

Article

Quantum Dots and Graphene Oxide Fluorescent Switch based Multivariate Testing Strategy for Reliable Detection of *Listeria Monocytogenes*

Yuhui Liao, Xiaoming Zhou, and Da Xing

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Quantum Dots and Graphene Oxide Fluorescent Switch
based Multivariate Testing Strategy for Reliable
Detection of *Listeria Monocytogenes*

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Abstract

Graphene oxide (GO) and quantum dots (QDs), as burgeoning types of nano-materials, have gained tremendous interests in the biosensor fields. In this paper, we designed a novel multivariate testing strategy which depended on the fluorescence resonance energy transfer (FRET) effect between quantum dots (QDs) and graphene oxide (GO). It integrates QDs-GO FRET principle and QDs probes of different emission peak into a platform, aims at multiplex gene detection of a human infectious and highly pathogenic pathogen, *Listeria monocytogenes* (*L. monocytogenes*). With the development of a multiplex Linear-After-The-Exponential (LATE) PCR system, the single stranded DNA (ssDNA) products of *hlyA* genes and *iap* genes are obtained by simultaneous amplification of the target genes. Then with the hybridization of ssDNA products and QDs probes, simultaneous homogeneous detection of two gene amplification products can be achieved by using GO as a fluorescence switch and monitoring the relevant emissions excited by single light source. The distinguishable signals corresponding to target genes are obtained. With this developed approach, genomic DNA from *L. monocytogenes* can be detected as low as 100fg/ μ L. And this platform possesses a good dynamic range from 10^2 fg/ μ L to 10^6 fg/ μ L. It is indicated that this platform possesses potential to be a reliable complement for rapid gene detection technologies and is capable of reducing the false negative and false dismissal probabilities in routine tests.

Keywords: multivariate testing strategy; quantum dots; graphene oxide; Linear-After -The-Exponential PCR; foodborne pathogenic bacteria

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1. Introduction

Graphene oxide (GO) and quantum dots (QDs), as burgeoning types of nano-materials, have gained tremendous interests in the biosensor fields for design and fabrication of biosensors due to their excellent physical and chemical properties. GO has a hydrophilic surface with carboxyl and phenol hydroxyl groups, possessing a good dispersion and excellent stability.¹⁻⁸ Owing to the π - π stacking effect between nucleic acid bases and GO, the adsorption of single stranded nucleic acid by GO turns into a stable interaction.^{9,10} Conversely, the formation of the double helix nucleic acid structure has a perfect hiding structure of nucleic acid bases, thus the adsorption capacity of GO is greatly reduced.¹¹ In addition, one outstanding property of GO is that it can be used as a fluorescence quenching agent with a broad absorption band through fluorescence resonance energy transfer (FRET).¹²⁻¹⁴ Relatively, QDs have been used as excellent fluorescent labels for biological imaging, sensing and diagnostics. It possesses a variety of advantages, such as high fluorescent quantum yield; narrow, symmetric and stable fluorescence, size-dependent tunable absorption and emission.¹⁵⁻¹⁹ With surprises, it appears that the FRET between QDs and GO results in an outstanding quenching effect. This effect can be used as a fluorescence switch to get a high signal to noise ratio (SNR) of biological sensing. Based on this principle, a few QDs-GO based bio-molecular sensing platforms have been developed in recent years.²⁰⁻²¹

Inspired by the excellent performance of QDs-GO FRET platform and size-dependent tunable emission of QDs, a novel multivariate testing strategy is designed. In this strategy, two kinds of quantum dots with differentiable emission wavelengths are employed as the probes corresponds to two separate target genes. By integrating the QDs-GO FRET principle and two quantum dots probes with different emission peak into a platform, the distinguishable signals corresponding to target genes are obtained. Based on the principles of probability statistics, the probabilities of independent random events occurring at the same time is far less than a single event occurring independently. Thus, multiplex gene detection

possesses the potential to provide a more reliable way than the single-gene testing. Combined with the severe food security problems, we migrate the multivariate testing strategy to detect the multiplex gene of *Listeria monocytogenes* (*L. monocytogenes*, a human infectious and highly pathogenic pathogen) for reduction of probabilities of false negative and false dismissal in routine tests.

L. monocytogenes are the etiologic microorganisms that transmit through the food chain and lead to listeriosis.²² In recent years, foodborne pathogenic bacteria have caused huge economic losses to society, posing a serious challenge to human health and food security. Therefore, analyses of the presence of pathogenic bacteria turned into standard practice for ensuring food security and quality.²³ Existing technologies for the foodborne pathogenic bacteria monitoring are mainly made up of conventional monitoring methods and the emerging rapid gene detection technologies. Conventional methods²⁴⁻²⁶ are on strength of the specific separation and enrichment to isolate viable bacterial cells in foods, are laborious and time-intensive, requiring several days to produce results. Meanwhile, the existing rapid gene detection technologies²⁷⁻²⁹ are mostly focused on the single-gene testing. It is not reliable enough for the infectious, widespread and highly pathogenic pathogen in routine tests. Furthermore, the repeatedly occurring of food safety incidents compelled us to reexamine the securities of existing technologies for foodborne pathogenic bacteria monitoring. Thus, considerable interests have been evoked in conceptions of multiplex gene detection.³⁰⁻³²

However, multiplex gene detection methods were confronted with the problem of multiplex feature signals giving out at one step operation. Thus, the similar absorption peaks and distinguishable emission peaks must be simultaneously provided, that greatly limits the practical application. In the actual process, electrophoresis^{33,34} and real-time quantitative methods^{35,36} are employed as the signal producing component by multiplex gene detection. Electrophoresis could get feature signals of the target gene according to the fragment size, but it is vexed with low sensitivity. Furthermore, real-time quantitative methods adopt SYBR green I as the signal amplifier. This means that these methods can just take the way of

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superposition on multiplex gene detection signal, but could not get the feature signals corresponding to the target gene separately. Fortunately, nano-materials fill the deficiency of multiplex gene detection techniques, make the fluorophores with different emission wavelength excited by a single light source possible.

Herein, we constructed a novel multiplex gene detection assay that depended on QDs and GO nano-platform. It aims at multiplex gene monitoring of *L. monocytogenes* that could overcome the false negatives and reduce false dismissal probability in routine tests. In this approach, the Linear-After-The-Exponential PCR (LATE-PCR),³⁷ an outstanding method could generate ssDNA amplification products, is employed as the amplification system. And the *iap* gene and *hlyA* gene of *L. monocytogenes* are chosen as the target genes. The overall concept of the strategy was shown in Scheme 1. This platform consists of three parts: multiplex LATE-PCR amplification, DNA hybridization, and GO-QDs signal detection system. When the genome of *L. monocytogenes* exists, the multiplex LATE-PCR amplification system could get ssDNA amplification products of the *iap* gene and *hlyA* gene at an efficiency between the linear amplification and exponential amplification. Then QDs probes are added in, and incubating with the ssDNA amplification products. After the sufficient hybridization of ssDNA amplification products and QDs probes. At the same time, the helper probes are imported to constitute a longer double-chain structure. Then, the single-stranded QDs-probes are quenched by GO. However, partial formation (40bp) of double-stranded DNA (dsDNA) by the hybridization of QDs probe and amplification products that lead to sufficient resistance to the quenching effect induced by GO. Therefore, the nano-platform could get the characteristic signals corresponding to the target genes. In addition, benefiting from the size-dependent tunable absorption and emission of QDs, more characteristic genes of *L. Monocytogenes* could be acceded to this platform as molecular target, according to the actual demands. Thus, it is demonstrated that the QDs-GO nano-platform has the potential to be a versatile strategy for multiplex gene monitoring.

2. Materials and Methods

2.1 Reagents

Listeria monocytogenes (CMCC54007), *Salmonella enterica* (CMCC50040) and *Escherichia coli* O157:H7 (GW1.2020) were obtained from Guangzhou Institute of Microbiology, China. Quantum dots labeled with streptavidin were synthesized by Wuhan JIAYUAN quantum dots co., Ltd (Wuhan, China). QDs-525, coated with 2-4 streptavidin, has a narrow symmetrical emission peak at 525nm. Otherwise, the emission peak of QDs-605 is at 605nm, coated with 4-8 streptavidin. Both QDs-525 and QDs-605 has a high excitation efficiency in the range of 200 nm to 300nm. Graphene oxide (1mg/ml) was purchased from Xianfeng Nanotechnologies Co., Ltd (Nanjing, China). Taq DNA Polymerase and deoxy-ribonucleoside triphosphate (dNTP) mix were the products of Takara Biotechnology (Dalian) CO., Ltd. All oligonucleotides and probes used in our research were synthesized and purified by HPLC at Invitrogen. SYBR I and SYBR II were purchased from Invitrogen. The reagents related to electrophoresis were purchased from Bio-Rad (Richmond, CA). Phosphate buffered saline (PBS) buffer (20×) were purchased from Shanghai Sangon Biotechnology Co. Ltd.

2.2 Extraction of genomic DNA

The genomic DNA of *L. Monocytogenes* (CMCC54007), *Salmonella enterica* (CMCC50040) and *Escherichia coli* O157:H7 (GW1.2020) were extracted according to the manufacturer's protocol from the TIANamp Bacteria DNA Kit (Tiangen biotech, Beijing, China). The extractions were quantified through a spectrophotometer (Eppendorf BioPhotometer, AG 22331 Hamburg, Germany) by measuring the optical density at 260nm.

2.3 Multiplex LATE-PCR system

The multiplex LATE-PCR system contained dNTP mix (0.2mM), taq DNA polymerase (0.025U/μl), 1×corresponding buffer, limiting primers and excess primers. The limiting primers and excess primers were designed according to the principle of LATE-PCR (Sanchez et al., 2004), reached a molar ratio of 1:40. The

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sequence of primers corresponded to *hlyA* (GenBank accession number AF253320) and *iap* (GenBank accession number AY174670) genes are listed out in table 1, yielding a 116nt fragment from the *hlyA* gene and a 137nt fragment from the *iap* gene.

2.4 Polyacrylamide gel electrophoresis

In order to verify the amplification feasibility of the multiplex LATE-PCR system, the products of amplification were analyzed on a Bio-rad slab electrophoresis system (Bio-Rad Laboratories, USA). A 10% native polyacrylamide gel (29:1 acrylamide: bis-acrylamide) loaded with 10μL samples was run at room temperature for 45minutes at 120 V, in 1×Tris-borate-EDTA (TBE), then followed the coloration of SYBR I and SYBR II and photographing by Bio-rad Digital imaging system.

2.5 Preparation of probes of Quantum Dots

In order to establish a multiplex-gene detection platform, two kinds of quantum dots labeled with streptavidin, QDs-525 and QDs-605 (JIAYUAN quantum dots co., Ltd, Wuhan, China) were employed as fluorophores of fluorescent probes. QDs-525 targeted the *iap* gene and QDs-605 corresponded to *hlyA* gene. Aiming at the target sequence, we designed two ssDNA probes labeled with biotin at the 5' terminal, respectively constituted as *iap*-probes and *hlyA*-probes with QDs-525 and QDs-605. The sequences of the ssDNA probes, labeled with biotin at the 5' terminal, are listed in table 2.

Preparation of probes of QDs follows the steps below. The ssDNA probes and QDs (1 uM) were mixed up at a molar ratio of 30:1, followed by thermostatic reactions at 37°C for 30 min. The disconnected ssDNA probes were filtrated by a Nanosep 100K OMEGA tubular ultrafiltration membrane (Pall, USA). After twice spinning and washing with PBS buffer (1X), the final products were re-dissolved in the PBS buffer (1X) and stored at 4°C.

2.6 Construction of the QDs-GO multiplex-gene-monitoring platform.

The construction of QDs-GO platform contains the following steps: the ssDNA products from the multiplex LATE-PCR amplification system were mixed up with a certain amount of QDs-probe. The final concentration of *hlyA*-probes was fixed at

15nM. In this concentration, QDs-605 gains adequate fluorescence intensity for the strategy of this platform. In order to make up for the lower quantum yield of QDs-525 and to equalize the nether more labeling rate of streptavidin, we set the concentration of *iap*-probe as 30nM as twice than the *hlyA*-probe. The mixture of amplification products and probes was incubated for 30min at 37°C. In this process, QDs probes would hybridize with amplification products and the helper probes (the sequences of helper probe are shown in table 3). Along with the partial formation (40bp) of double-stranded DNA (dsDNA) that lead to sufficient resistance to quenching effect induced by GO. Then the fluorescence was measured by a Perkin-Elmer LS55 luminescence spectrometer (USA) after incubating for 10min.

3. Results and Discussions

3.1 Characterization of QDs probes formation and GO

The characterization of QDs probes formation and GO were executed. We firstly observed the surface morphology of GO nano-sheet by atomic force microscopy. The homogeneous sheet were shown in Fig 1 (A). The result show that the size of single GO sheet is about 1 μ m. Furthermore, the particle size of the QDs are measured by the particle size analyzer. The results were shown in Fig 1 (B). The average diameter of streptavidin labeled QDs-525 is 28.42 ± 2.83 nm, and the QDs-605 is 51.11 ± 5.11 nm. The diameters above include the hydration layer of surface of QDs. Then we studied the initial surface charge of QDs which show a negative charge. The value of zeta potential were -9.94 ± 0.75 mV and -17.45 ± 2.13 Mv. While the DNA labeled on the QDs, the surface charge of QDs showed an obvious change (see in Fig 1 (C) (D)). The charge of DNA labeled QDs appeared a negative enhancement which was contributed by the negative charge of DNA probes.

3.2 Parameters of optimization for the QDs-GO multiplex-gene-monitoring platform

The concentration of GO has a strong effect on the performance of this nano-platform. At a high concentration of GO, the amplification products could be adsorbed onto the GO surface. This leads to a drastic decrease of the sensitivity.

Nevertheless, the low concentration of GO could give rise to a background fluorescence signal that causes the decrease of SNR. To get the optimized concentration of GO, the effect of GO concentration on the fluorescence quenching ability was evaluated by setting GO concentrations as 4 μ g/mL, 8 μ g /mL, 12 μ g/mL, 16 μ g/mL, 20 μ g/mL and 24 μ g/mL, respectively. The concentration of QDs-525 probe was 30nM, reaching a molar ratio to QDs-605 at 2:1. As shown in Fig. 2 (A), with the increase of the GO concentration, the quenching efficiency synchronously ascended. When the GO concentration was at 16 μ g/mL, the quenching efficiency remained at a stable level. Further addition of the GO solution could not produce a significant increase in quenching efficiency. Therefore, we employed 16 μ g/mL of GO as the optimum choice for the platform.

On the other hand, time dynamics of adsorption is also an important parameter for the platform. With a short adsorption time employed, QDs probes could not be effectively adsorbed onto GO. However, a long incubation time may result in random adsorption of hybrid products by GO. In order to improve the efficiency of the nano-detection platform, the GO adsorption time optimization experiments were executed. The *iap* and *hlyA* probes were respectively fixed at 30nM and 15nM with the GO concentration as 16 μ g/mL. Then at a different time point, the adsorption efficiency was recorded in Fig. 2 (B). It is indicated that with the increase of adsorption time, the adsorption efficiency gradually increased. When the adsorption time was 10 min, the adsorption efficiency was stable. Therefore, 10 minutes was chosen as the optimal adsorption time in subsequent experiments.

In addition, the hybridization time of amplification products and QDs probe has a direct bearing on the SNR. For the optimal hybridization time, 1ng/ μ L genomic DNA was added to the nano-platform and optimization experiments were executed at different time point of hybridization. As shown in Fig. 2 (C) (D), the SNR increased with the extension of hybridization time and reached a stable level after 30min. Therefore, 30 minutes was employed as the optimal hybridization time.

3.3 Sensitivity results of QDs-GO multiplex gene monitoring platform and data analysis

For verifications of the amplification system, 1ng genomic DNA of *L. monocytogenes* was amplified by the multiplex LATE-PCR amplification system. The amplification products were detected by 10% polyacrylamide gel electrophoresis. As shown in Fig. 3 (A), the products of multiplex LATE-PCR amplification system can be stably produced from three paralleled amplification experiments. In addition, we evaluated the sensitivity of the QDs-GO multiplex gene monitoring platform. In this design, the concentration of genomic DNA was varied from 10fg/ μ L to 10^7 / μ L. After amplifying by multiplex LATE-PCR amplification systems, the amplification products of target genes were mixed with pre-prepared QDs probes and helper probes. The mixture was incubated at 37°C for 30 minutes. Then, GO was added to the system, reaching a final concentration of 16ug/mL and leading to a quenching effect on the excess QDs probes within 10 minutes. Finally, changes in the fluorescence intensity of the final mixture were observed and recorded in Fig. 3 (B). The fluorescence intensity synchronously decreased with the reduction of genomic DNA. When the concentration of genomic DNA decreased to 10fg/ μ L, the fluorescence intensity tended to be coincident with the control group. Nevertheless, the group with 100fg/ μ L genomic DNA had an obvious enhancement compared with the control group. It was demonstrated that the QDs-GO multiplex gene monitoring platform achieved a sensitivity of 100fg/ μ L. We analyzed the linear regression analysis of the fluorescence intensities with different genomic DNA concentrations for verification on the reliability and feasibility of this platform. Fig. 3 (C) shows the linear regression analysis of monitoring of the *iap* gene. It is found that the results of sensitivity have a good linear relation and an R^2 value of 0.9746 was obtained. Meanwhile, the linear regression analysis of monitoring of the *hlyA* gene are shown in Fig. 3 (D), achieving an R^2 value of 0.9651. This indicates the feasibility and reliability of the platform used for multiplex gene monitoring of *L. monocytogenes*. And this platform possesses a good dynamic range from 10^2 fg/ μ L to 10^6 fg/ μ L.

3.4 Specificity of the QDs-GO multiplex gene monitoring platform

Evaluation of specificity is an important quality index in biological monitoring

methodology. To further evaluate the performance of the platform, the genomic DNA of *Salmonella enterica*, *E.coli O157:H7* and *L. Monocytogenes* with an isometric concentration of $10^6\text{fg}/\mu\text{L}$ were also selected and respectively executed in this platform. As shown in Fig. 4 (A), the fluorescence intensity of *Salmonella enterica* and *E.coli O157:H7* exhibited no significant enhancement, respectively, while the *L. Monocytogenes* gave dramatic response, which confirms that this platform has highly responsive specificity to *L. Monocytogenes*.

For discrimination of *L. Monocytogenes*. response vs that of non-target species, we mixed *L. Monocytogenes* with common food borne pathogen-s, *salmonella enterica* and *E.coli O157:H7*. Then followed the standard program of this platform. The results shows that this strategy could discriminate the *L. Monocytogenes* from the mixed system (see in Fig 4 (B)). The milk sample also got obviously characteristic signal. Thus, this method possesses the preferable discrimination performance. In addition, we detected the low level response of the target *L. Monocytogenes* vs high level of non-target species (see in Fig 4 (B)), the results also proved the discrimination capacity of this platform.

3.5 Data supporting for the false negative and false dismissal probabilities reductions

The original intention for constructing this platform is reductions of the false negative and false dismissal probabilities. For the data supporting of reducing the false negative and false dismissal probabilities, we tested 100 cultured *L. Monocytogenes* samples with this platform. The results are supplied in Fig 5. It revealed that single gene testing of *iap* gene had a false negative probability of 11 percent, and the *hlyA* gene is 12 percent. Inversely, the multivariate testing strategy achieved 3 percent. In addition, 100 spiked milk samples were also tested (see in Fig 6). The results proved the reducing the false negative and false dismissal probabilities again and shows a better performance. We also found that the false negative and false dismissal probabilities were increasing with the complexity level of substrate where *L. Monocytogenes* grow in. The milk sample reached a higher false negative and false dismissal probabilities with single gene test (*iap*, 15 percent;

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3 *hlyA* 13 percent) than the conventional method of culture medium. Thus, this
4 platform could significantly reduce the probabilities of false negatives and false
5 dismissal.
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8 9 **4. Conclusions**

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11 In summary, it is demonstrated that the multiplex gene monitoring platform could
12 be a rapid, sensitive and reliable method for detections of *L. Monocytogenes*. To the
13 best of our knowledge, it is the first reported example of a multiplex gene
14 monitoring platform for foodborne pathogen detection, based on the GO-QDs
15 nano-platform. The proposed method consists of multiplex LATE-PCR
16 amplification, DNA hybridization and GO-QDs signal detection system. Benefitting
17 from the high amplification efficiency of LATE-PCR, excellent quenching ability of
18 GO and the high quantum yield of QDs, three remarkable advantages were achieved
19 by this platform, compared to the conventional assays. Firstly, the whole detection
20 process is rapid, being accomplished in 1.5 hours. It meets the rapid detection
21 requirements exactly. Secondly, this platform achieved a high sensitivity level of
22 100fg/ μ L that insured the feasibility for routine inspection and observation. Thirdly,
23 this platform was aimed at multiplex gene monitoring. The emergence of one or
24 more characteristic fluorescence peaks corresponding to the target genes could be
25 regarded as a positive result that significantly reduces the probabilities of false
26 negatives and false dismissal in routine tests. Taken as a whole, this platform
27 possesses the potential to be a versatile strategy towards to the monitoring of
28 infectious, widespread and highly pathogenic foodborne pathogen.
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Figure captions

Scheme. 1. The principle of the QDs-GO multiplex-gene-monitoring platform for *Listeria monocytogenes*.

Fig. 1. The characterization of QDs probes formation and GO. (A) AFM images of GO. (B) Particle size of QDs. (C) Potential variation between labelled and unlabelled QDs-525. (D) Potential variation between labelled and unlabelled QDs-605.

Fig. 2. Parameters optimization for the QDs-GO multiplex-gene-monitoring platform. (A) Evaluation of the effect of GO concentration on the quenching ability of QDs. (B) Time dynamics of QDs probes adsorption. (C) Hybridization time optimization of *iap*-probe. (D) Hybridization time optimization of *hlyA*-probe.

Fig. 3. Sensitivity results and data analysis. (A) Electrophoresis identification of the multiplex LATE-PCR amplification. Lanes H1 to H3 are the LATE-PCR amplification products of *hlyA* gene, and lanes I1 to I3 are *iap* gene's. H11 to H13 represent the three paralleled experiments of multiplex LATE-PCR. (B) Fluorescence spectroscopy experiments for multiplex-gene-monitoring of *Listeria monocytogenes* derived from different concentrations of genomic DNA. (C) Linear regression analysis of monitoring on *hlyA* gene. (D) Linear regression analysis of monitoring on *iap* gene.

Fig. 4. Specificity of the QDs-GO multiplex-gene-monitoring platform. (A) Specificity for equivalent concentration of food-borne pathogenic bacteria. (B) Specificity for discriminative concentration. S, E, LM represent the *Salmonella enterica*, *Escherichia coli* and *L. Monocytogenes* respectively (at a concentration of 10^5 fg/ μ L). hS and hE are corresponded with *Salmonella enterica* and *Escherichia coli* at a high concentration of 10^7 fg/ μ L. ILM is *L. Monocytogenes* with lower concentration of 10^3 fg/ μ L.

Fig. 5. Detections of 100 medium cultured *L. Monocytogenes* samples by the QDs-GO multiplex-gene-monitoring platform. (A) The detection signals of the cultured *L. Monocytogenes* (sample ID from 1 to 25), (B) Sample ID from 26 to 50, (C) Sample ID from 51 to 75, (D) Sample ID from 76 to 100. (See in Fig 5 of the manuscript)

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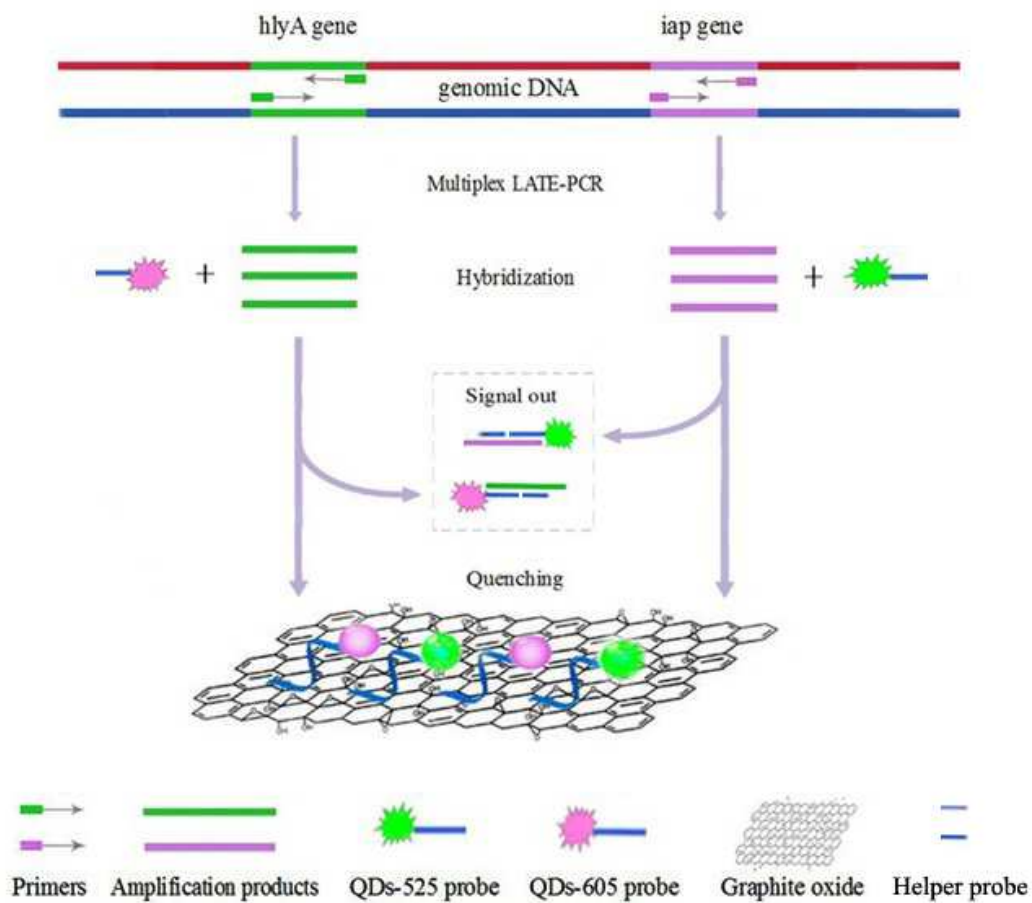
Fig. 6. Detections of 100 spiked milk samples by the QDs-GO multiplex-gene-monitoring platform. (A) The detection signals of the milk cultured *L. Monocytogenes* (sample ID from 1 to 25), (B) Sample ID from 26 to 50, (C) Sample ID from 51 to 75, (D) Sample ID from 76 to 100. (See in Fig 6 of the manuscript)

Table captions

Table 1. The sequences of primers.

Table 2. The sequences of 5'-biotin-labeled probes.

Table 3. The sequences of the helper probes



Scheme. 1

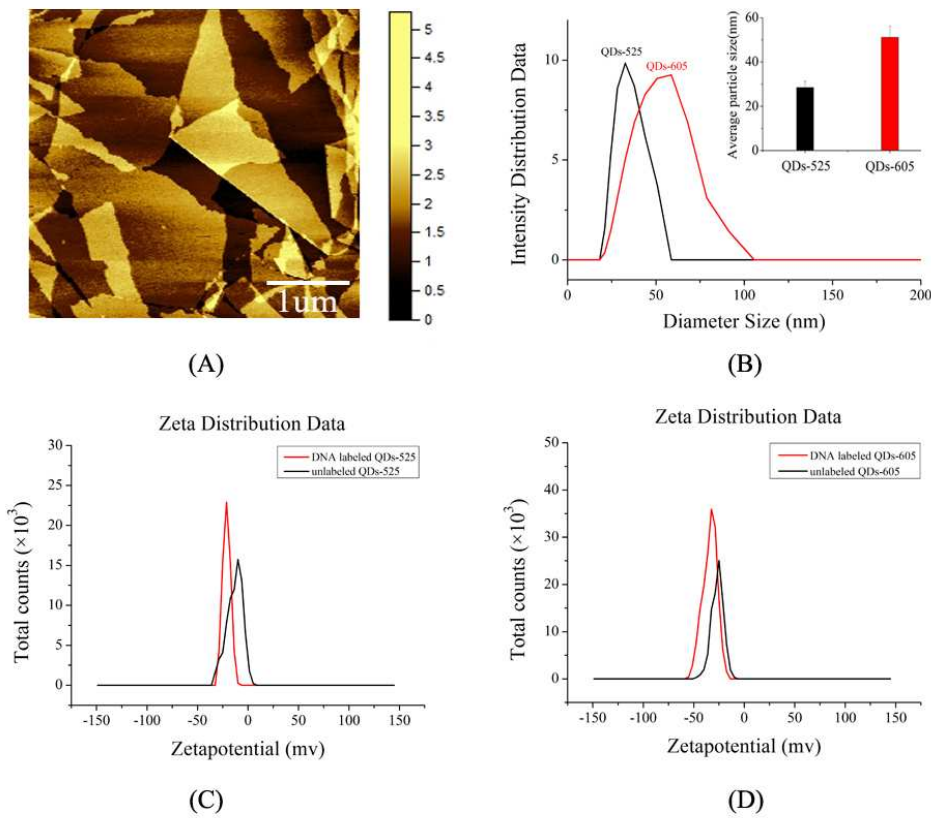


Fig. 1

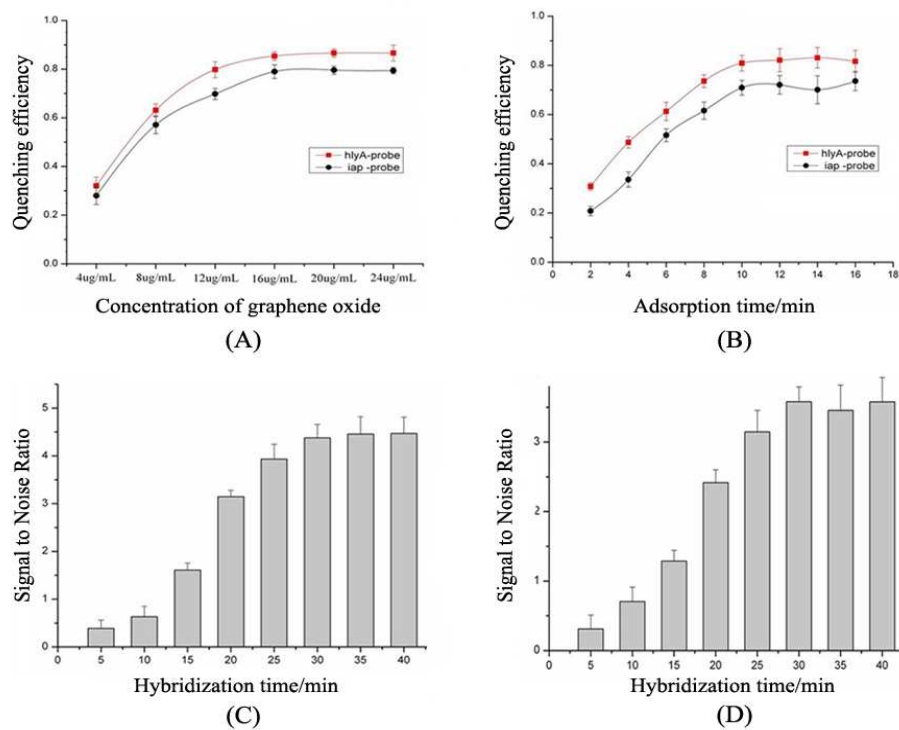


Fig. 2

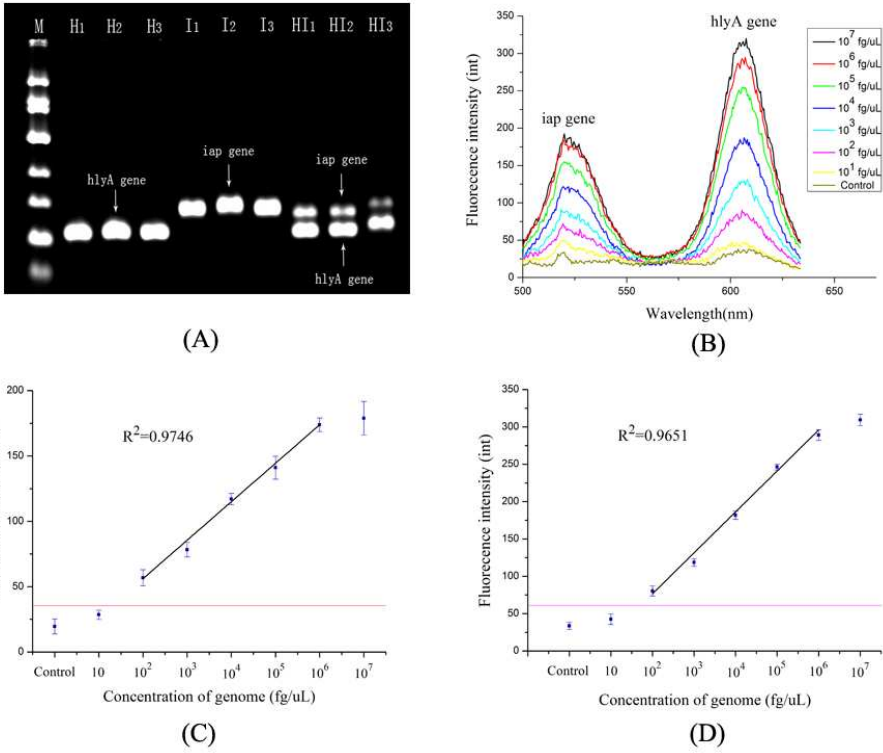
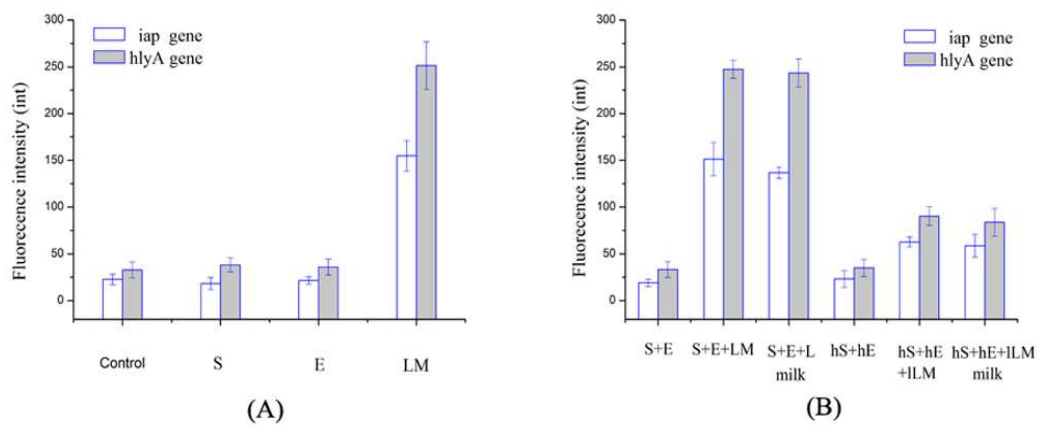


Fig. 3

**Fig. 4**

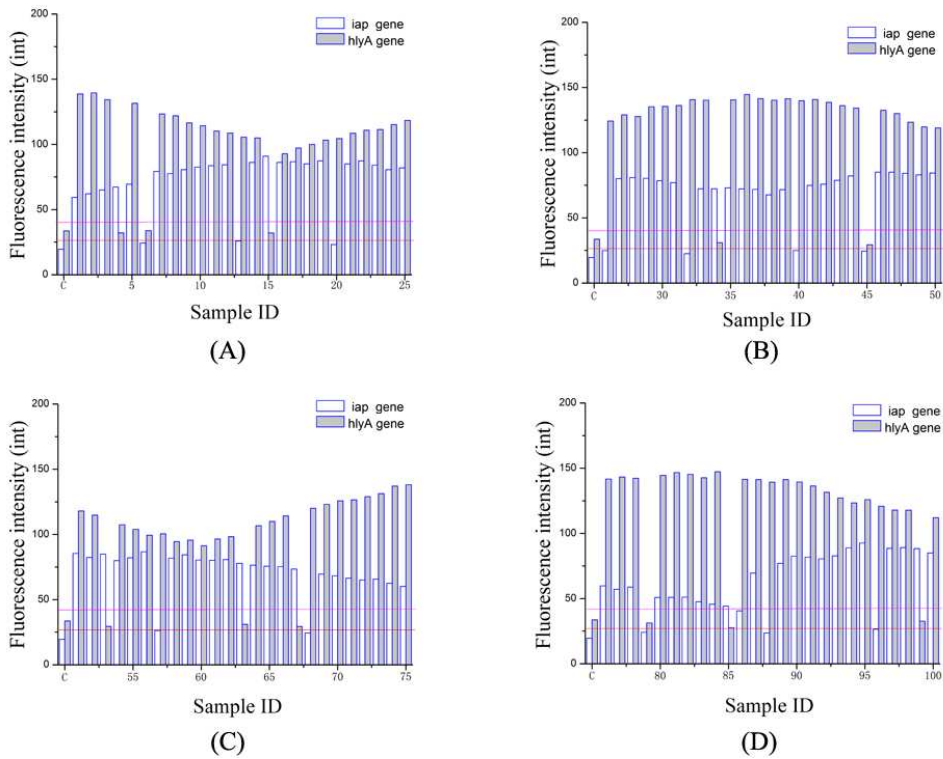


Fig. 5

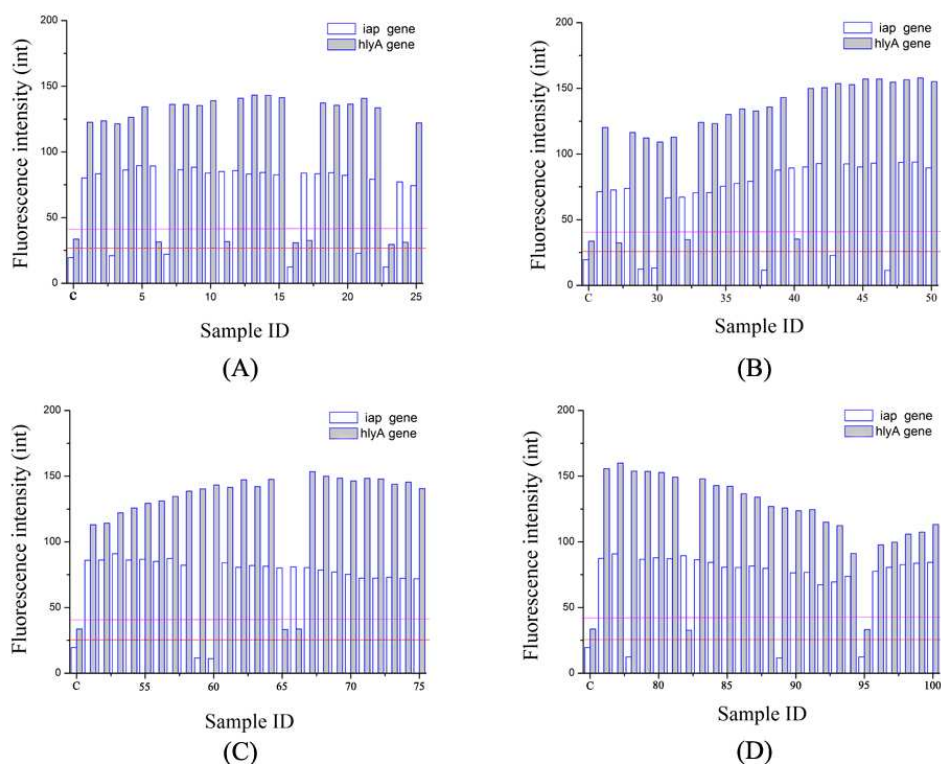
**Fig. 6**

Table 1

target genes	limiting primers' sequence(5'-3') and theoretical annealing temperature at 1000nM		excess primers' sequence(5'-3') and theoretical annealing temperature at 1000nM	
<i>hlyA</i>	GCTGCCGTAAGTGGGAAA	70.4°C	ATGATTGAACTTCATCTT	59.9 °C
	TCTGTCTCAG		TTGC	
<i>iap</i>	CTACTCAACAAGCTGCAC	72.1 °C	GACAGCGTGTGTAGTAG	61.1 °C
	CTGCTGCAGA		CAT	

Table 2

target genes	sequence(5'-3') of 5'-biotin-labeled probes
<i>hlyA</i>	GCTGCCGTAAGTGGGAAATCTGTCTCAGGTGATGTAGAAT
<i>iap</i>	CTACTCAACAAGCTGCACCTGCTGCAGAAACAAAACTGA

Table 3

target genes	sequence(5'-3') of helper probes
<i>hlyA</i>	TAACAAATATCATCAAAAATTCTTCCTTCAAAGCCGTAAT
<i>iap</i>	AGTAAACAAACTACACAAGCAACTACACCTGCACCTAAA

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