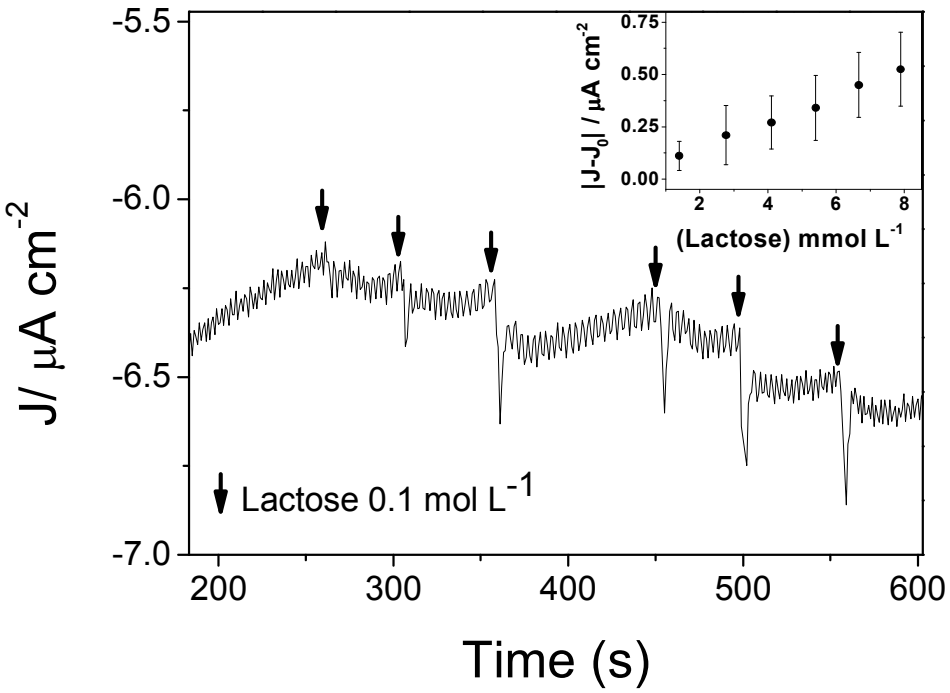


Figure 4. Amperometric response of biosensor ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-}Gal)_{10}$ in sodium acetate buffer pH 5.5 and GOx. The inset shows the current density as a function of lactose concentration.

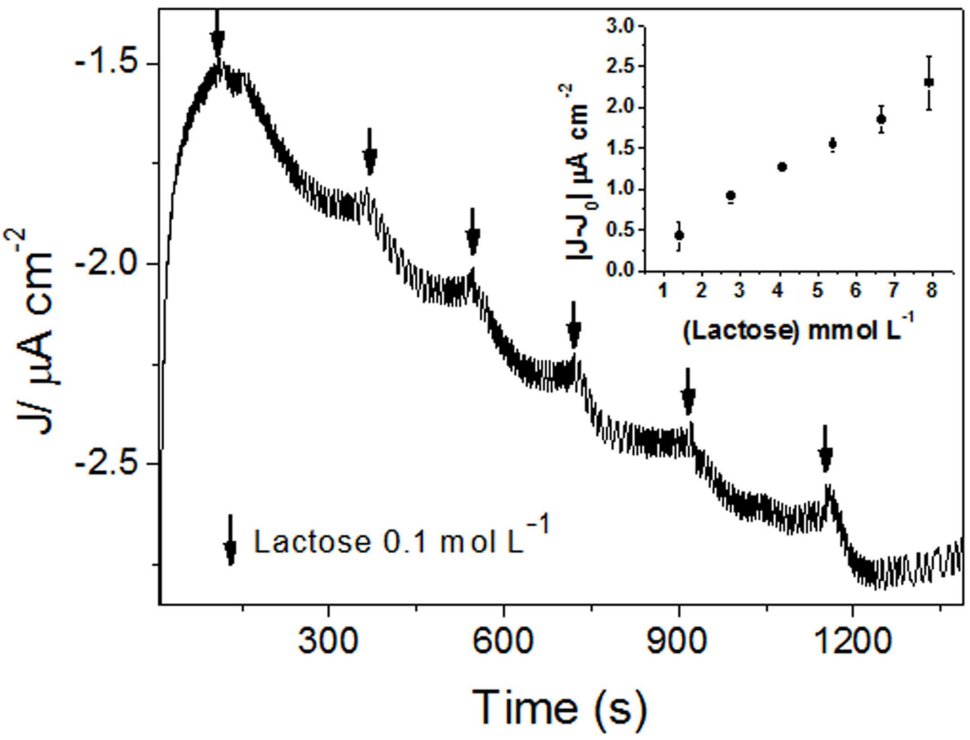


Figure 5. Amperometric response of biosensor ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_{30}$ in sodium acetate buffer pH 5.5 and GOx. The inset shows the current density versus lactose concentration.

A stronger response was obtained for the biosensor made with the 30-bilayer LbL film in Figure 5, with a clear signal transduction for detecting the lactose aliquots. Figure 6 shows the analytical curves for ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_n$ biosensors, with n= 10 and 30. The sensitivity, inferred from the slope of the fitted curve, increased with the number of bilayers, probably owing to the larger amount of β-Gal immobilized. The sensitivity achieved in the biosensors with a linear response was 0.064 and 0.31 µA $mmol^{-1}$ cm^{-2} lactose, respectively. The apparent Michaelis-Menten constant [49] was determined as being 8.26 mmol L^{-1} and 8.24 mmol L^{-1} for the 10 and 30-bilayer LbL films, respectively, to be compared with 1.31 mmol L^{-1} [50] and 1.25 mmol L^{-1} [51] for the free enzyme. The values for the LbL films are similar to reports in the literature, e.g 5.18 mmol L^{-1} [52], 5.2 mmol L^{-1} [53], but one has to consider that the film architectures differed or the films were fabricated with other methods.

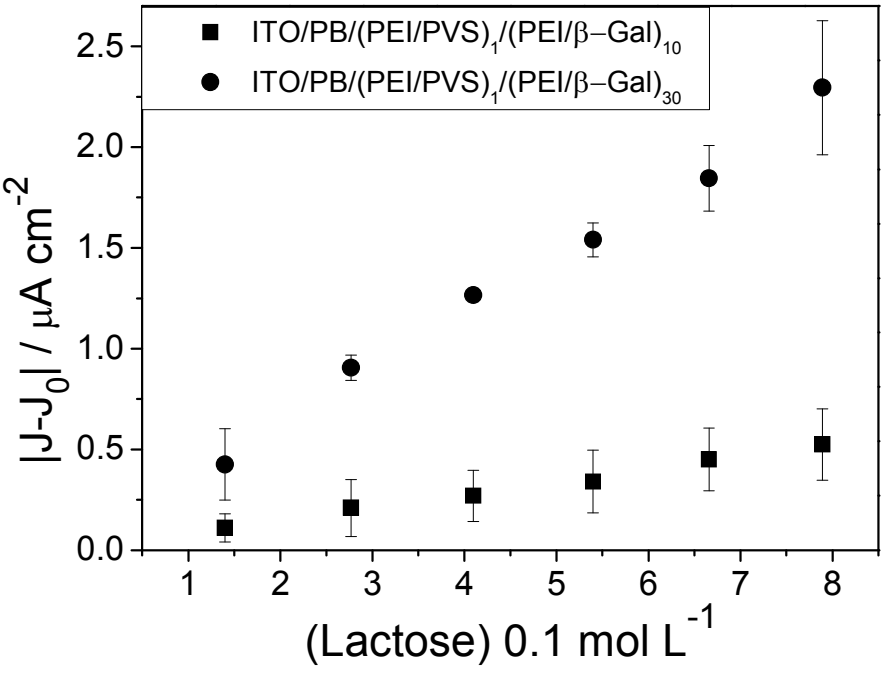


Figure 6. Linear range of analytical curves extracted from LbL films with 10 and 30 bilayers.

The limit of detection for the biosensors was 4.22 mmol L^{-1} for ITO/PB/(PEI/PVS)$_1$(PEI/β-Gal)$_{10}$ and 1.13 mmol L^{-1} for ITO/PB/(PEI/PVS)$_1$(PEI/β-Gal)$_{30}$. The PEI/β-Gal-based biosensor displayed a larger limit of detection than others reported in the literature, according to Table 1, but its sensitivity is still sufficient to detect lactose in commercial milk. Indeed, the lactose concentration in pure milk is typically of the order of 100 mmol L^{-1},[54] a hundred fold our limit of detection.

Table 1 – Biosensors for detecting lactose. The spectrometric method is based on the color change while the amperometric method uses the change in current as a function of time with a fixed applied potential.

Authors	Method of detection	Limit of detection (mmol L^{-1})
Conzuelo, F.; Gamella, M.;	Amperometric	4.6 x 10^{-4}

Campuzano, S.; Ruiz, M. A.; Reviejo, A. J.; Pingarrón, J. M., 2010		
Fornera, S.; Yazawa, K.; Walde, P., 2011	Spectrometric	0.10
Göktuğ, T.; Sezgintürk, M. K.; Dinçkaya, E., 2005	Amperometric	0.58
This work	Amperometric	4.22 and 1.13

The successful detection of lactose implies that β-Gal had its activity (and therefore structure) preserved in the PEI/β-Gal LbL films. We have confirmed with CD dichroism measurements reported in the Support Information that immobilization of β-Gal in PEI/ β-Gal LbL films led to a small loss of α-helices (from 74 to 69%) compared to the enzyme free in solution. This is in contrast to the much more extensive denaturing of β-Gal in LbL films with poly(allylamine hydrochloride) (PAH), as also indicated in the Supplementary Information. Therefore, the choice of PEI for building the LbL films has been justified. We have also tried to detect lactose using amperometry with LbL films containing the two enzymes, namely β-Gal and GOx immobilized in the same film, but the results were poor, probably because the active sites of one of the enzymes was blocked.

Effects from interferents. Effects from interferents represent the major difficulty for a biosensor in real applications. With the architecture used here, comprising a PB layer under the LbL films, detection was performed at 0.0 V vs. SCE, which helped prevent interferent effects. This is demonstrated in the results of Figure 7, from experiments where the unbiased electrode ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_{30}$ (0.0 V vs SCE) were firstly subjected to 0.1 mol L^{-1} lactose solution until the current reached a steady-state value, and then successive injections of

interferents were made, as indicated by coloured arrows. The interferents caused no detectable change in current, with the exception of ascorbic acid which made the current to increase rather than decrease at it occurs for lactose. Therefore, though ascorbic acid gives a signal, it can still be distinguished from lactose, highlighting the specificity of the biosensor. As expected, glucose made the current to decrease, which could seem to compromise the ability to detect lactose. However, this can be circumvented with a glucose biosensor coupled to the lactose biosensor, for the concentration of lactose would be the difference in the signal.

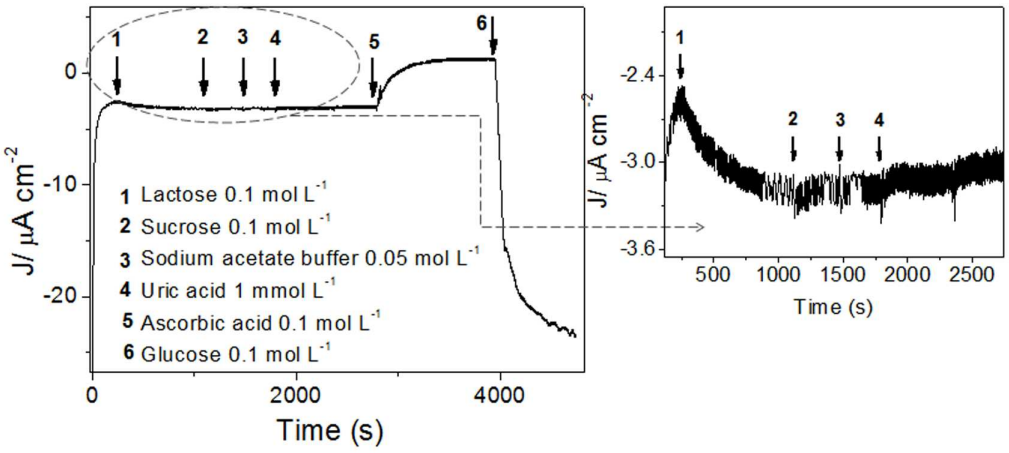


Figure 7 - Tests with interferents, titration 100 μL of (1) lactose 0.1 mol L^{-1}, (2), sucrose 0.1 mol L^{-1}, (3) sodium acetate buffer 0.05 mol L^{-1}, (4) uric acid 1 mmol L^{-1}, (5) ascorbic acid 0.1 mol L^{-1}, (6) glucose 0.1

Biosensor stability. The stability of the biosensors was investigated in terms of their performance for discriminating lactose. The biosensors were stored in sodium acetate buffer (pH 5.5) at 10°C when not in use. For the ITO/PB/$(PEI/PVS)_1(PEI/\beta\text{-Gal})_{30}$ system, the response was unaltered for 12 days, after which the signal decreased. All measurements were made in duplicate and the stability tests confirmed the film reproducibility.

CONCLUSIONS

The LbL technique was proven suitable for immobilizing β-Gal, with LbL films deposited on a PB-modified ITO electrode being used for detecting lactose. The amperometric biosensor was not as sensitive as similar ones in the literature but its sensitivity is sufficient for detecting lactose in actual applications, especially as it has been proven robust against interferents and displayed a stable performance over time. Moreover, the molecular architecture of the biosensor allows for further developments in terms of optimizing performance and being amenable to miniaturization for point-of-care use.

In addition to confirming the successful adsorption of β-Gal in the LbL films, SFG vibrational spectroscopy was useful to indicate that sensing lactose is accompanied by a decrease in the orientational order of the immobilized enzymes. This appears to be the first observation ever of molecular rearrangements induced by lactose detection, and opens the way for the identification of intermolecular interactions responsible for biosensing. It is also a first step toward understanding the mechanism of molecular recognition, which is crucial for any biological application.

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SUPPORTING INFORMATION

The LbL film growth monitored by the UV-vis spectroscopy and circular dichroism spectra were reported. This material is available free of charge via the Internet at http://pubs.acs.org/.

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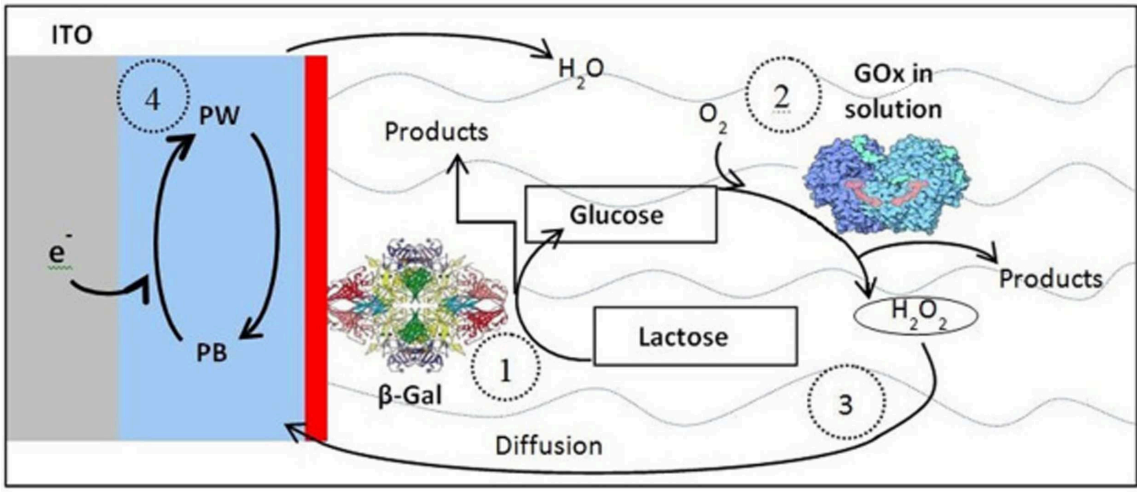
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